



+



Computed in Luxembourg

Computational Sciences
Luxembourg



Data-driven modelling and simulation: fracture and medical simulations



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Computed in Luxembourg

Computational Sciences Luxembourg



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Phuoc Huu Bui
Franz Chouly
Michel Duprez
Vanessa Lleras
Claudio Lobos
Alexei Lozinski
Pierre-Yves Rohan
Satyendra Tomar



Department of Computational Engineering & Sciences

Legato Team

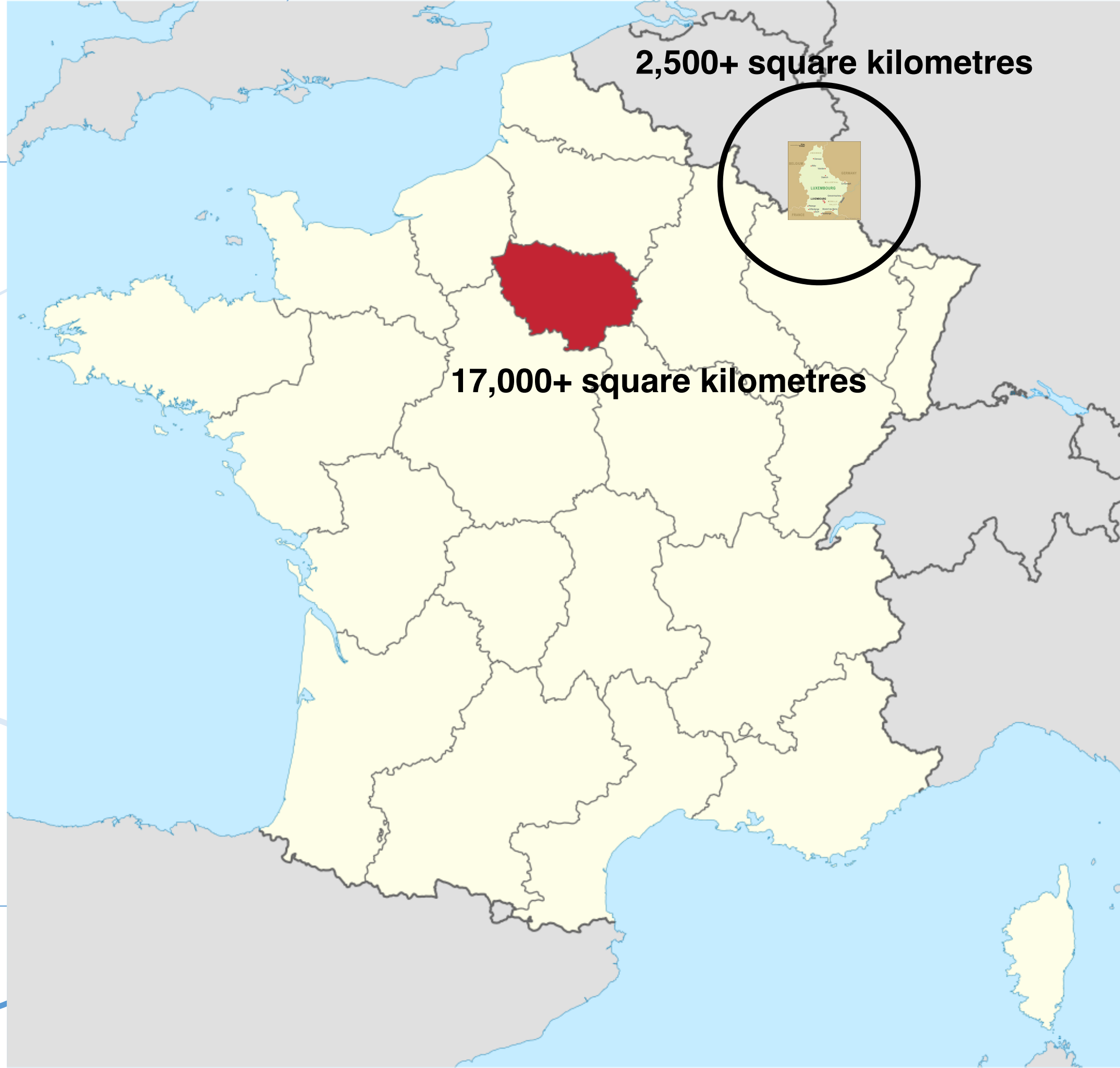


Detailed presentation: IGA, Fracture, Errors, Free Boundaries <http://hdl.handle.net/10993/31487>







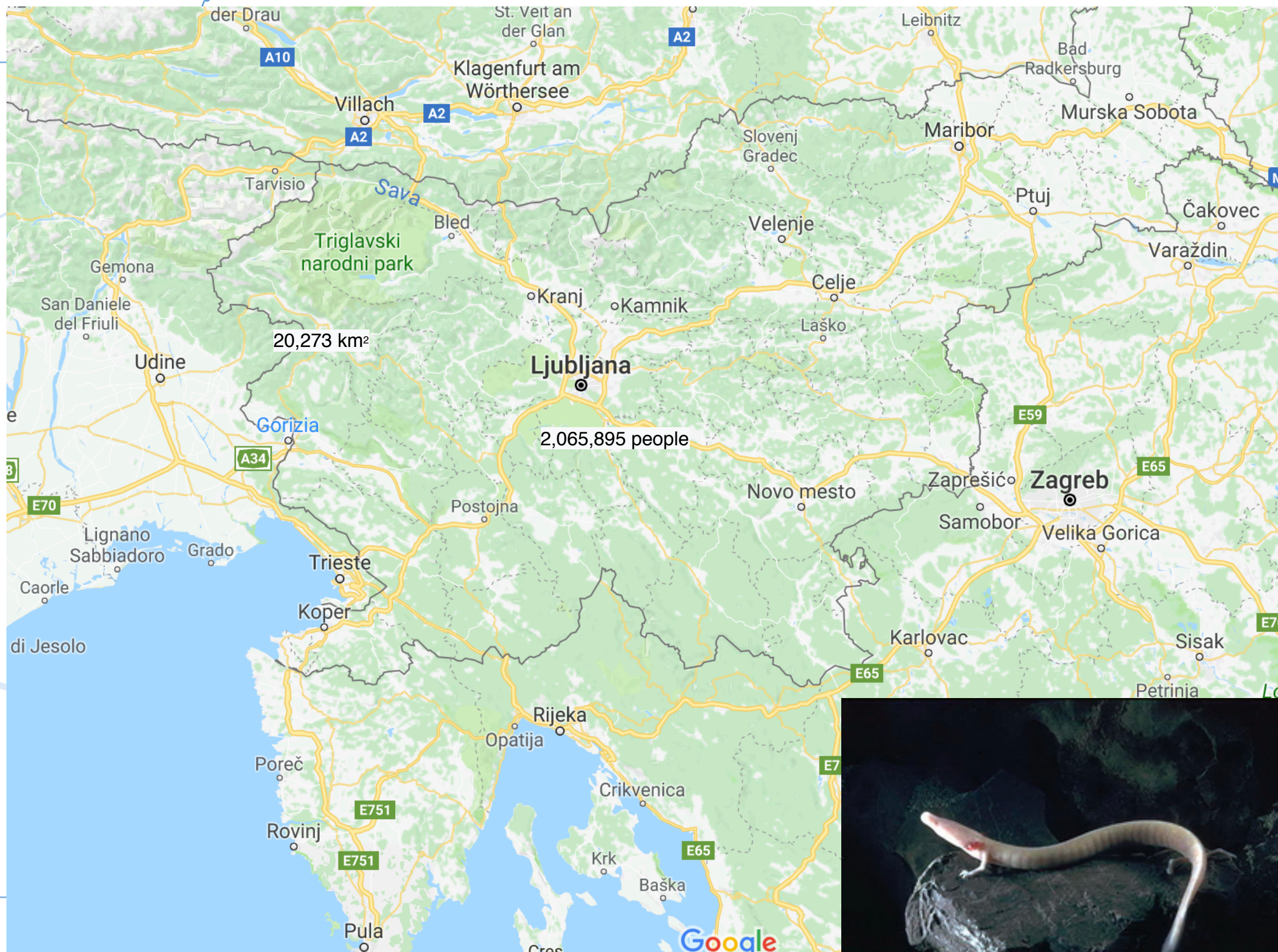


2,500+ square kilometres

17,000+ square kilometres







Olm can be found in [Postojna cave](#) and other caves in the country.



Stéphane BORDAS

Today at 5:53 PM



Climb to Ljubljana castle x 2. D+450m

Distance

8.02km

Elevation Gain

446m

Average Pace

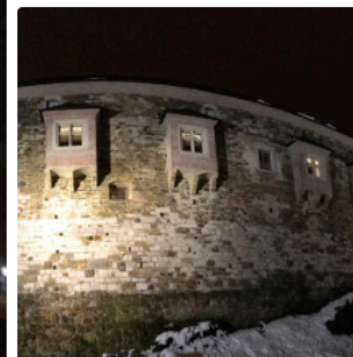
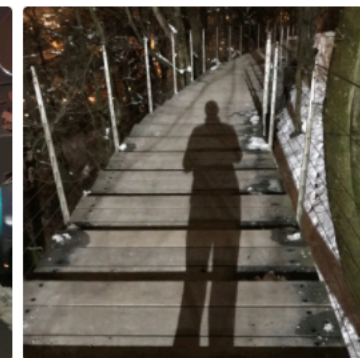
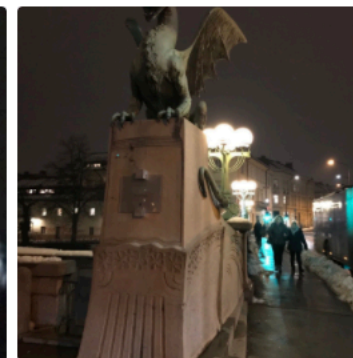
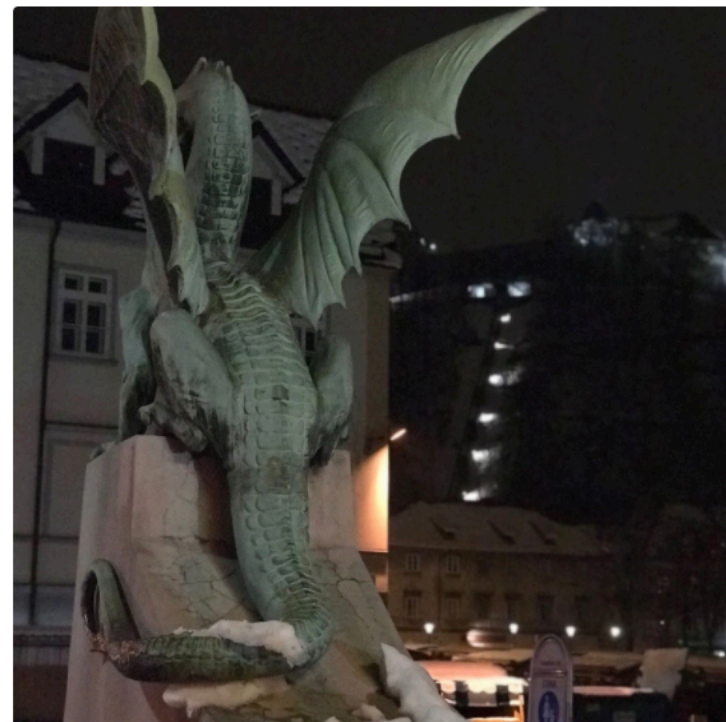
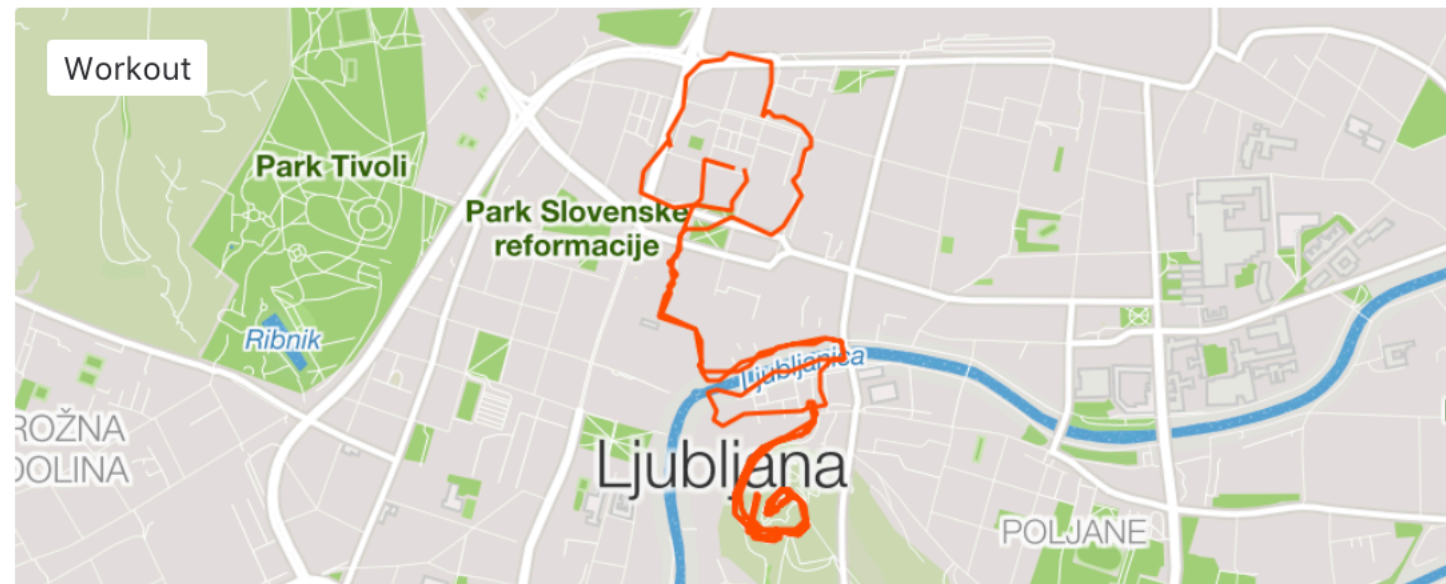
6:52/km

Achievements



Na Stolbi 8 Climb **7th overall** (3:35)

This ain't easy. **PR** (3:39)



February Climbing Challenge



Nice work, Stéphane!

2,050 m

Total Elevation

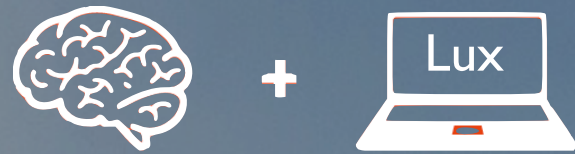
16

Total Runs

1,127 / 53,321

Current Rank

Overall Leaderboard		
1	Igor Sa	57,415 m
2	Evanio Valentini	35,298 m
3	Juanjo Cabrera Martinez	33,656 m
4	Chris Norris	31,810 m
5	Lucilene Damiani	31,046 m
...		
1,125	Andy Ford	2,050 m
1,126	Jan Salke	2,050 m
1,127	Stéphane BORDAS	2,050 m
1,127	Damien Lane	2,050 m
1,127	Ricardo C	2,050 m



Computed in Luxembourg

Computational Sciences Luxembourg



Medicine

The average drug developed by a major pharmaceutical company costs at least \$4 billion, and it can be as much as \$11 billion.

Mechanics

The development cost of the A380

11 billion euros...

of the dreamliner...

\$32 billion

The background of the entire cover is a repeating pattern of various pills and capsules in different colors (green, blue, red, orange, yellow) and shapes (round, oval, capsule).

The Economist

FEBRUARY 3RD-9TH 2018

Theresa May: dead woman standing still
Ponzi schemes in China
Higher education, lower returns
Pity the pangolin

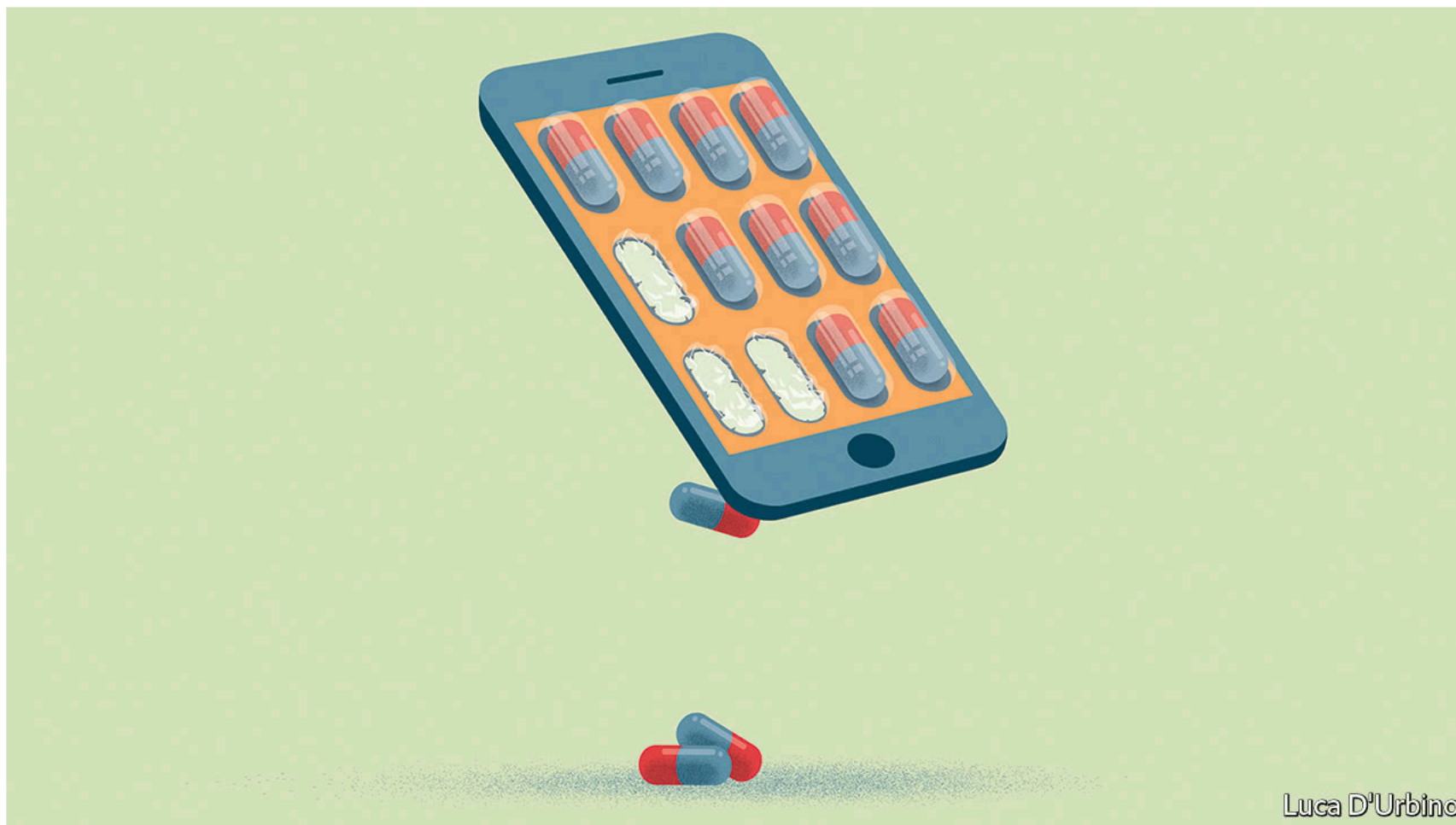
Doctor You

How data will transform health care

Tech giants go to med school

Apple and Amazon's moves in health signal a coming transformation

The world's biggest tech firms see a rich opportunity in health care, which could mean empowered patients, better diagnosis of disease and sharply lower costs



Print edition | Business >

Feb 3rd 2018

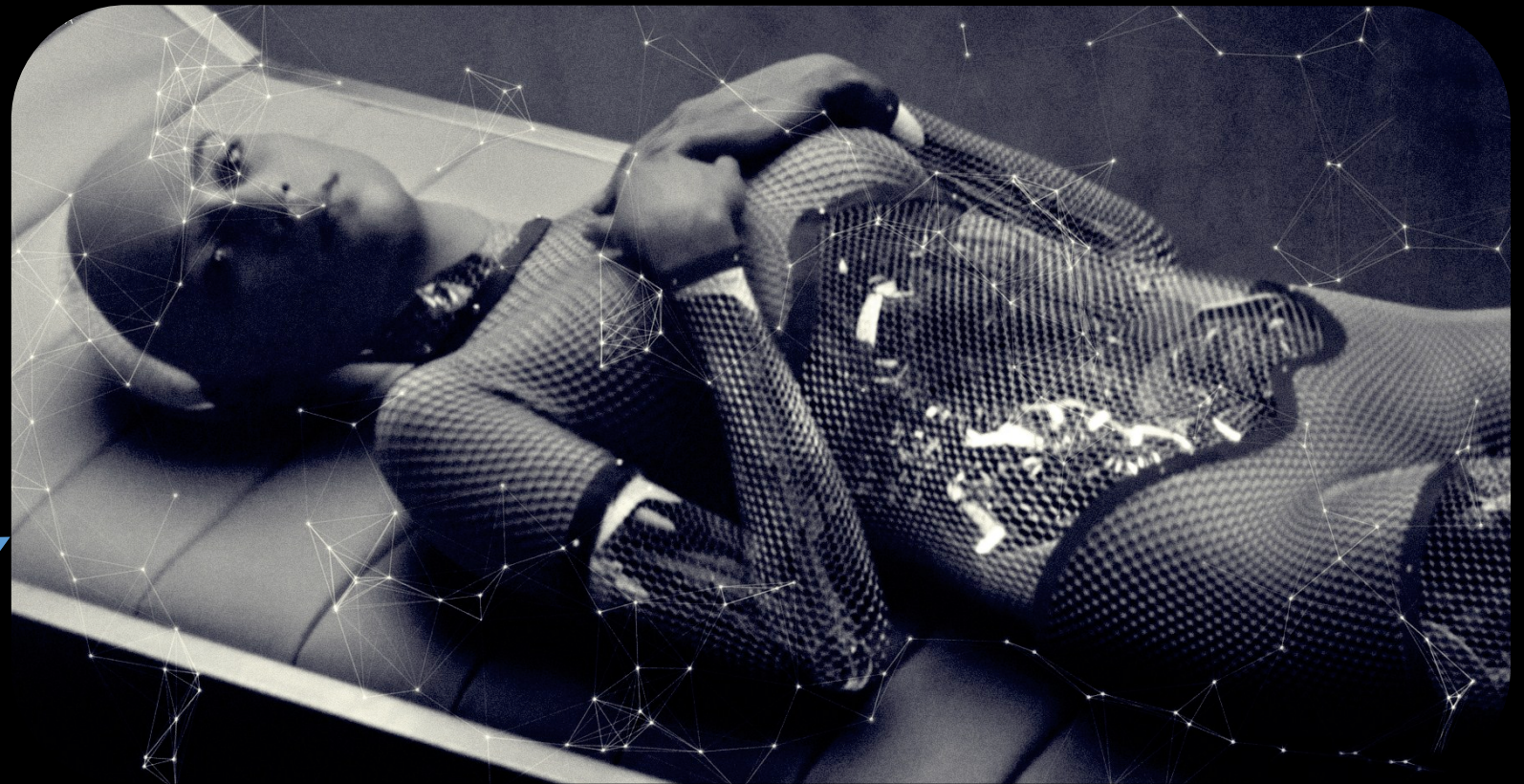








DIGITAL TWIN OF...

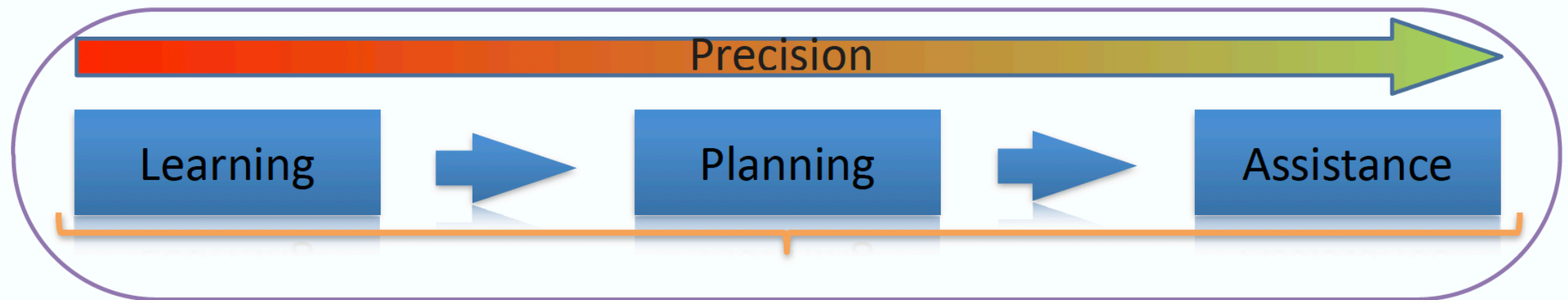


Alex Garland, *Ex Machina*, 2015

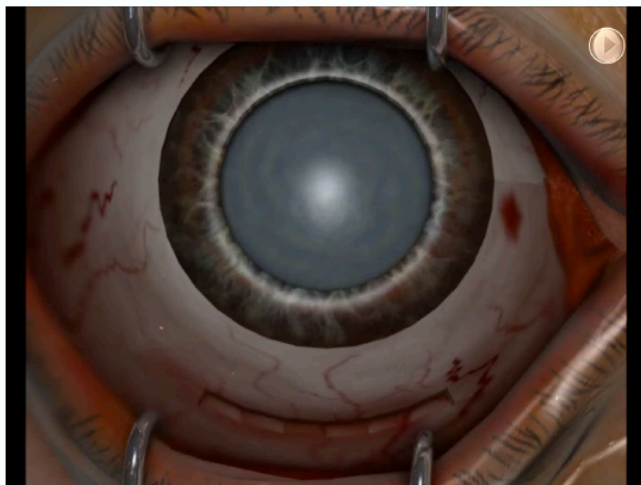


Surgical simulation

RealTcut

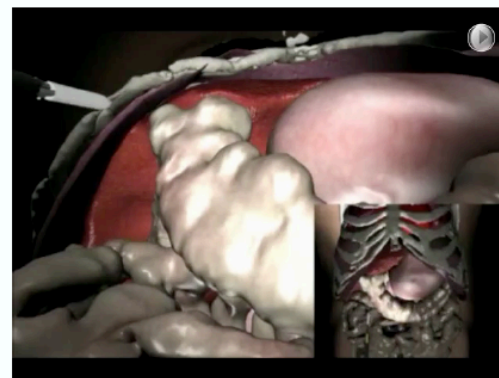


Cataract Surgery



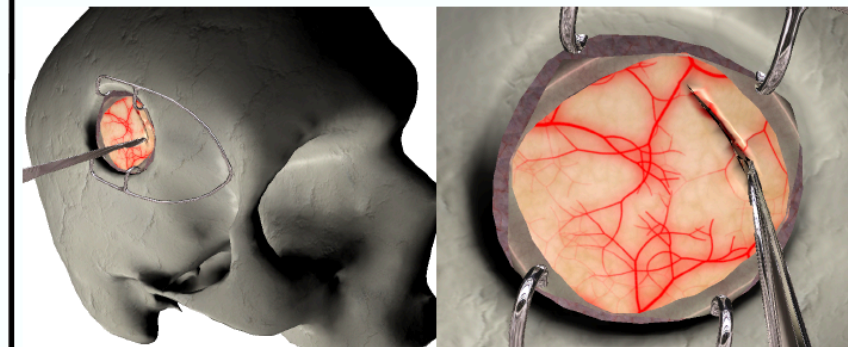
Inria

Abdominal minimally invasive surgery simulation (Inria, Shacra)



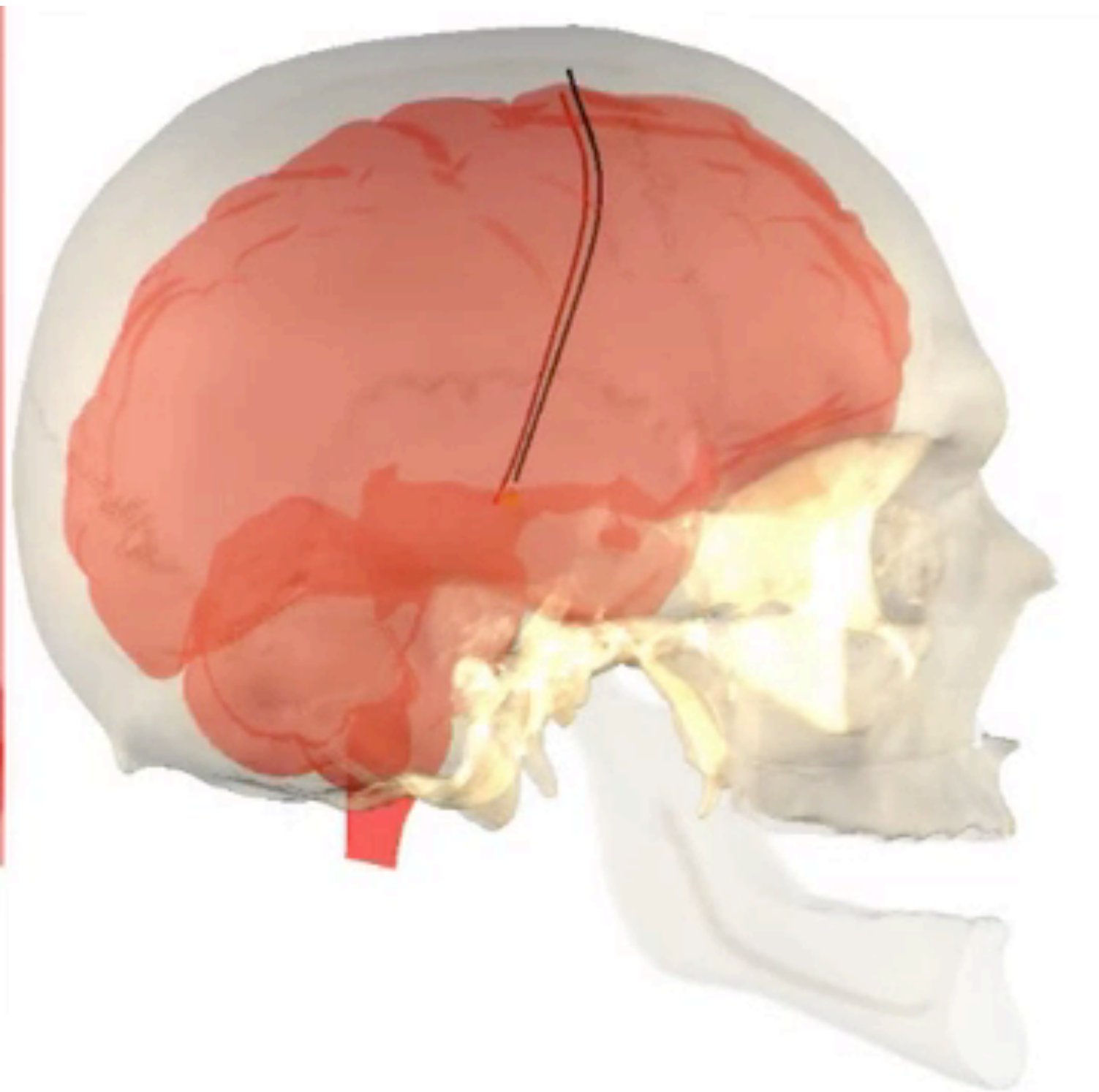
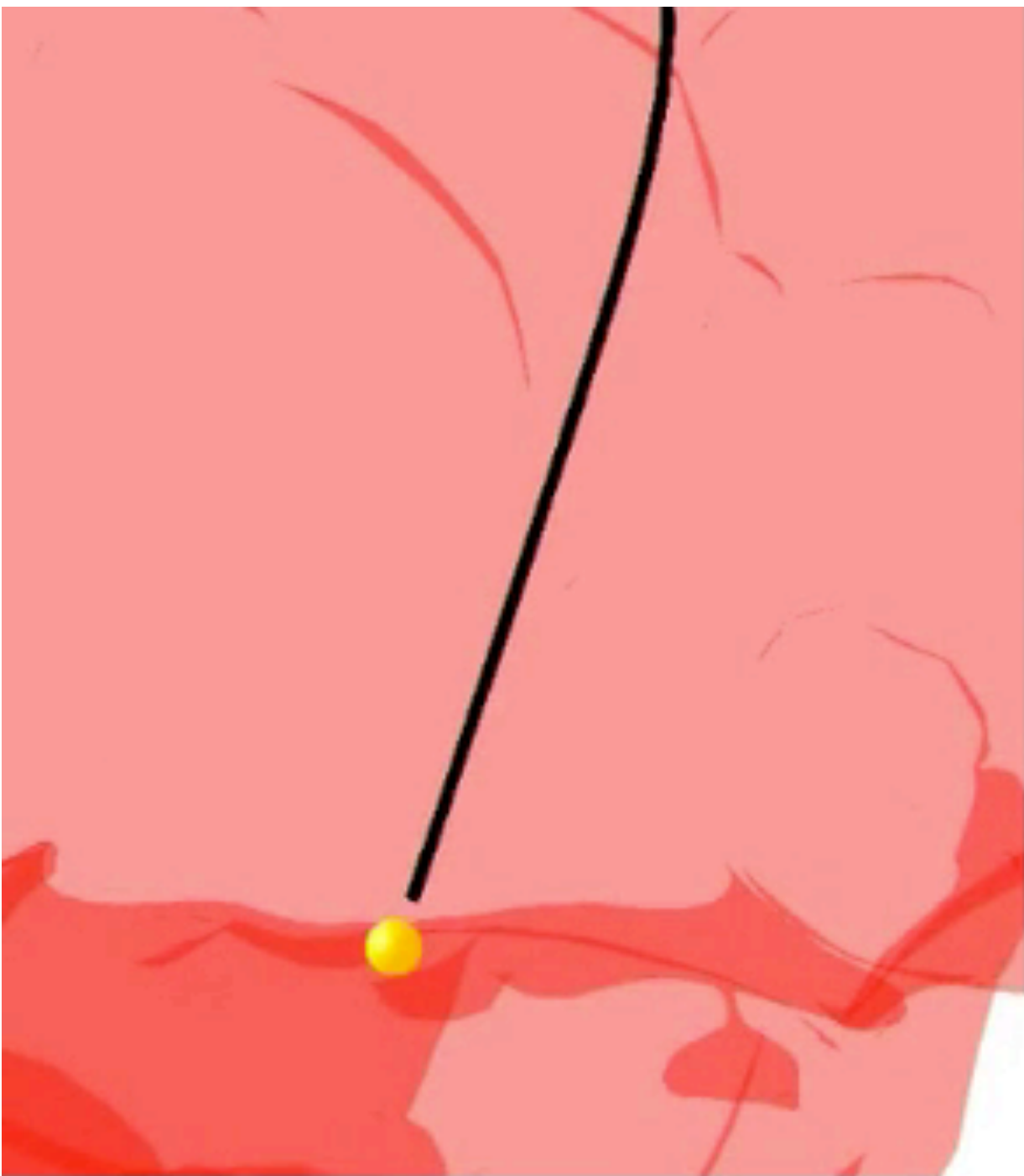
Inria

First implicit, interactive method for cutting with contact

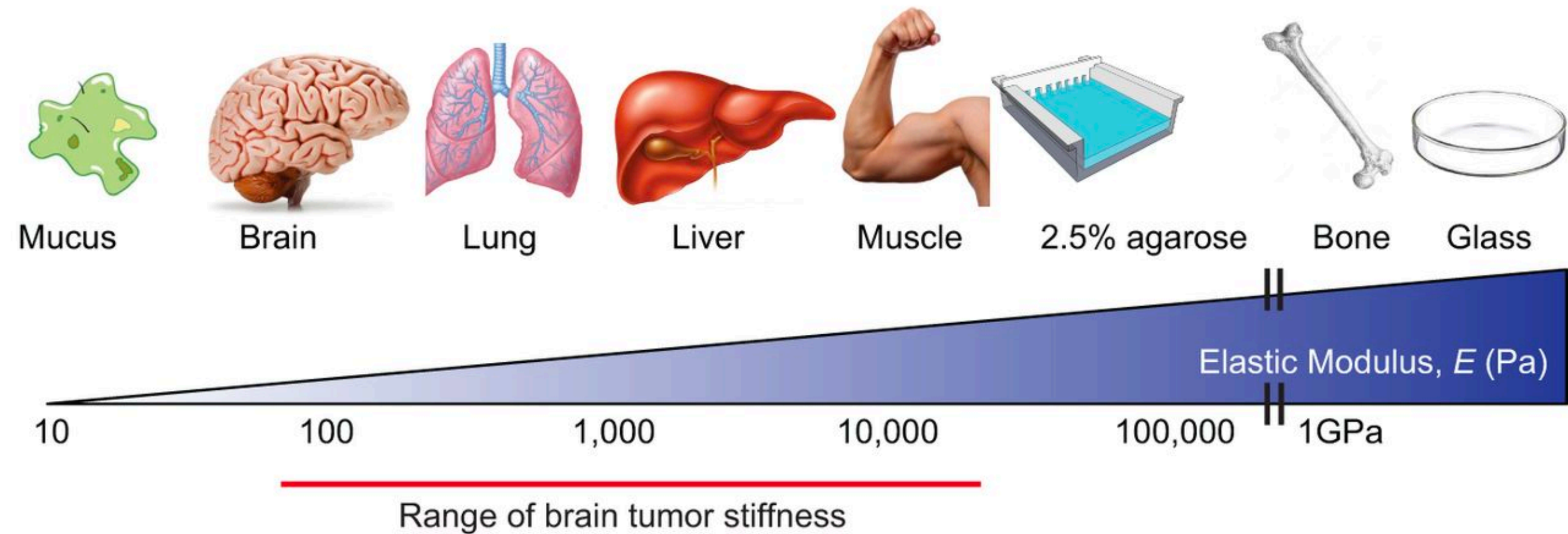


[Courtecuisse et al., MICCAI, 2013 and Medical Image Analysis, 2014]

YOU!



Deep-brain stimulation

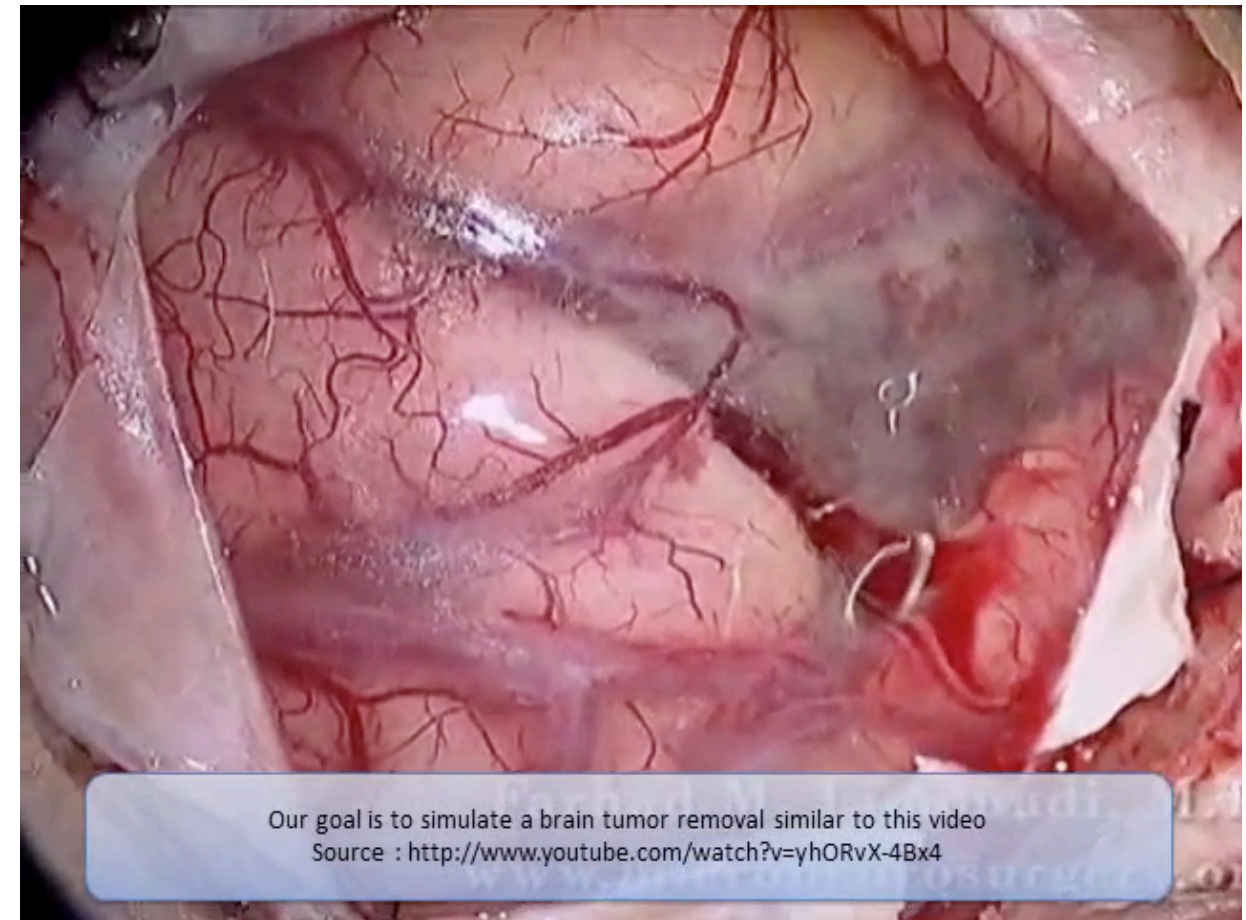
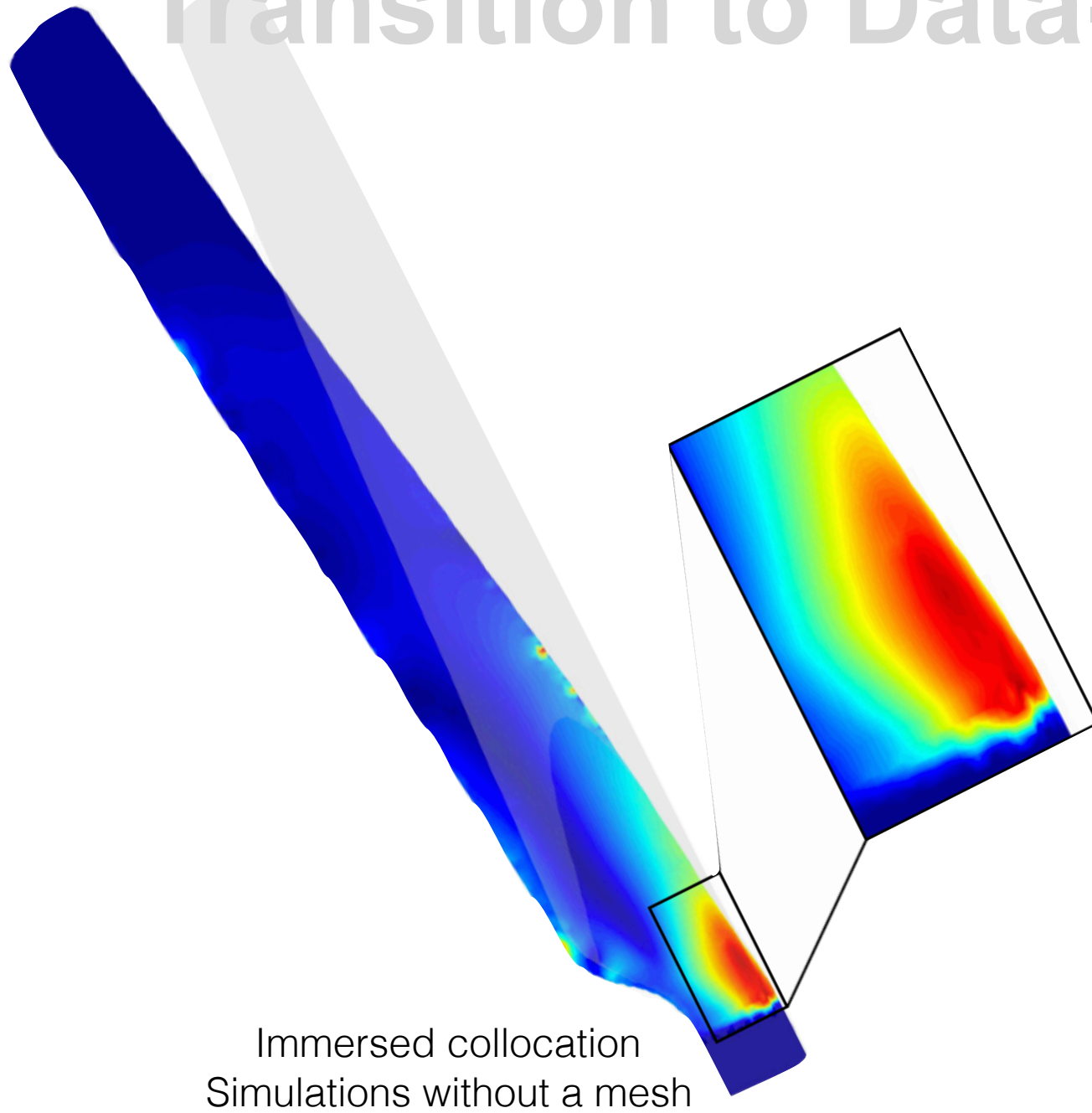


Tissue mechanics regulate brain development, homeostasis and disease

J. Matthew Barnes, Laralynne Przybyla, Valerie M. Weaver

J Cell Sci 2017 130: 71-82; doi: 10.1242/jcs.191742

Computational Sciences & Transition to Data-Driven Modelling



Real-time cutting, MEDIA2014, IEEE2017

Engineering

Personalised medicine



Quantify the quality of the simulation

physical problem

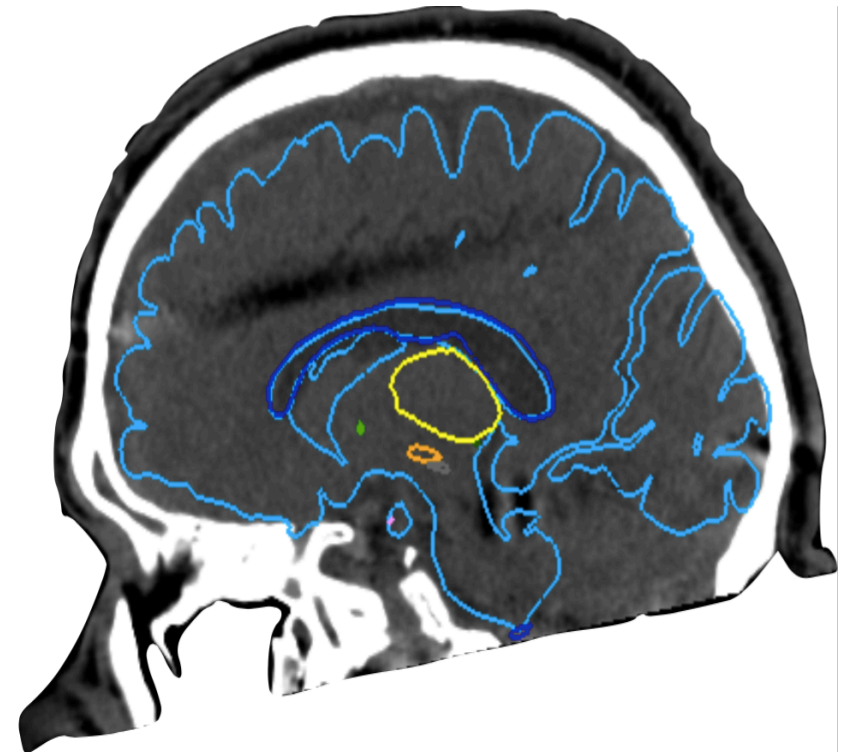


Quantify the quality of the simulation

physical problem



Bijar, Rohan, Perrier & Payan 2015



Quantify the quality of the simulation

physical problem



mathematical
model



Quantify the quality of the simulation

physical problem

mathematical
model

$$\min_{\mathbf{u} \in \mathbf{V}} \frac{1}{2} \int_{\Omega} \boldsymbol{\sigma}(\mathbf{u}, \beta) : \boldsymbol{\varepsilon}(\mathbf{u}) \, d\mathbf{x} - \int_{\Omega} \mathbf{g} \cdot \mathbf{u} \, d\mathbf{x}$$

with

$$\boldsymbol{\sigma}(\mathbf{u}, \beta) = \underbrace{\boldsymbol{\sigma}_P(\mathbf{u})}_{\substack{\text{passive} \\ \text{material}}} + \underbrace{\boldsymbol{\sigma}_A(\beta)}_{\substack{\text{muscular} \\ \text{activation}}} \left\{ \begin{array}{l} \boldsymbol{\sigma}_A(\beta) = \beta T e_A \otimes e_A \\ e_A : \text{fiber direction} \\ T : \text{tension} \\ \beta : \text{activation} \end{array} \right.$$

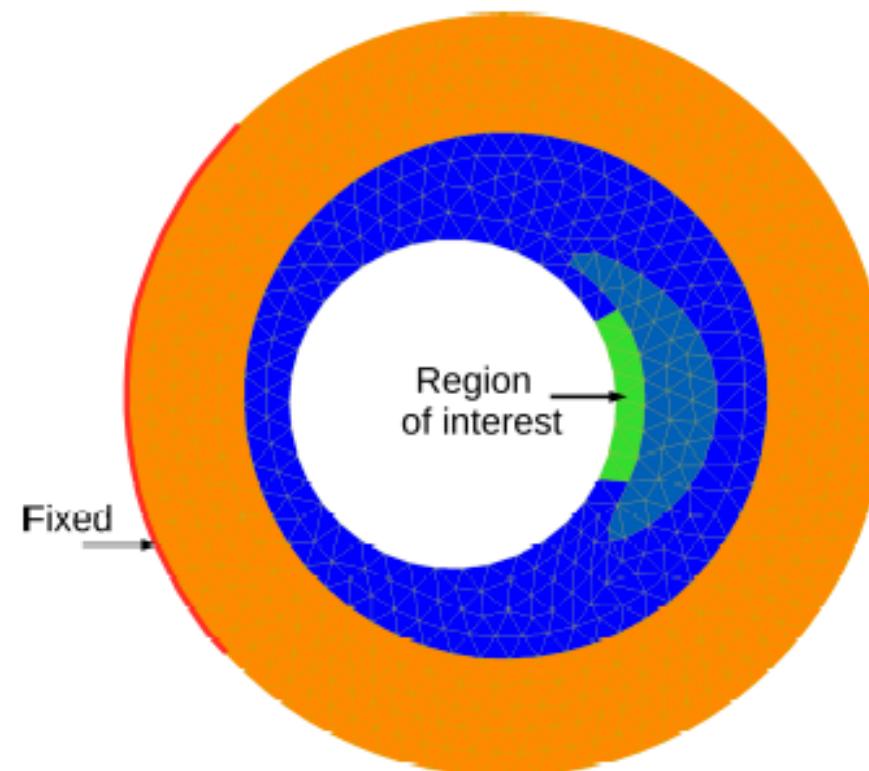
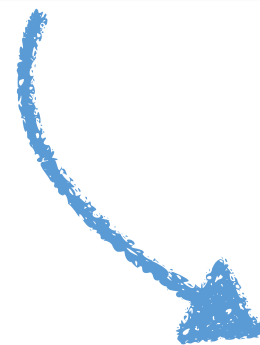
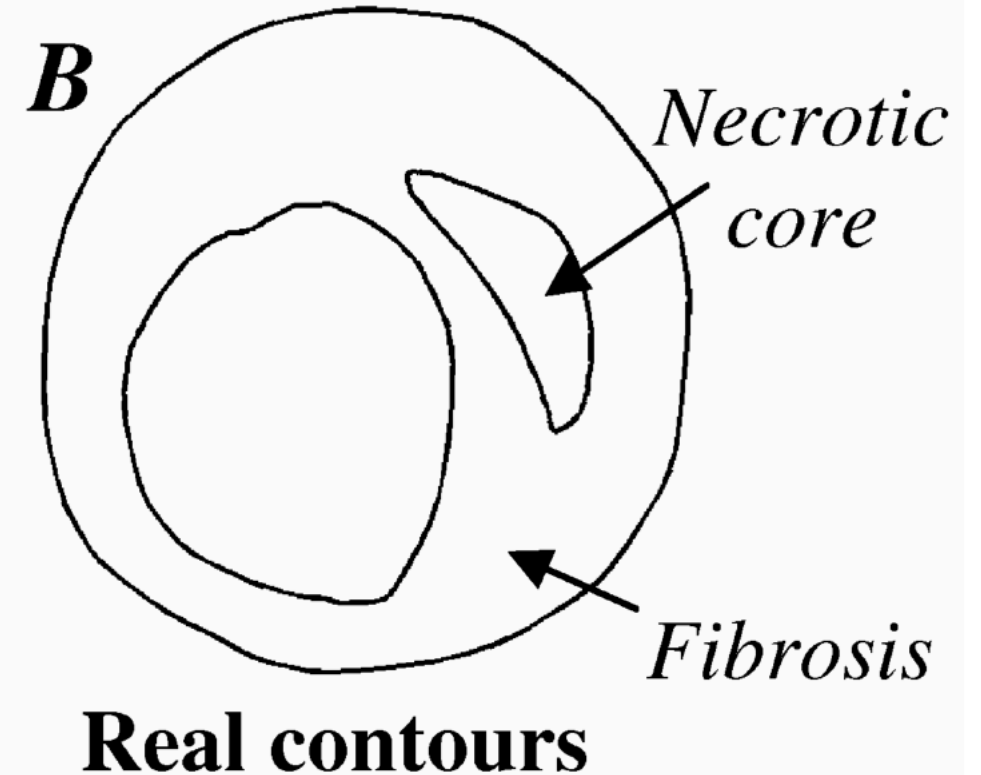
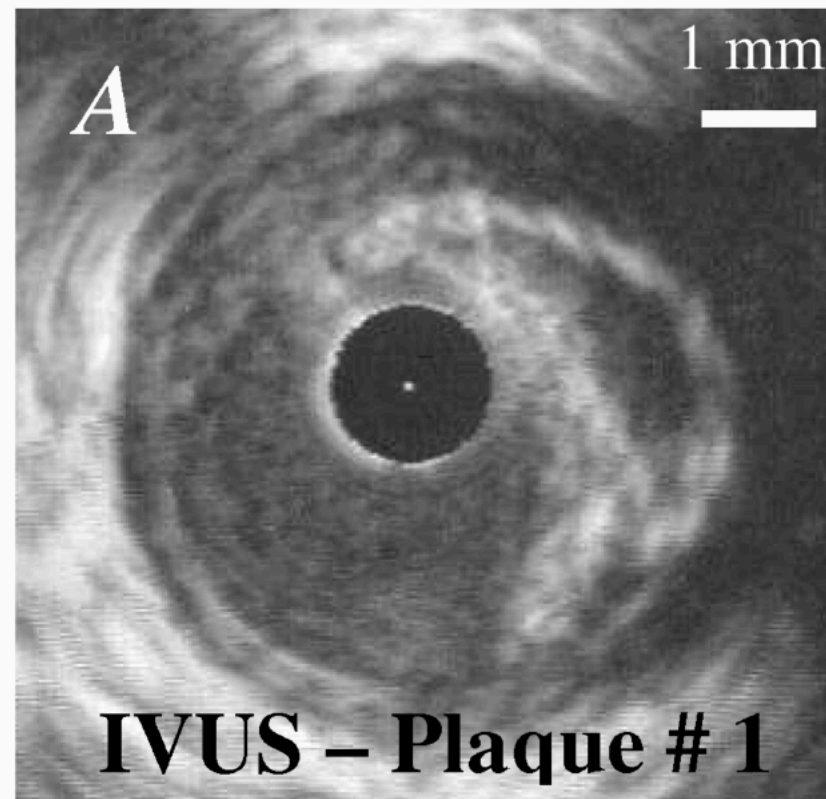
Material model and governing equations



Quantify the quality of the simulation

physical problem

mathematical model

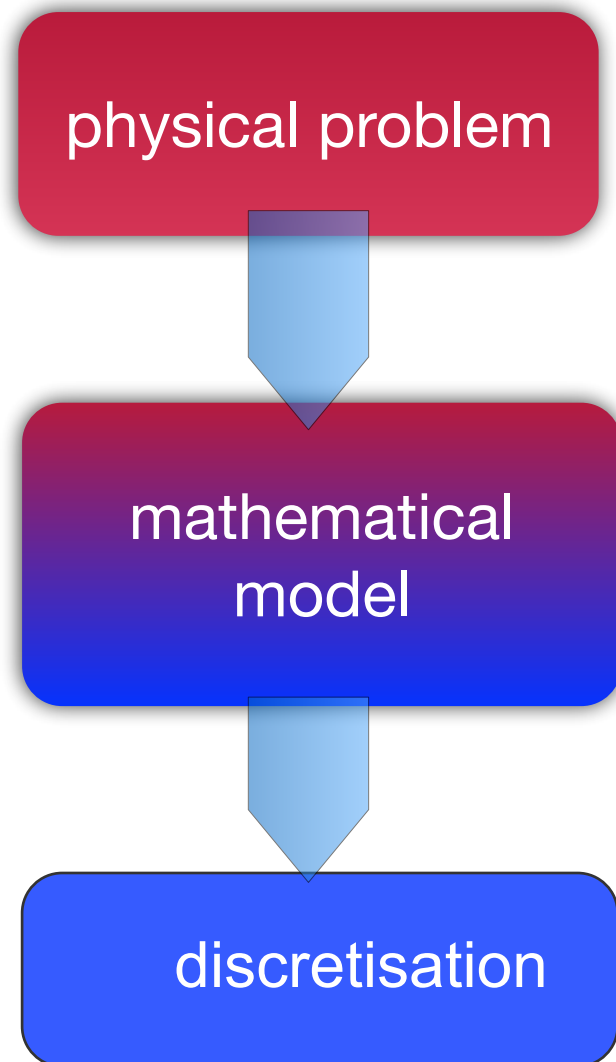


Geometry and
Boundary Conditions



RealTCut

Quantify the quality of the simulation

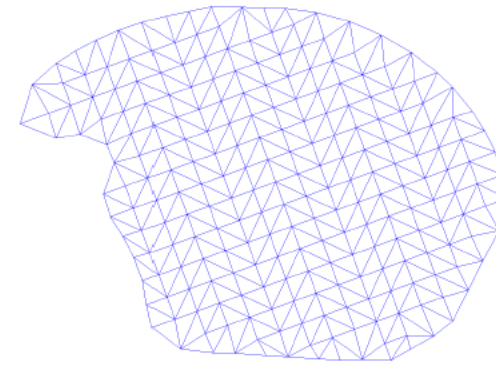


Quantify the quality of the simulation

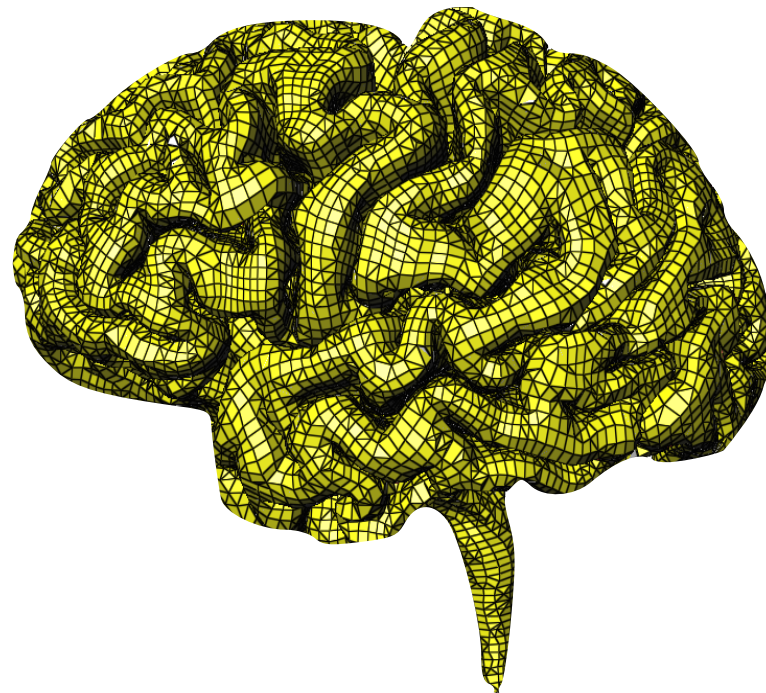
physical problem

mathematical
model

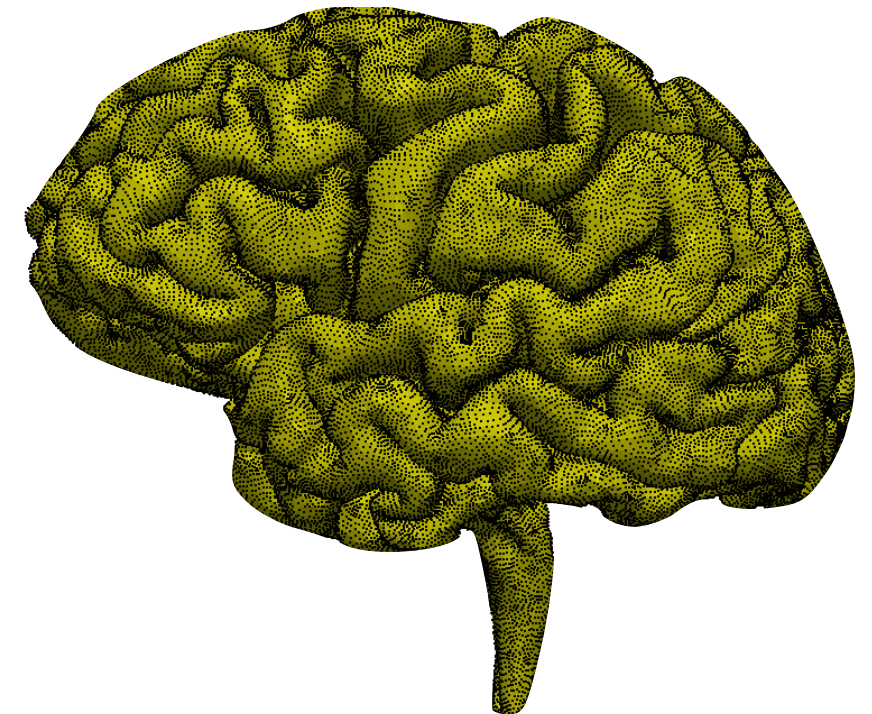
discretisation



Finite element mesh
of a tongue with F. Chouly et al.



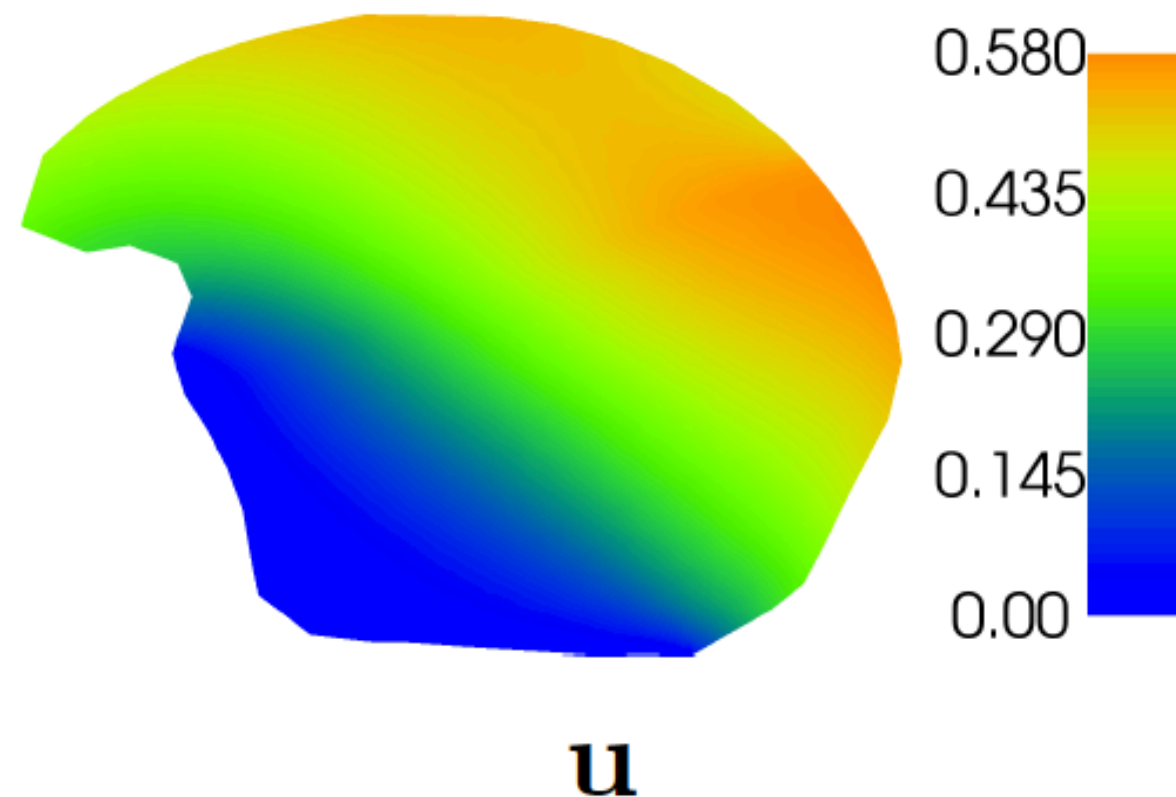
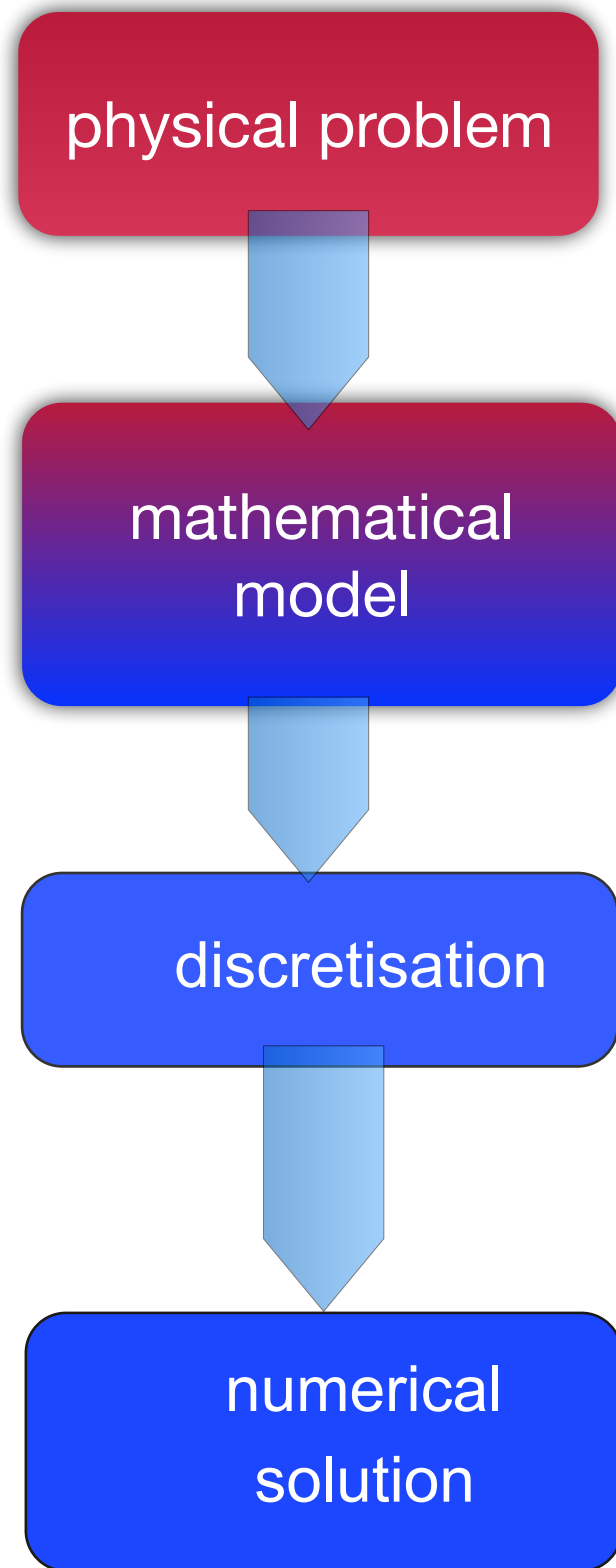
Hexahedral mesh of a brain
with Bruno Lévy, Inria



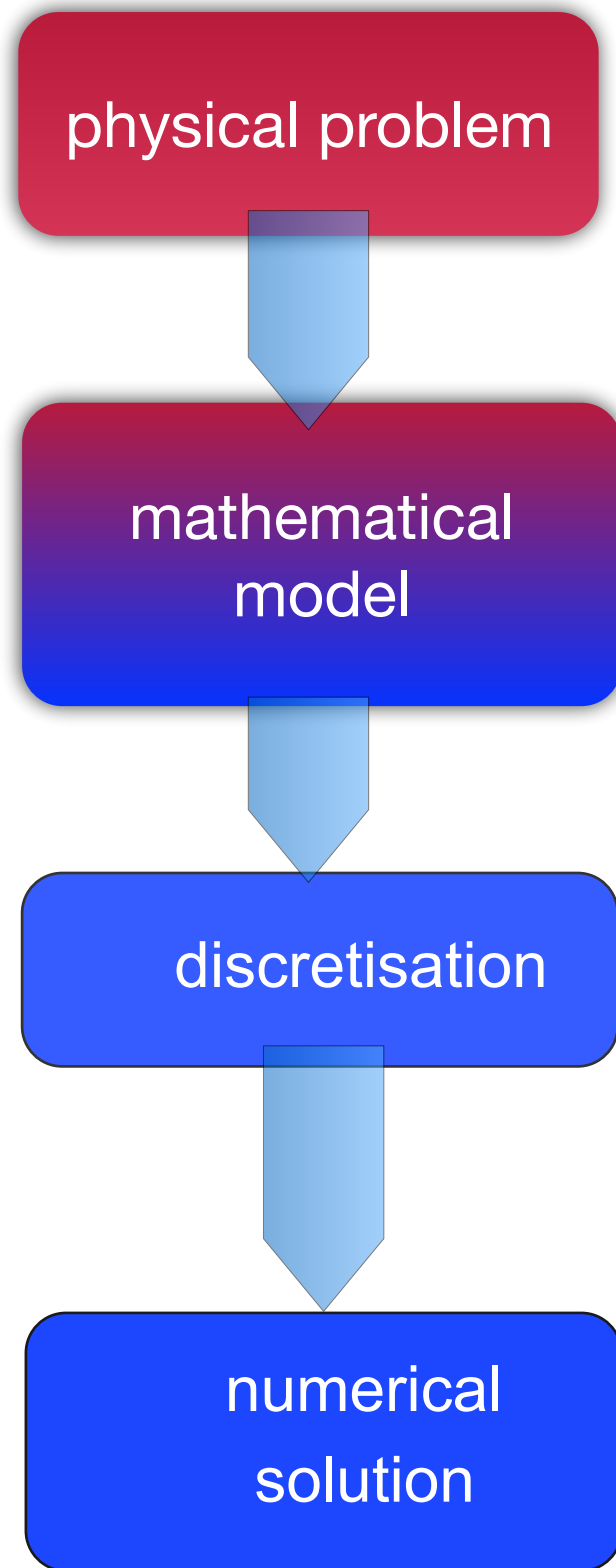
Meshless brain discretization
with Bruno Lévy, Inria



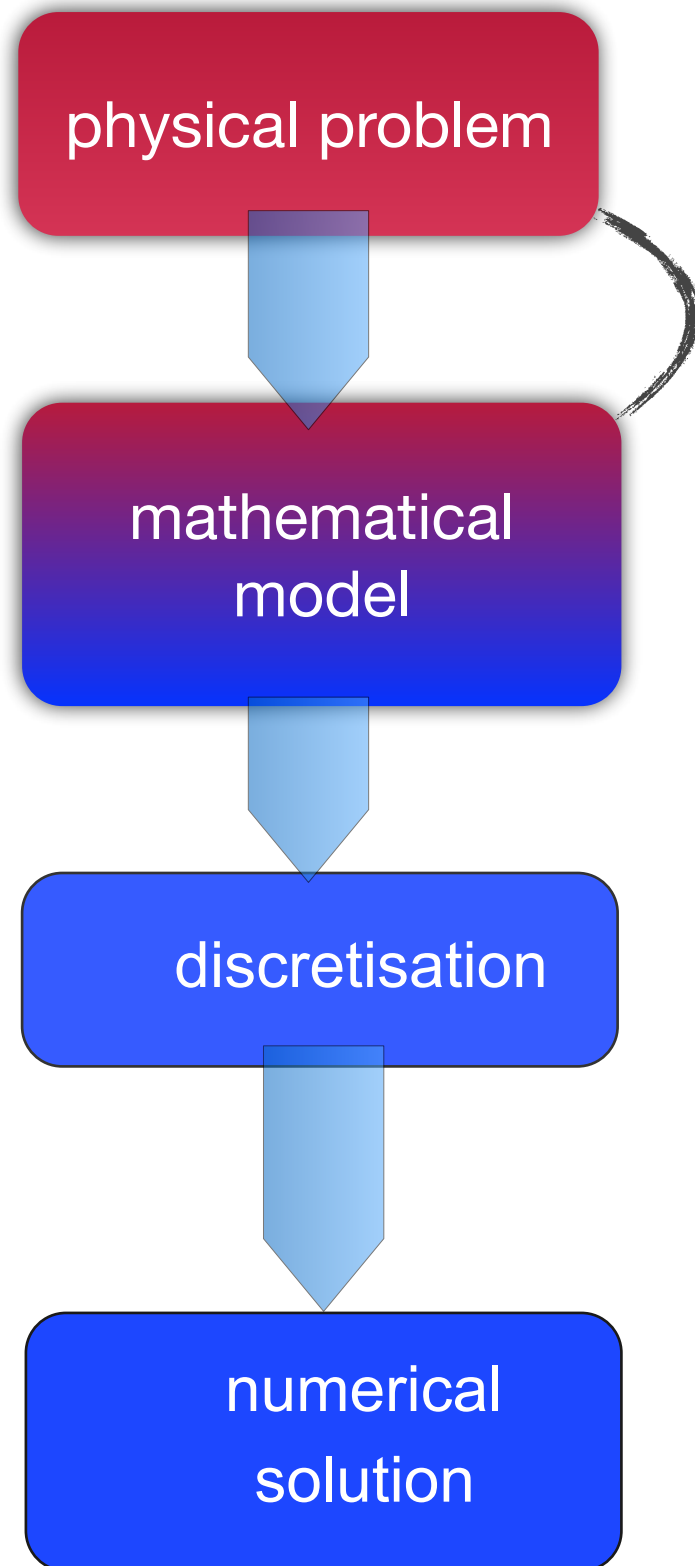
Quantify the quality of the simulation



Quantify the quality of the simulation



Quantify the quality of the simulation



Bijar, Rohan, Perrier & Payan 2015

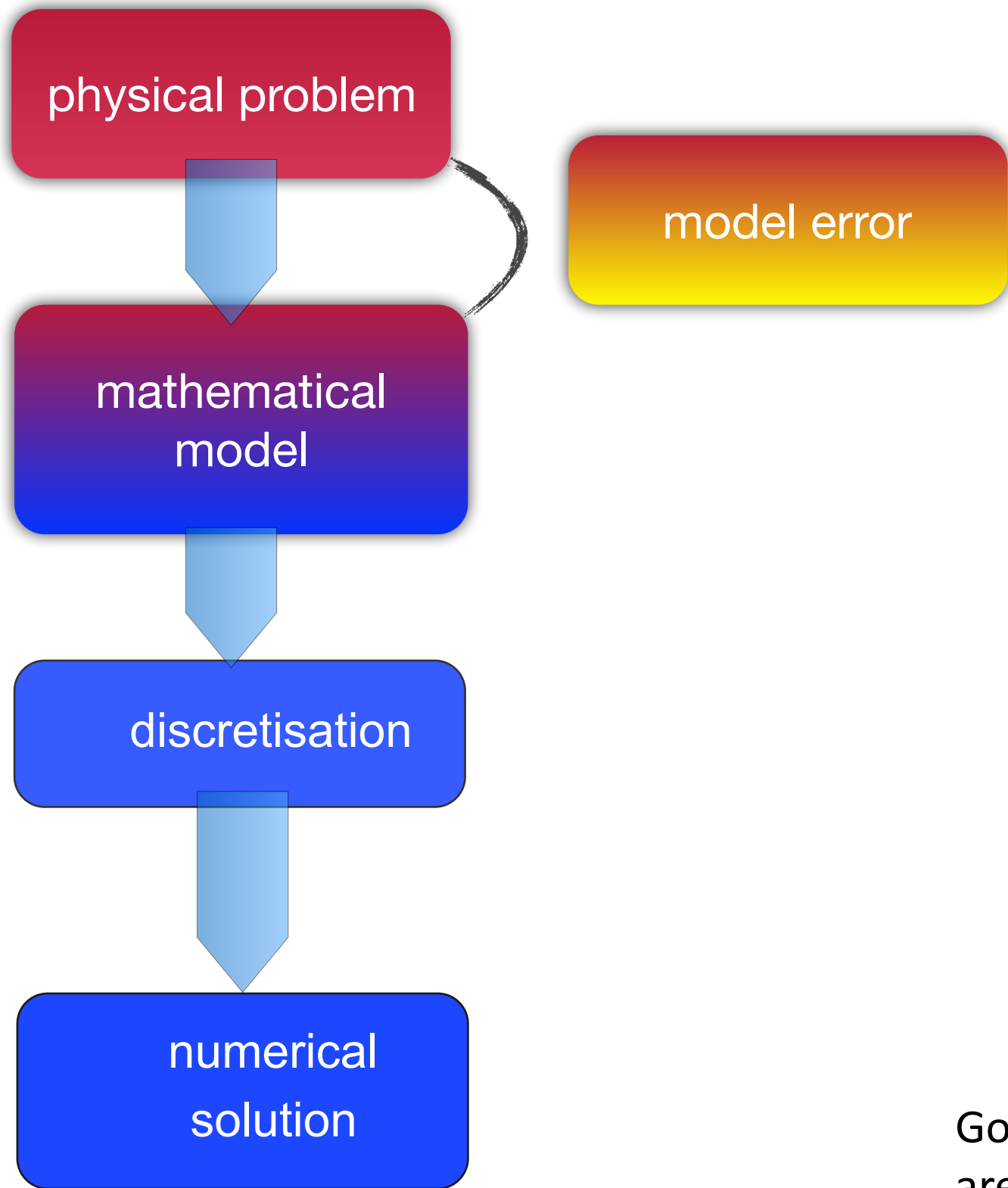
$\neq$

$$\min_{\mathbf{u} \in \mathbf{V}} \frac{1}{2} \int_{\Omega} \boldsymbol{\sigma}(\mathbf{u}, \beta) : \boldsymbol{\varepsilon}(\mathbf{u}) \, d\mathbf{x} - \int_{\Omega} \mathbf{g} \cdot \mathbf{u} \, d\mathbf{x}$$



RealTCut

Quantify the quality of the simulation



Bijar, Rohan, Perrier & Payan 2015

$\neq$

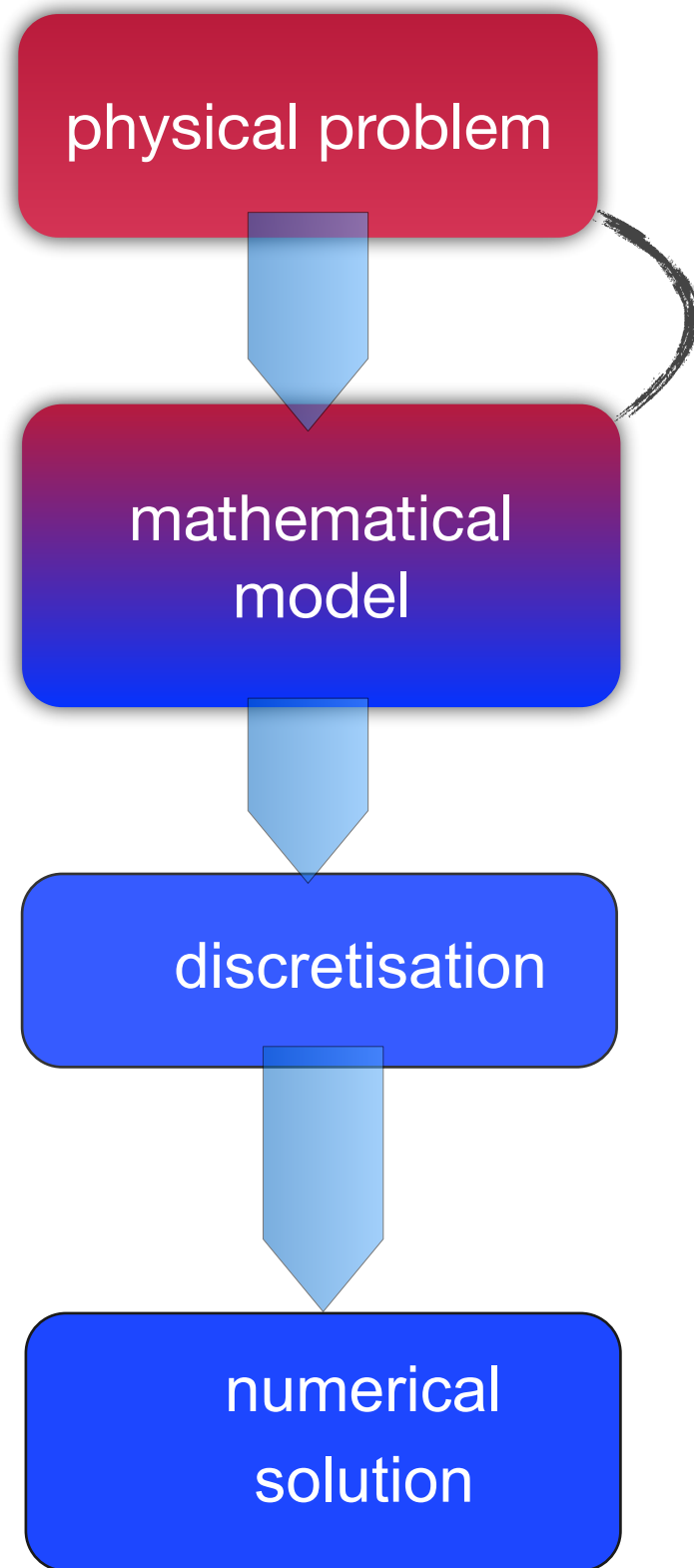
$$\min_{\mathbf{u} \in \mathbf{V}} \frac{1}{2} \int_{\Omega} \boldsymbol{\sigma}(\mathbf{u}, \boldsymbol{\beta}) : \boldsymbol{\varepsilon}(\mathbf{u}) \, d\mathbf{x} - \int_{\Omega} \mathbf{g} \cdot \mathbf{u} \, d\mathbf{x}$$

Governing equations and material models
are erroneous

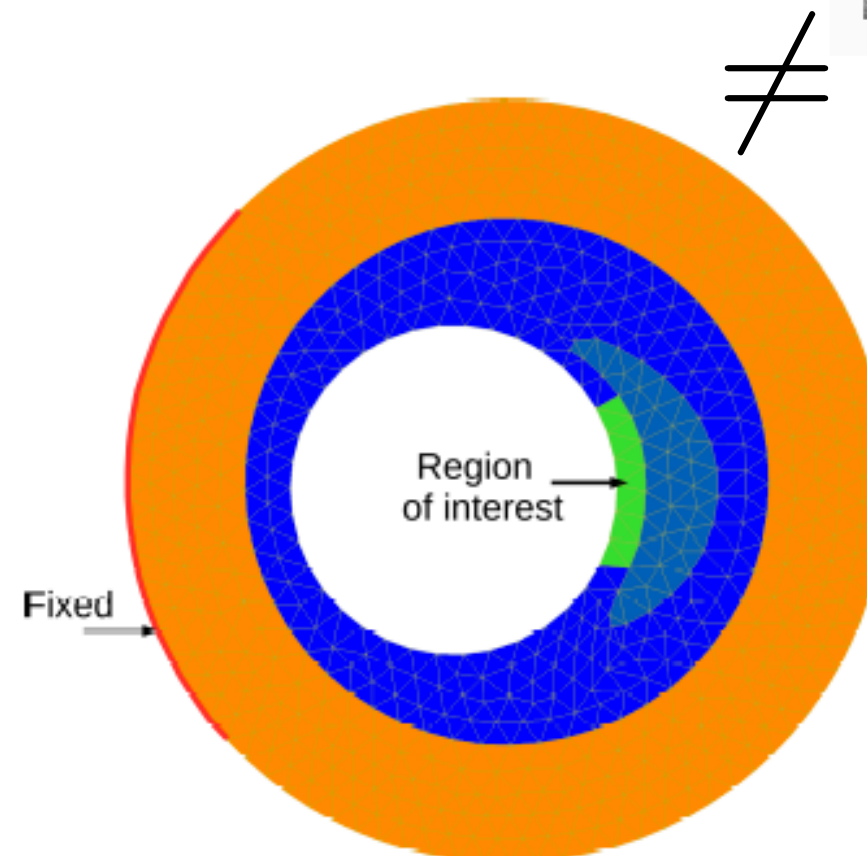
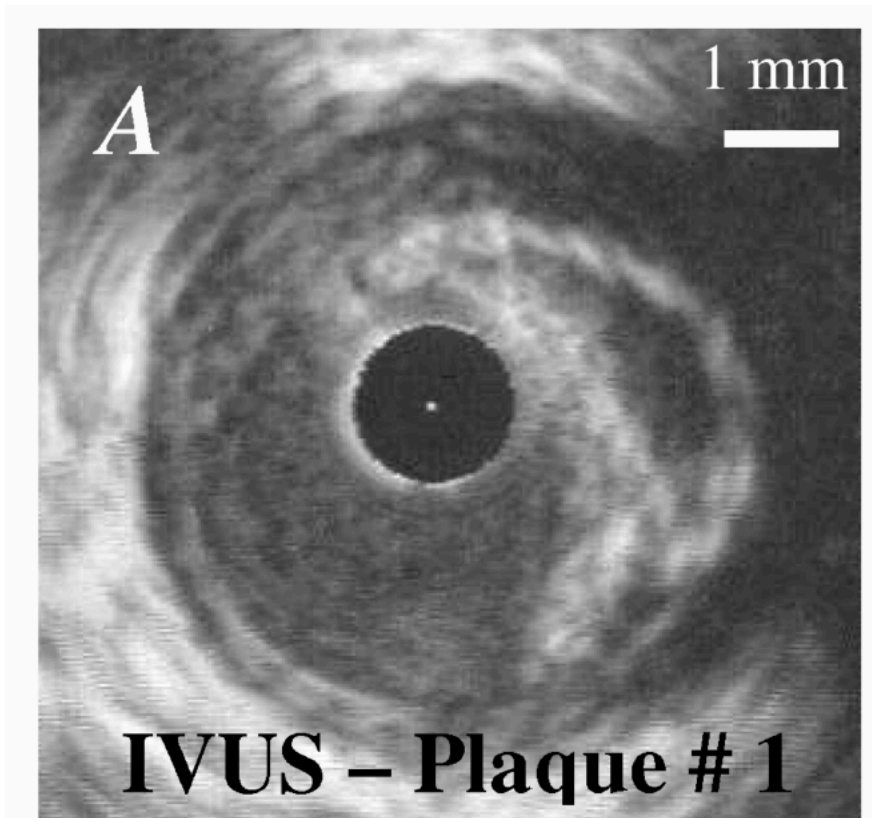


RealTCut

Quantify the quality of the simulation

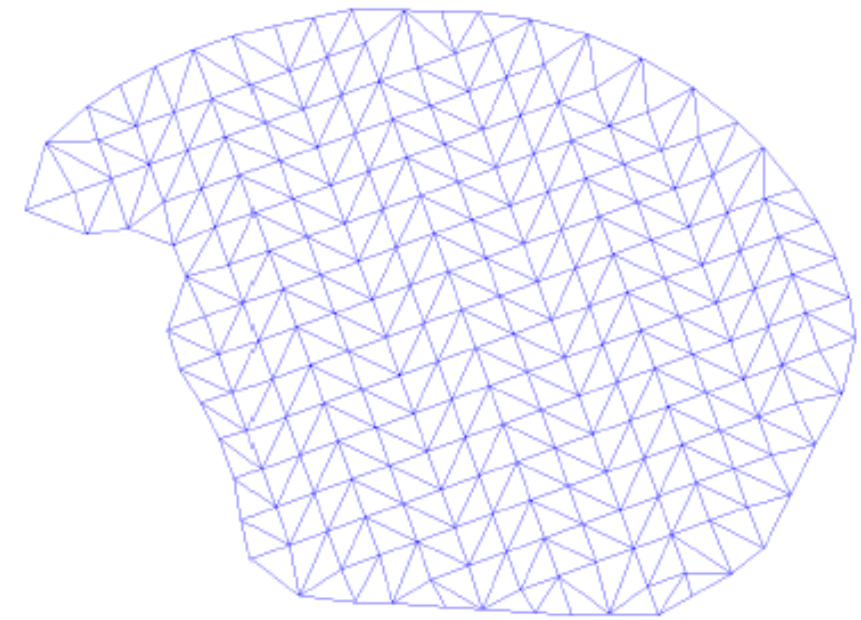
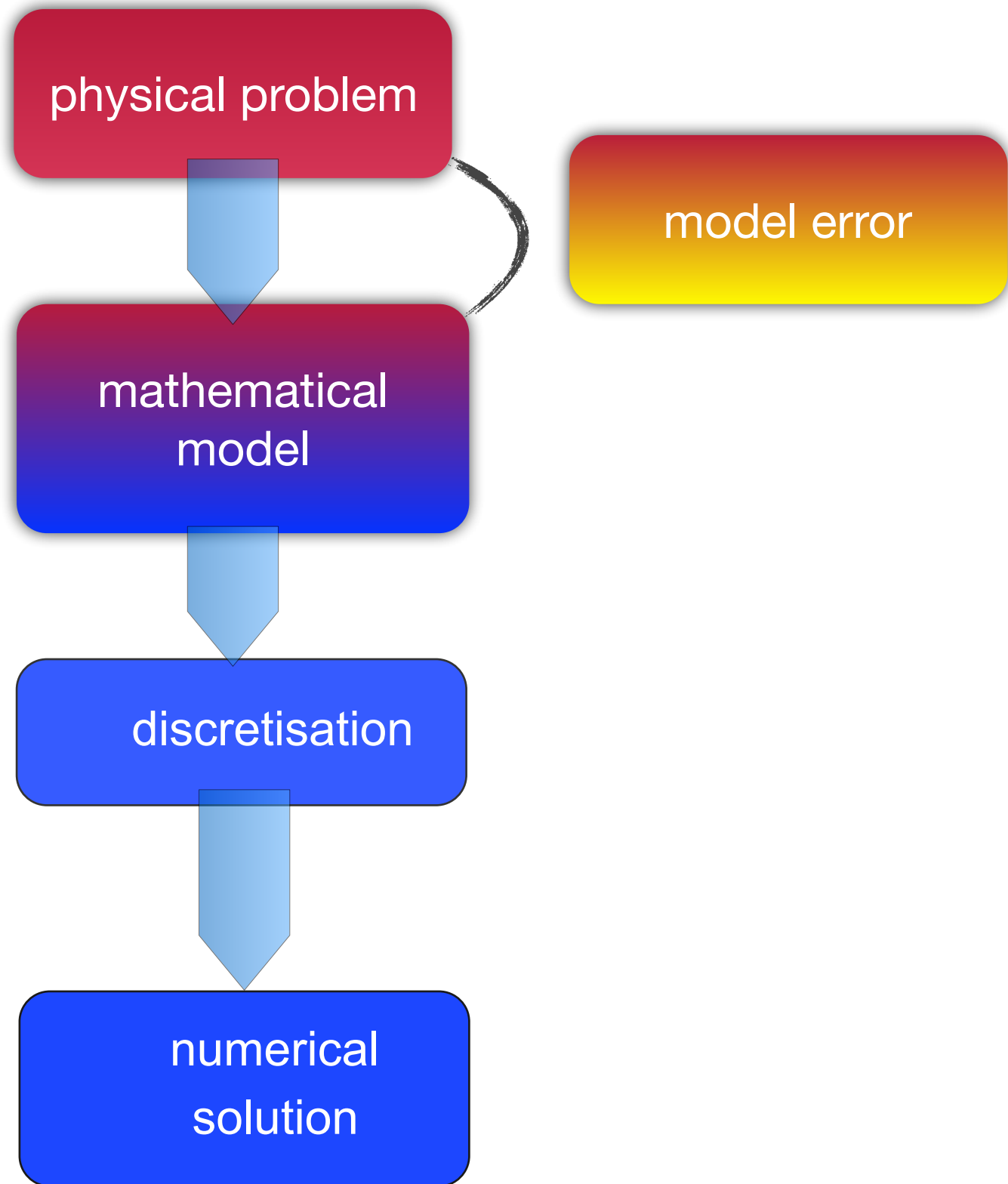


model error

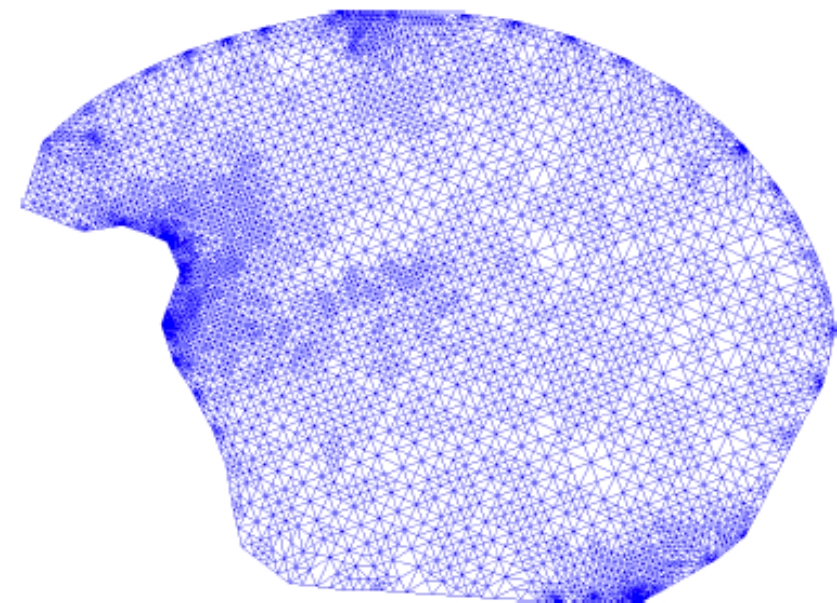


Geometry and boundary conditions are not known exactly

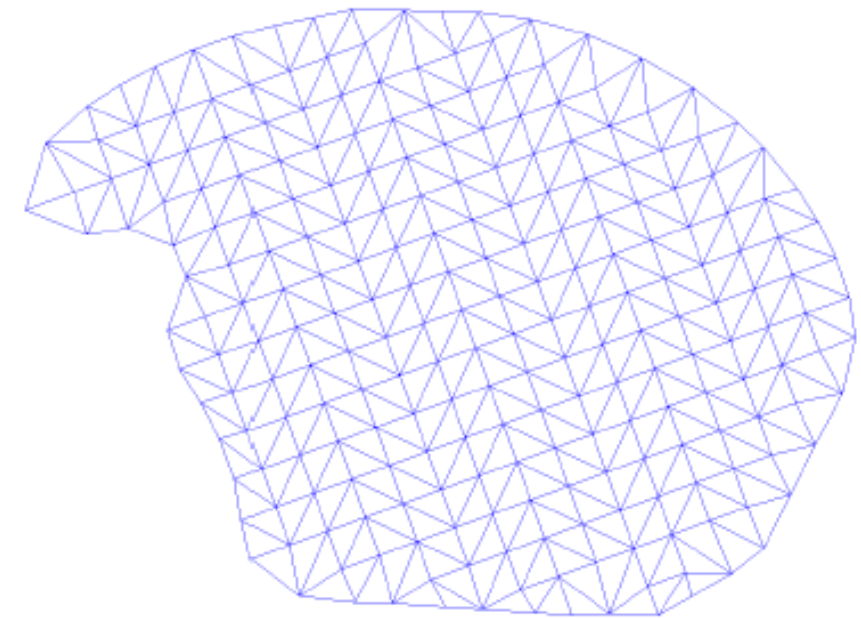
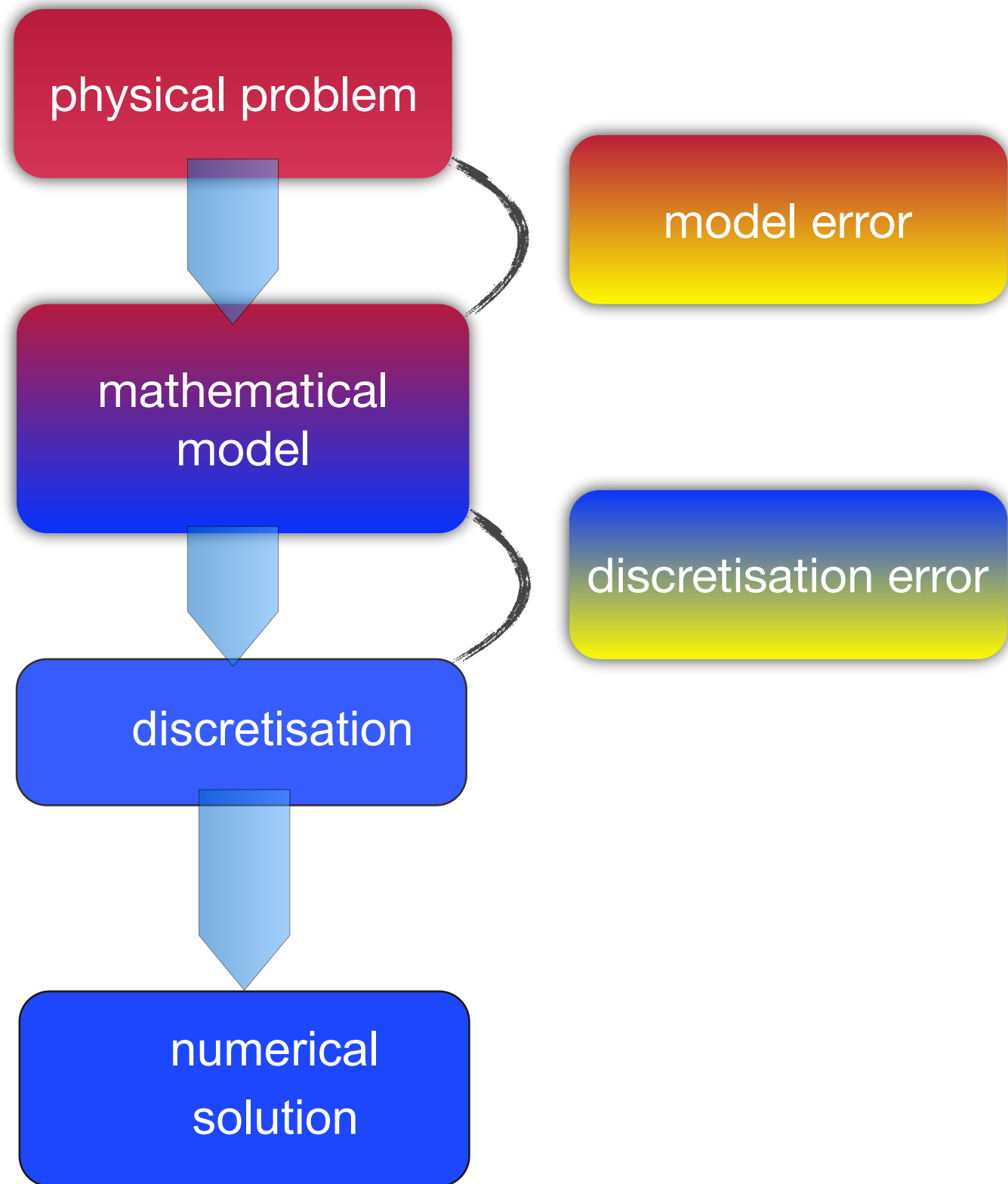
Quantify the quality of the simulation



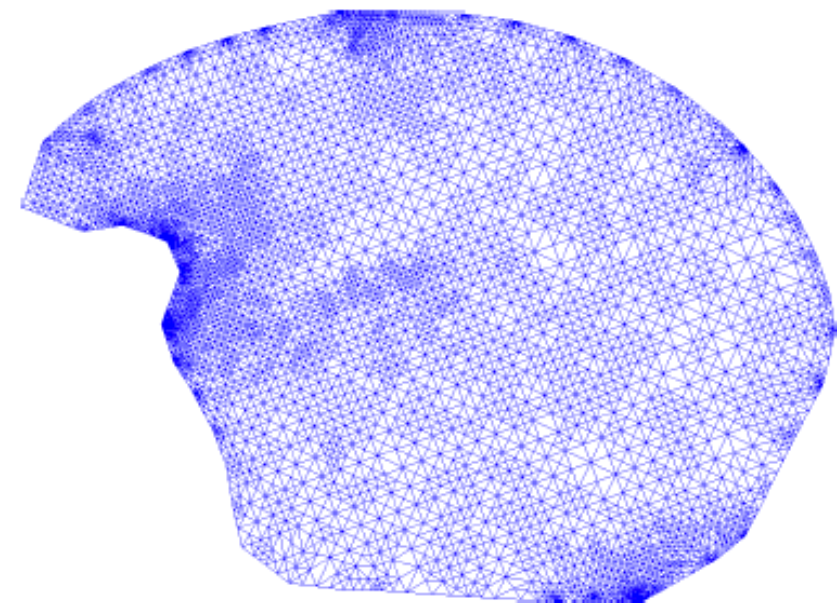
vs.



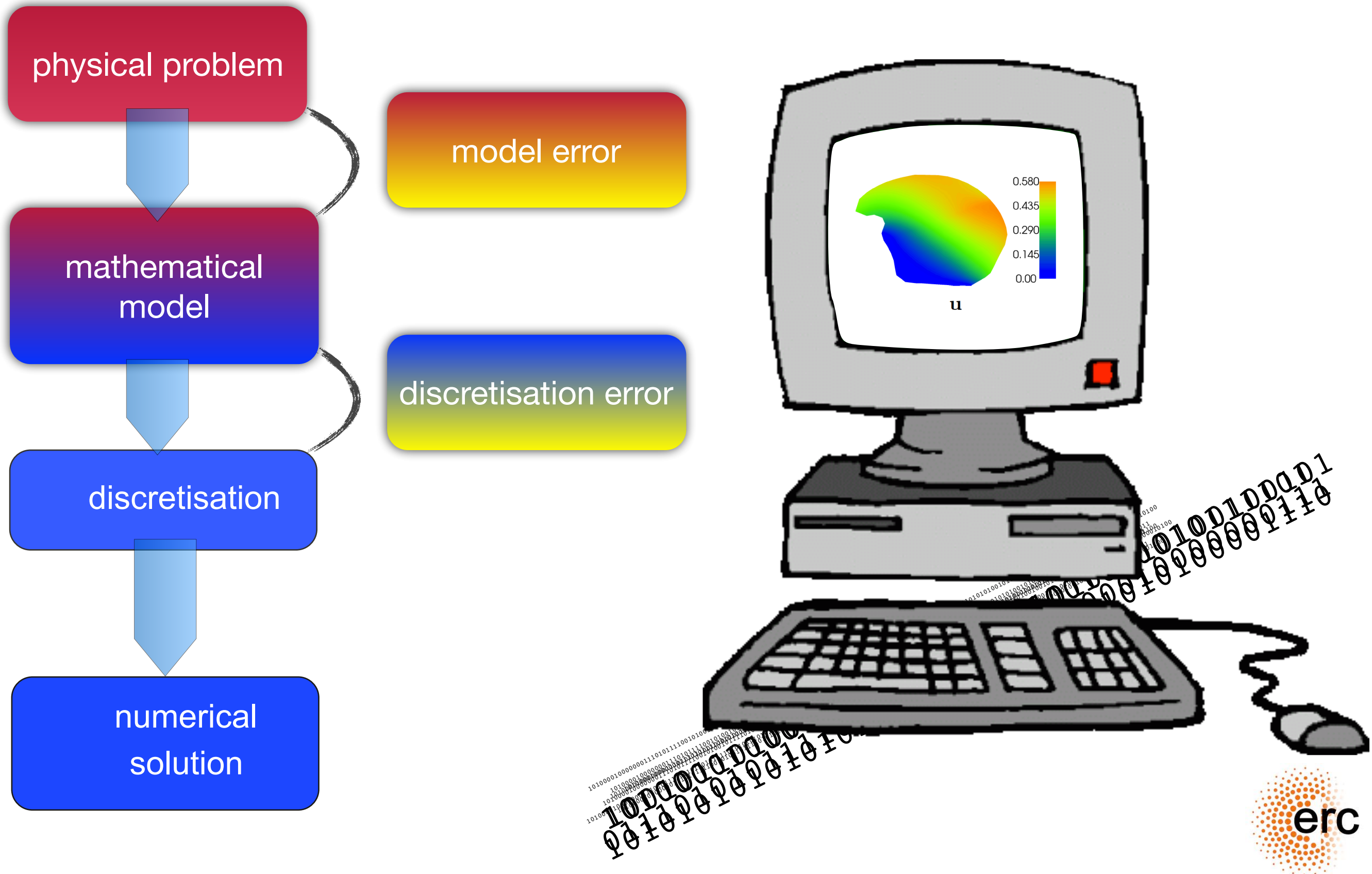
Quantify the quality of the simulation



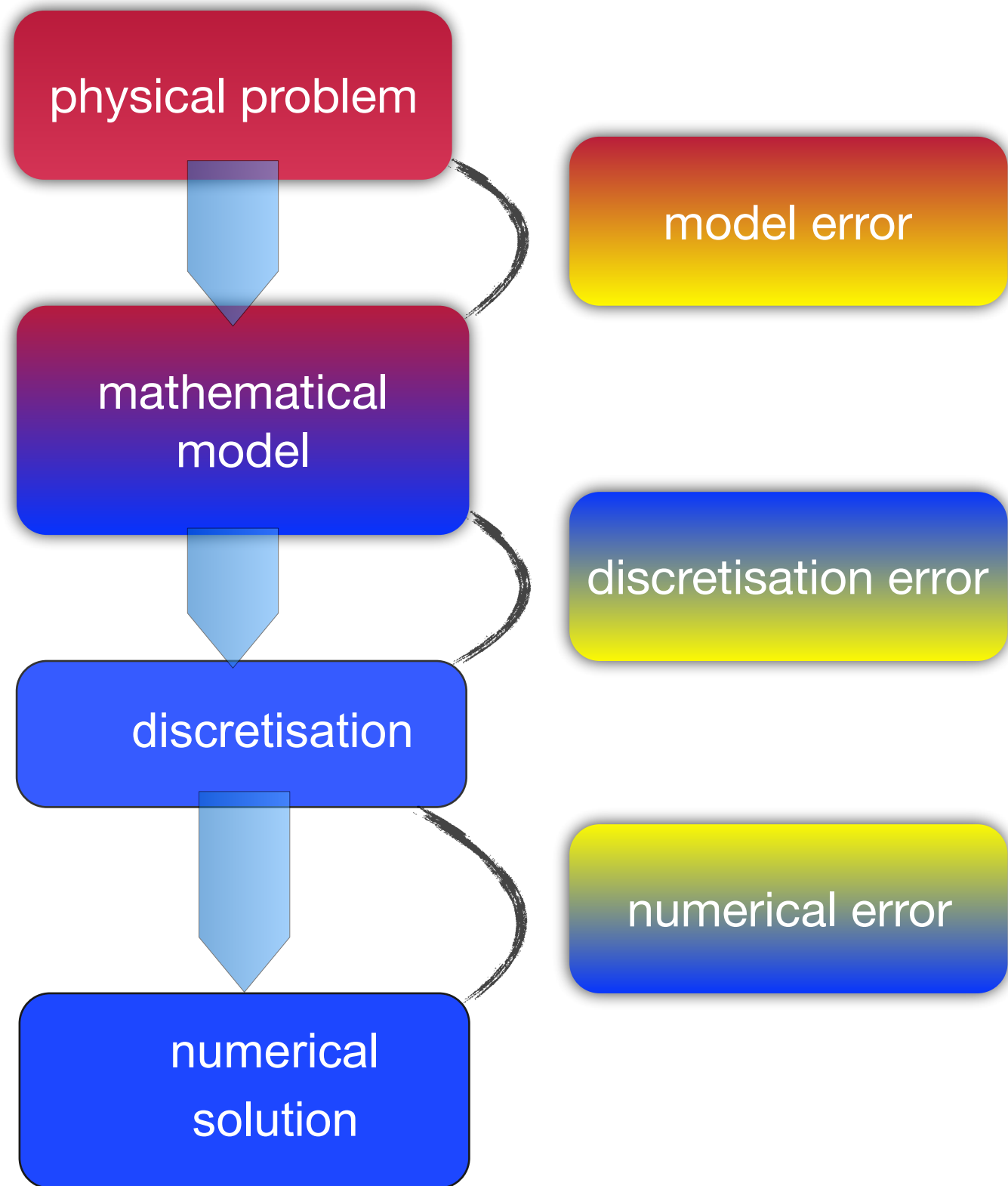
vs.



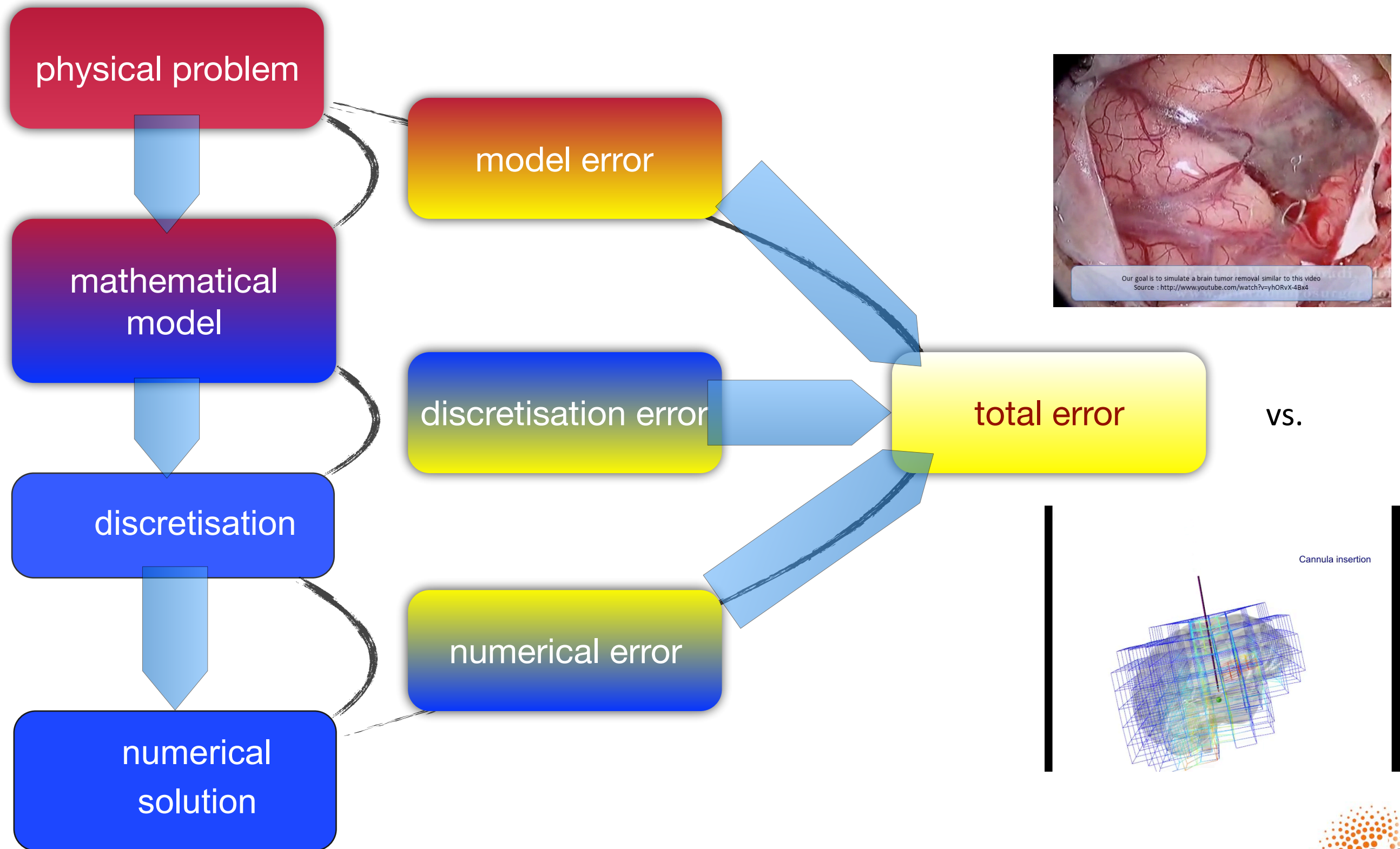
Quantify the quality of the simulation



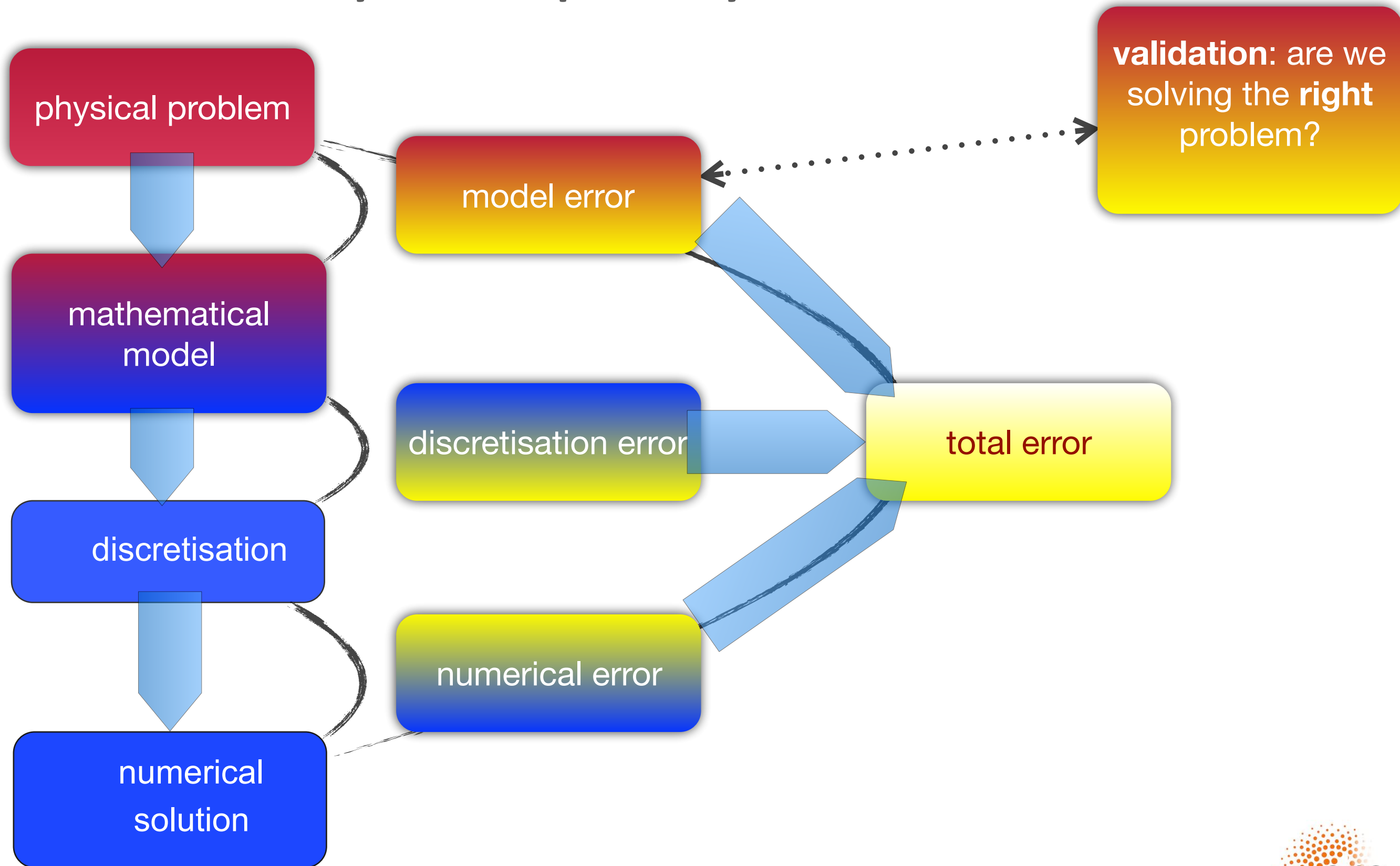
Quantify the quality of the simulation



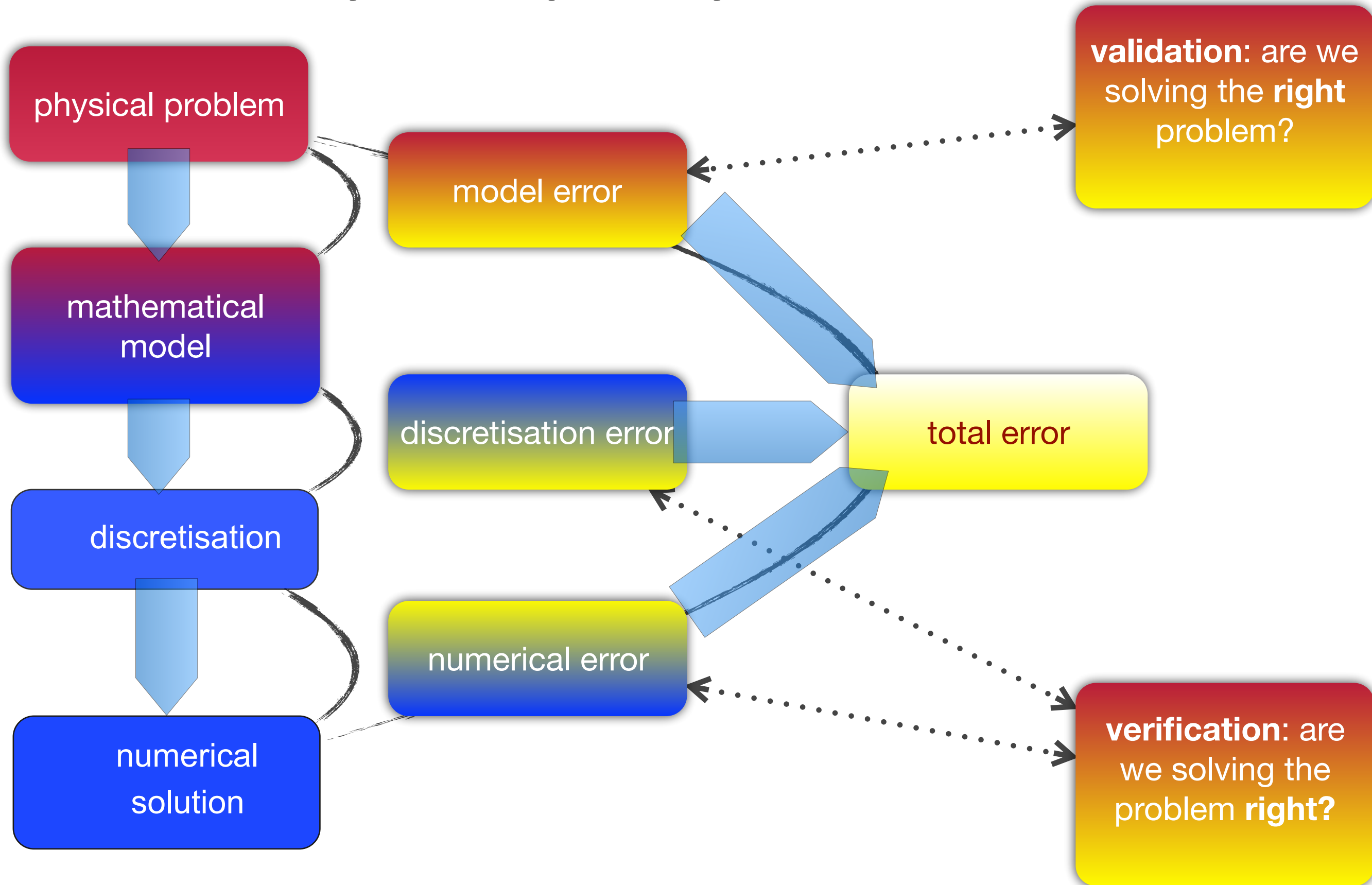
Quantify the quality of the simulation



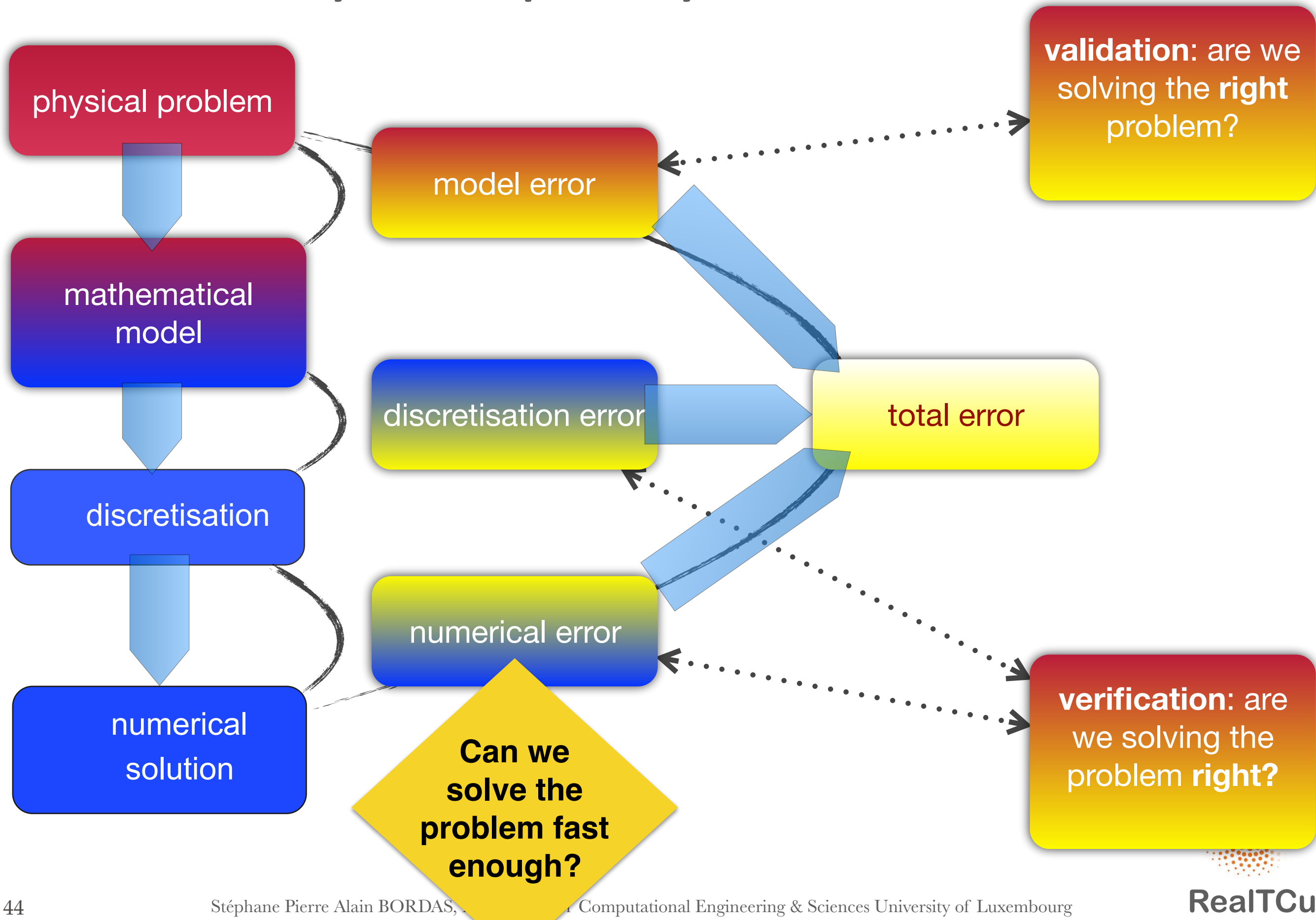
Quantify the quality of the simulation



Quantify the quality of the simulation



Quantify the quality of the simulation



ERC: first love



ERC: first love

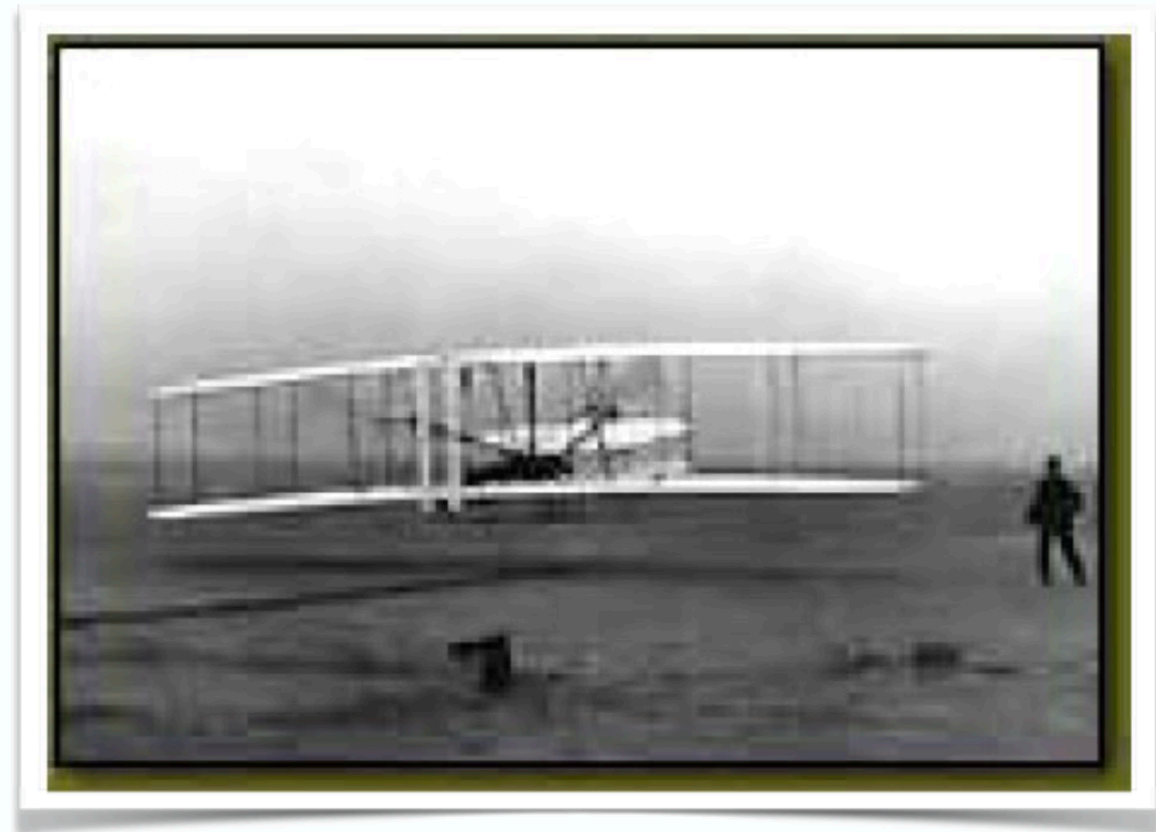


RealTCut

Wilbur and Orville Wright, 1903

Wright Flyer

10:35am Dec 17, 1903

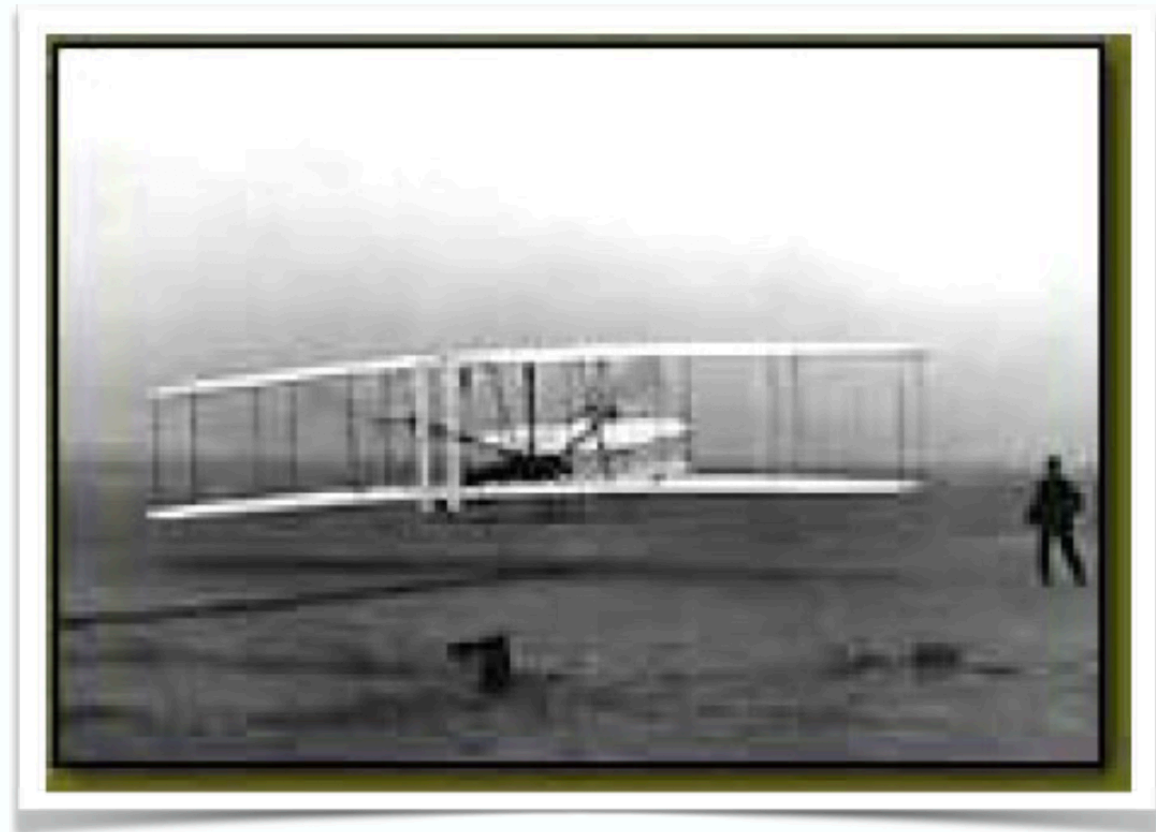


Wilbur and Orville Wright, 1903

On Dec 14 Wilbur won the coin toss, made the first attempt and stalled

Orville made the first flight on Dec. 17

12 seconds & 120 ft



Aircraft safety

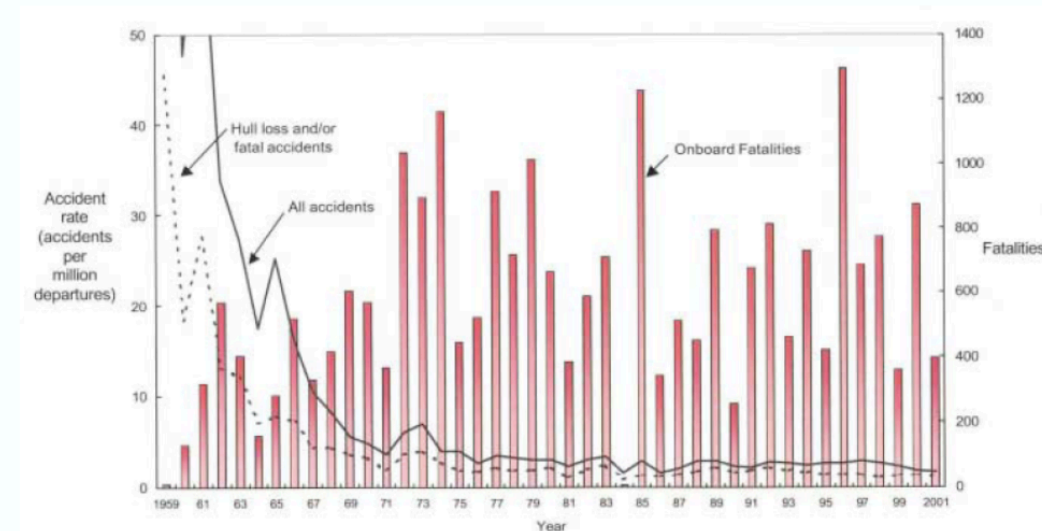
20,000 years



RealTCut

Worldwide statistics

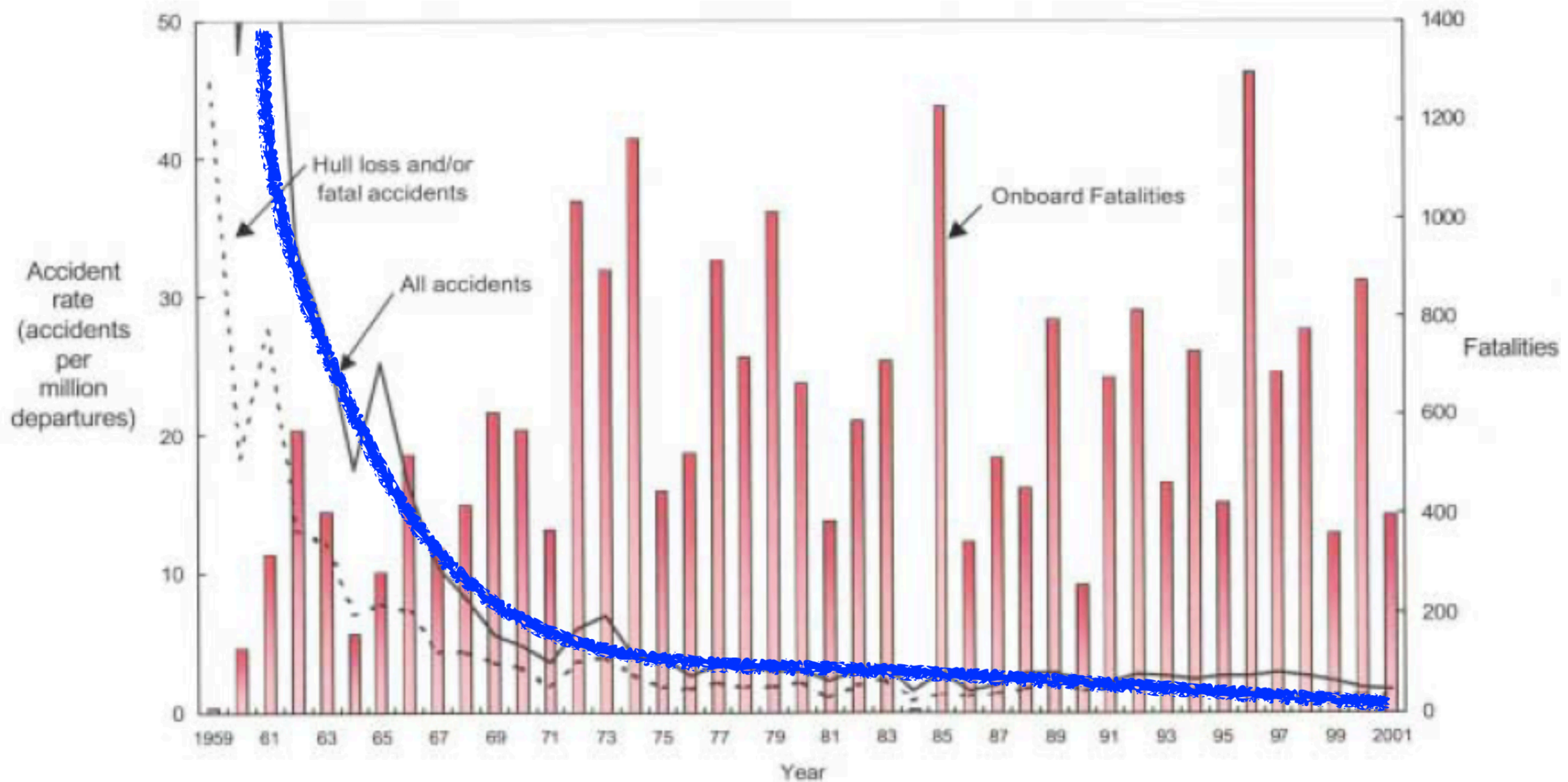
[1959-2001] 1,307
commercial jet aircraft
losses



Today:

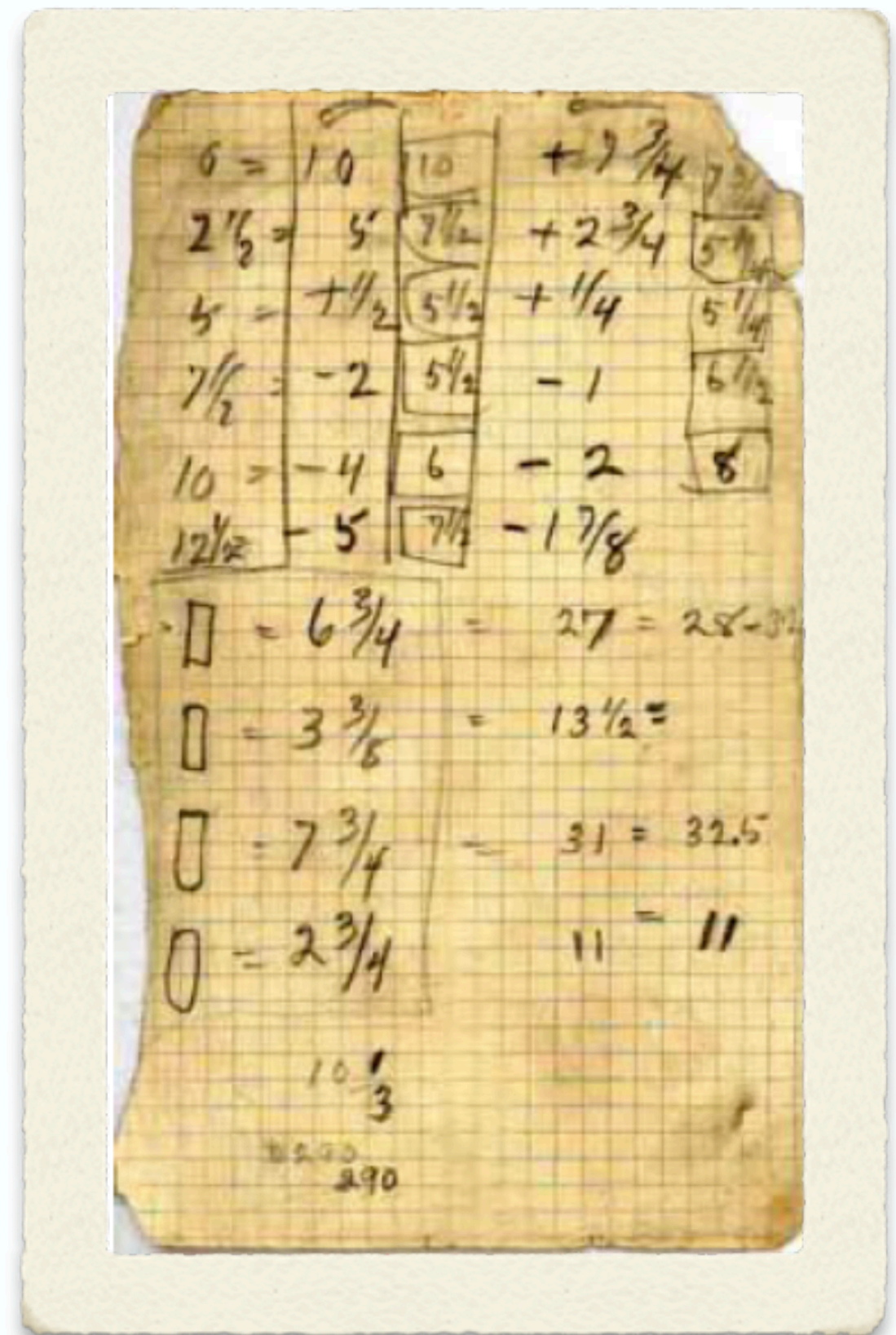
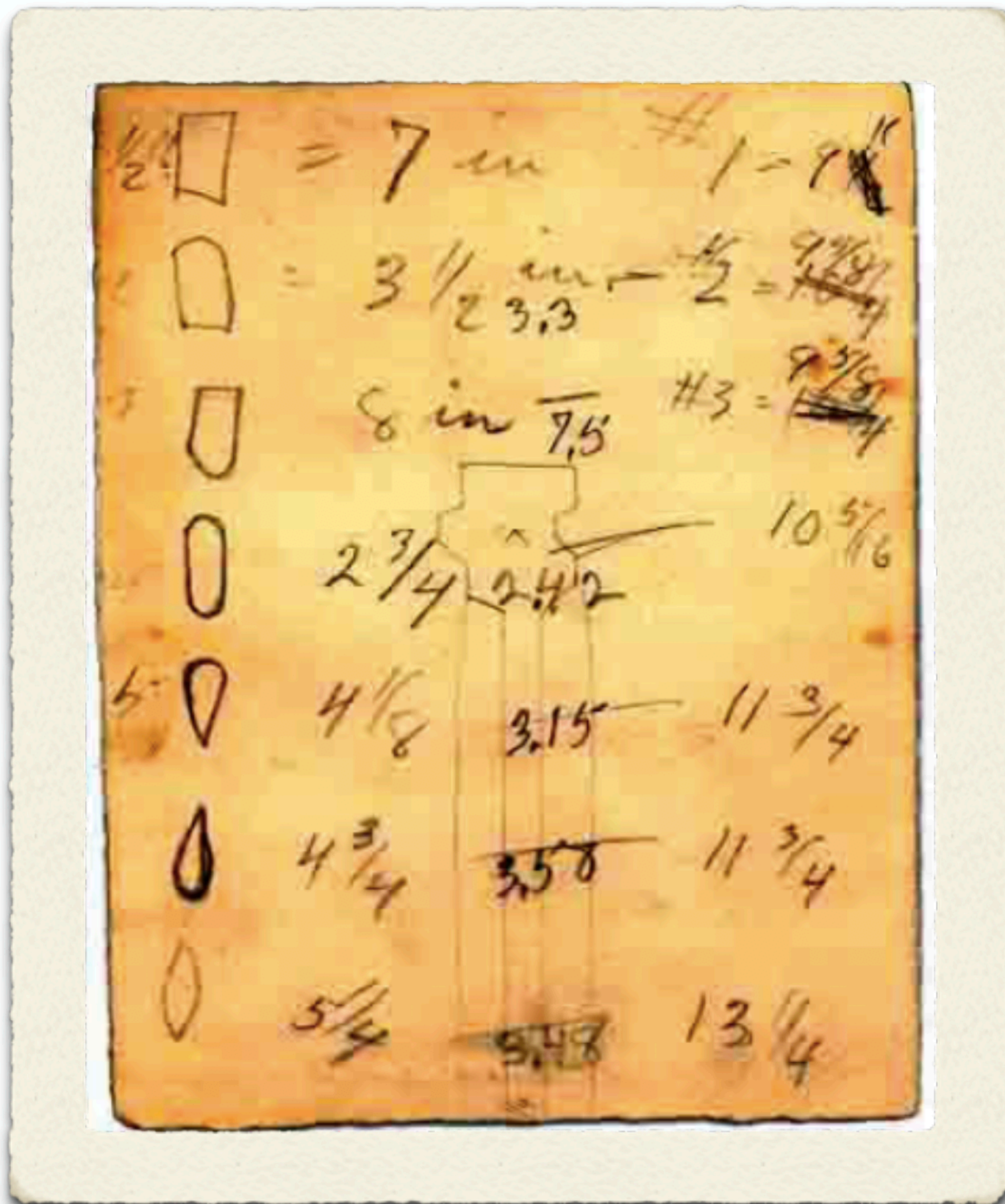
1 accident per
1,000,000
departures

Accident rates and fatalities/year



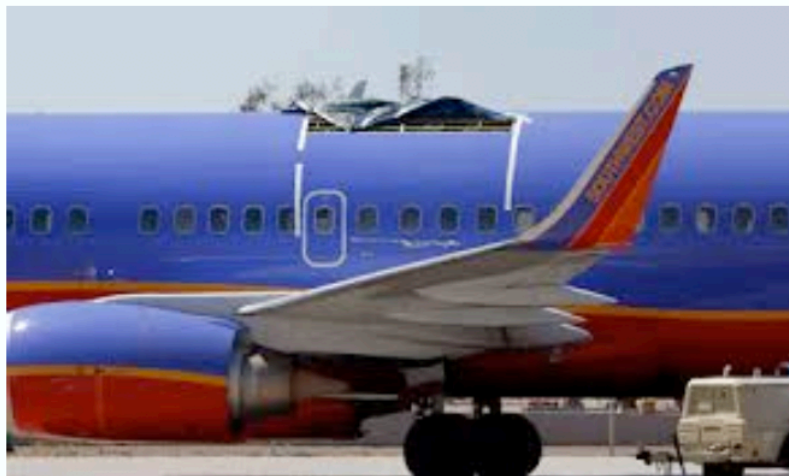
Source: Flight Safety Foundation/Boeing Commercial Airplane Group

Learning from intuition & theory



Learning from experience

Increased practical understanding of mechanics — in particular fracture and fatigue



Aloha airlines accident - fatigue cracks at corners

Novel convertible aircraft

Learning from experiments

World's largest wind tunnel (2014)

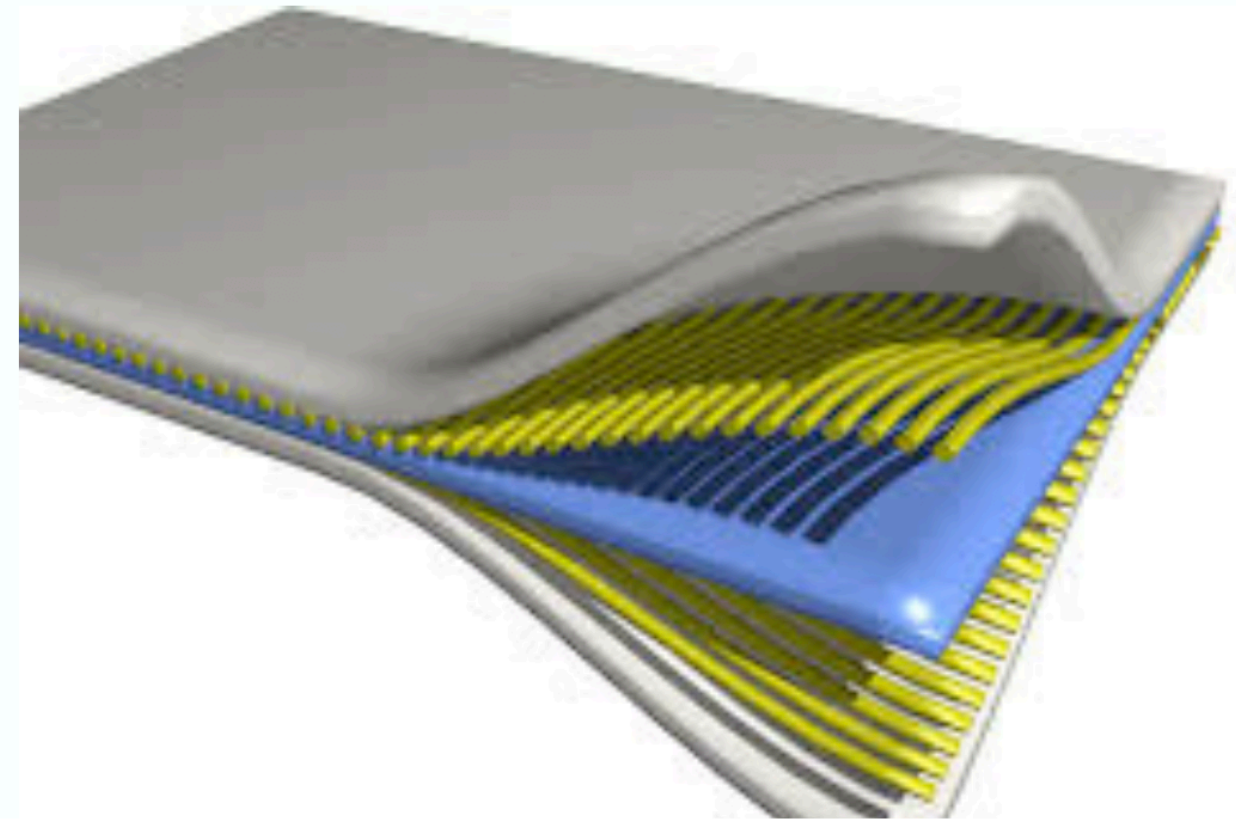


Replica of the 1901 Wright Wind Tunnel
(constructed with assistance from Orville
Wright)

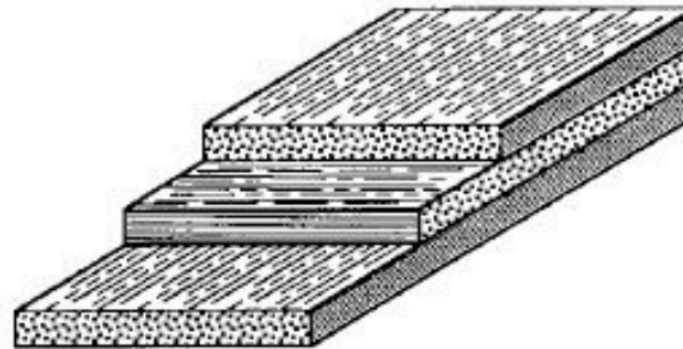
New materials for more payload

Introduction of composite materials have reduced the weight of structures by 20%

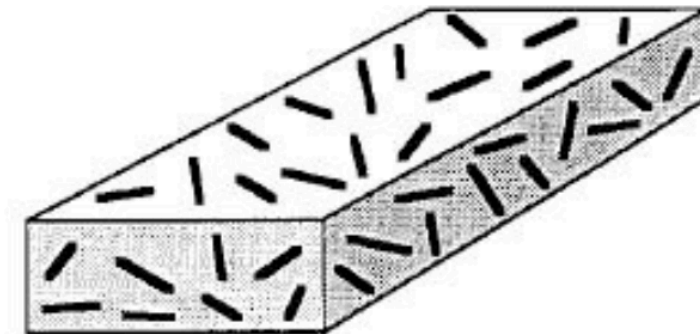
Over 1,000km saving of 8,660kg of fuel
[A340-300]



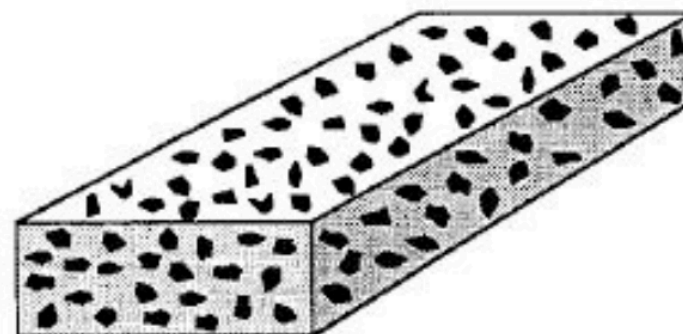
Continuous Fibers



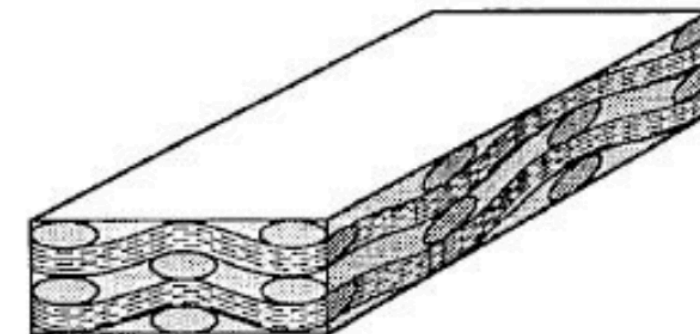
Discontinuous Fibers, Whiskers



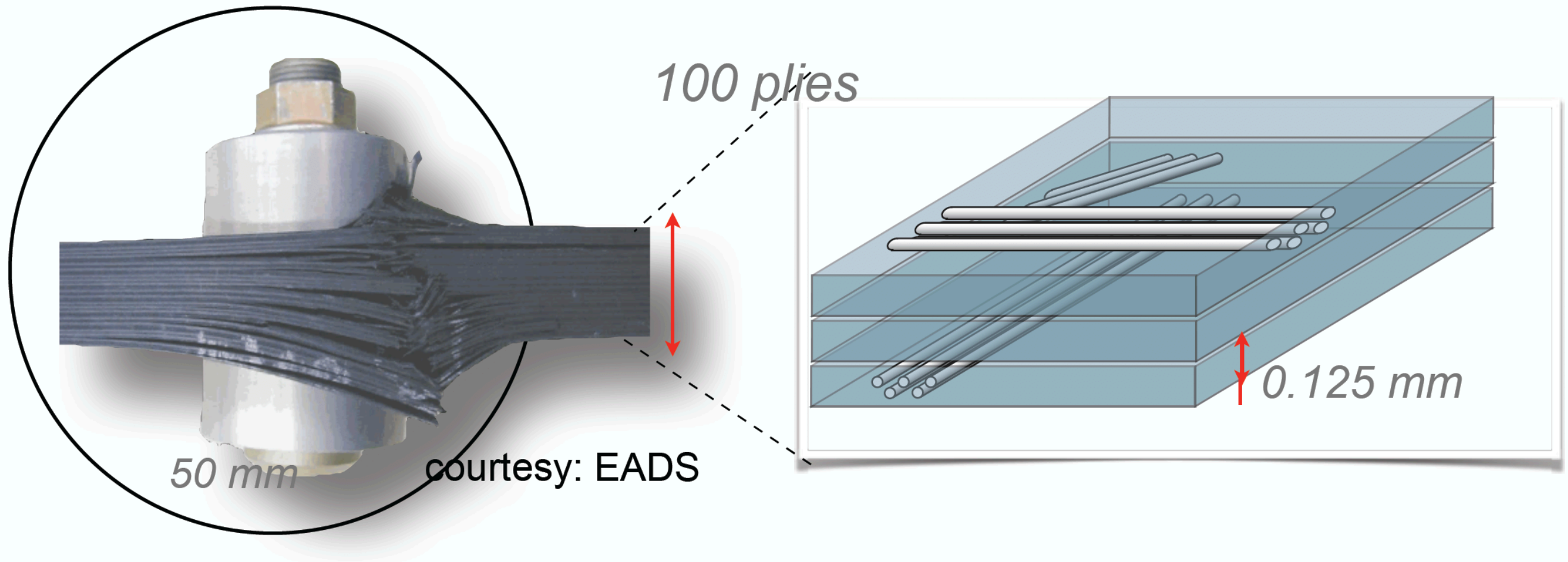
Particles



Fabric, Braid, Etc.



A bolted joint



- 5 elements through the thickness of a ply => 0.025mm/element
- 50mm bolted joint area => 2,000 elements
- 50mm x 50mm x 100 plies => $2,000 \times 2,000 \times (100 \times 5)$
=> **2 billion elements**

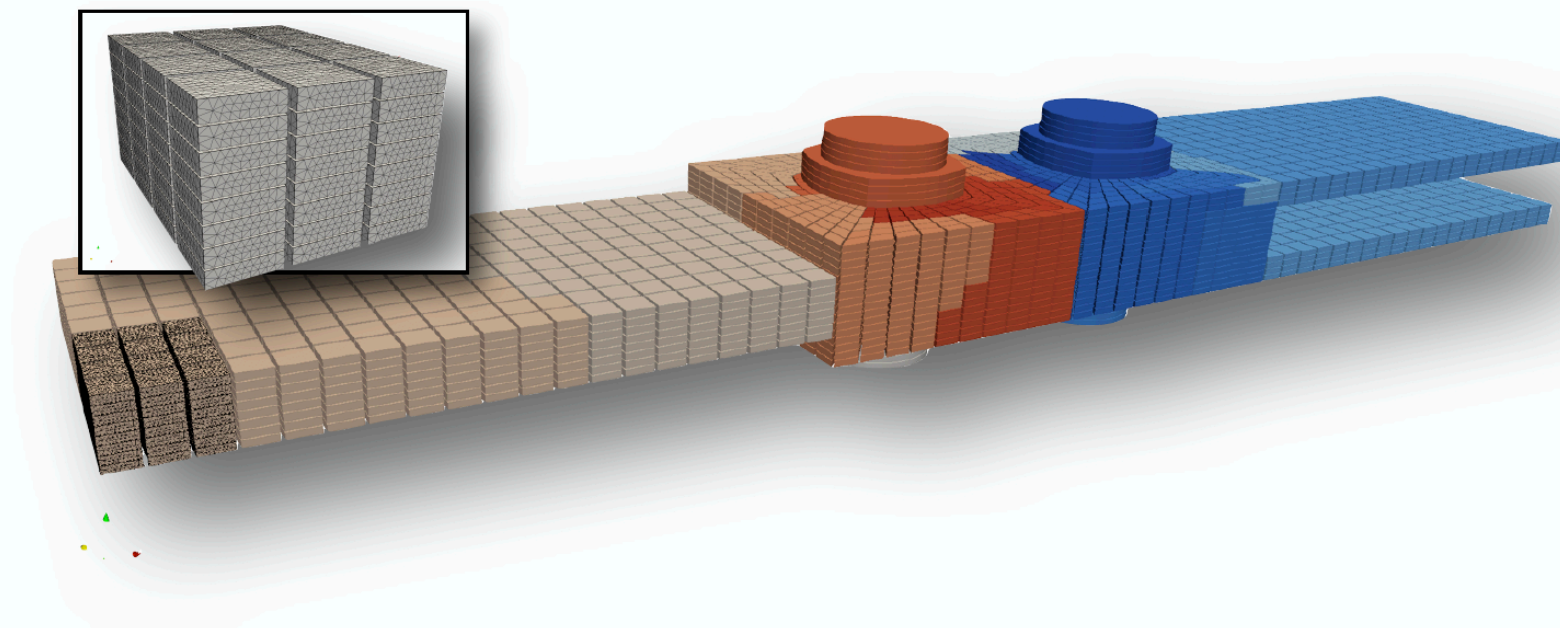
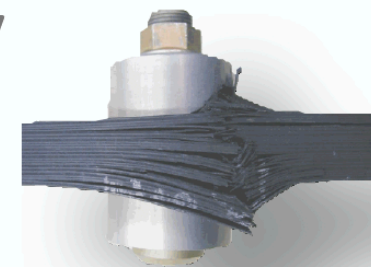
A380 giant



Large structures

whose behaviour is governed by
small-scale effects

=> intractable problem size

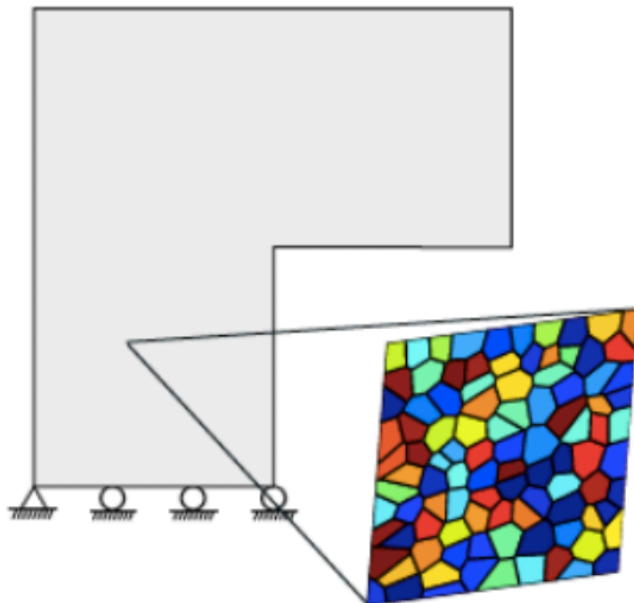


Challenge

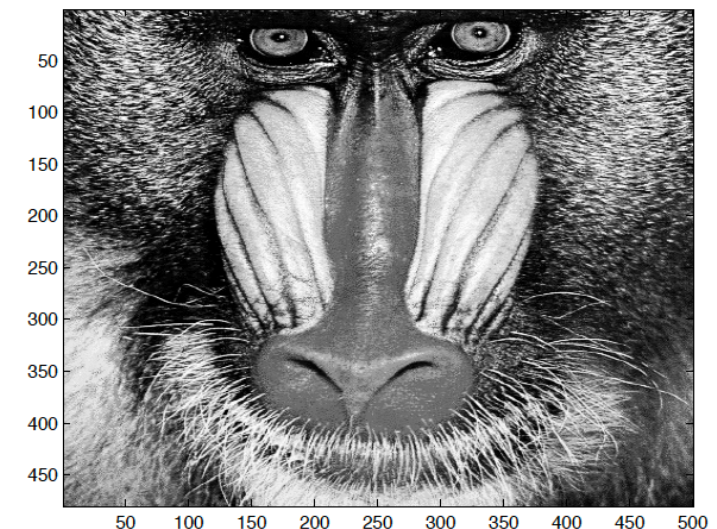
- Reduce the problem size
- Preserve essential features

Reduce computational
expense
Control the error

Physics based model
reduction a.k.a. Multiscale
Methods



Algebraic based model
reduction a.k.a. Machine
Learning



A simple approach to reducing problem size

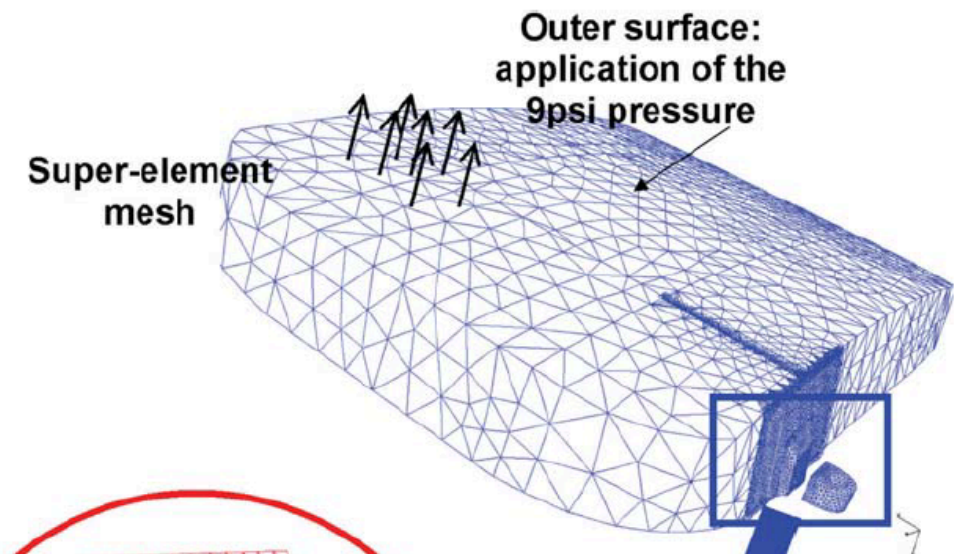
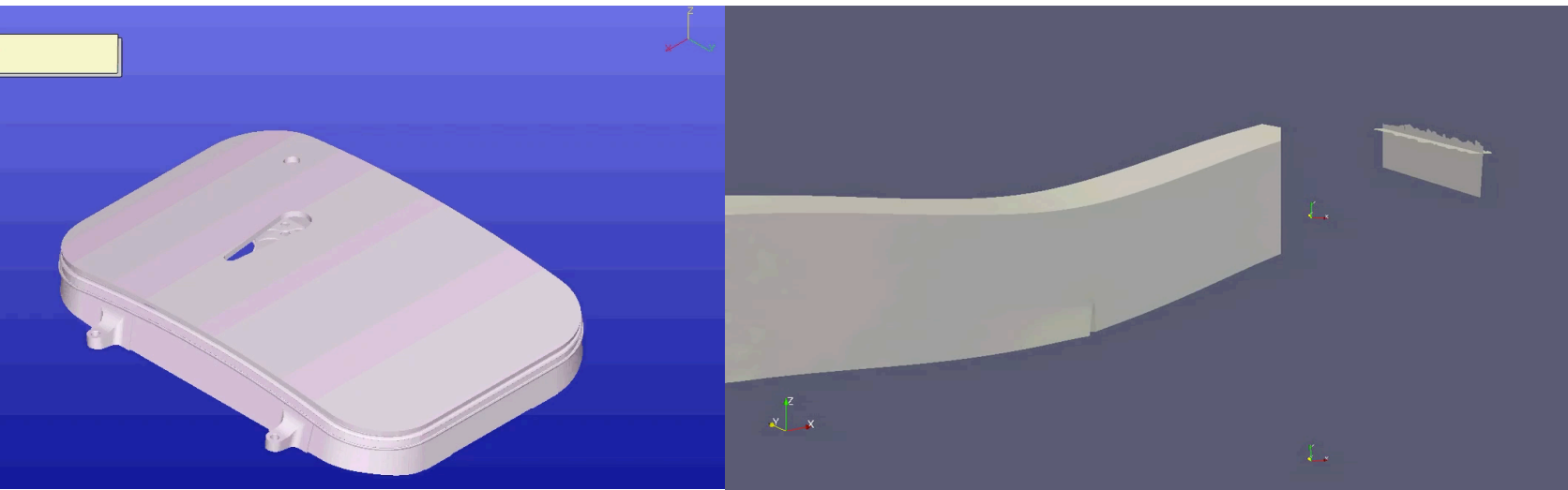
Adaptivity driven by error
estimators



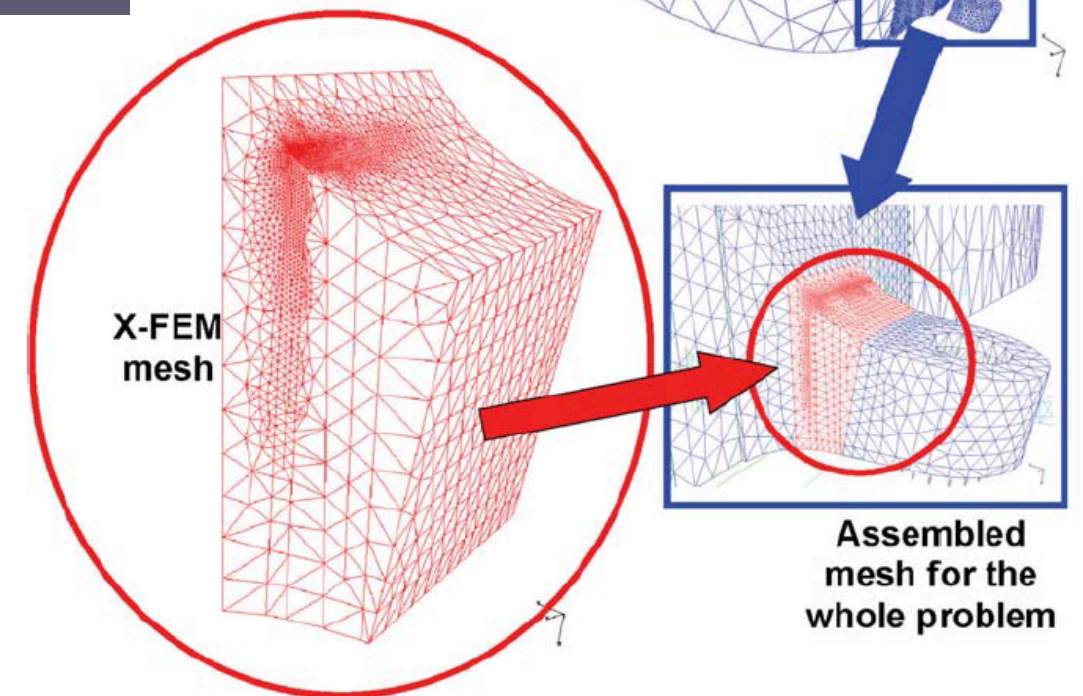
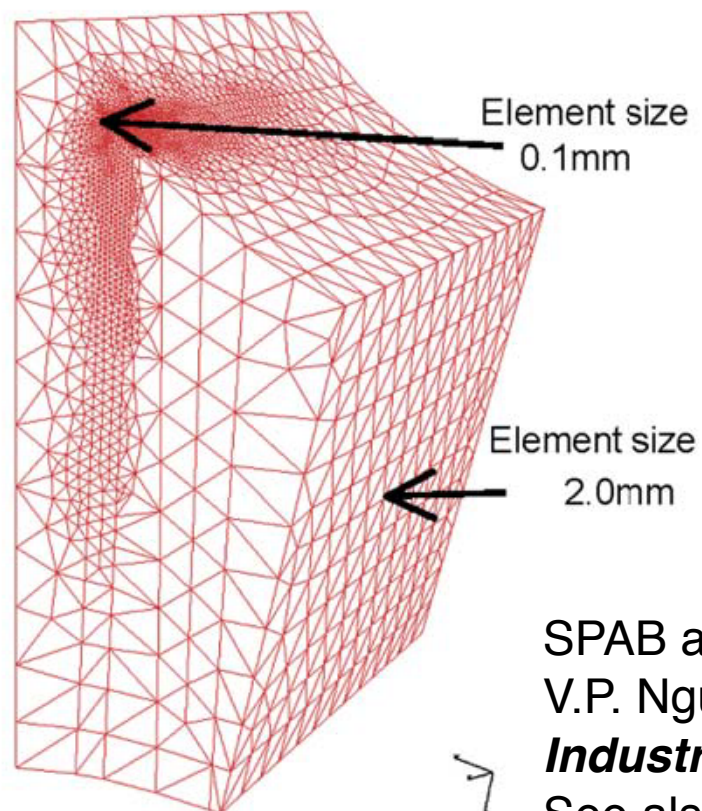
1999-2003 Damage Tolerance Assessment of Aerospace Structures PhD



How often should we inspect a structure for flaws?



ad hoc mesh refinement



SPAB and B. Moran, Engineering Fracture Mechanics, 2006

V.P. Nguyen et al. XFEM C++ Library IJNME, 2007

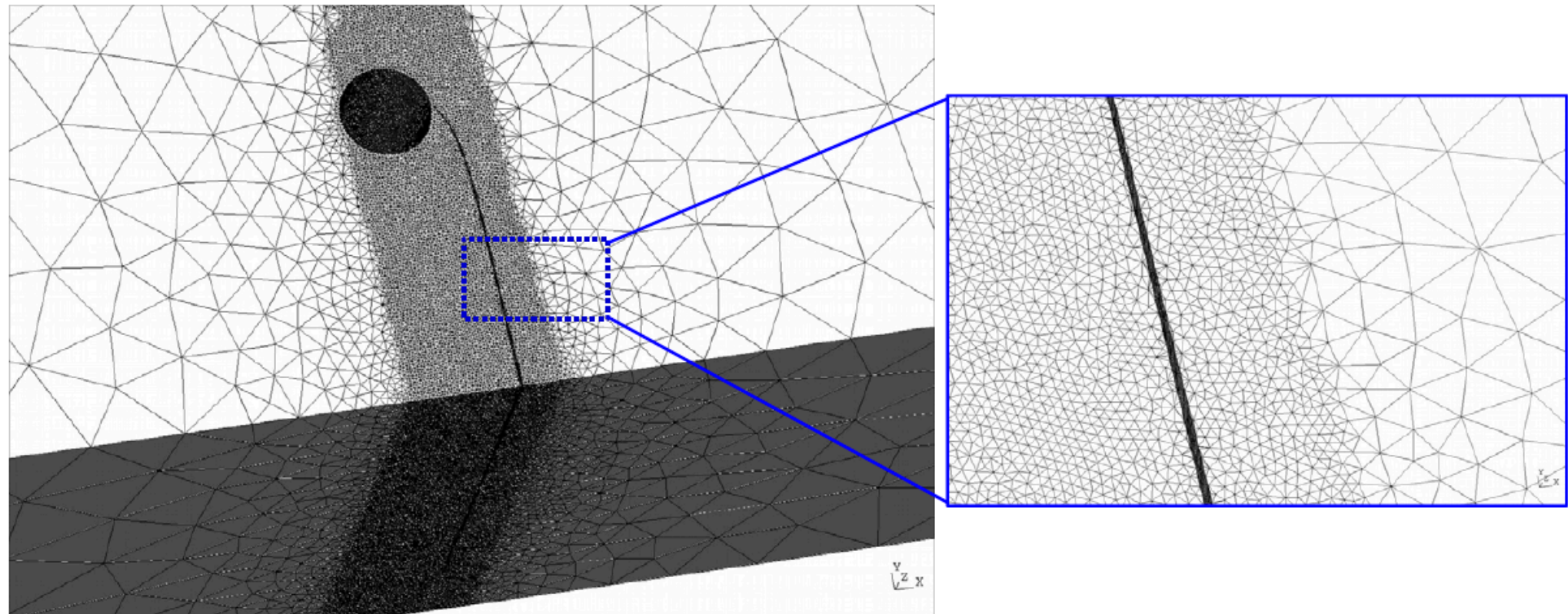
Industrial applications of extended finite element methods

See also E. Wyart et al, EFM, IJNME, 2008



RealTCut

Refine along the “expected” crack path...



Before: mesh “finely” in the region where the crack is “expected” to propagate

Y. Jin, O. Pierard, et al. Comput. Methods Appl. Mech. Engrg. 318 (2017) 319–348

O.A. González-Estrada et al. Computers and Structures 152 (2015) 1–10

O.A. González-Estrada et al. Comput Mech (2014) 53:957–976

C. Prange et al. IJNME 91.13 (2012): 1459-1474.

M. Duflot, SPAB, IJNME 2007, CNME 2007, IJNME 2008.

J-J. Ródenas Garcia, IJNME 2007

F.B. Barros, et al IJNME 60.14 (2004): 2373-2398.

M. Rüter CMECH (2013) 1;52(2):361-76.

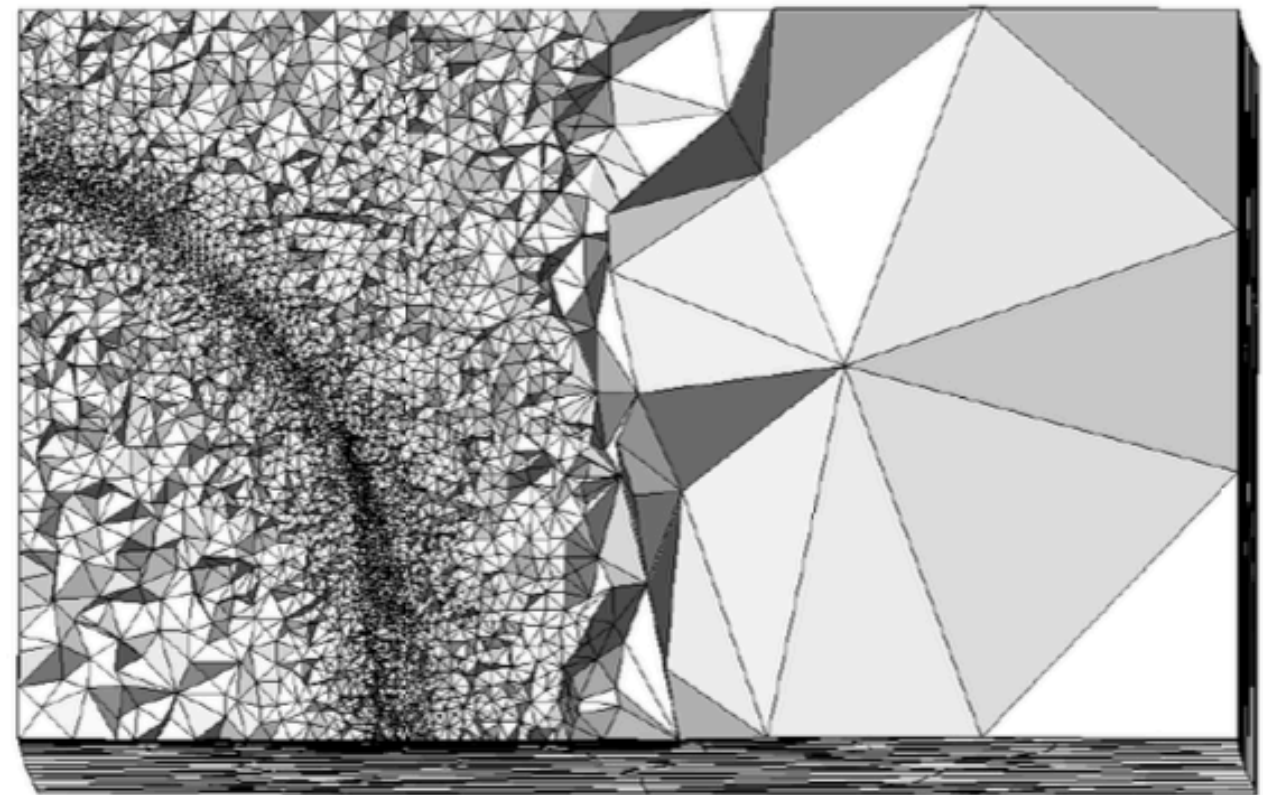
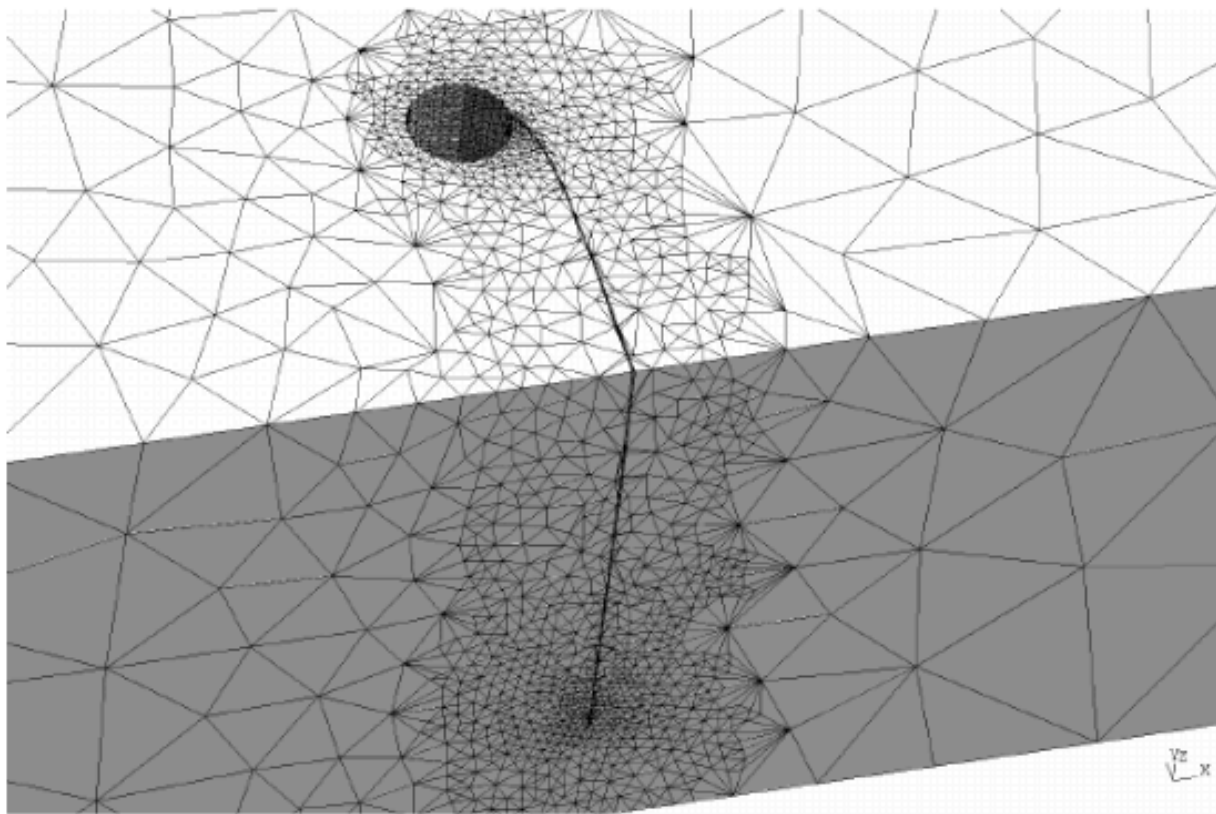
J. Panetier IJNME 81.6 (2010): 671-700.

P. Hild, CMECH (2010): 1-28.



RealTCut

Much better... adapt the discretisation locally



After: determine mesh refinement adaptively using a (goal-oriented) error estimate

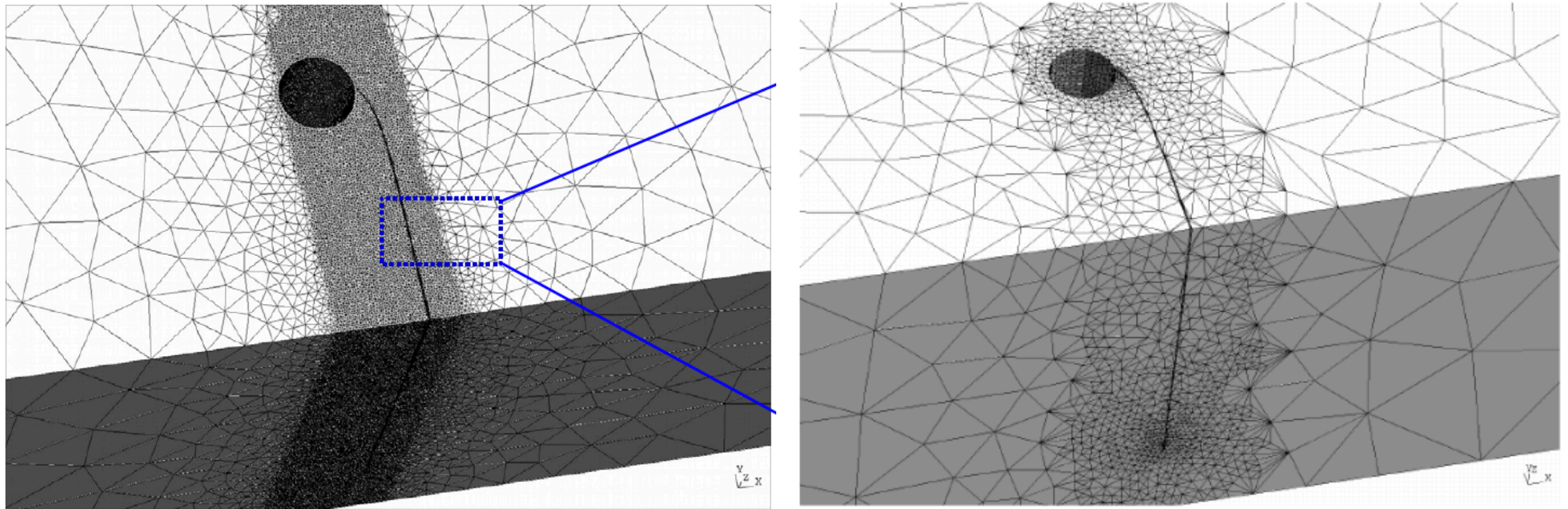
Y. Jin, O. Pierard, et al. Error-controlled adaptive extended finite element method for 3D linear elastic crack propagation Comput. Methods Appl. Mech. Engrg. 318 (2017) 319–348

M. Duflot, SPAB, IJNME 2007, CNME 2007, IJNME 2008.



RealTCut

Much better... adapt the discretisation locally



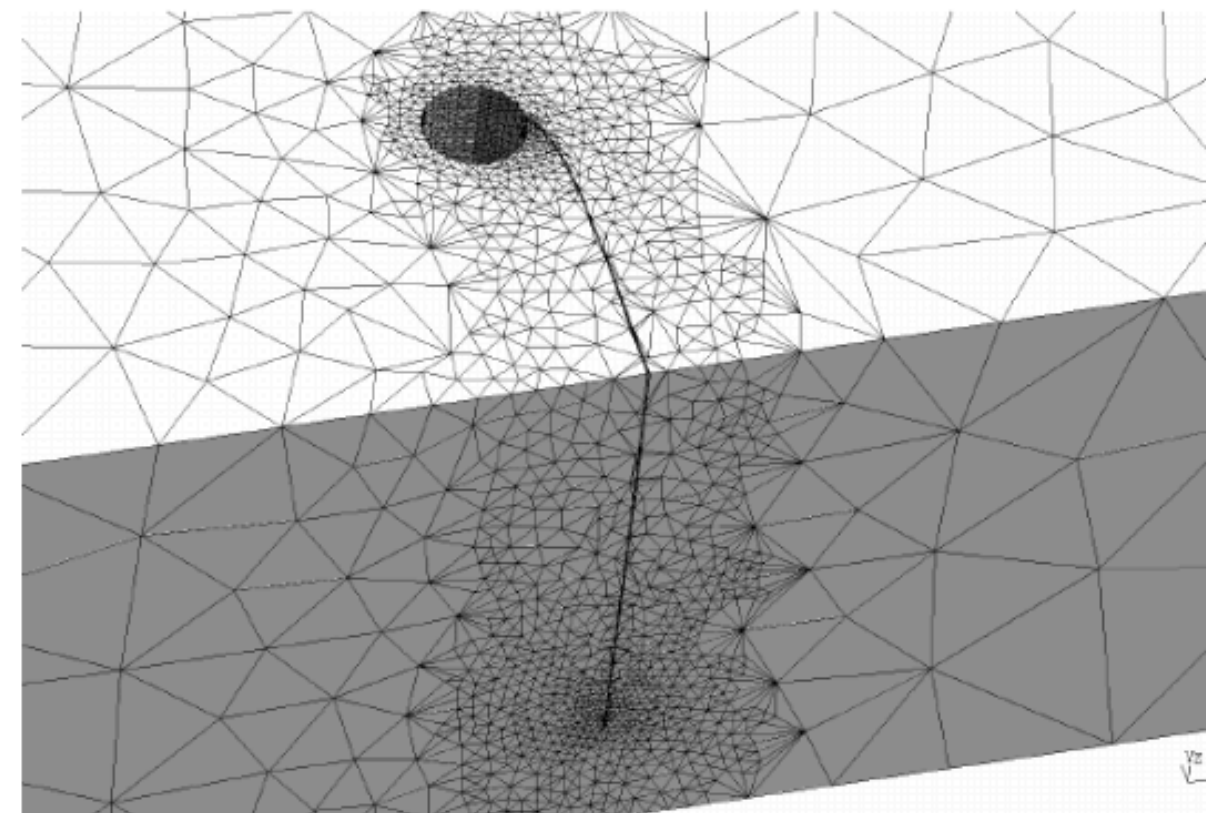
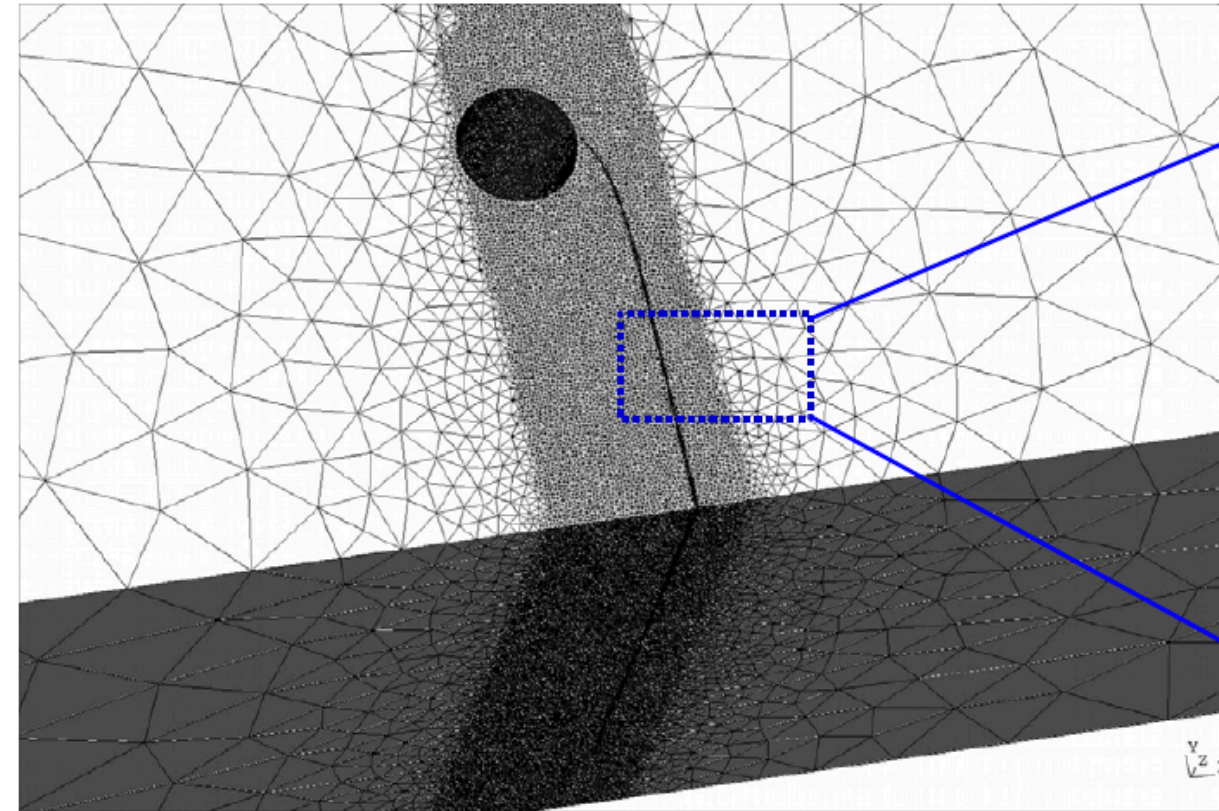
Orders of magnitude fewer elements

Y. Jin, O. Pierard, et al. Error-controlled adaptive extended finite element method for 3D linear elastic crack propagation Comput. Methods Appl. Mech. Engrg. 318 (2017) 319–348
M. Duflot, SPAB, IJNME 2007, CNME 2007, IJNME 2008.



TAKE HOME MESSAGE

UNIFORM MESH
REFINEMENT IS NOT AN
OPTION



LIMITATIONS

No material is
homogeneous... nor linear
elastic...

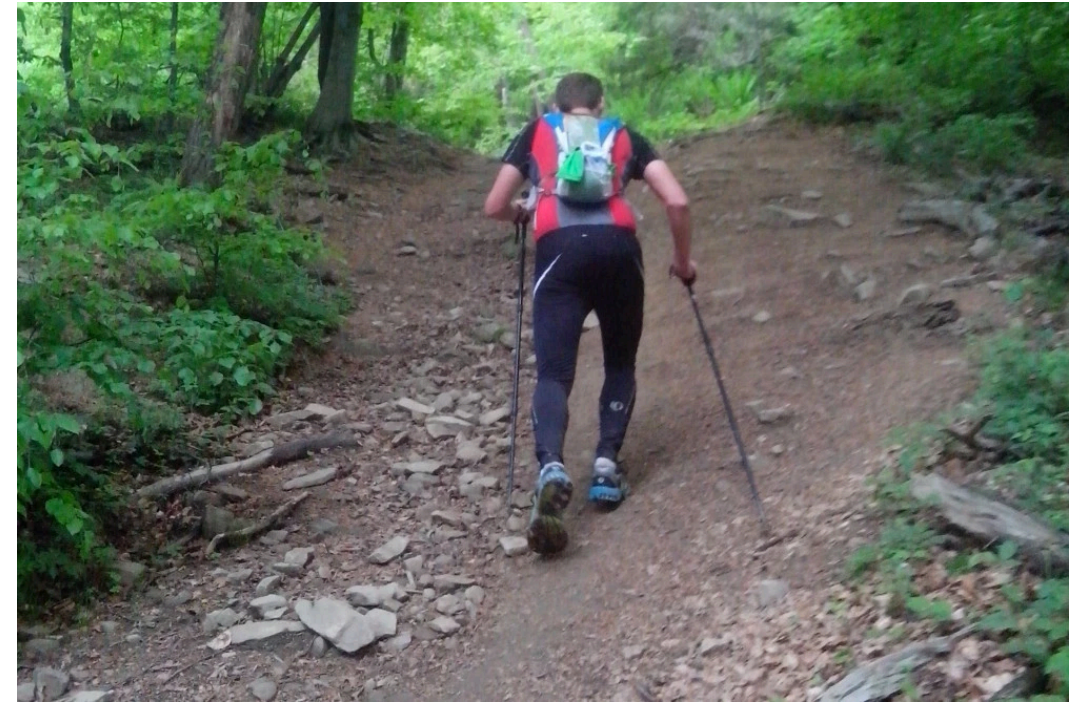
Multi-scale methods...



From your first love to the ERC



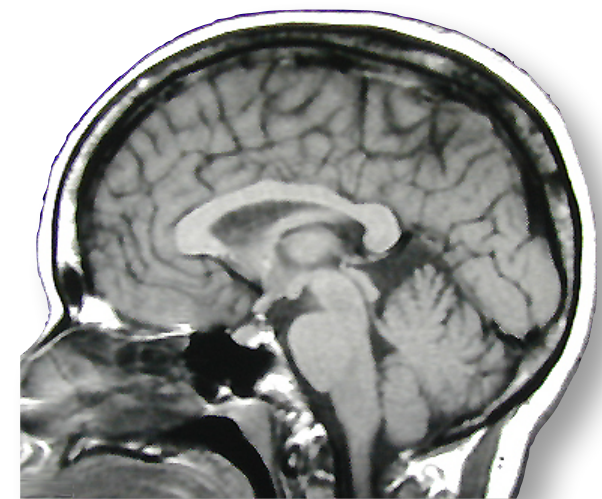
hiking - 20km D+500m



ultra-marathon 52km D+2500m



aerospace

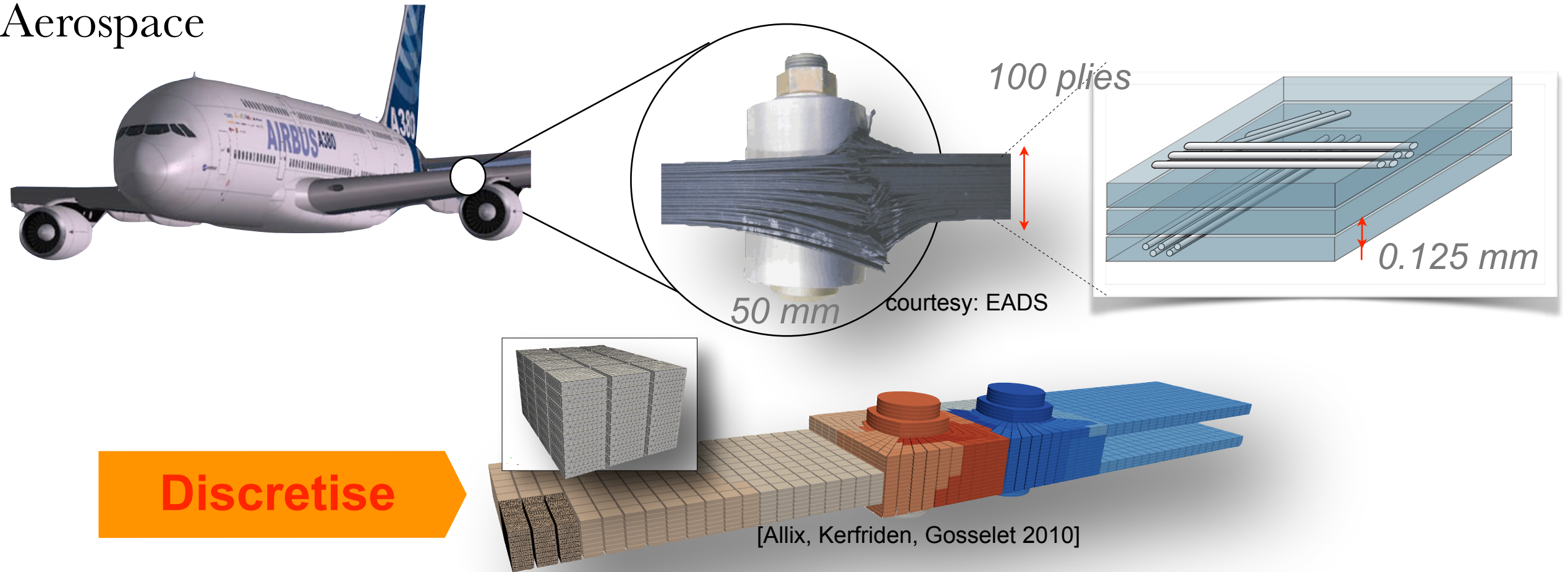


biomechanics



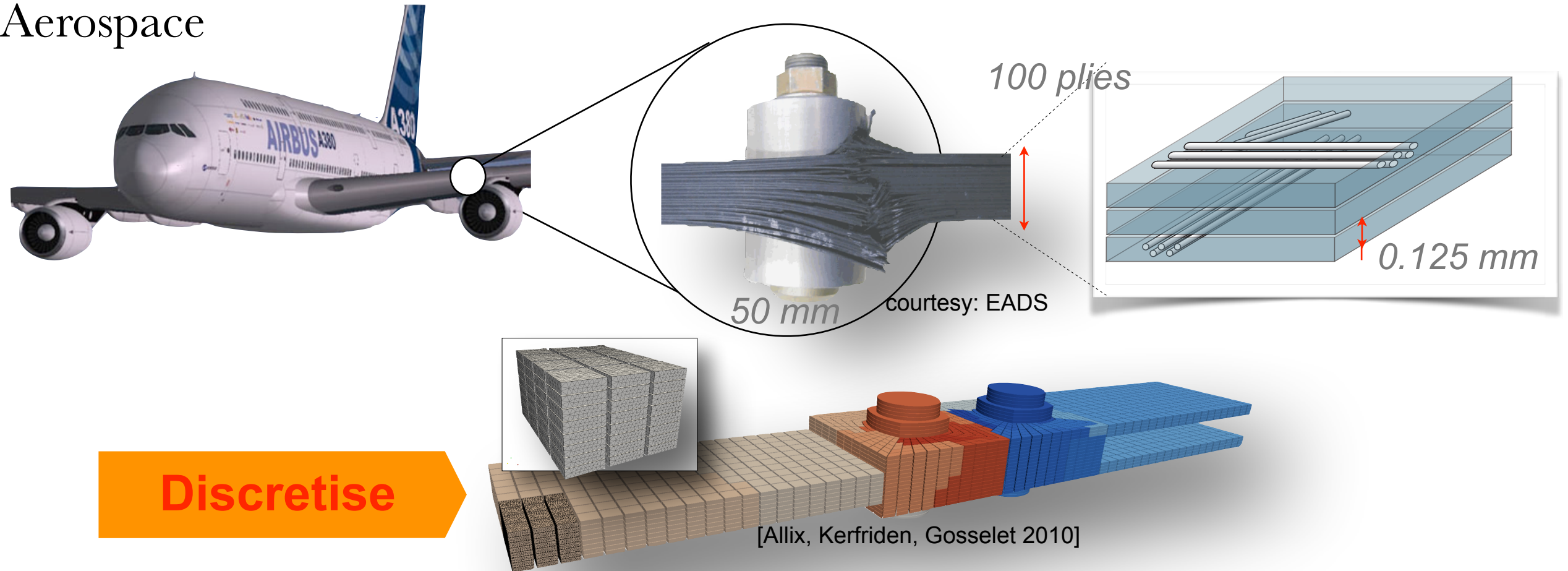
Motivation: multiscale fracture of engineering structures and materials

Aerospace

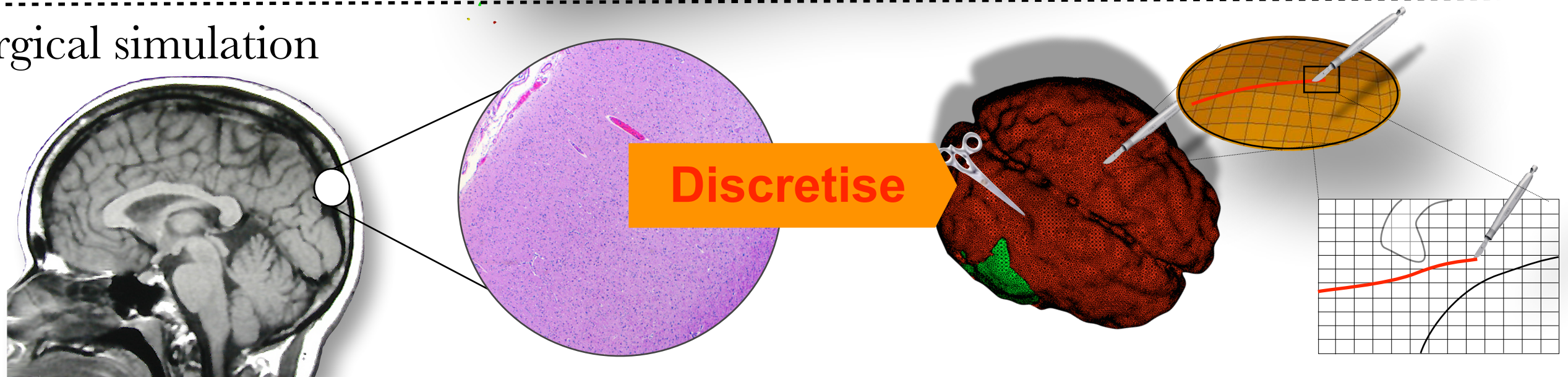


Motivation: multiscale fracture of engineering structures and materials

Aerospace

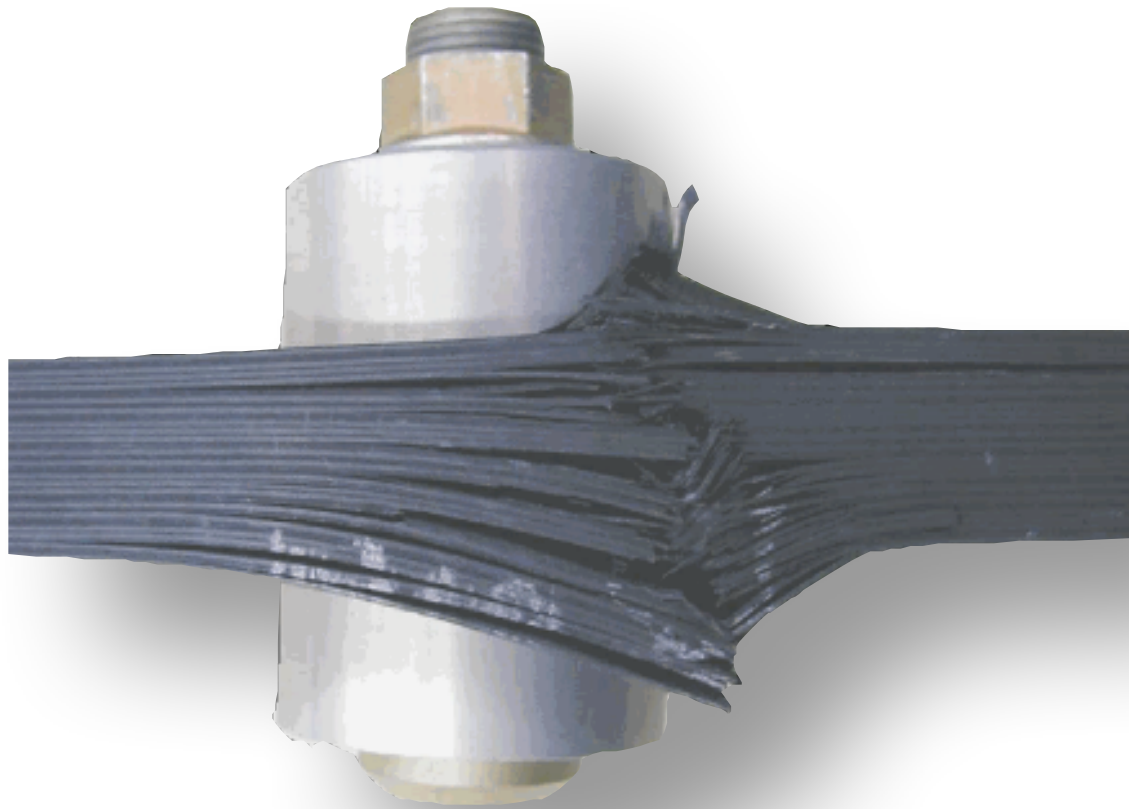


Surgical simulation

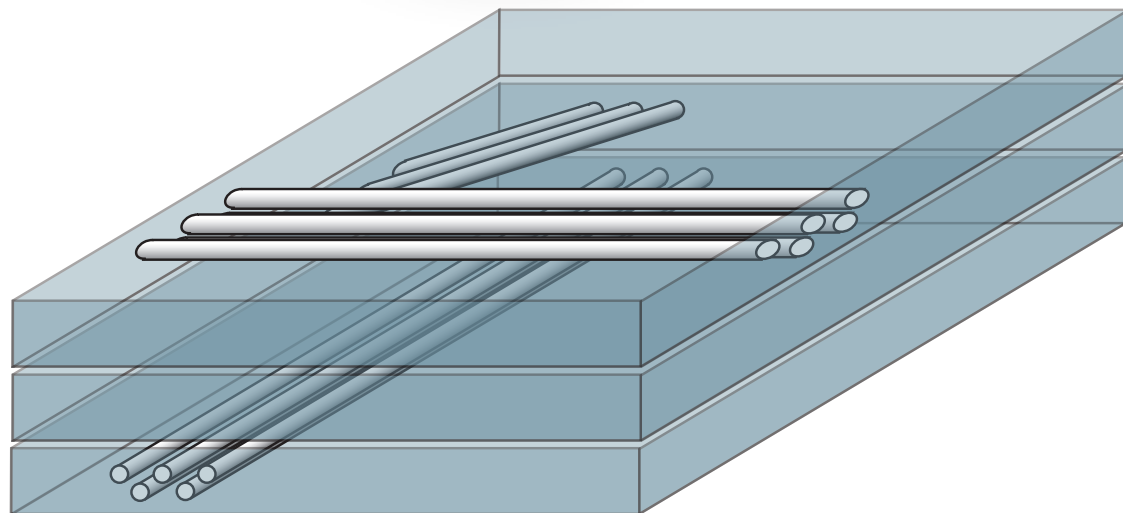


► Reduce the problem size while controlling the quality for problems involving (free) interfaces

Aero

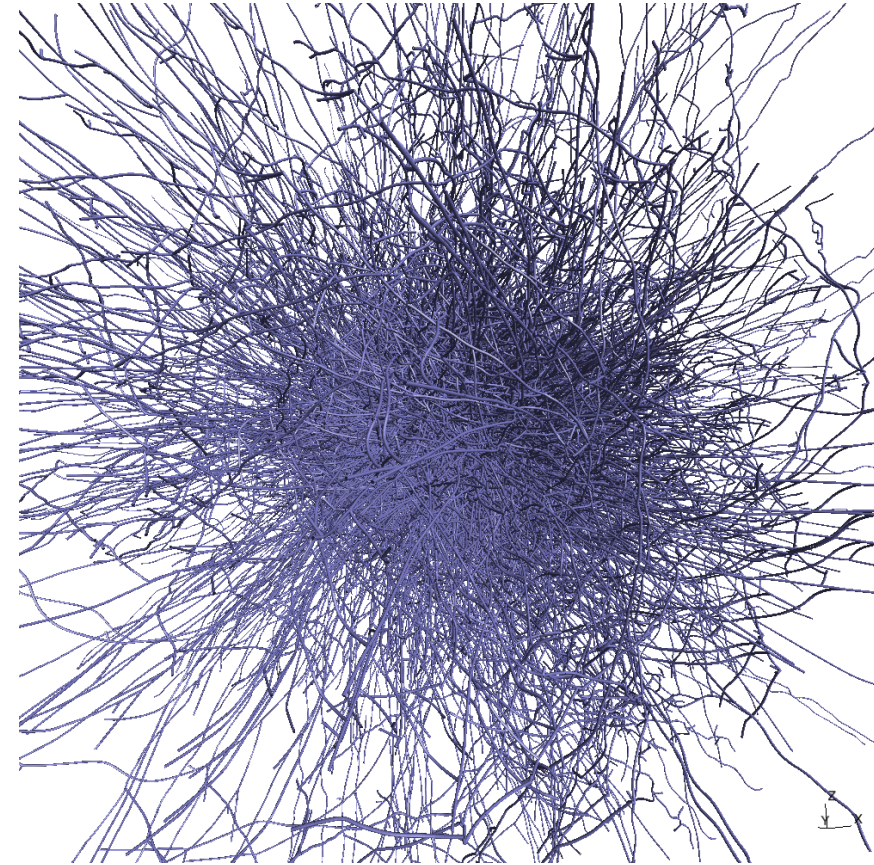


Bolted joint Courtesy EADS

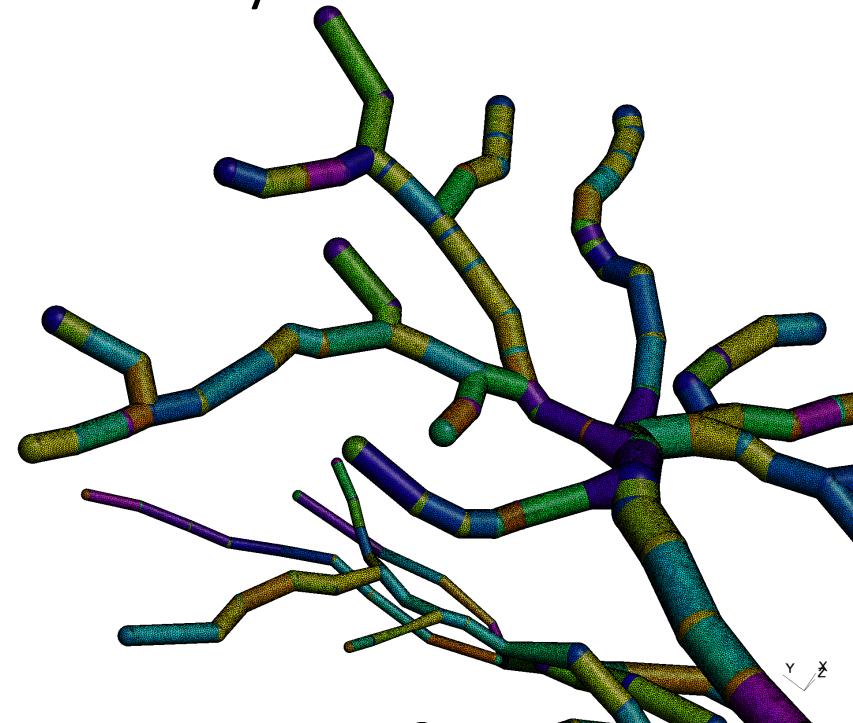


Multi-scale fibre lay-up Courtesy EADS

Bio



Courtesy JF Remacle Gmsh



Courtesy JF Remacle Gmsh



ms

sec

min

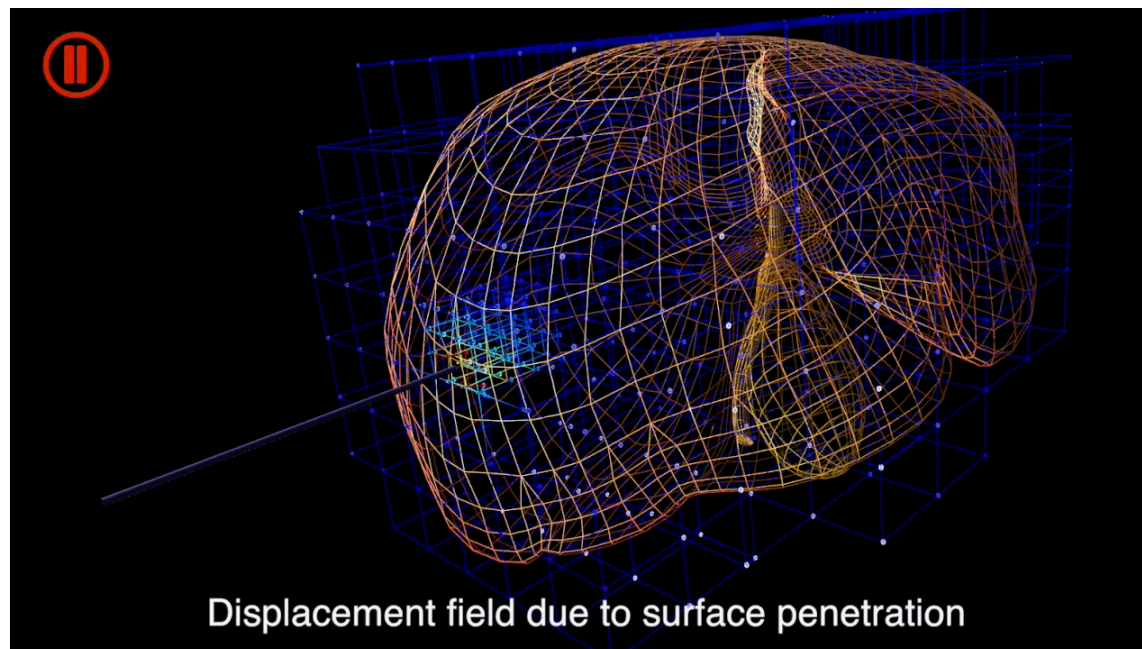
Speed

min

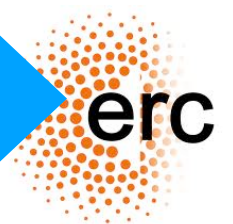
hours

days

Surgical
guidance

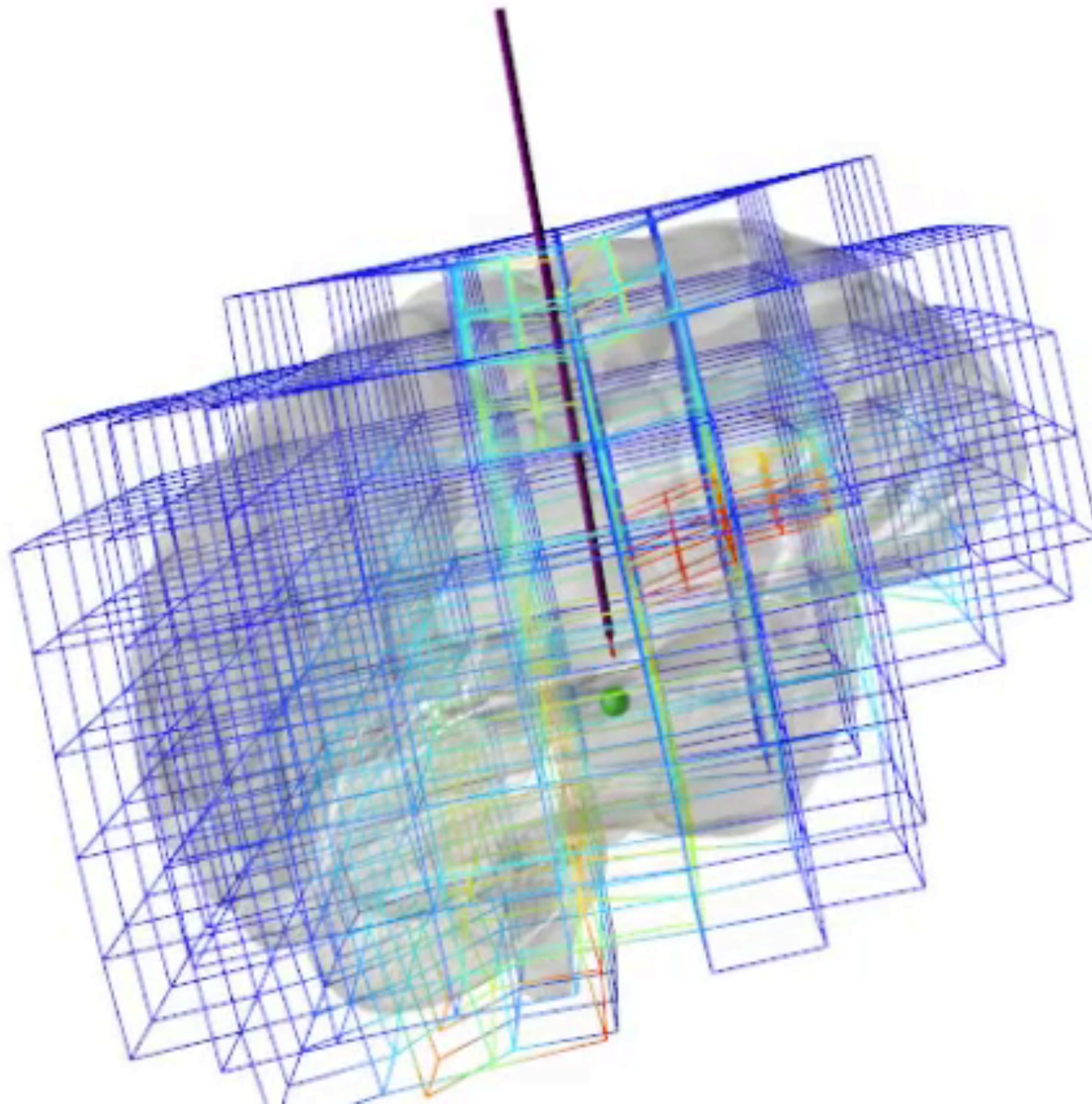


User Expertise & Accuracy of the Simulation

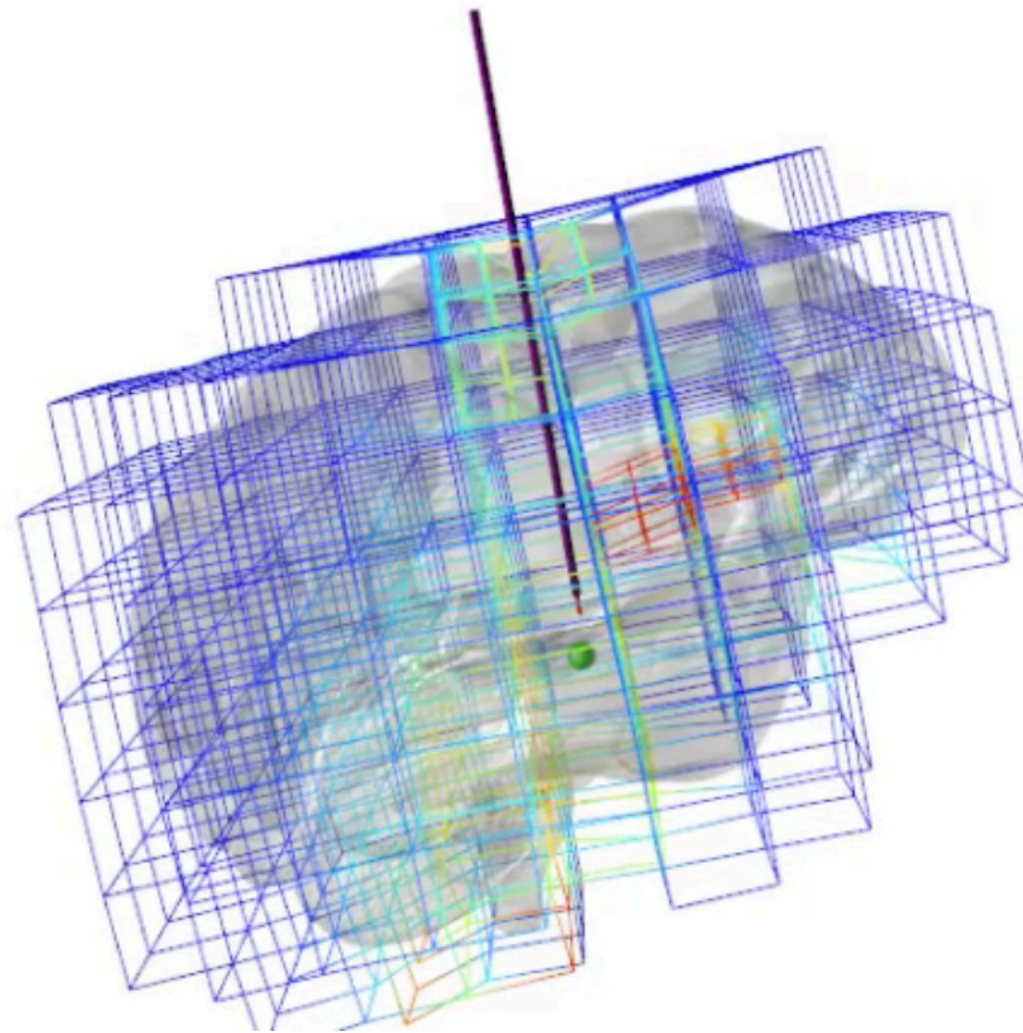


RealTCut

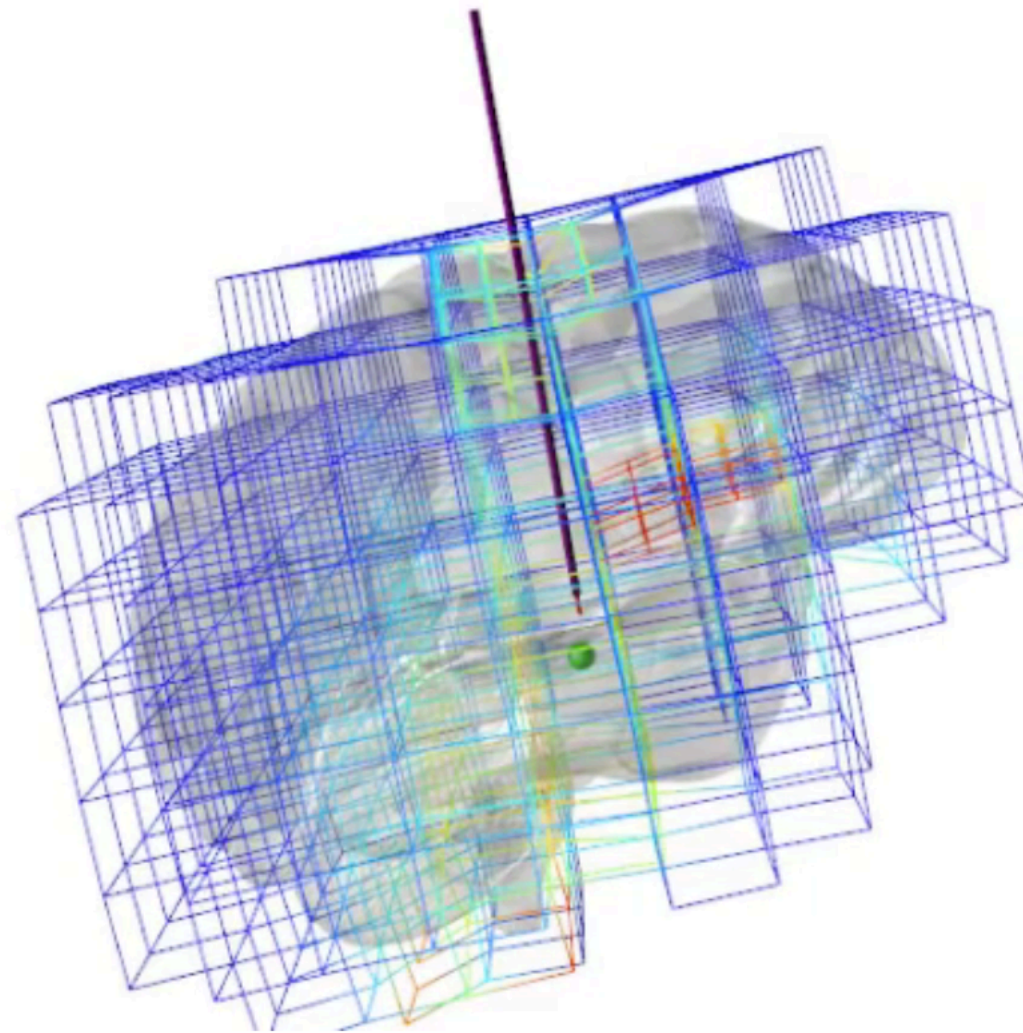
Cannula insertion



**CHALLENGE: everything happens
close to the needle... focus the
computational expense**



CHALLENGE: everything happens close to the needle... focus the computational expense



But HOW can we decide where and what the element size should be?



QUESTIONS

Local mesh refinement is necessary, but where?
how?

We do not know the exact solution. How can we
find out where the mesh should be refined?

Engineers are interested in specific quantities of
interest, not in the “energy” norm, which is what
mathematics uses most naturally.

What else is missing?



Model of contractile tissue

$$\min_{\mathbf{u} \in \mathbf{V}} \frac{1}{2} \int_{\Omega} \boldsymbol{\sigma}(\mathbf{u}, \beta) : \boldsymbol{\varepsilon}(\mathbf{u}) \, d\mathbf{x} - \int_{\Omega} \mathbf{g} \cdot \mathbf{u} \, d\mathbf{x}$$

with

$$\boldsymbol{\sigma}(\mathbf{u}, \beta) = \underbrace{\boldsymbol{\sigma}_P(\mathbf{u})}_{\substack{\text{passive} \\ \text{material}}} + \underbrace{\boldsymbol{\sigma}_A(\beta)}_{\substack{\text{muscular} \\ \text{activation}}} \left\{ \begin{array}{l} \boldsymbol{\sigma}_A(\beta) = \beta T e_A \otimes e_A \\ e_A : \text{fiber direction} \\ T : \text{tension} \\ \beta : \text{activation} \end{array} \right.$$

where

Cowin & Humphrey 2001

Payan & Ohayon 2017

Biomechanics of Living Organs : Hyperelastic Constitutive Laws for Finite Element Modeling.



a posteriori error estimates

$$\mathbf{u} \in \mathbf{V} : a(\mathbf{u}, \mathbf{v}) = l(\beta, \mathbf{v}) \quad \forall \mathbf{v} \in \mathbf{V}$$

$$a(\mathbf{u}, \mathbf{v}) = \int_{\Omega} \boldsymbol{\sigma}_P(\mathbf{u}) : \boldsymbol{\varepsilon}(\mathbf{v}) \, d\mathbf{x} \quad l(\beta, \mathbf{v}) = \int_{\Omega} \boldsymbol{\sigma}_A(\beta) : \boldsymbol{\varepsilon}(\mathbf{v}) \, d\mathbf{x} + \int_{\Omega} \mathbf{g} \cdot \mathbf{v} \, d\mathbf{x}$$

Prediction of a **quantity of interest** (e.g., local strain or stress) :

$$J : \mathbf{V} \ni \mathbf{u} \mapsto J(\mathbf{u}) \in \mathbb{R}.$$

(Goal-oriented) discretization error : $|J(\mathbf{u}) - J(\mathbf{u}_h)|$?

Exact solution : $\mathbf{u} \in \mathbf{V}$

MEF approximation : $\mathbf{u}_h \in \mathbf{V}_h$

Dual Weighted Residuals (DWR)

$$J(\mathbf{u}) - J(\mathbf{u}_h) = a(\mathbf{u}, \mathbf{z}) - a(\mathbf{u}_h, \mathbf{z}) = \underbrace{l(\mathbf{z}) - a(\mathbf{u}_h, \mathbf{z})}_{\text{residual}} =: \eta_h(\mathbf{z})$$

where $\mathbf{z} \in \mathbf{V}$ s.t. $a(\mathbf{v}, \mathbf{z}) = J(\mathbf{v}) \quad \forall \mathbf{v} \in \mathbf{V}$ (dual problem)

➡ **global estimator** : η_h

Local representation

$$\begin{aligned} J(\mathbf{u}) - J(\mathbf{u}_h) &= \sum_{K \in \mathcal{K}_h} \langle R_K, \mathbf{z} - \pi_h \mathbf{z} \rangle_K + \langle R_{\partial K}, \mathbf{z} - \pi_h \mathbf{z} \rangle_{\partial K} \\ &=: \sum_{K \in \mathcal{K}_h} \eta_K(\mathbf{z} - \pi_h \mathbf{z}) \quad \text{local estimator} \end{aligned}$$

$\pi_h \mathbf{z}$: interpolant of dual solution

R_K / $R_{\partial K}$: residual contributions on K / ∂K

➡ **local estimators** : η_K

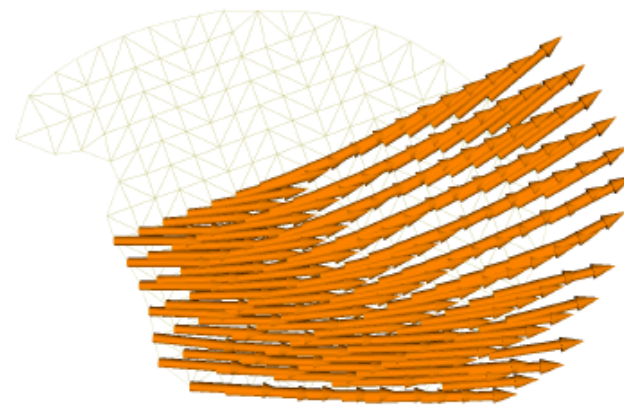
Becker & Rannacher 1997, 2001

Rognes & Logg 2013 (FEniCS)

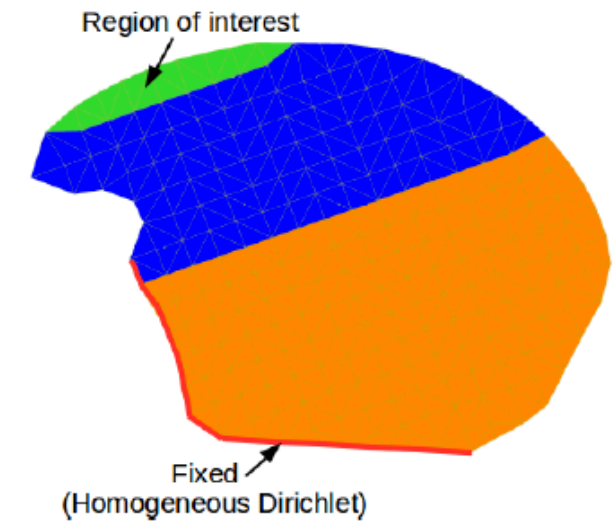
Genioglossus activation



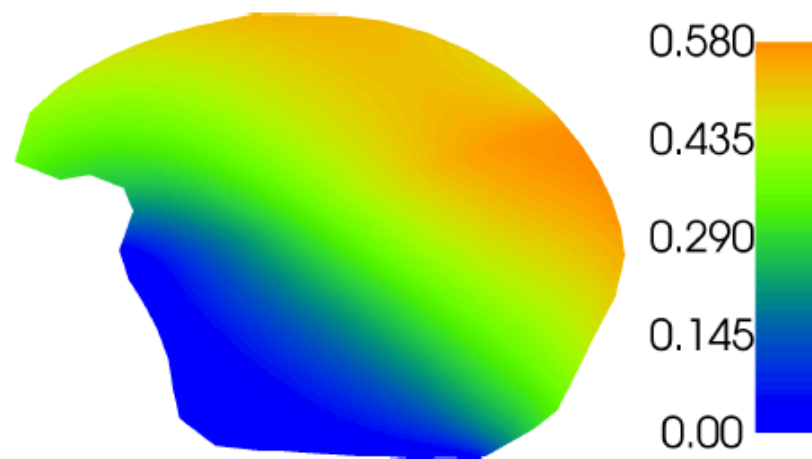
Bijar, Rohan, Perrier &
Payan 2015



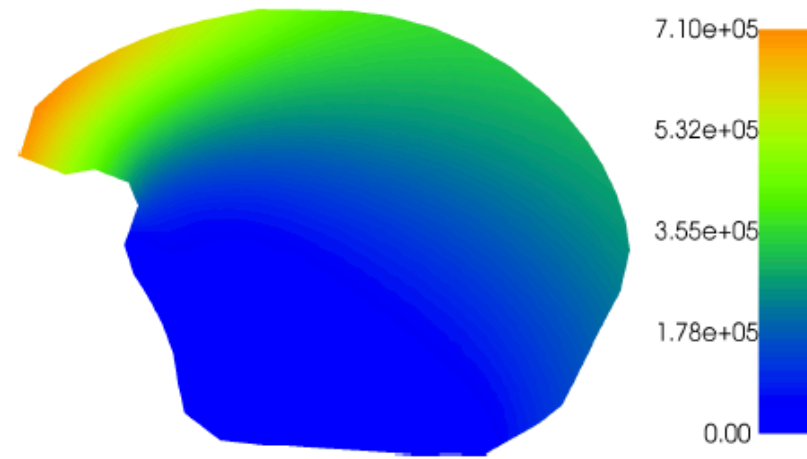
fibers
(genioglossus)



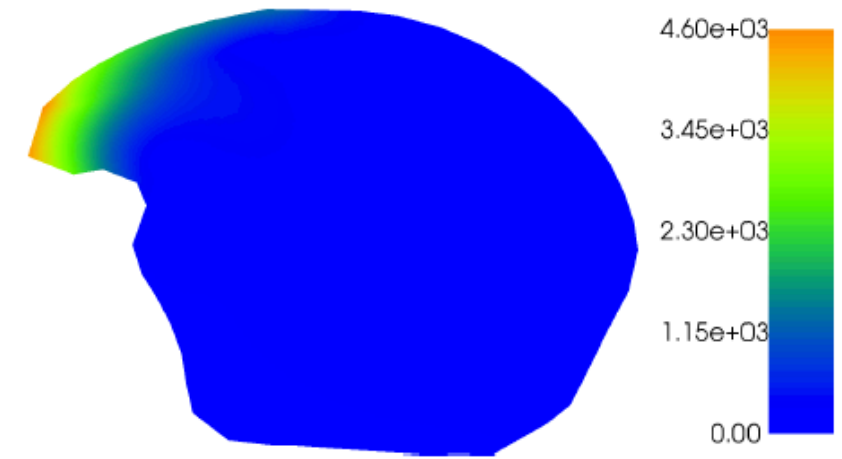
region of interest ω (green)



$\mathbf{u}$



$\mathbf{z} / J_1$



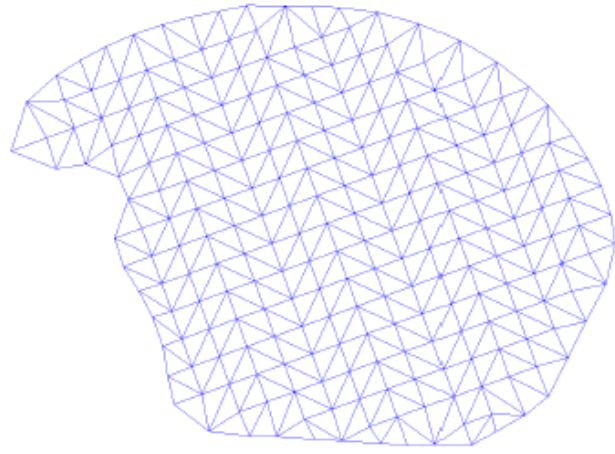
$\mathbf{z} / J_2$

$$J_1(\mathbf{u}) := \int_{\omega} (u_x + u_y) d\mathbf{x}$$

$$J_2(\mathbf{u}) := \int_{\omega} \operatorname{div} \mathbf{u} d\mathbf{x}$$

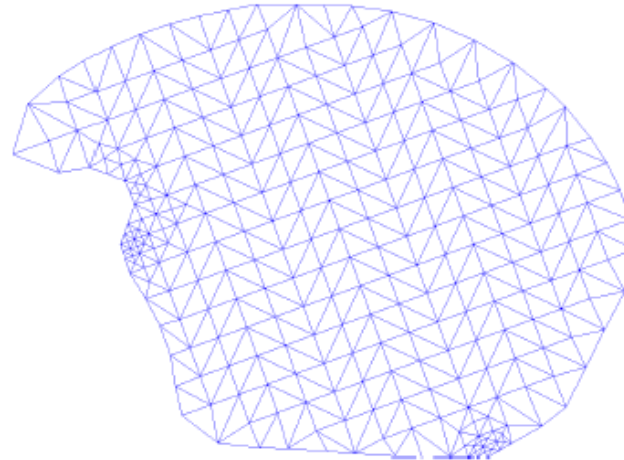
Genioglossus activation

J_1 :



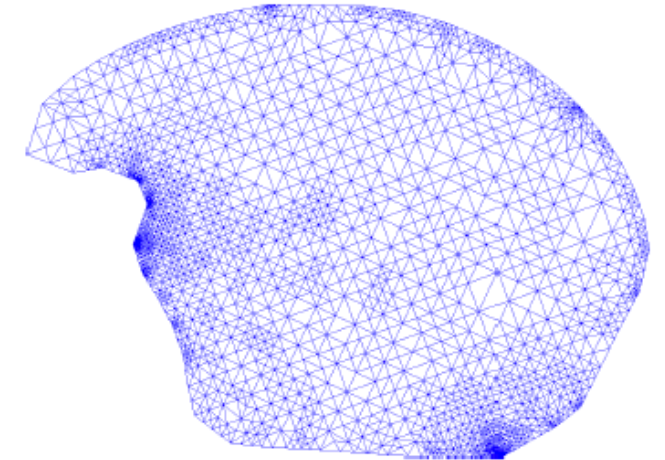
init

(N=426, $\varepsilon = 1.10^{-2}$)



2nd iteration

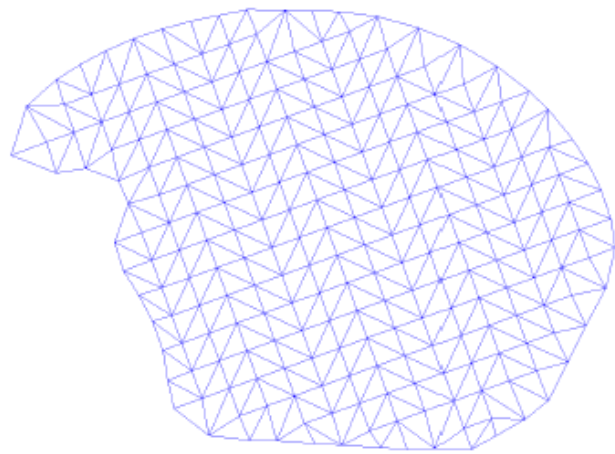
(N=523, $\varepsilon = 3.10^{-3}$)



8th iteration

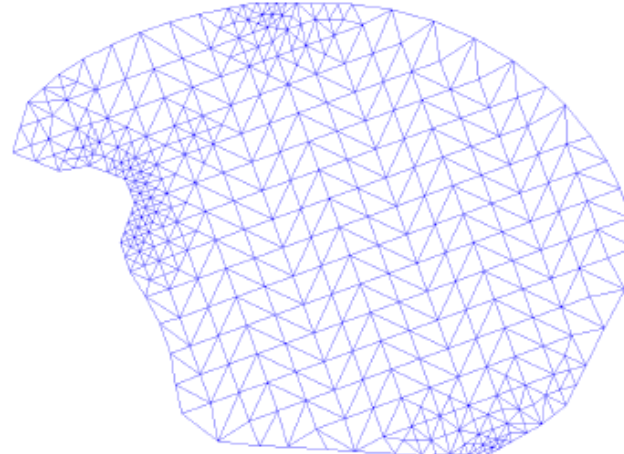
(N=5143, $\varepsilon = 4.10^{-5}$)

J_2 :



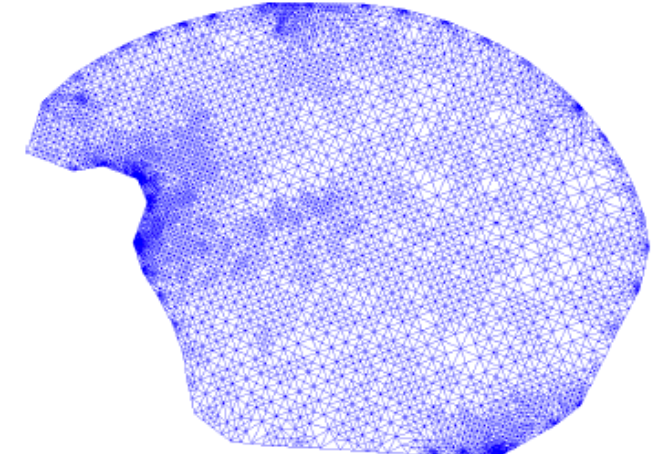
init

(N=426, $\varepsilon = 3.10^{-2}$)



2nd iteration

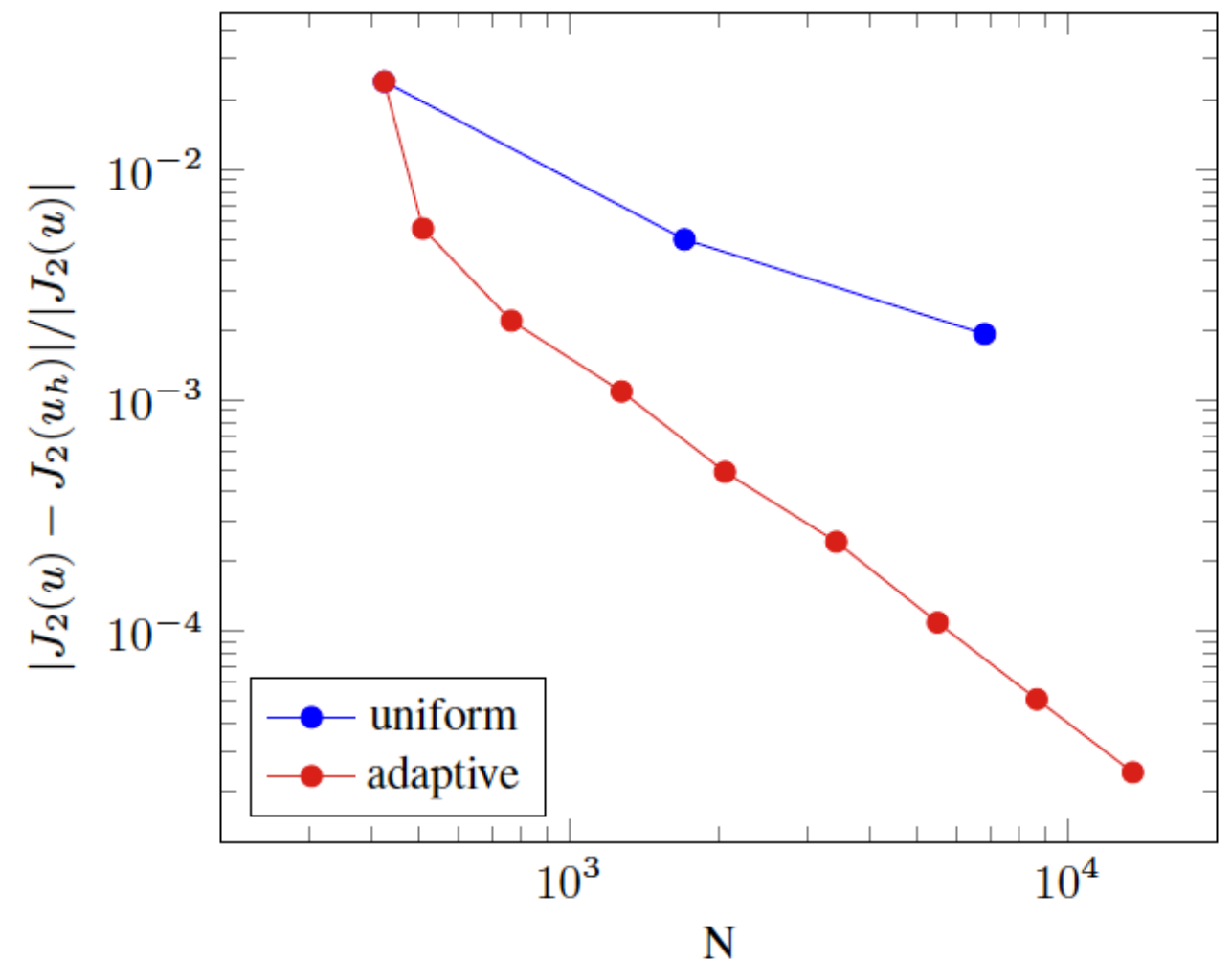
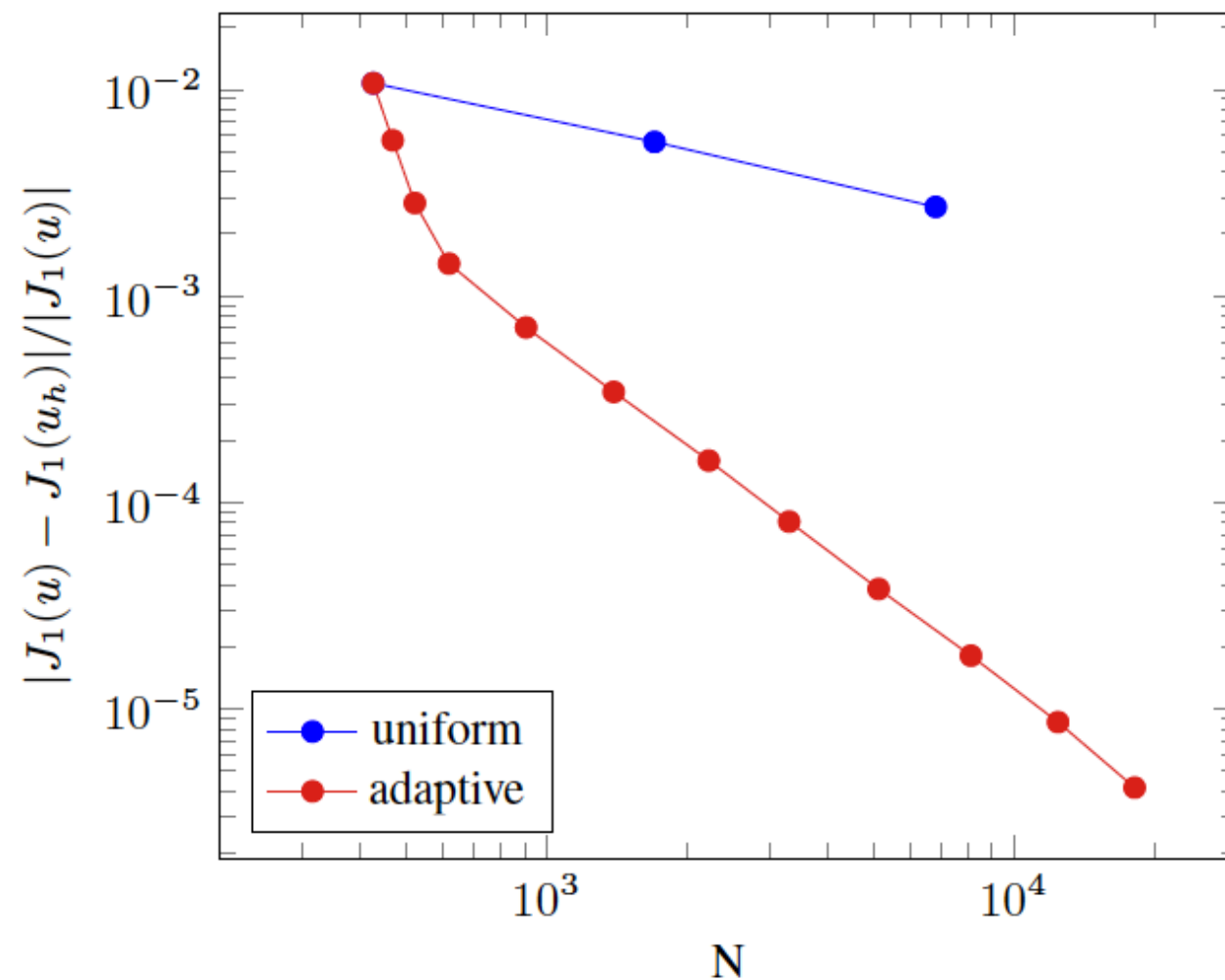
(N=766, $\varepsilon = 2.10^{-3}$)



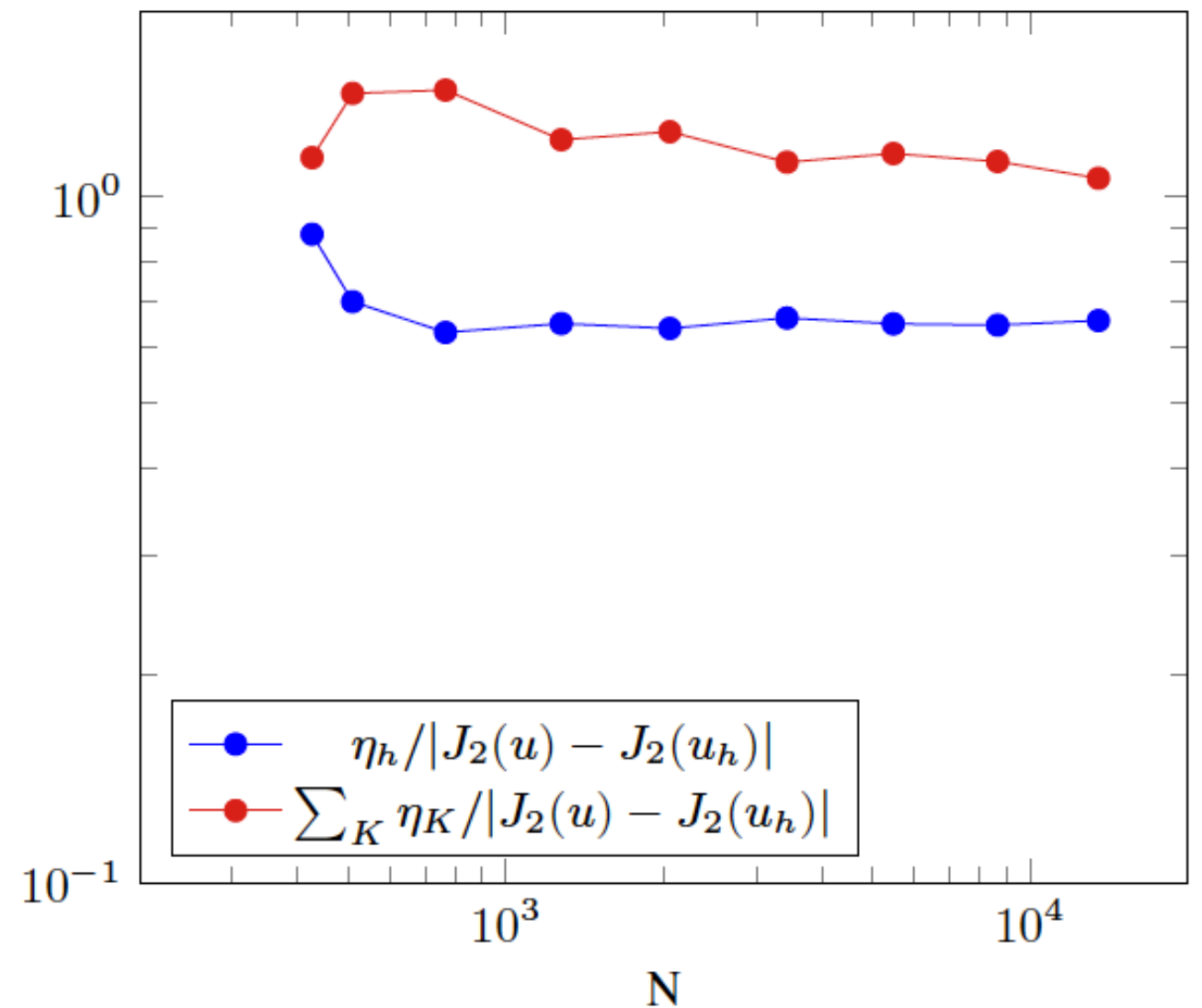
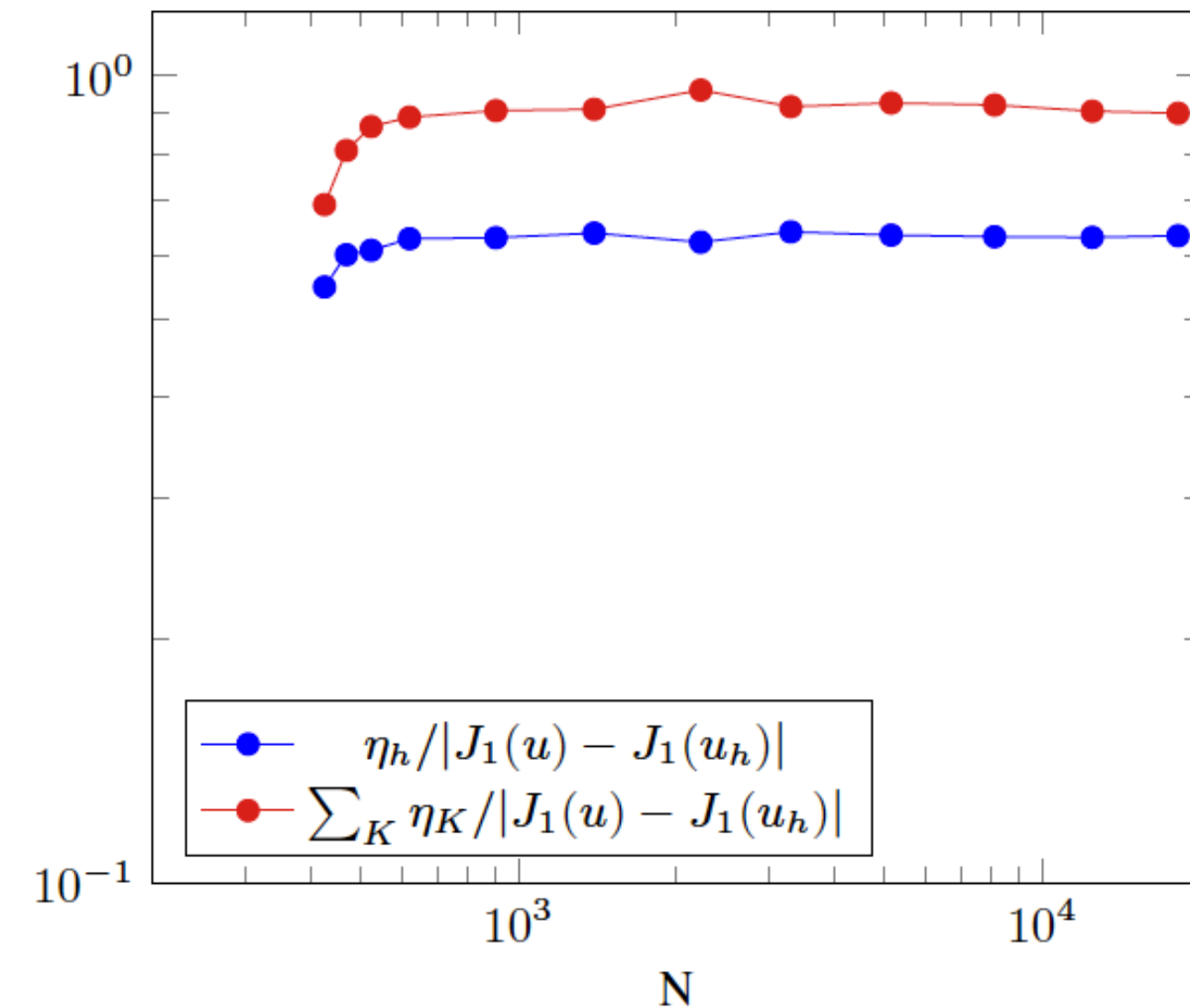
8th iteration

(N=13513, $\varepsilon = 2.10^{-5}$)

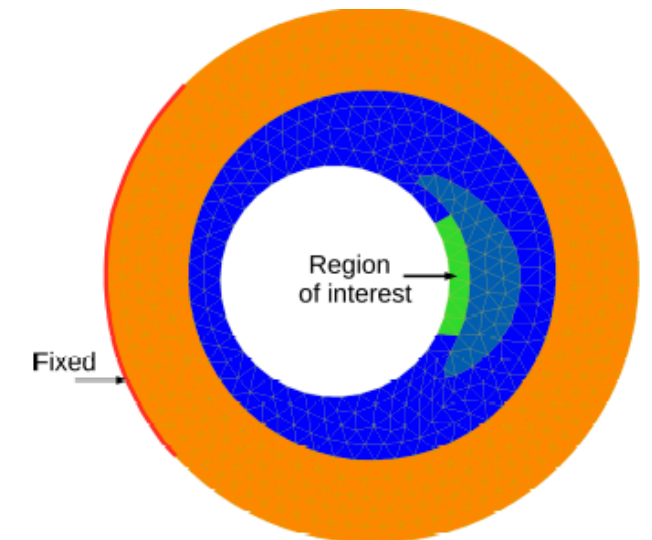
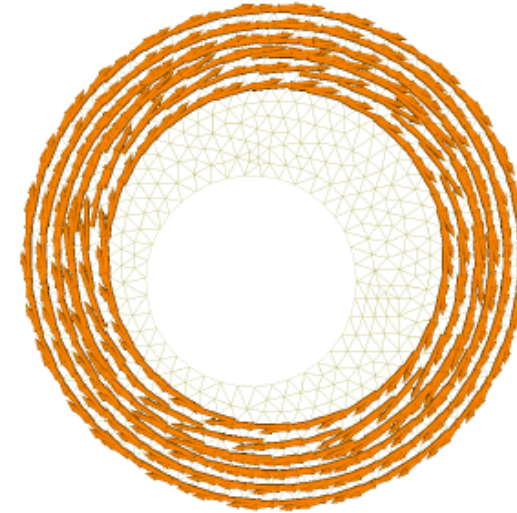
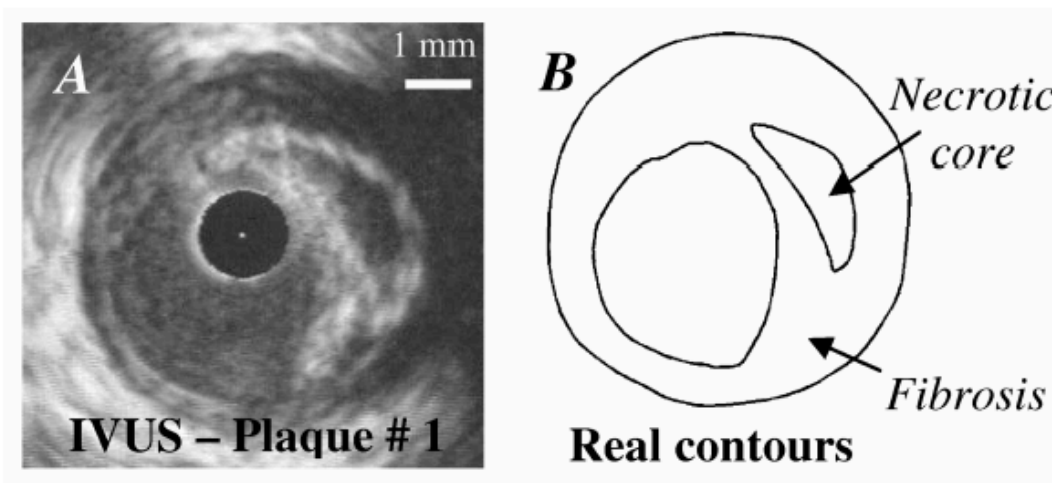
Effect of adaptive refinement



Effectivity of the error indicator



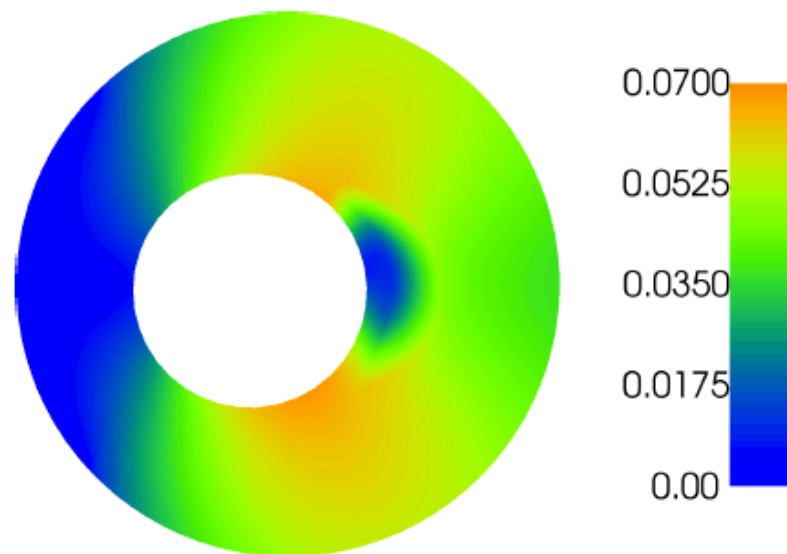
Arterial wall activation



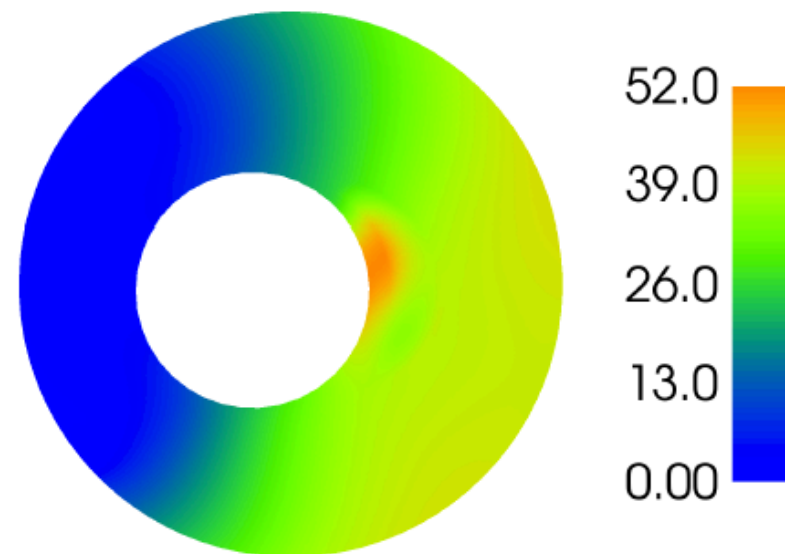
Le Floc'h et.al 2008

media

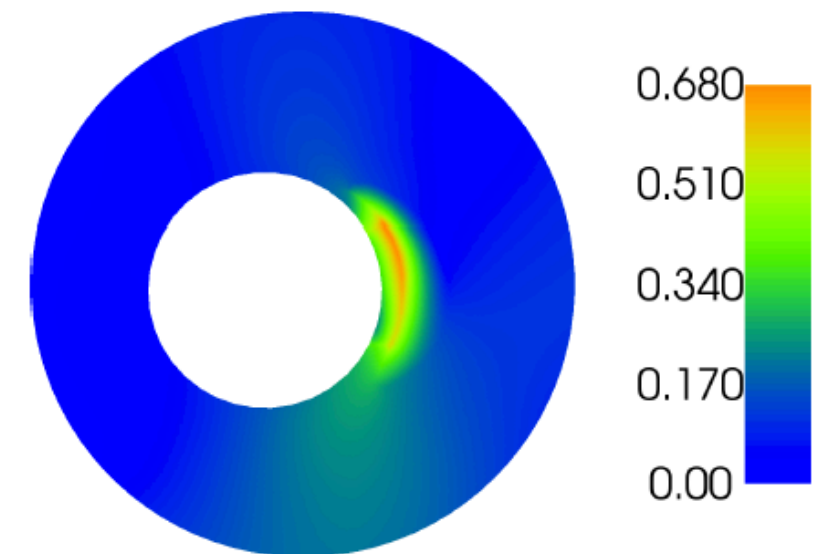
region of interest ω (green)



$\mathbf{u}$



$\mathbf{z} / J_1$

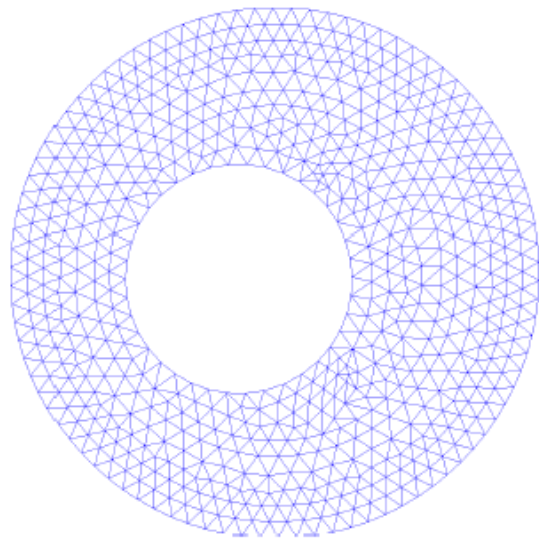


$\mathbf{z} / J_2$

$$J_1(\mathbf{u}) := \int_{\omega} (u_x + u_y) d\mathbf{x}$$

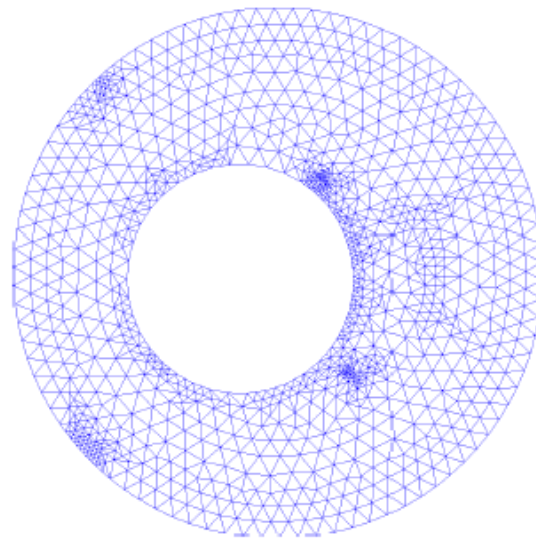
$$J_2(\mathbf{u}) := \int_{\omega} \text{div } \mathbf{u} d\mathbf{x}$$

$J_1 :$



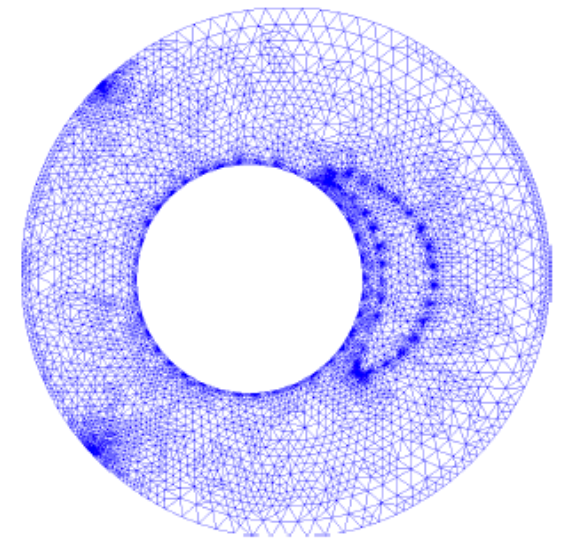
init

(N=1242, $\varepsilon = 0.4$)



2nd iteration

(N=2079, $\varepsilon = 0.05$)



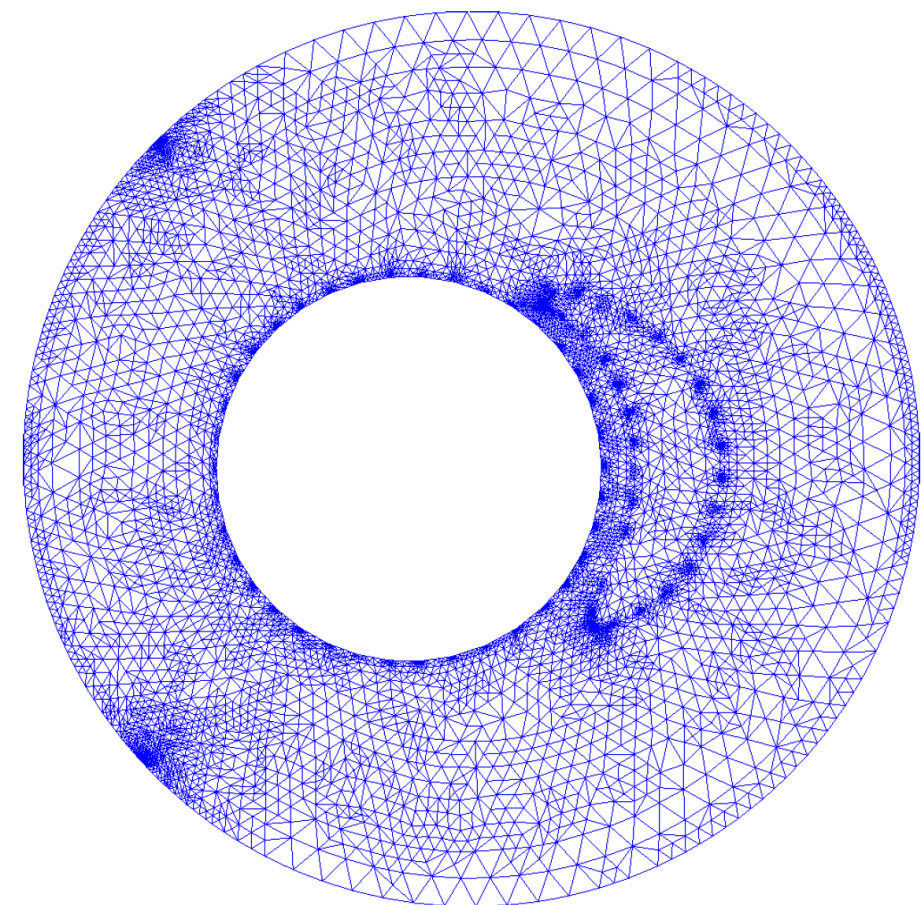
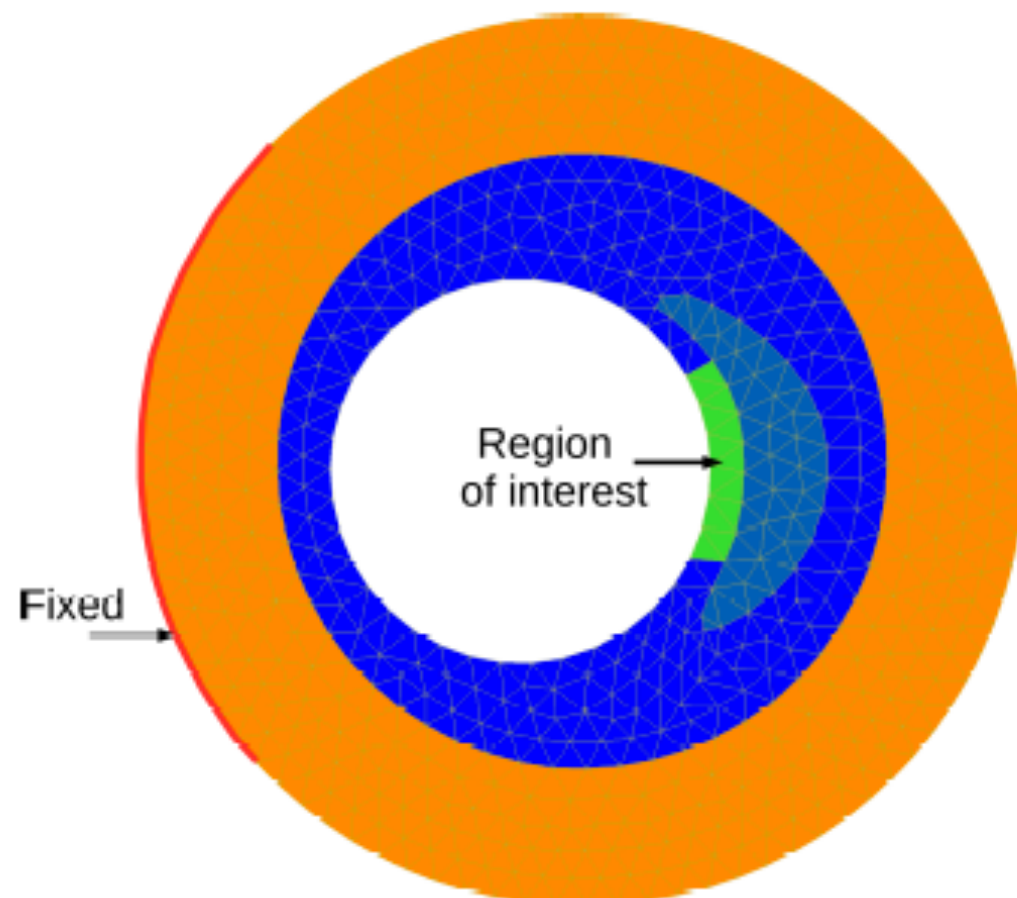
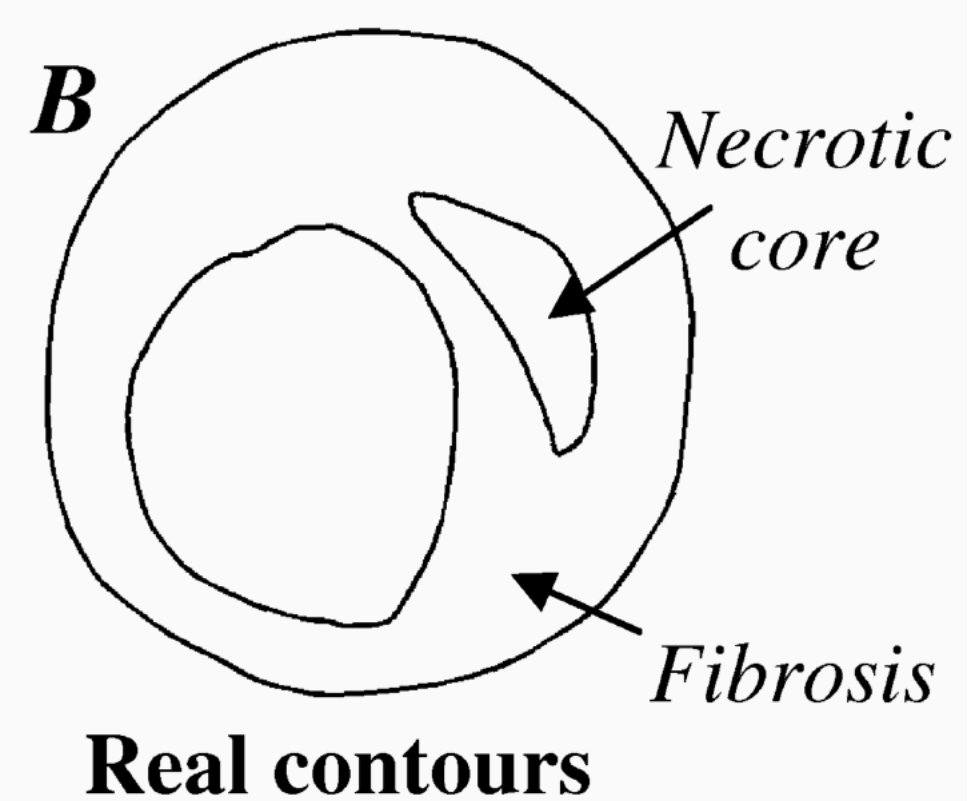
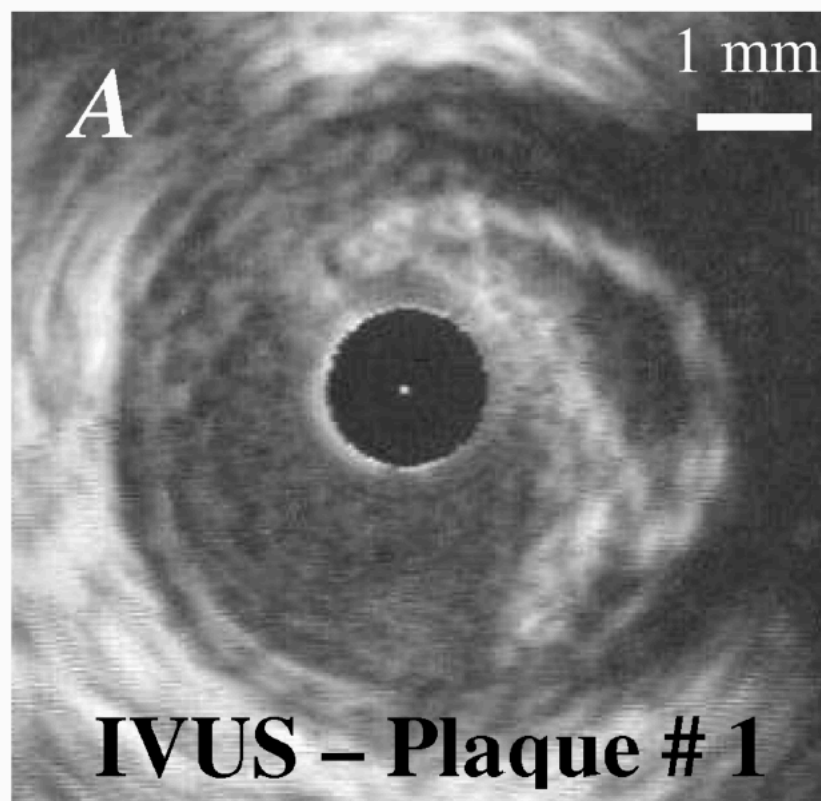
6th iteration

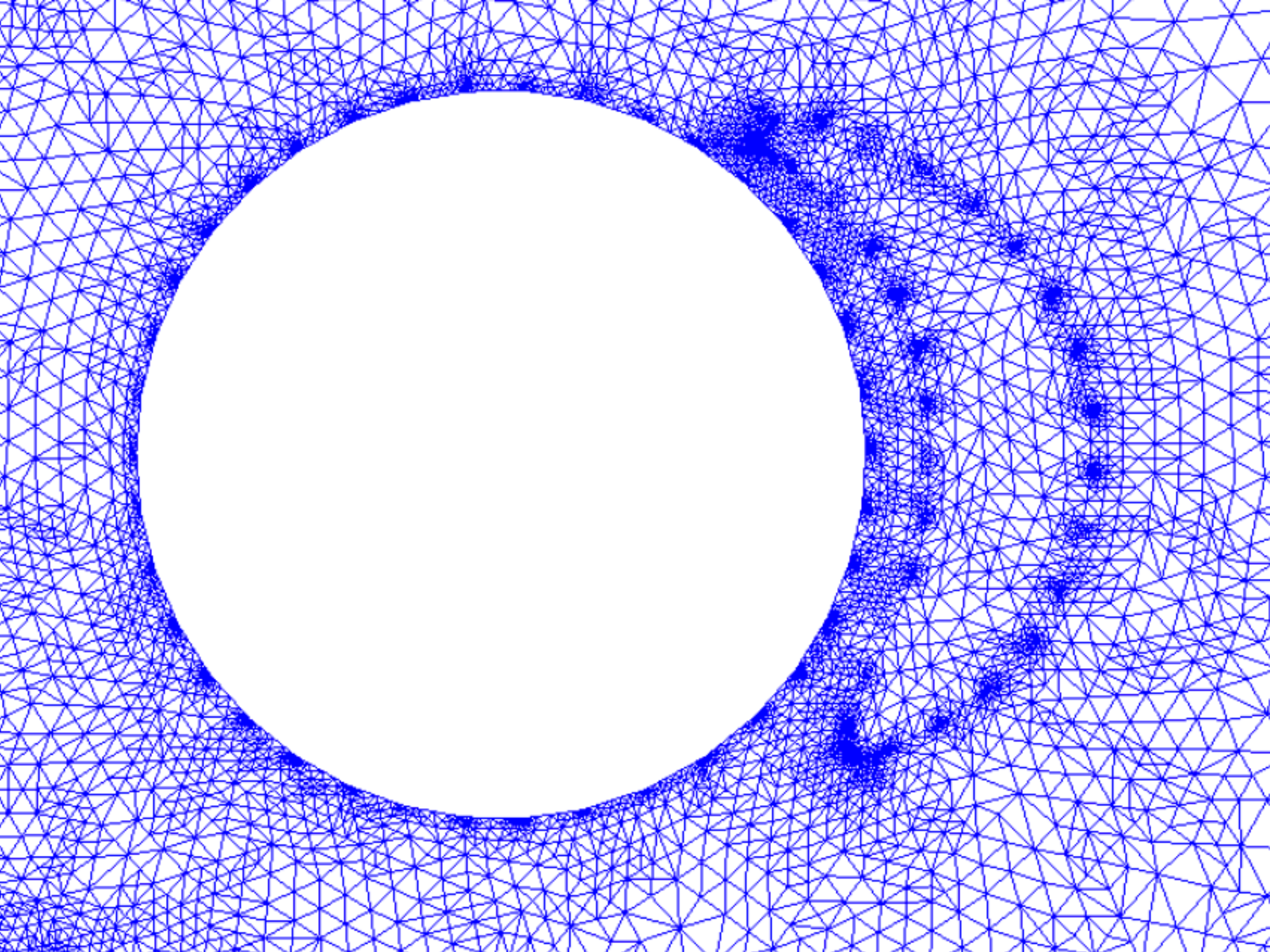
(N=15028, $\varepsilon = 3.10^{-3}$)

J_2 : similar results.

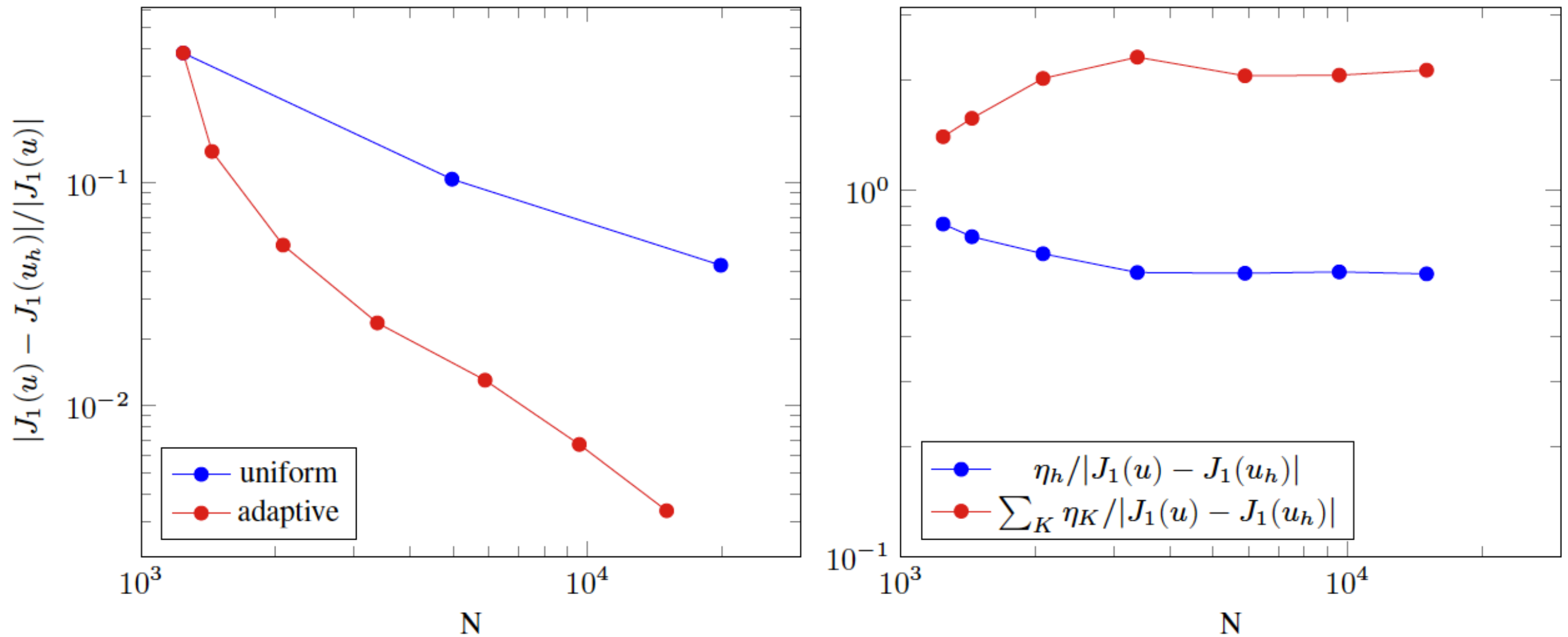


RealTCut



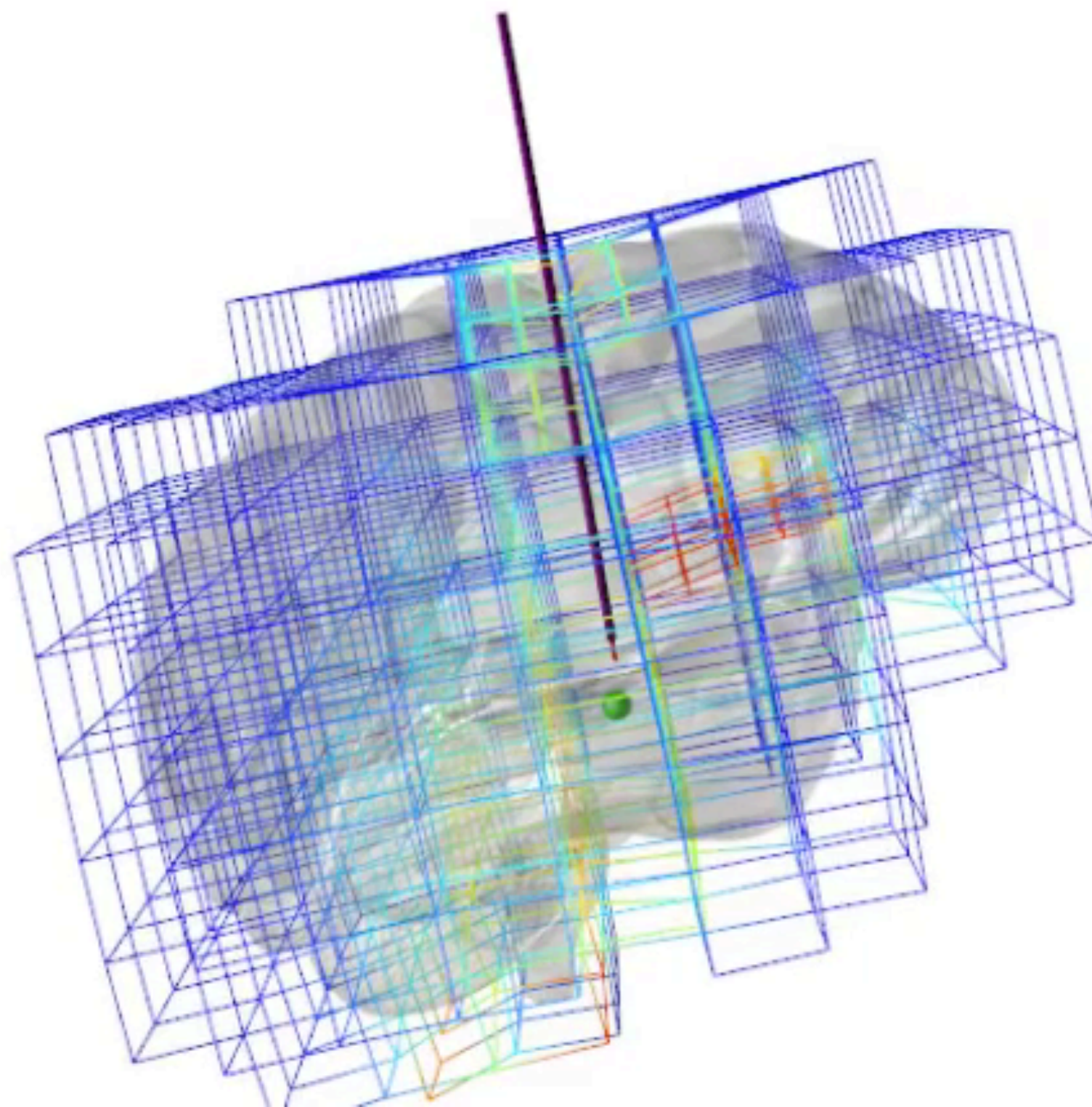


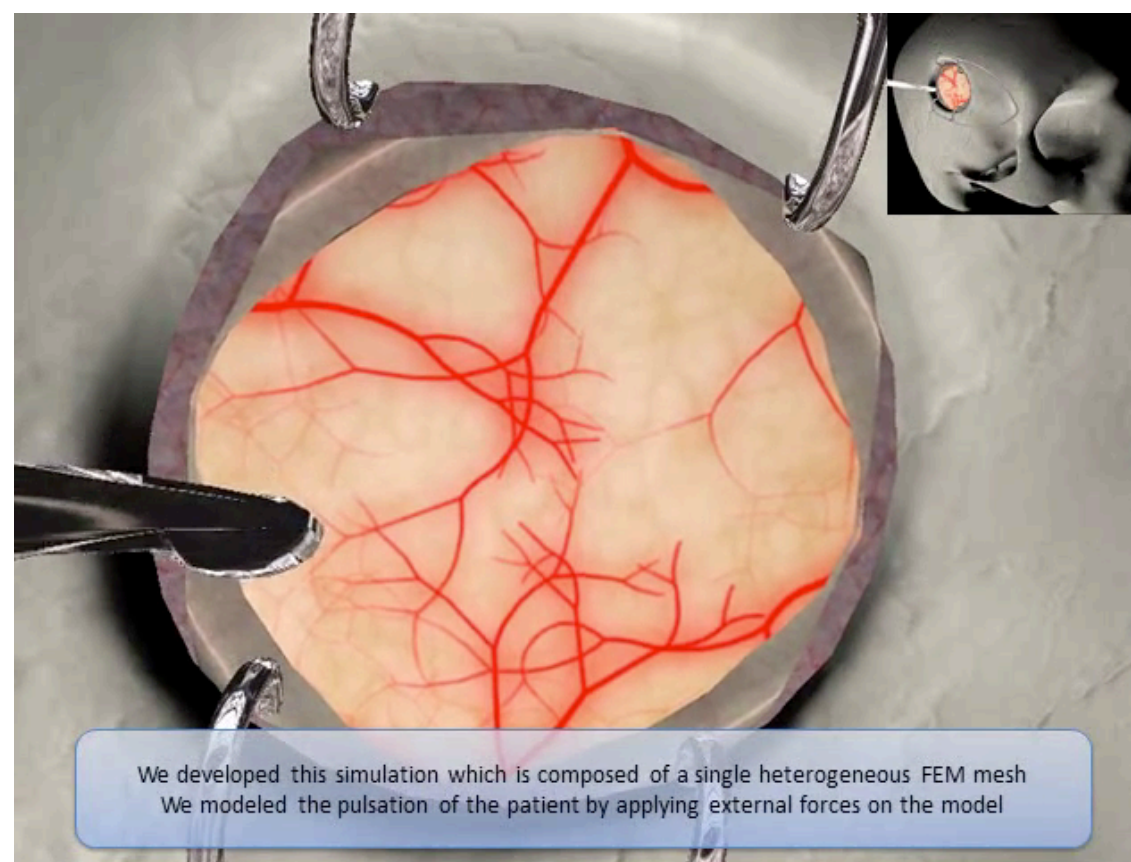
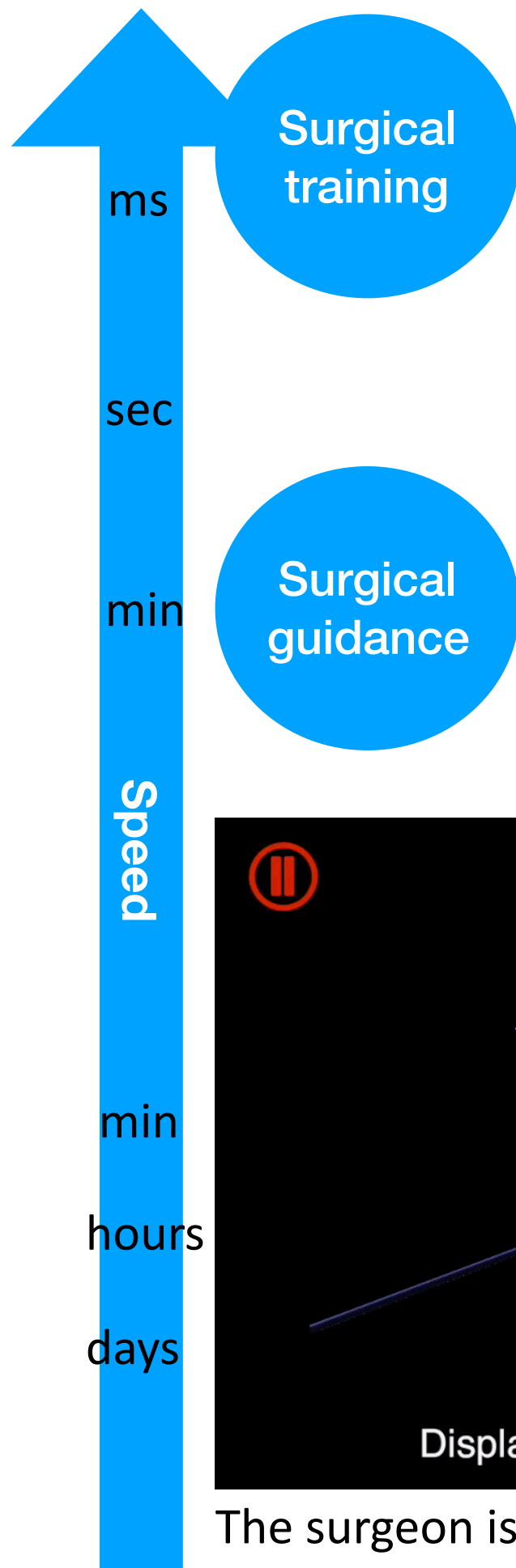
Effectivity



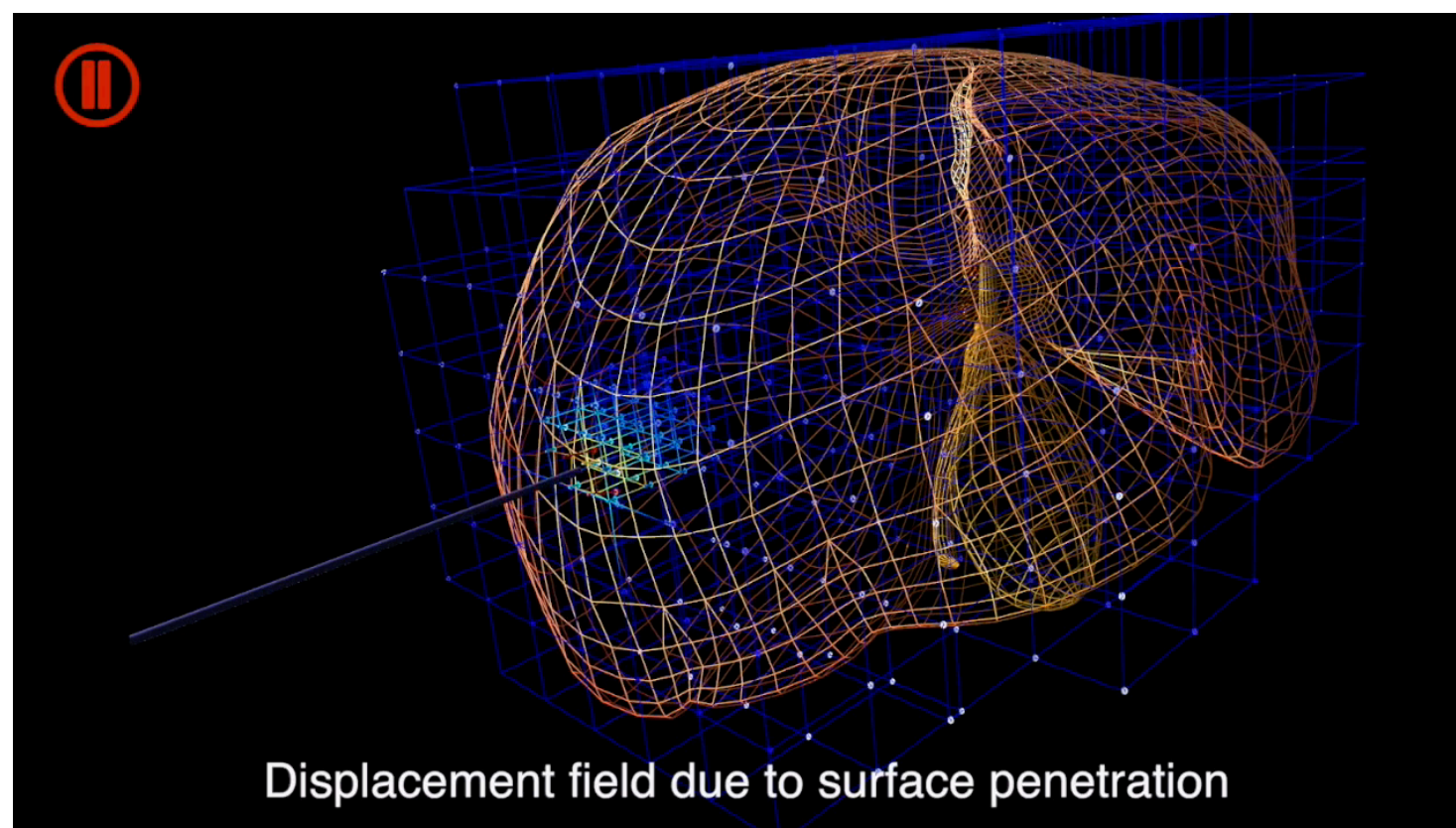
uniform vs. adaptive (left) / efficiency (right)

Cannula insertion





The surgeon trains as on a flight simulator
Courtecuisse et al, MEDIA, 2014



The surgeon is guided during the operation Bui et al, IEEE TBME, 2017



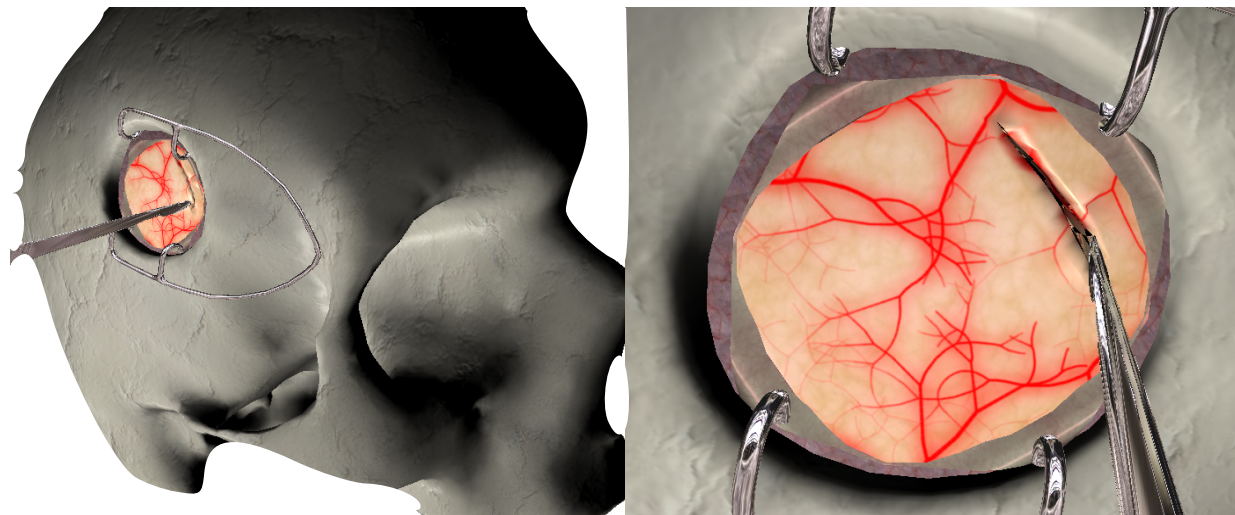
RealTCut

NEXT CHALLENGES

ERC RealTCut

Train surgeons safely on simulators

- ▶ Generic material models: *a priori*.
- ▶ Errors in quantities of interest for cuts in linear materials.
- ▶ Interactive simulations (solution in ms).



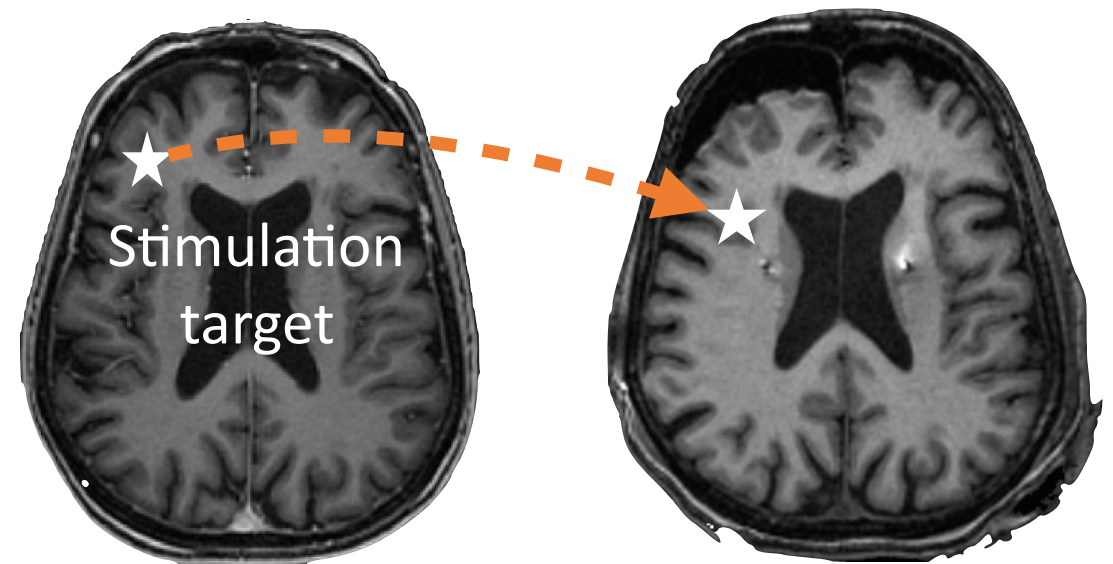
Courtecuisse, 2014, Implicit method for cutting in real-time. MEDIA

A generic organ is sufficient.

Future

Surgical assistance and planning

- ▶ Data-driven material models (real-time).
- ▶ Error control in quantities of interest for strong non-linearities, multi-field...
- ▶ Clinical time scales (solution in minutes).

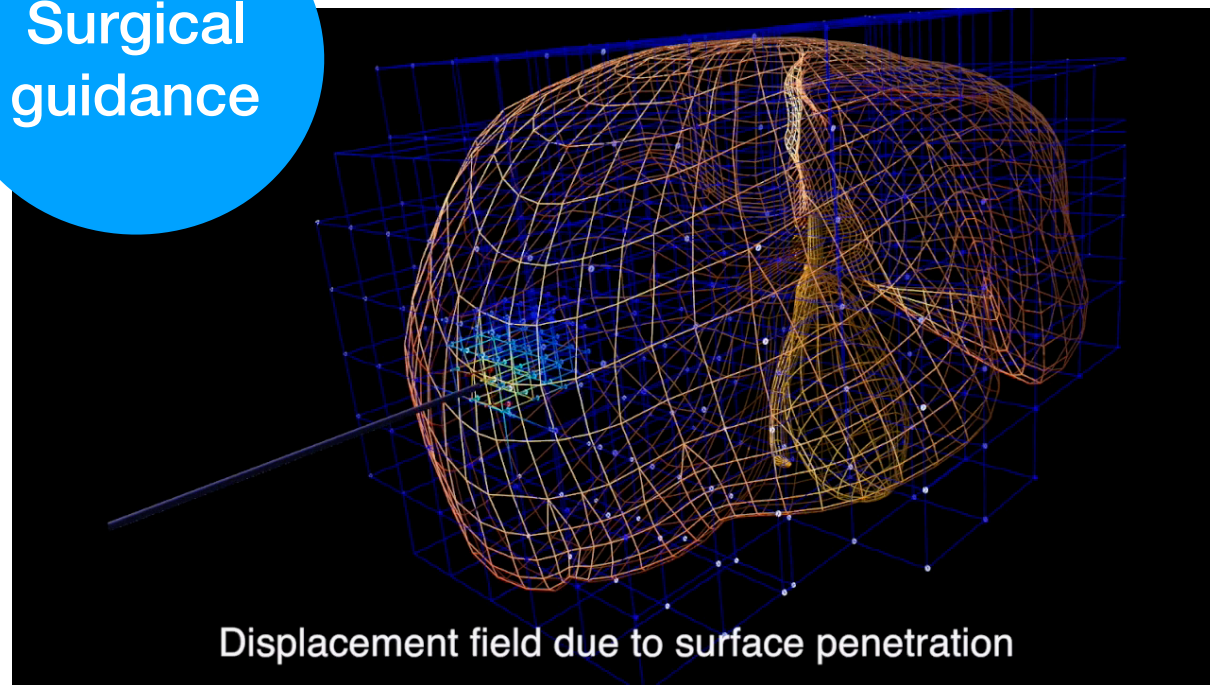


Predict shift of brain target.

Patient specificity is essential.

From surgical training to surgical planning and assistance

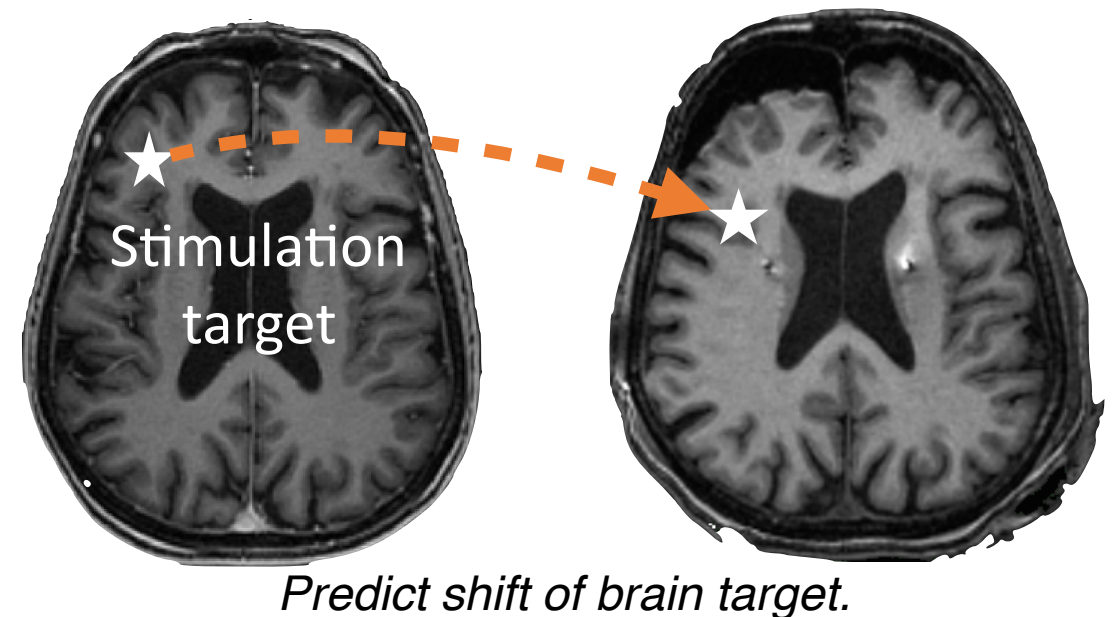
Surgical
guidance



QUESTION: What (material) model should be used for a given patient?

Future Surgical assistance and planning

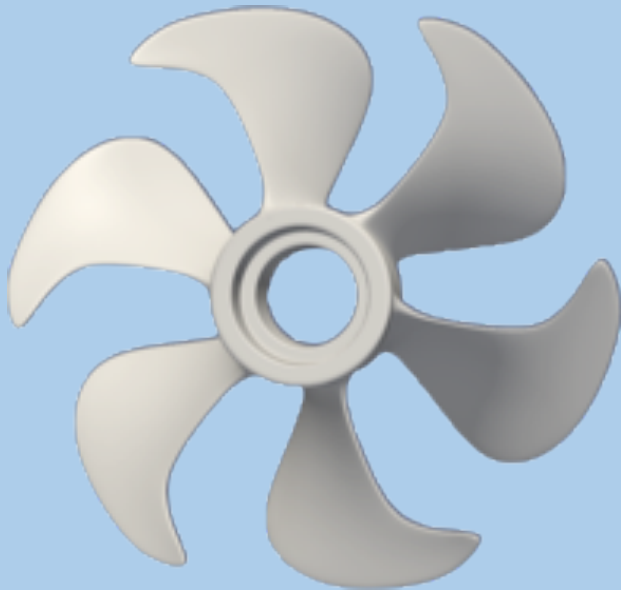
- ▶ Data-driven material models (real-time).
- ▶ Error control in quantities of interest for strong non-linearities, multi-field...
- ▶ Clinical time scales (solution in minutes).



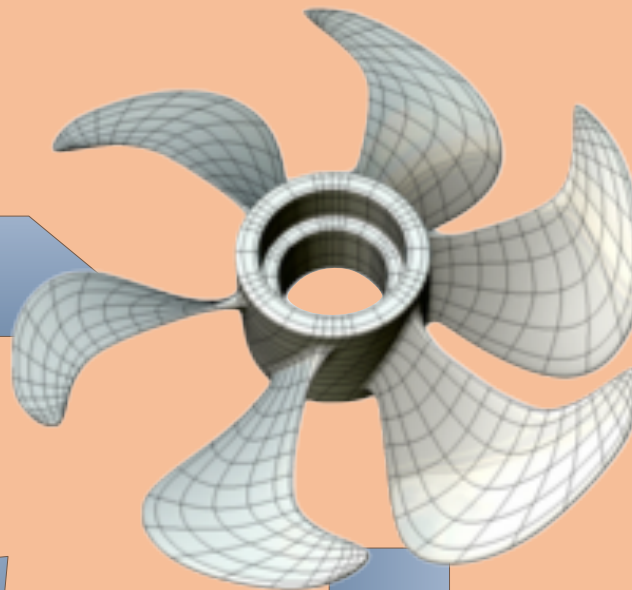
Patient specificity is essential.

What we do in engineering modelling and simulations

GEOMETRICAL MODEL



DISCRETISATION



Verification

MATERIAL MODELS

Phenomenological

Elasticity/Plasticity

Crack growth law (Paris...)

Fracture energy

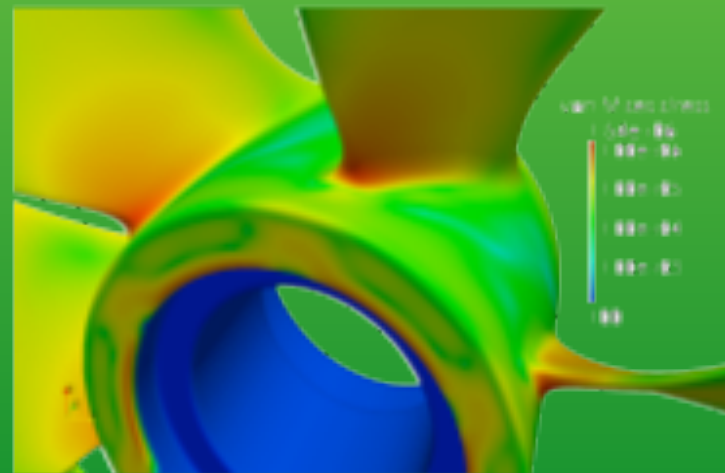
Maximum tensile strength

Multi-scale

Debonding, Fibre pull-out

Fibre breakage, interface fracture, grains, dislocations,

NUMERICAL SOLUTION



A POSTERIORI
ERROR
CONTROL

Validation & parameter identification

EXPERIMENTS

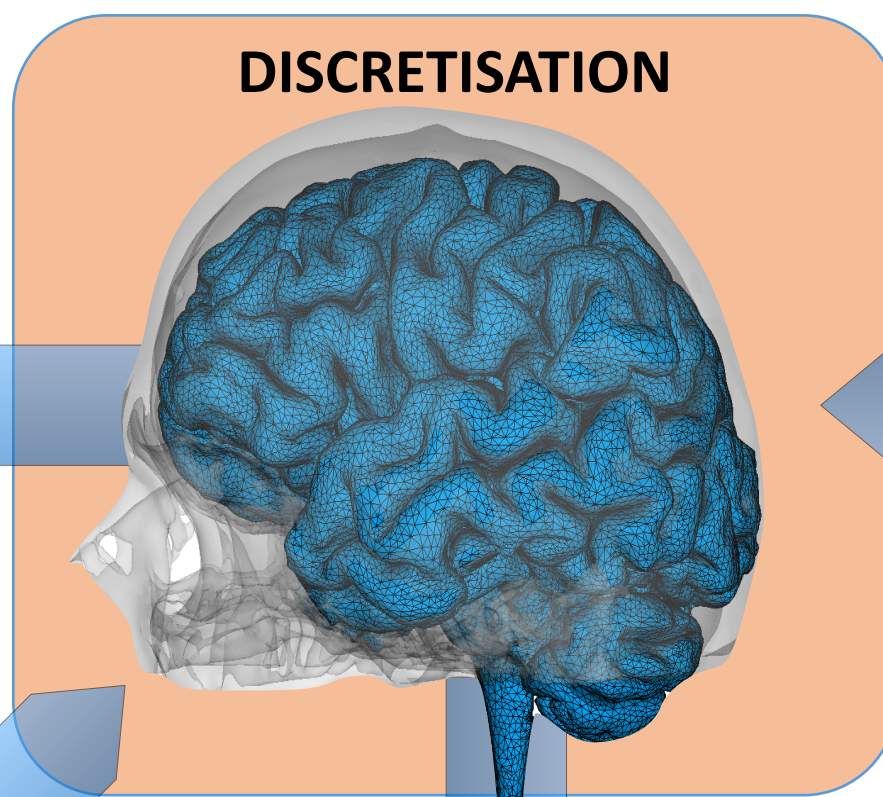
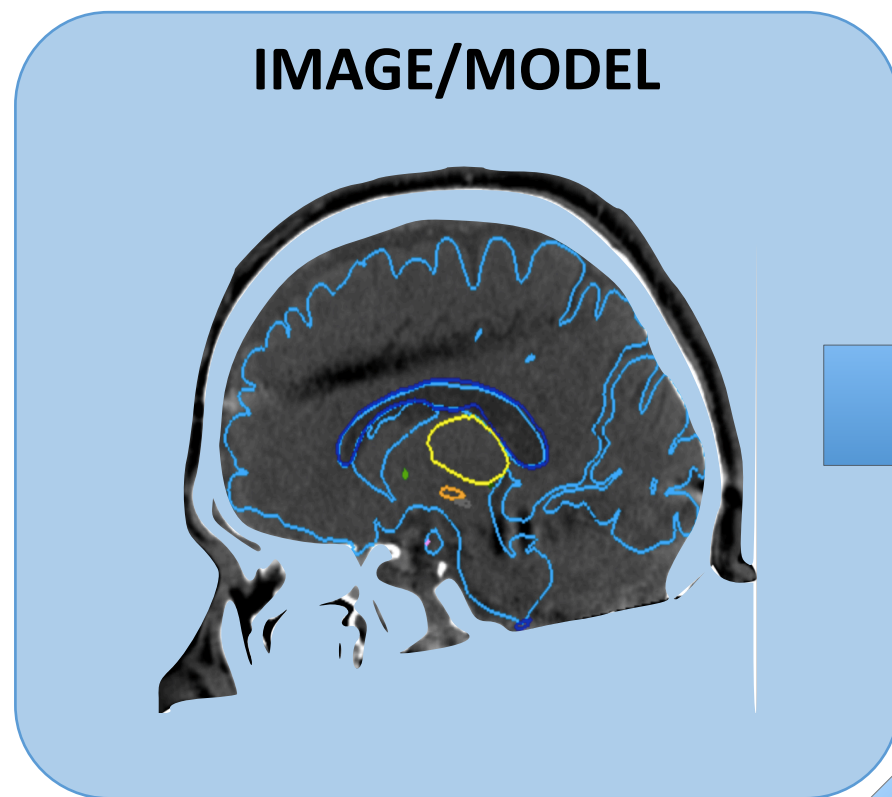
CONVENTIONAL APPROACH



RealTCut

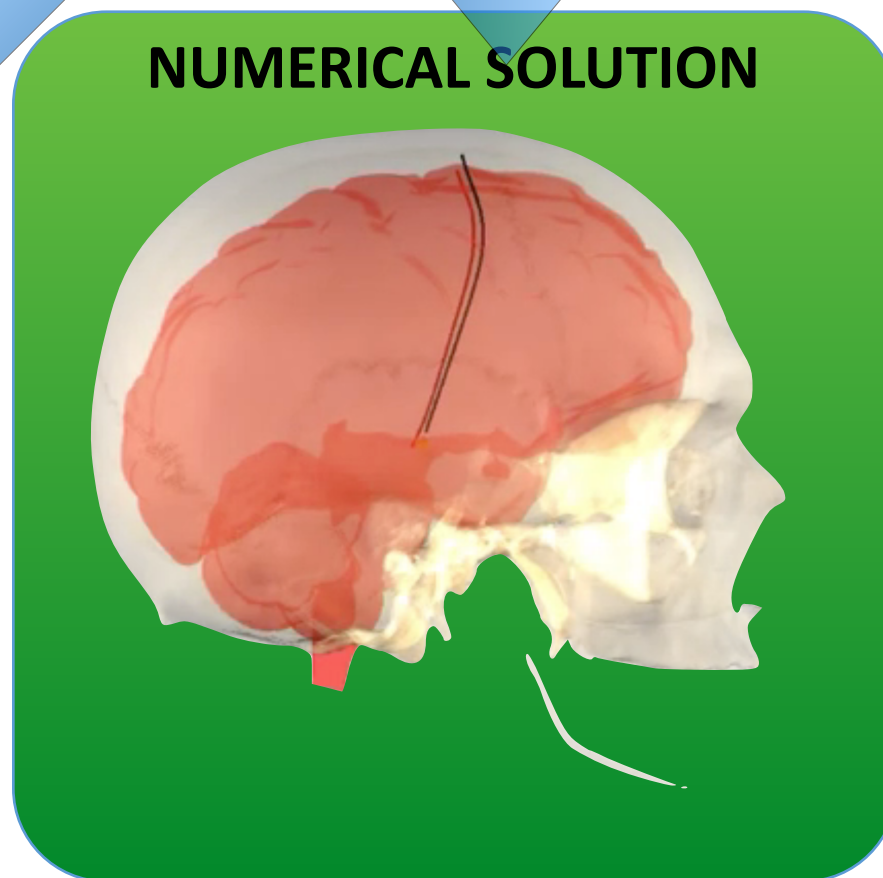
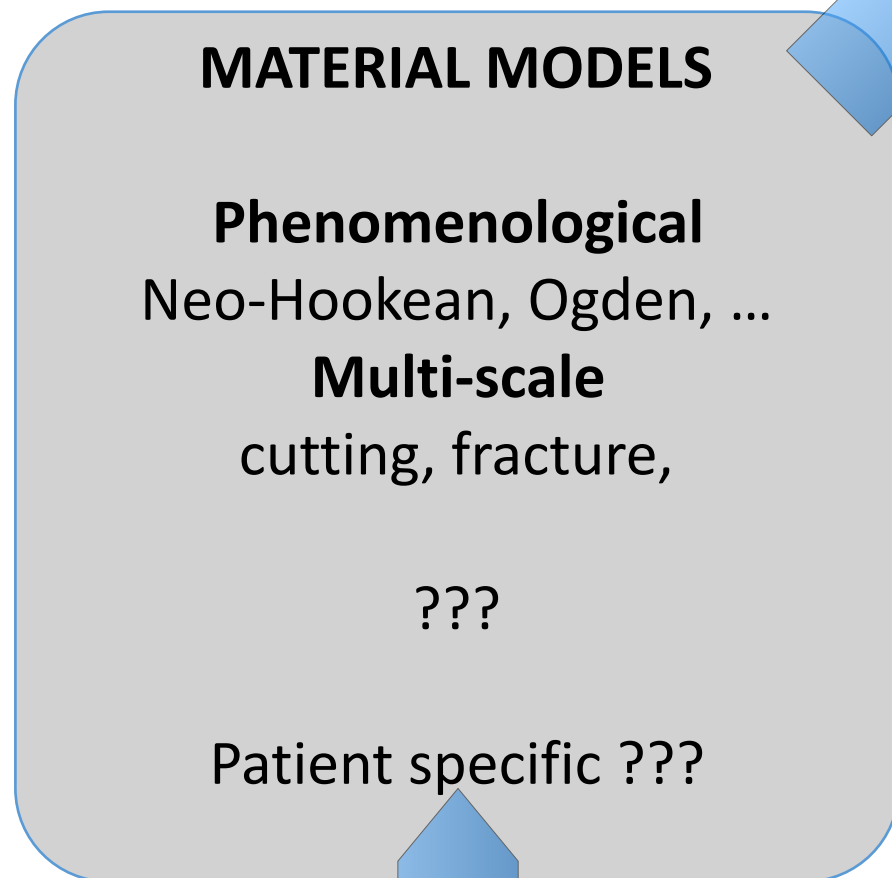
We cannot do in biomechanics...





Verification

**A POSTERIORI
ERROR
CONTROL**



Validation & parameter identification

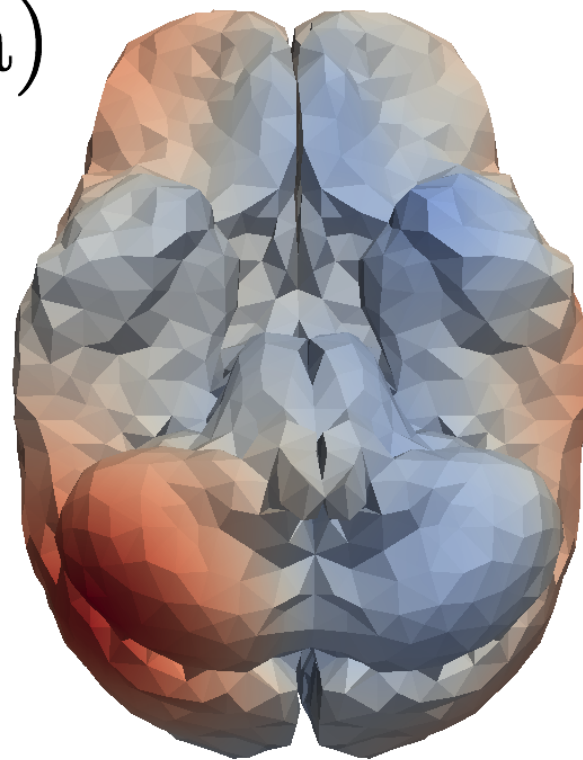
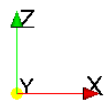
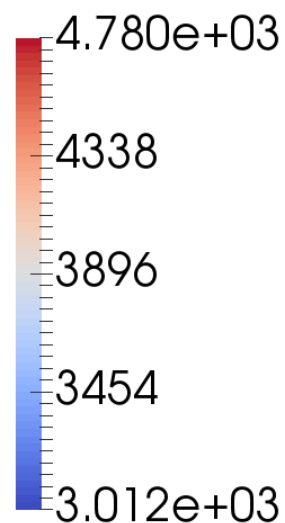


Assuming the material model is representative, what is the influence of each parameter in the model?

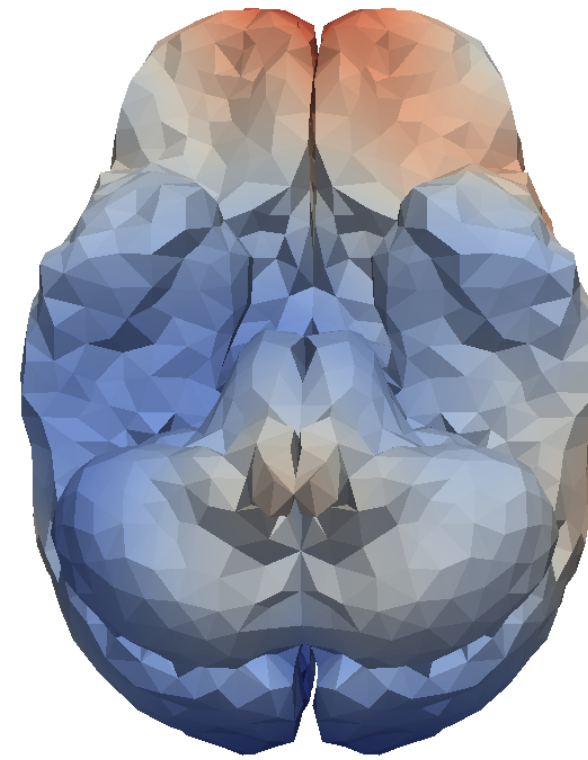
- Different methods: Karhunen–Loève expansion [Adler 2007], Fast Fourier transform [Nowak 2004].

Randoms fields

C_1 (MPa)



Realisation 1



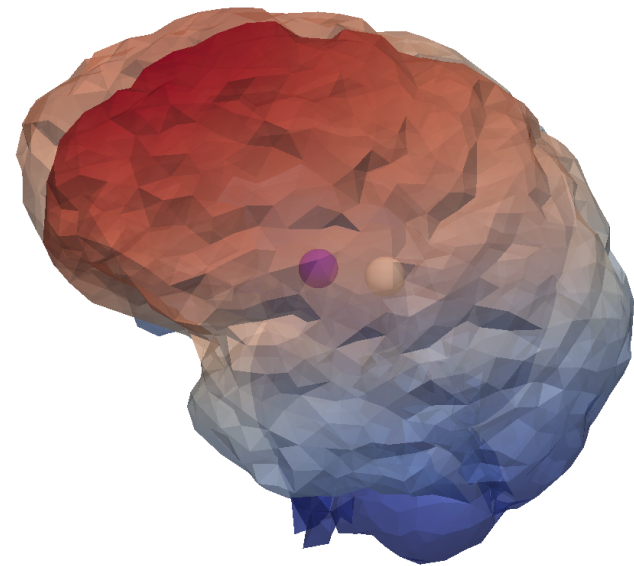
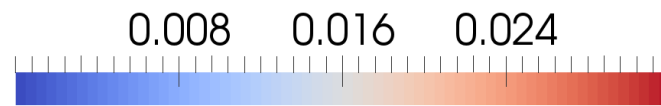
Realisation 2

Two realisations of RF, with a log-normal distribution, for the parameter C_1 (in MPa).



Confidence level in predicting the target location

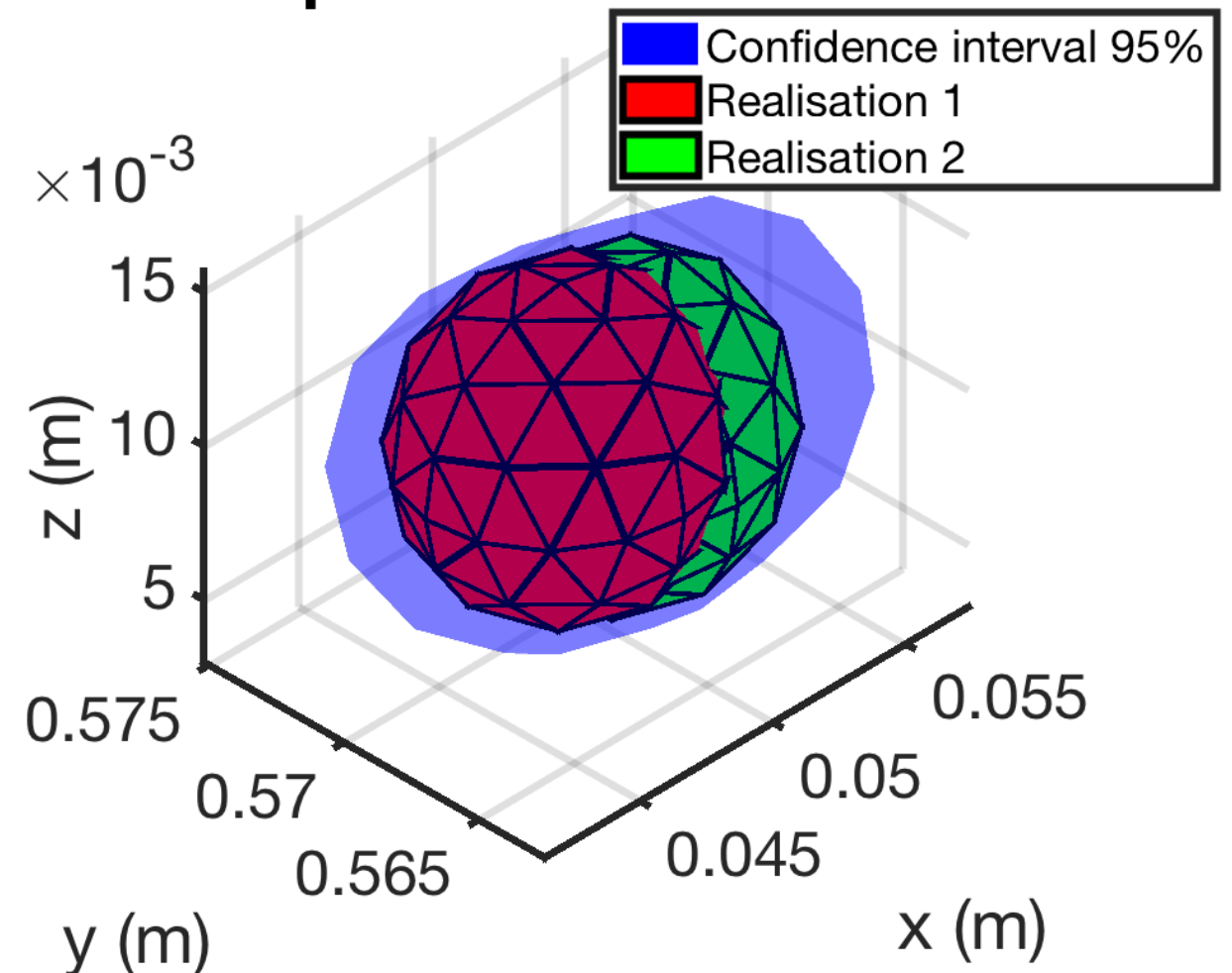
Displacement magnitude (m)



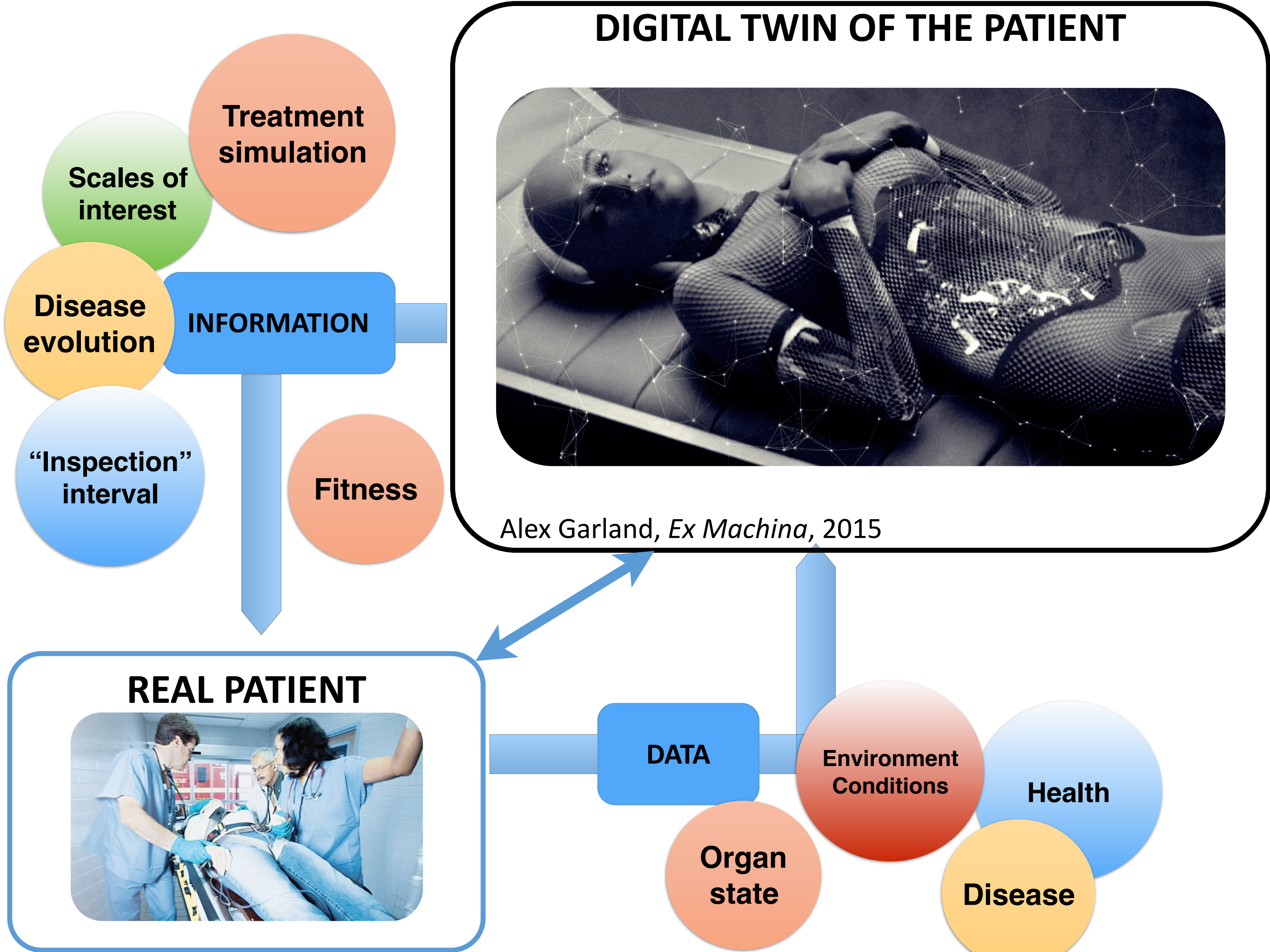
● Initial

● Deform

Sphere deformation



What is the influence of material parameters on computed quantities of interest?



Digital twin concept

Actual aircraft

Digital aircraft model

Life prediction and
extension

Situation awareness

High fidelity modeling
and simulation

Certification and
design methods

**Requires real-time data
assimilation, and model
update...**

Medicine

The average drug developed by a major pharmaceutical company costs at least \$4 billion, and it can be as much as \$11 billion.

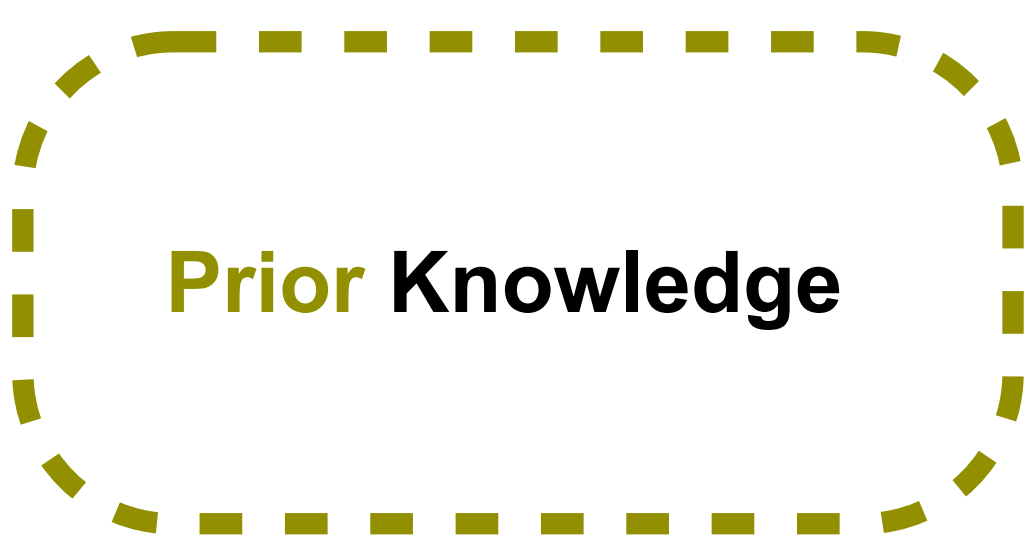
Mechanics

The development cost of the A380

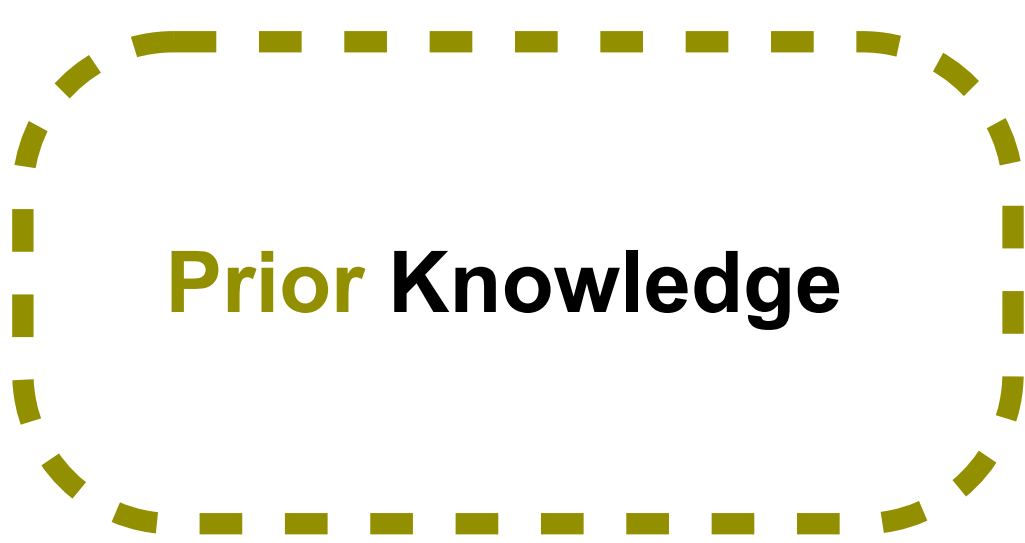
11 billion euros...

of the dreamliner...

\$32 billion



Prior Knowledge

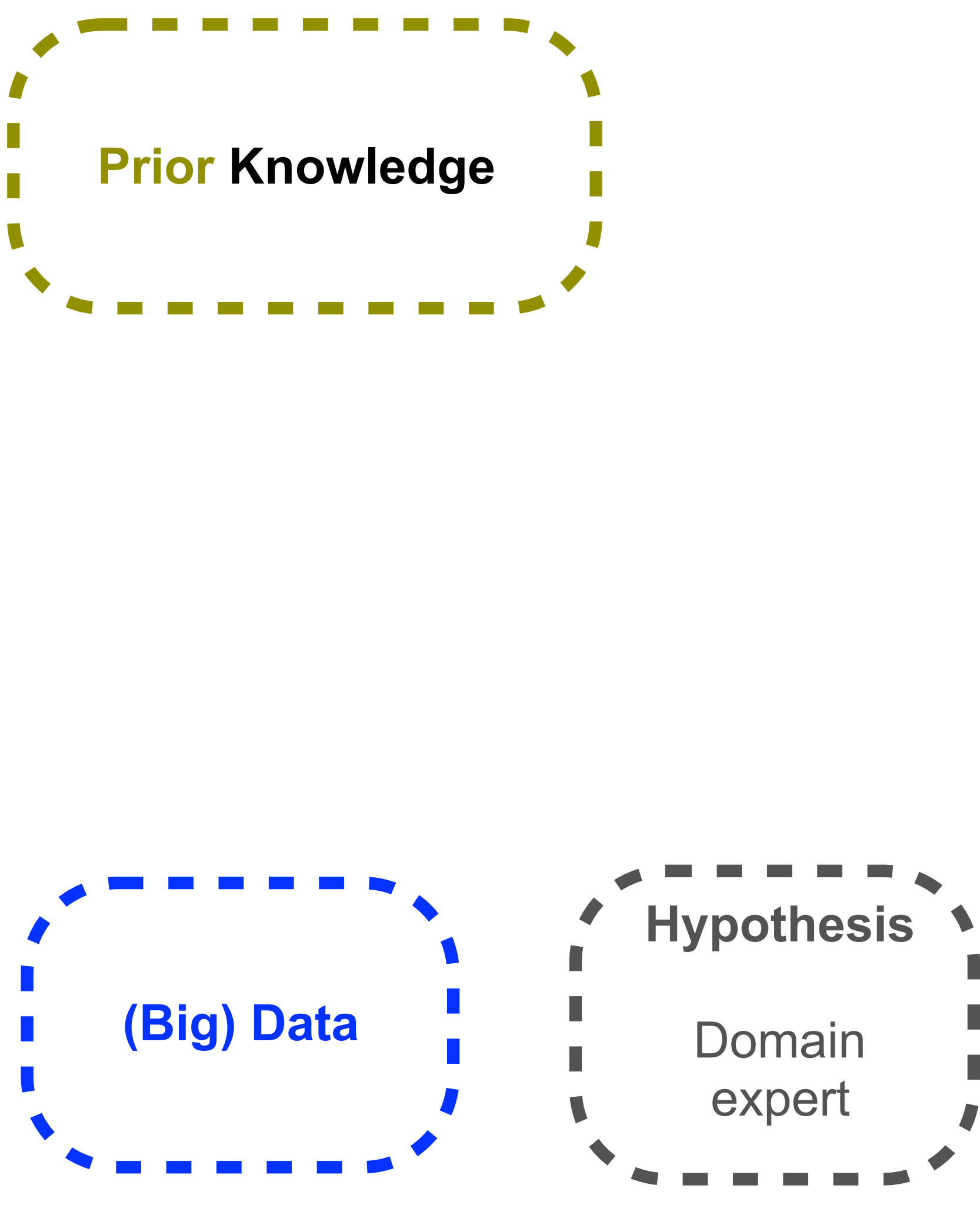


Prior Knowledge



Hypothesis

Domain
expert



Prior Knowledge

(Big) Data

Hypothesis

Domain
expert

Prior Knowledge

The diagram illustrates a workflow or knowledge integration process. At the top, a dashed olive-green circle contains the text 'Prior Knowledge'. Below this, a large rounded rectangle with a black border contains two overlapping rounded rectangles: 'Computational Science' on the left and 'HPC' on the right. At the bottom left, a dashed blue circle contains the text '(Big) Data'. At the bottom right, a dashed dark-gray circle contains the text 'Hypothesis' and 'Domain expert' stacked vertically.

**Computational
Science**

HPC

(Big) Data

Hypothesis

Domain
expert

Prior Knowledge

**Computational
Science**

HPC

Conclusions

(Big) Data

Hypothesis

Domain
expert

Prior Knowledge



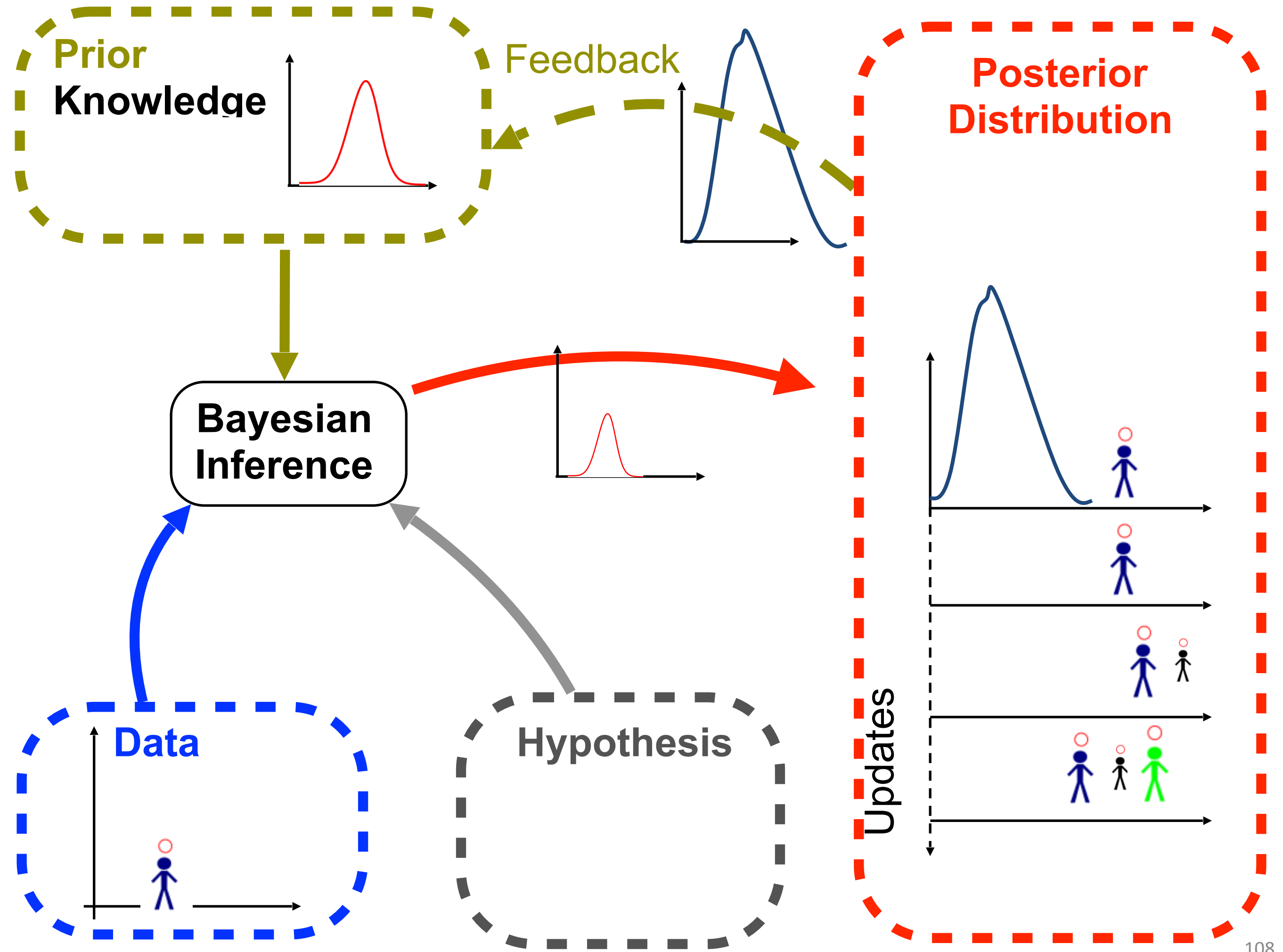
Data-driven modelling

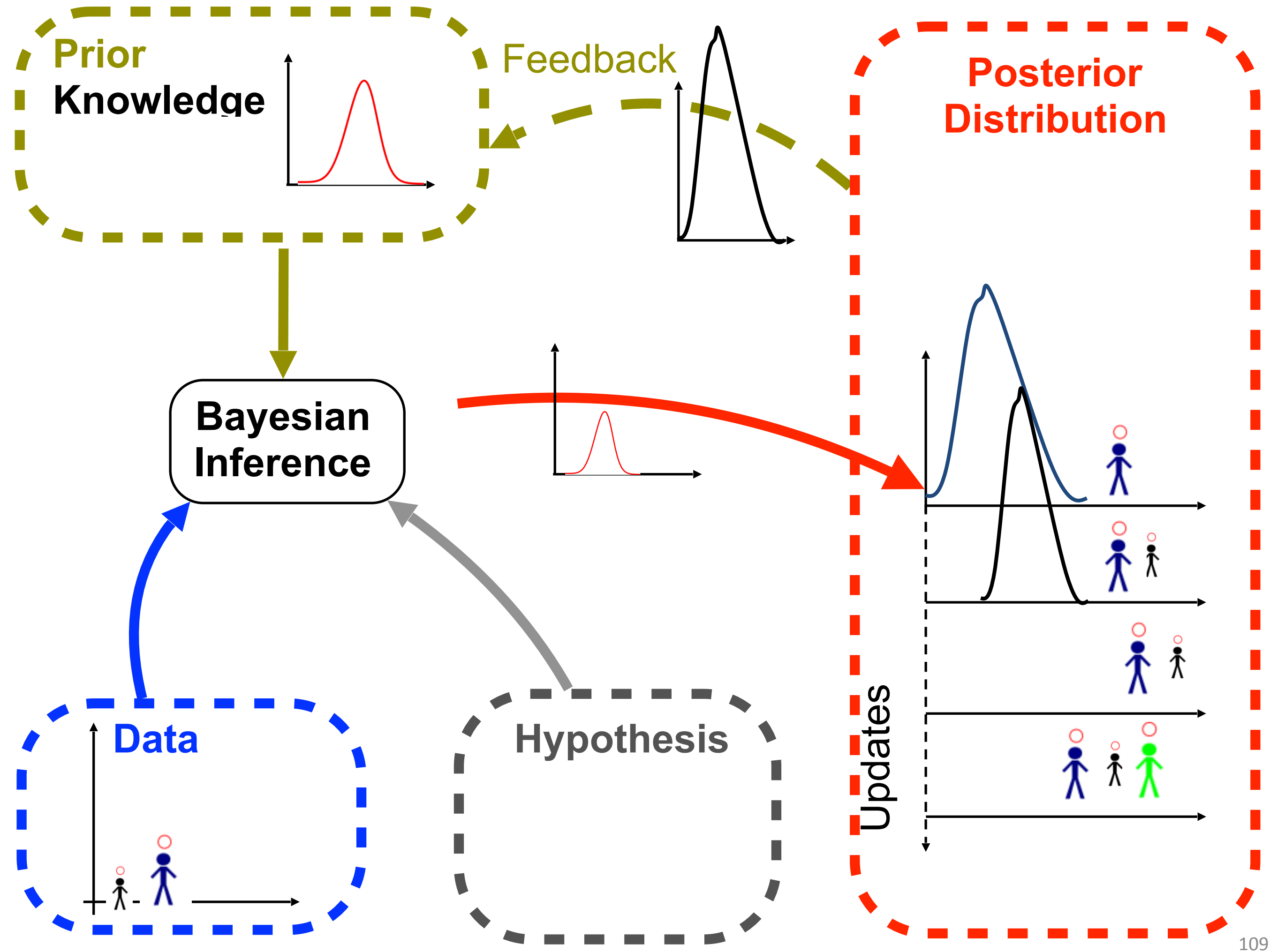
Conclusions

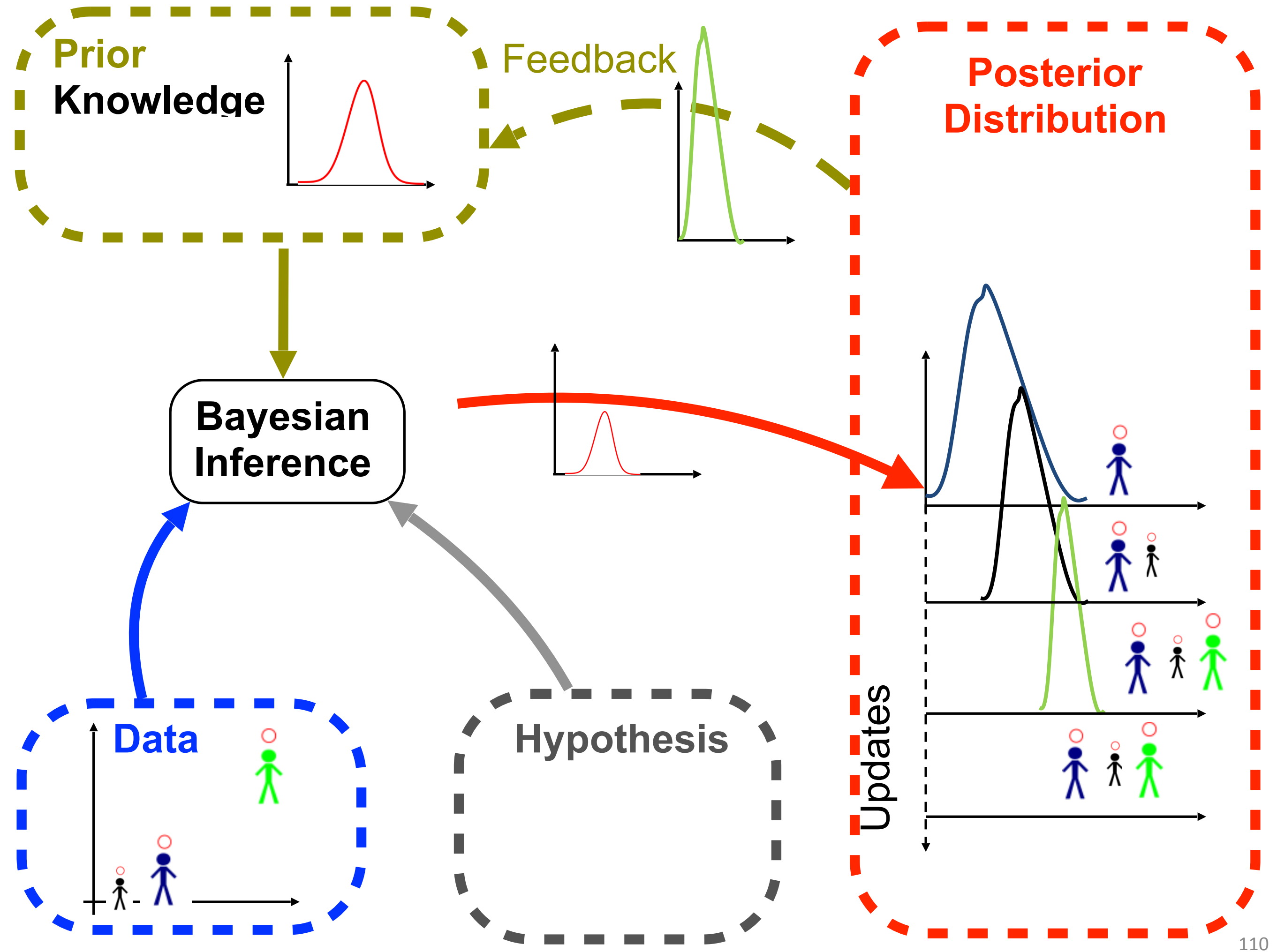
(Big) Data

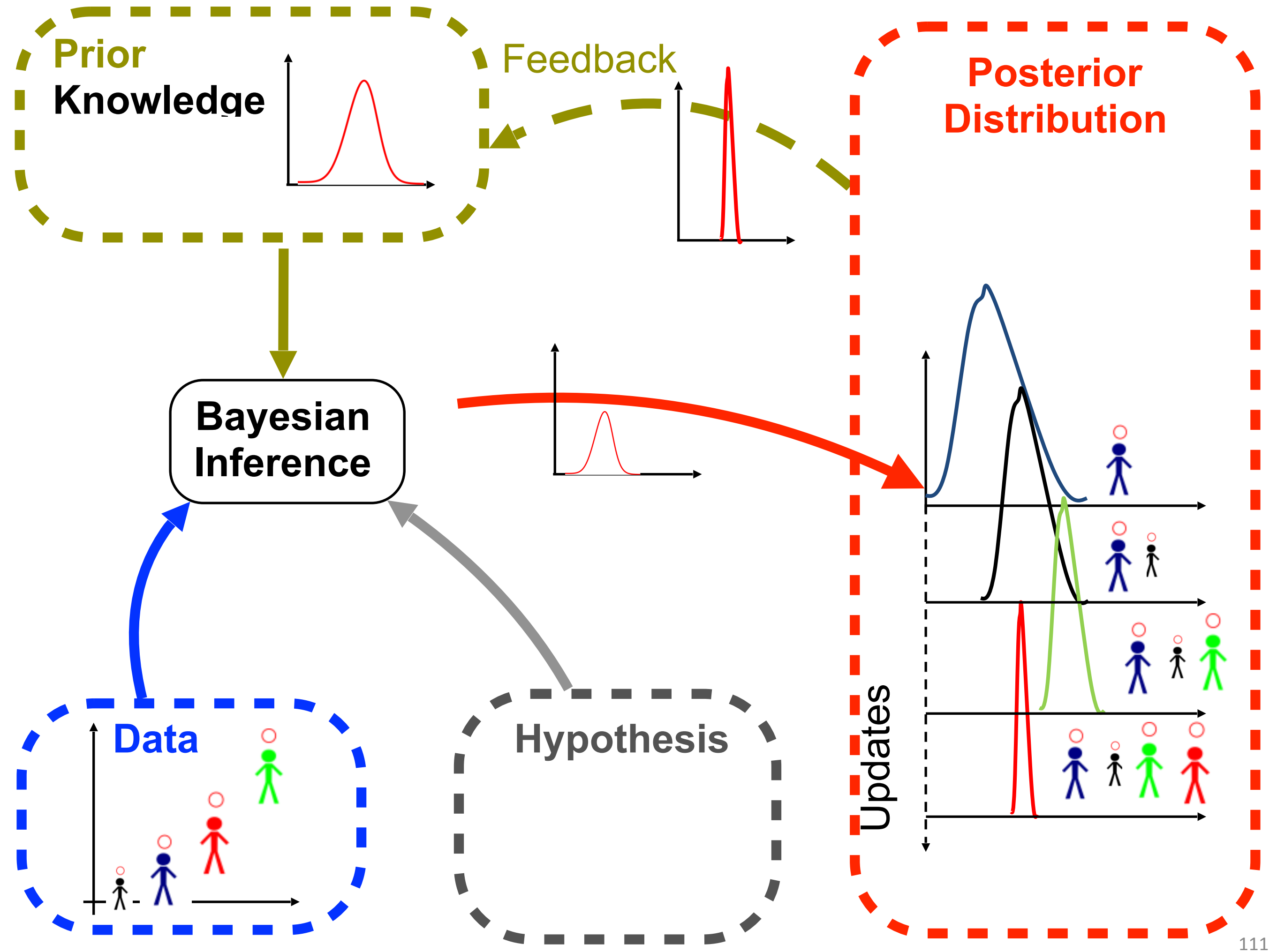
Hypothesis

Domain
expert









Conclusions

- **Understanding and optimisation of fracture of heterogeneous materials**
 - multi-scale methods are being developed
 - these methods are expensive
 - model selection remains an open problem
 - variability of the material properties exacerbate these difficulties
 - taking into account realistic situations remains elusive
 - coupling with sensing systems may be the future

... mechanical twinning

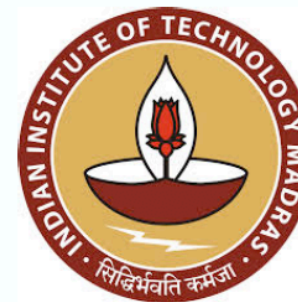
real-time simulations could also help engineers gain insight into complex non-intuitive phenomena by allowing to probe, quickly, the parameter space and design space



Partners and Funding



UNIVERSIDAD DE CHILE



UNIVERSIDAD POLITÉCNICA DE VALENCIA

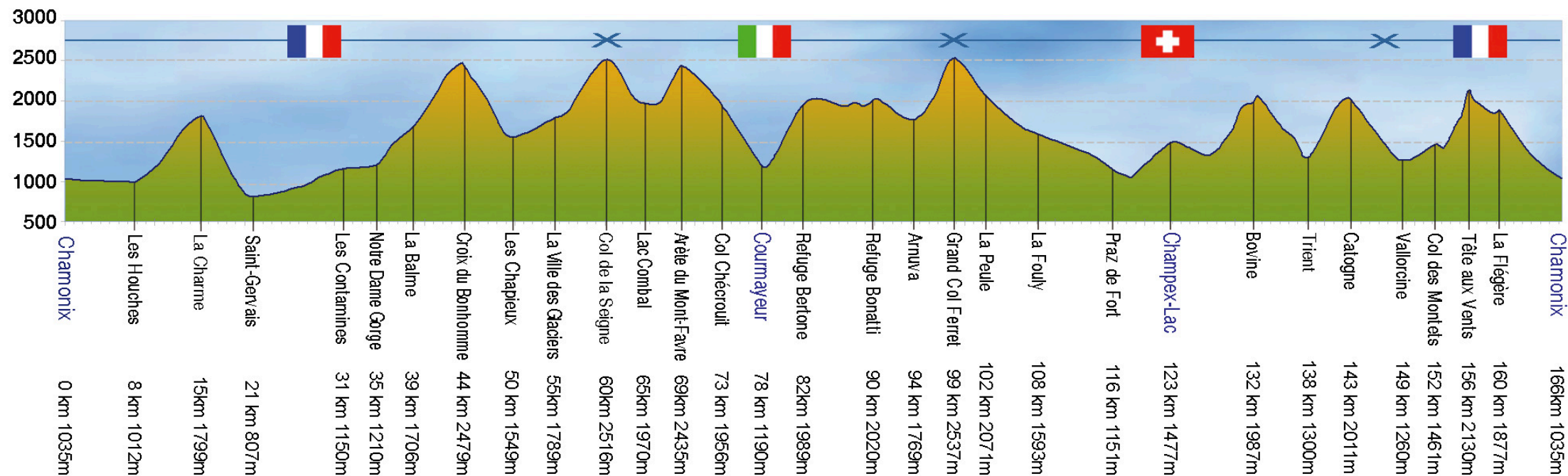


BOSCH
Technik fürs Leben

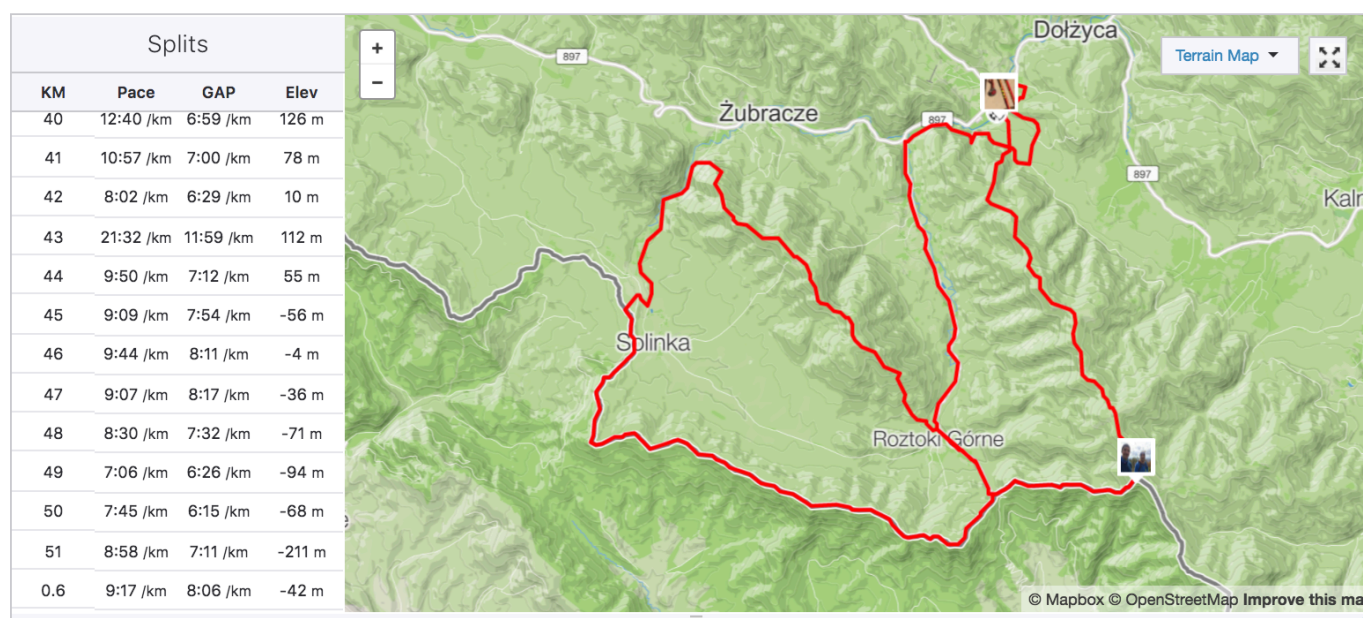


Rolls-Royce®

*inu*Tech



UTMB 177km running D+ 10,300m



52km running D+ 2500m

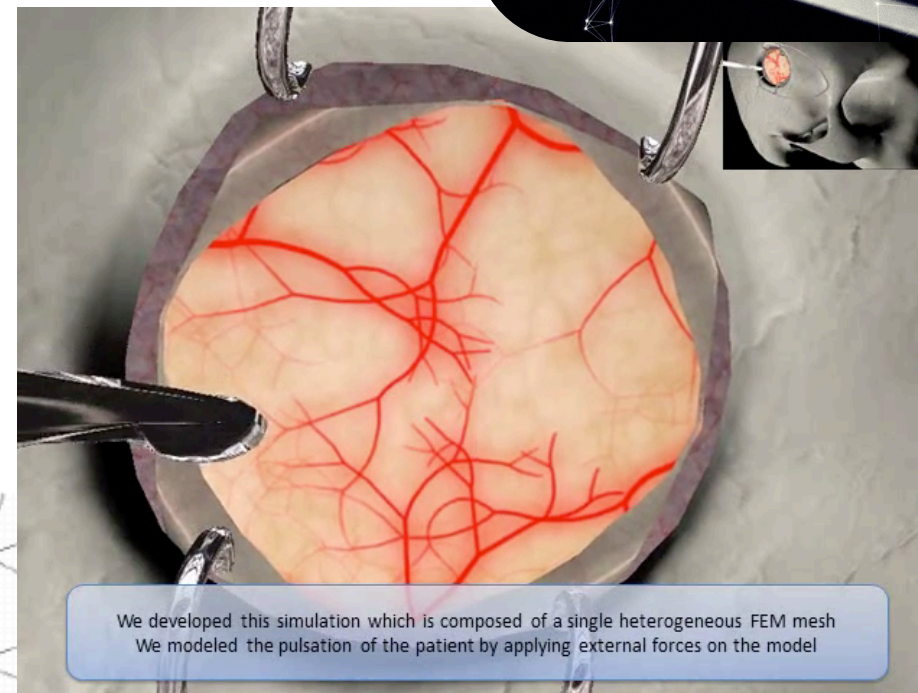


20km walking D+500m

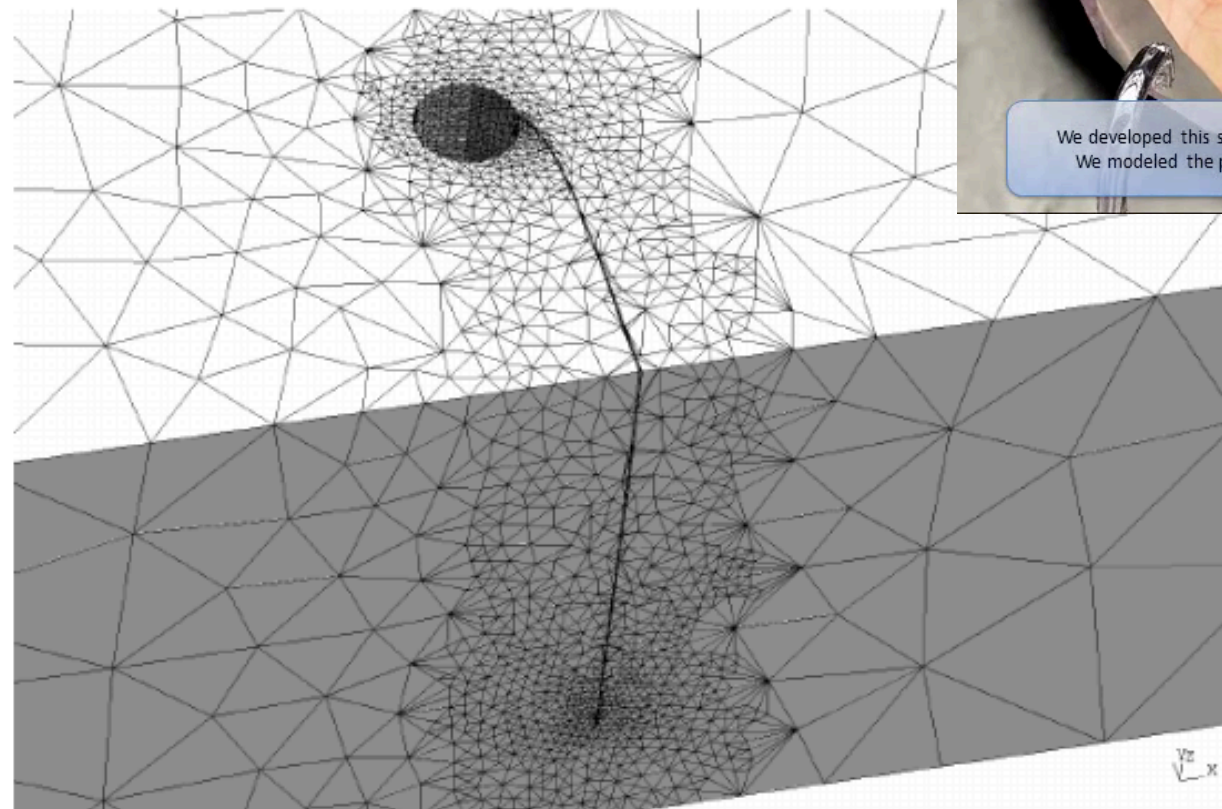


Alex Garland, *Ex Machina*, 2015

Personalised surgery
medicine



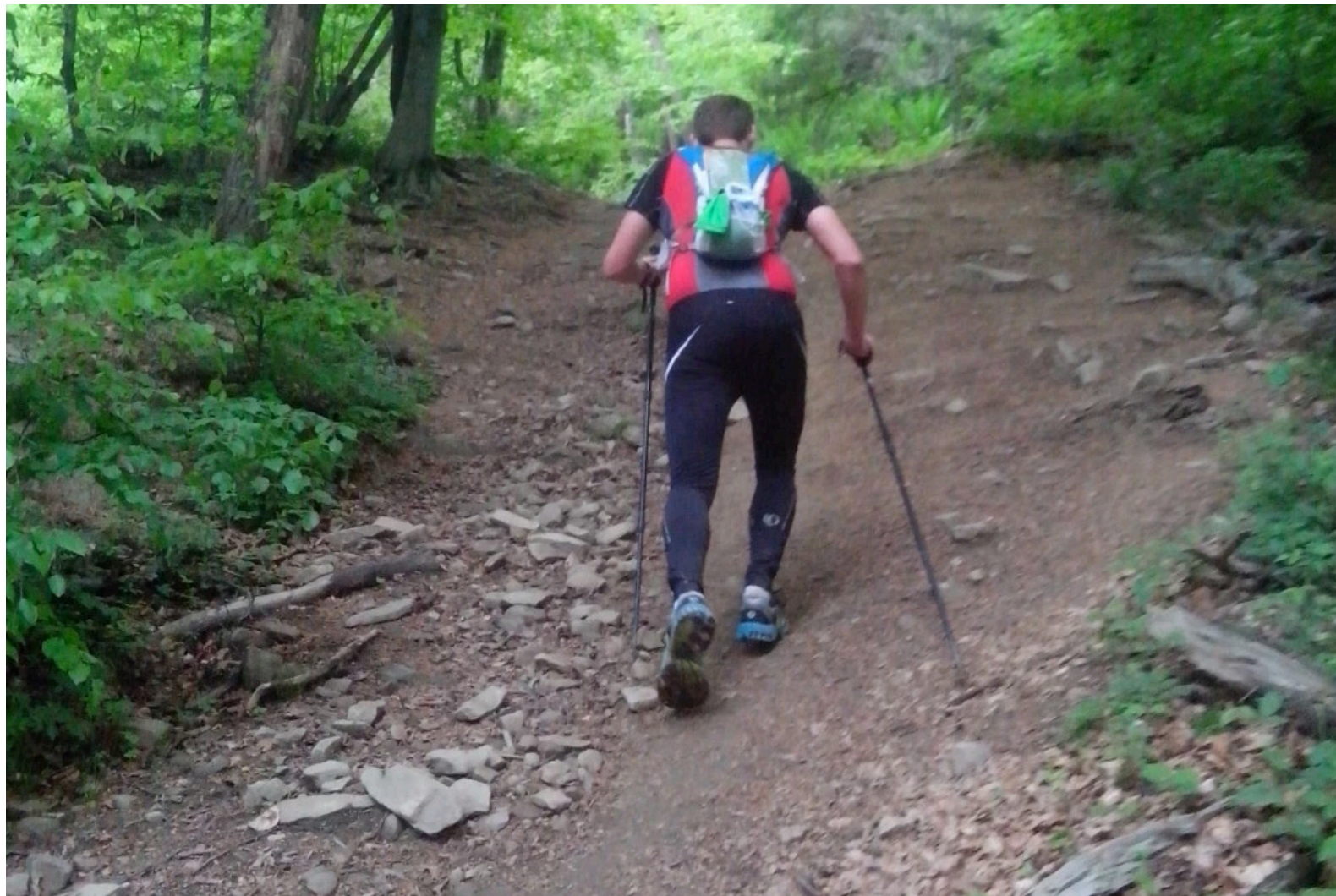
Error-controlled
surgical training



Error-controlled fracture mechanics

A bit of suffering...

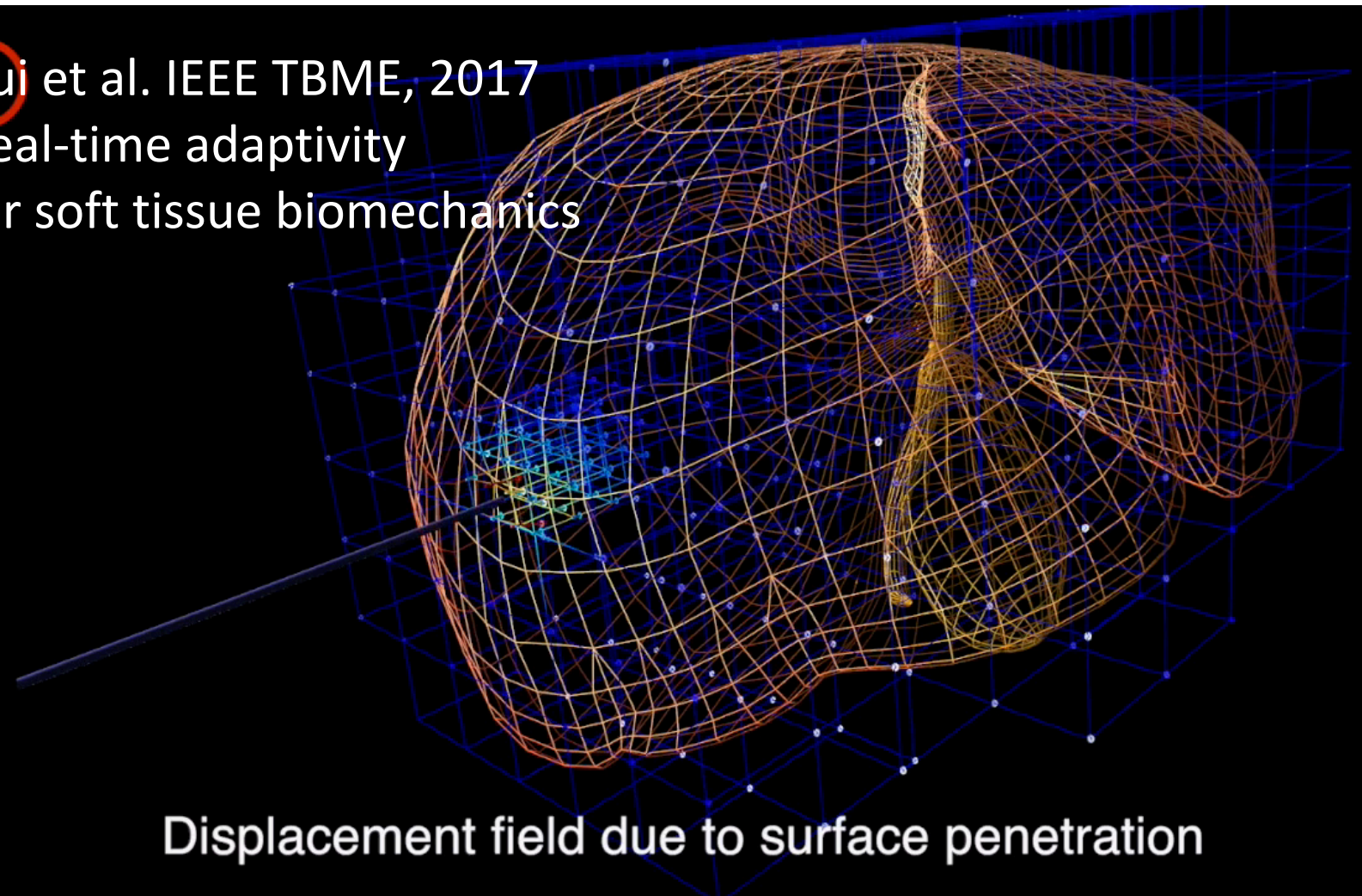
$$\overbrace{\pi(\text{param.}|\text{obs.})}^{\text{Posterior}} = \frac{\overbrace{\pi(\text{param.})}^{\text{Prior}} \times \overbrace{\pi(\text{obs.}|\text{param.})}^{\text{Likelihood}}}{\underbrace{\pi(\text{obs.})}_{\text{Evidence}}}$$



But much more fun!

$$\overbrace{\pi(\text{param.}|\text{obs.})}^{\text{Posterior}} = \frac{\overbrace{\pi(\text{param.})}^{\text{Prior}} \times \overbrace{\pi(\text{obs.}|\text{param.})}^{\text{Likelihood}}}{\underbrace{\pi(\text{obs.})}_{\text{Evidence}}}$$

Bui et al. IEEE TBME, 2017
Real-time adaptivity
for soft tissue biomechanics



Thank you for your attention!



<http://legato-team.eu>

Download the presentation here: <http://hdl.handle.net/10993/34088>



CAST

Numerical analysis

LMB, Besançon, UMR CNRS 6623 (Franz Chouly, Alexei Lozinski)

LMAP, Pau, UMR CNRS 5142 (Roland Becker, Daniela Capatina, Robert Luce)

IMAG, Montpellier, UMR CNRS 5149 (Vanessa Lleras)

IMT, Toulouse, UMR CNRS 5219 (Patrick Hild)

ICJ, Lyon, UMR CNRS 5208 (Yves Renard)

MATHISCE, EPFL, Lausanne, Suisse (Marco Picasso)

Computational mechanics and modelling

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LMB, Besançon, UMR CNRS 6623 (Julien Yves Rolland)

National Physics Laboratory, Londres, Royaume-Uni (Stéphane Chrétien)

I2M, Marseille, UMR CNRS 7373 (Michel Duprez, Florence Hubert)

Meshes

SME TexiSense, Grenoble (Marek Bucki, Mathieu Bailet, Antoine Perrier)

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ERC RealTCut

Agence Math Entreprises (“Convention Projets Exploratoires MethASim”).

CAST

Biomechanics

TIMC-IMAG, Grenoble, UMR CNRS 5525 (Yohan Payan, Jacques Ohayon, Jean-Louis Martiel)

GIPSA-Lab, Grenoble, UMR CNRS 5216 (Pascal Perrier)

Institut de Biomécanique Humaine Georges Charpak, Arts&Métiers Paris-Tech (Pierre-Yves Rohan)

FEMTO-ST, Besançon, UMR CNRS 6174 (Emmanuelle Jacquet, Jérôme Chambert, Arnaud Lejeune)

Reference

S Bordas, M Bucki, F Chouly, M Duprez, V Lleras, C Lobos, A Lozinski, PY Rohan, S Tomar. Quantifying discretization errors for soft-tissue simulation in computer assisted surgery : a preliminary study. 2017. hal-01616322. Proceedings EuroMech 595

Meshes

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ERC RealTCut

Agence Math Entreprises (“Convention Projets Exploratoires MethASim”).

More details

**Multi-scale fracture FOE,
Seattle**

[http://orbilu.uni.lu/
bitstream/10993/18804/1/
FOE_Seattle_Bordas.pdf](http://orbilu.uni.lu/bitstream/10993/18804/1/FOE_Seattle_Bordas.pdf)

[http://orbilu.uni.lu/
bitstream/10993/18804/2/
FOE_Seattle_Bordas_Movi
e.m4v](http://orbilu.uni.lu/bitstream/10993/18804/2/FOE_Seattle_Bordas_Movie.m4v)

**3D Fracture isogeometric
methods**

Other presentations and papers

What makes Data Science different?

<http://hdl.handle.net/10993/30235>

Error control in deep brain stimulation simulations

<http://hdl.handle.net/10993/30937>

Energy-minimal crack growth

<http://hdl.handle.net/10993/29414>

Uncertainty Quantification in biomechanics

<http://hdl.handle.net/10993/28618>

Real-time error estimation for needle insertion

<http://hdl.handle.net/10993/28624>

Bayesian parameter identification in mechanics

<http://orbi.lu.uni.lu/bitstream/10993/29561/3/template.pdf>

<http://orbi.lu.uni.lu/bitstream/10993/28631/1/1606.02422v4.pdf>

Plenary talk at DAMAS2017, Kitakyushu, Japan

<http://hdl.handle.net/10993/31720>

Plenary talk at XDMS2017, Umeå, Sweden

<http://orbi.lu.uni.lu/handle/10993/31487>

2017 Short course Lecture Notes, CISM, Udine, Italy

<http://hdl.handle.net/10993/31585>

Other course material

http://orbi.lu.uni.lu/bitstream/10993/31585/37/UDINE_2017_ShortCoursePDF_files_BORDAS.zip

http://orbi.lu.uni.lu/bitstream/10993/31585/38/UDINE_2017_CourseNotes_Powerpoint_BORDAS.zip

http://orbi.lu.uni.lu/bitstream/10993/31585/39/UDINE_2017_CourseNotes_Keynote_BORDAS.zip

http://orbi.lu.uni.lu/bitstream/10993/31585/40/UDINE_2017_handwrittenNotes_BORDAS.pptx

ABOUT THE AUTHOR

Live your life to the fullest

The Butcher's Race

by haveolimits



“Somebody behind me is gasping wheezily. The branches are beating my calves and face, the stones splattering from under my shoes. I hear the voice of tens of feet. Around me the woods and the darkness. High in the beech branches, the flashing moon.