

# Using Bayes' theorem to infer the material parameters of human tissue

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# Overview

- Motivation.
- Bayesian approach to inversion.
- Relate classical optimisation techniques to the Bayesian inversion approach.
- Using a domain specific language for variational forms to solve the equations.
- Low-rank updates to deal with high-dimensional posterior covariance.
- Example problem: sparse surface observations of a solid block.

Motivation.

PHILIPS

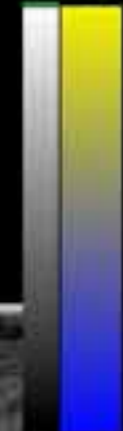
L12-5/SmPrt AdBrst

FR 15Hz  
R1

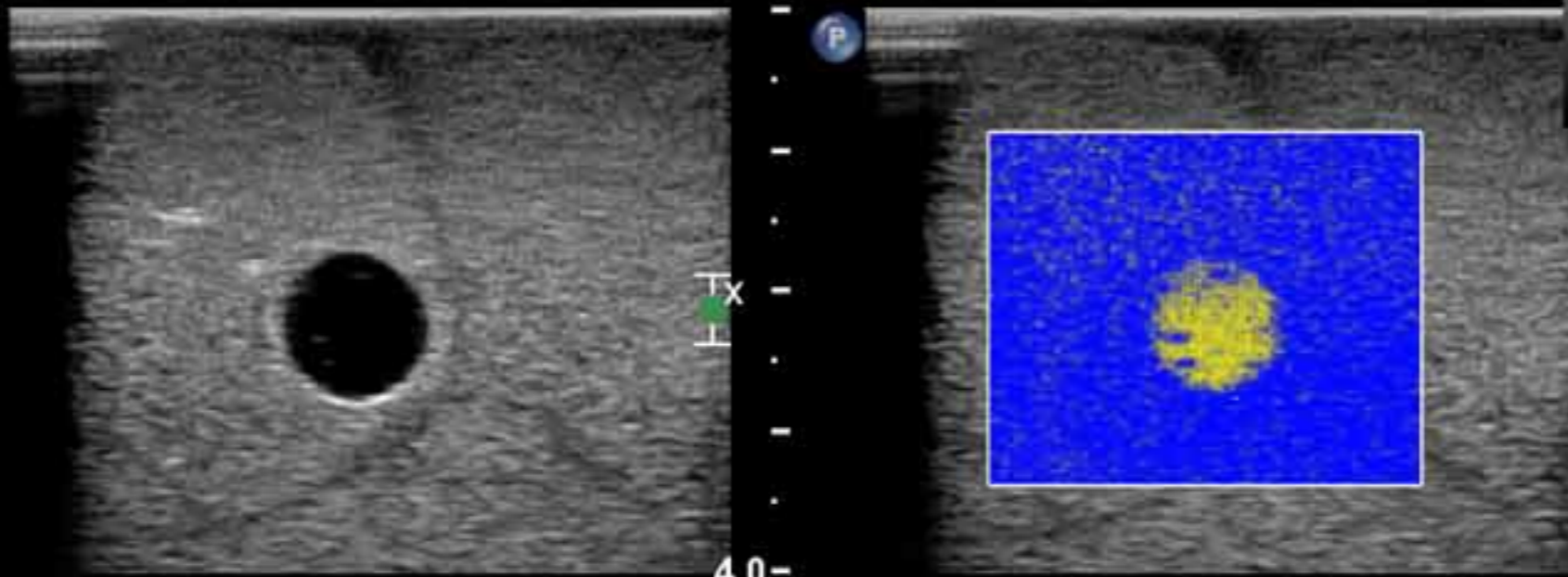
2D  
77%  
C 60  
P Med  
Res

ELASTO:  
Opt 1  
S Med  
P High  
D Med

M3 M2  
A

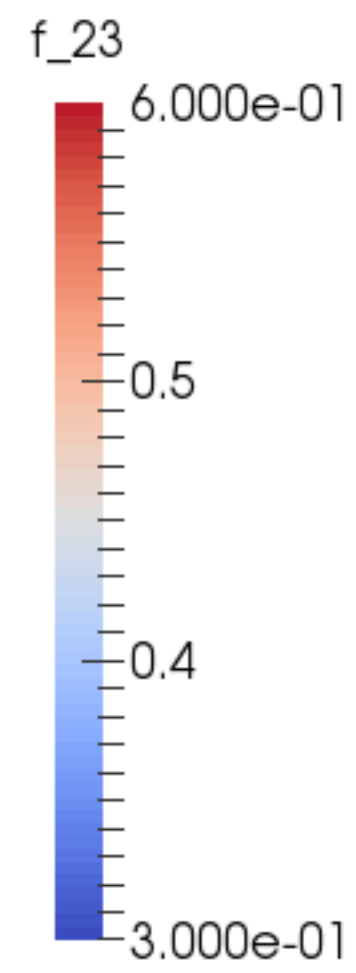
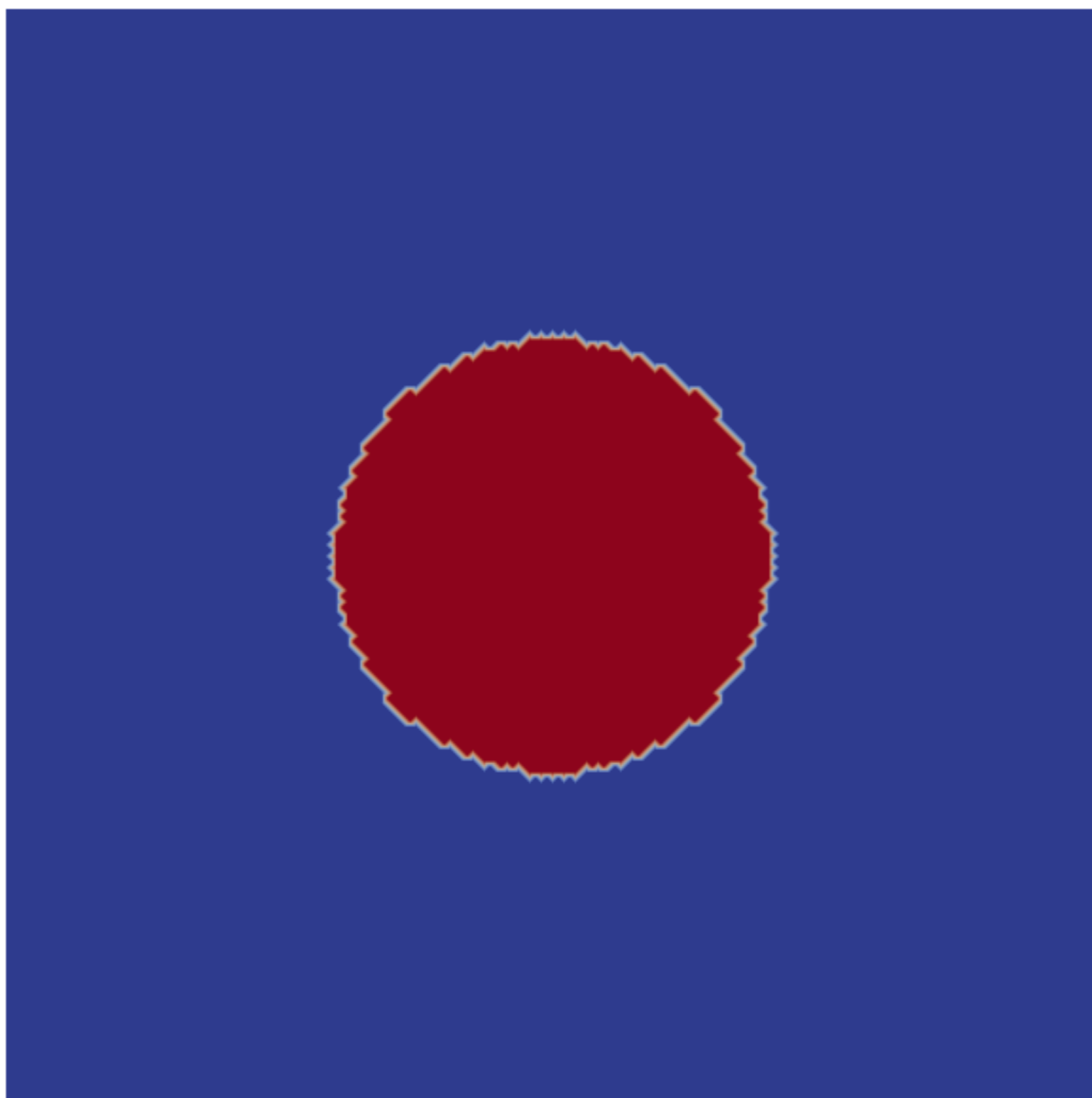


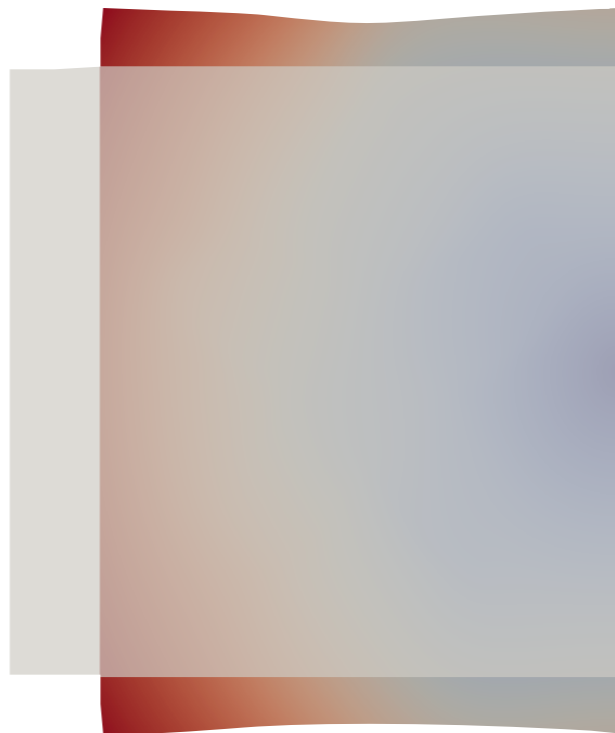
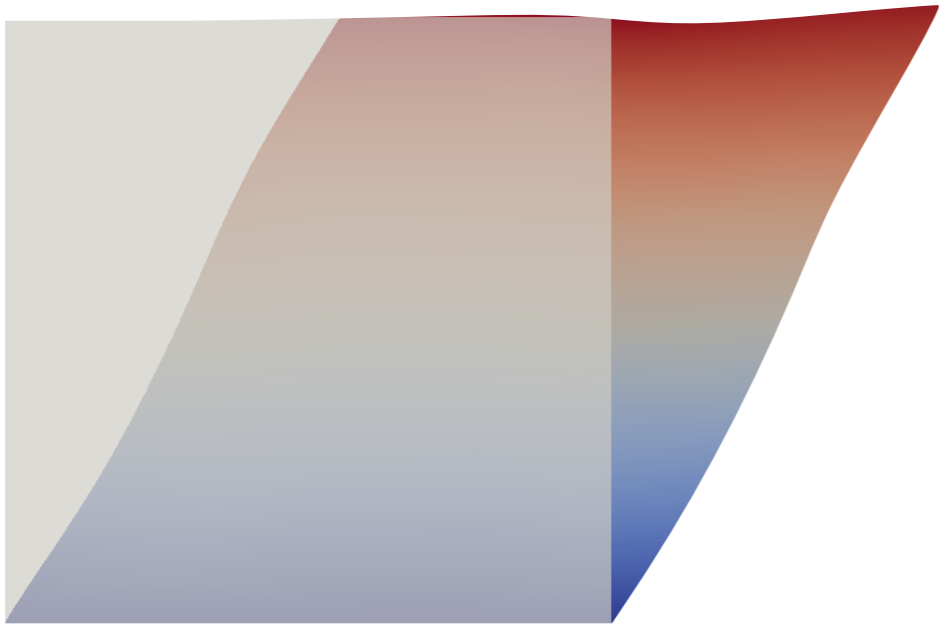
E

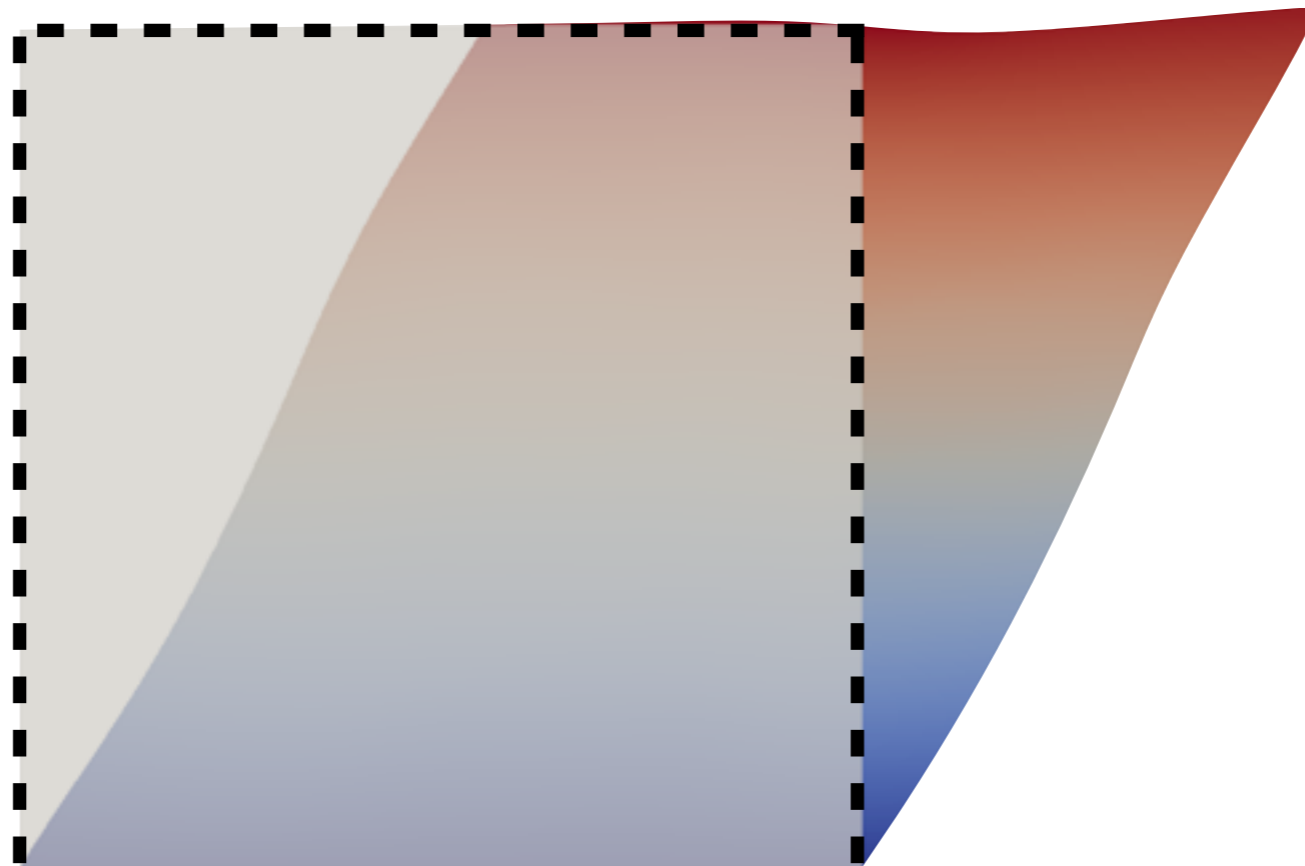


BREAST CYST  
ANECHOIC IMAGING

Source: Phillips







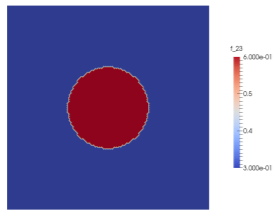
Q: What can we infer about the parameters inside the domain, just from displacement observations on the outside?

Q: Which parameters am I most uncertain about?

# Framework



$$X \sim \mathcal{N}(\bar{x}, \Gamma_{\text{prior}})$$



Parameter

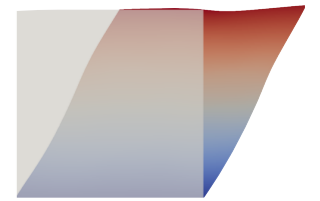
$x$

Map

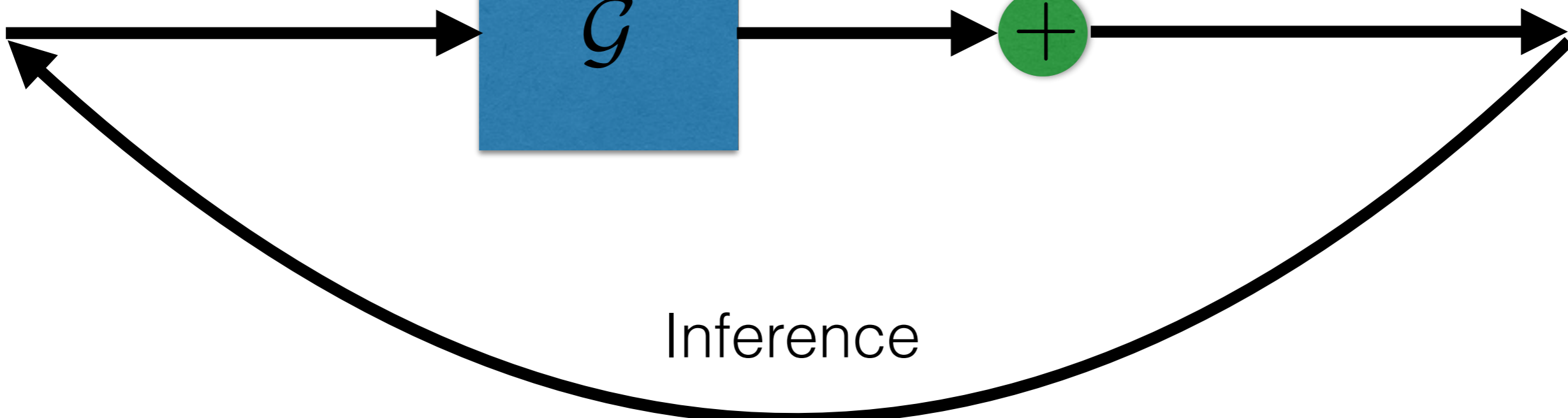


$y$

$$E \sim \mathcal{N}(0, \Gamma_{\text{noise}})$$



$y_{\text{obs}}$



Inference

$$\pi_{\text{posterior}}(x | y) \propto \pi_{\text{likelihood}}(y | x) \pi_{\text{prior}}(x)$$

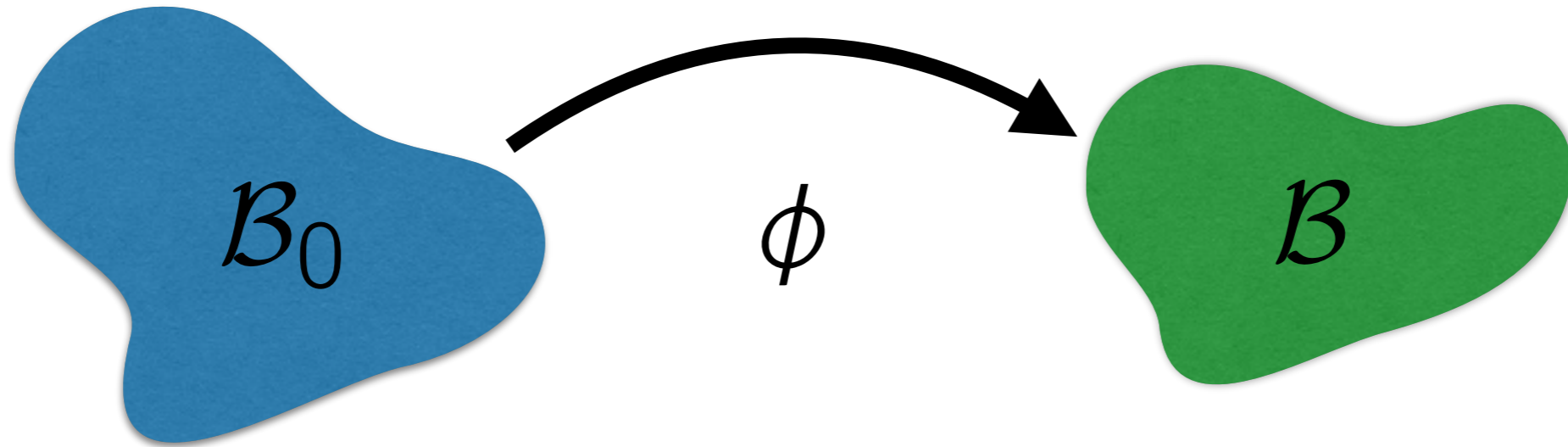
$$\pi_{\text{posterior}}(x|y) \propto \exp \left( -\frac{1}{2} \|y - \mathcal{G}(u)\|_{\Gamma_{\text{noise}}^{-1}}^2 - \frac{1}{2} \|x - \bar{x}\|_{\Gamma_{\text{prior}}^{-1}} \right)$$

$$\mathcal{G} : \mathcal{X} \rightarrow \mathcal{Y}$$

## **Inverse Problems: A Bayesian perspective.**

*Stuart, Acta Numerica (2010).*

*Contribution:* Bayesian inverse problems in an infinite-dimensional setting. *When is a Bayesian inverse problem well-posed?*



The displacements  $y$  for a given material parameter  $x$  are defined by a the minimum point of the following Lagrangian:

$$\mathcal{L}(y, x) = \int_{\Omega} \psi(y, x) dx - \int_{\Gamma} t \cdot y ds$$

where the energy density functional  $\psi$  is defined through the following equations:

$$\psi(u, x) = \frac{x}{2}(I_c - d) - x \ln(J) + \frac{\lambda}{2} \ln(J)^2,$$

$$\mathbf{F} = \frac{\partial \phi}{\partial X} = \mathbf{I} + \nabla y,$$

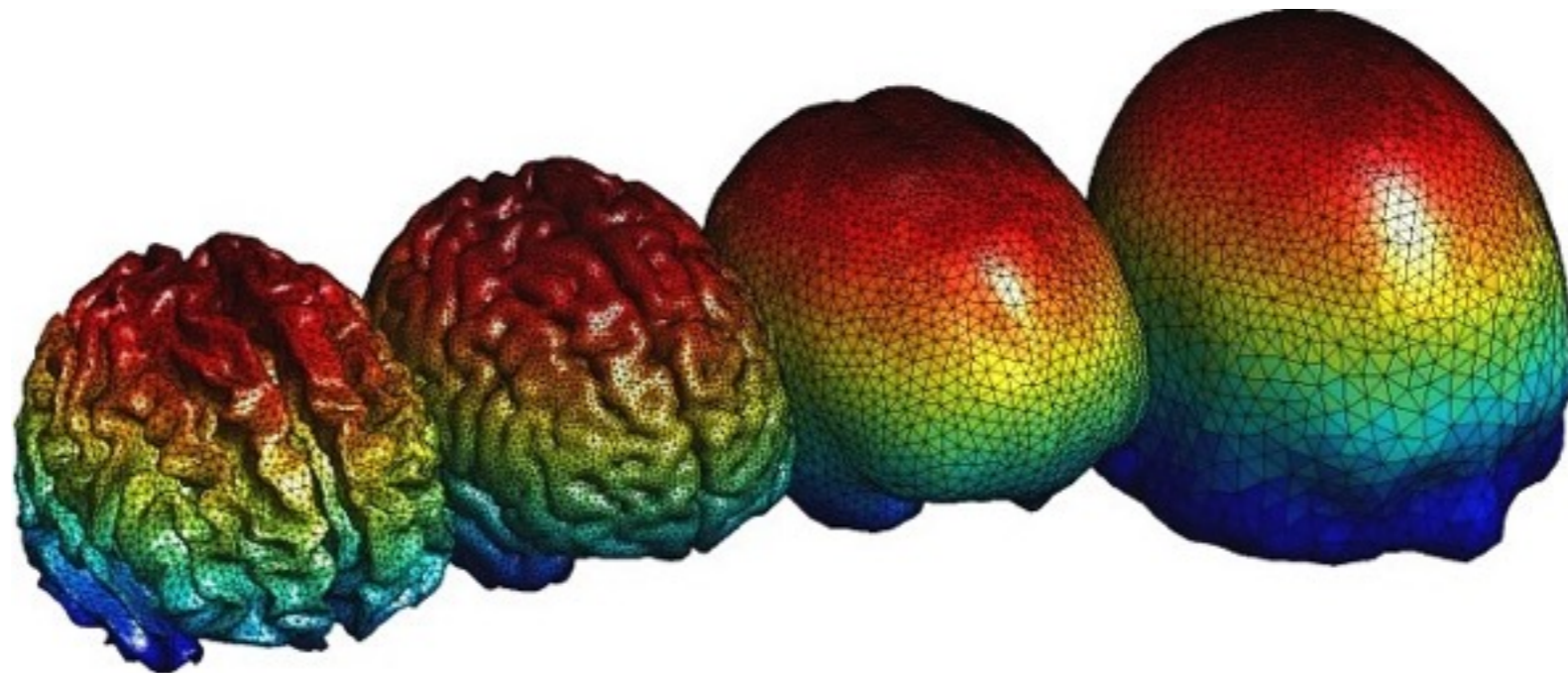
$$\mathbf{C} = \mathbf{F}^T \mathbf{F},$$

$$I_c = \text{tr}(\mathbf{C}),$$

$$J = \det \mathbf{F}.$$

Even once discretised (Finite Element Method)

$$\mathcal{G}_h : \mathbb{R}^n \rightarrow \mathbb{R}^m$$



Colin27 brain atlas

20% extension test, 16 Core Xeon, 1.12 million cells, ~29 secs.

$$n = 1,112,000$$

# Problems

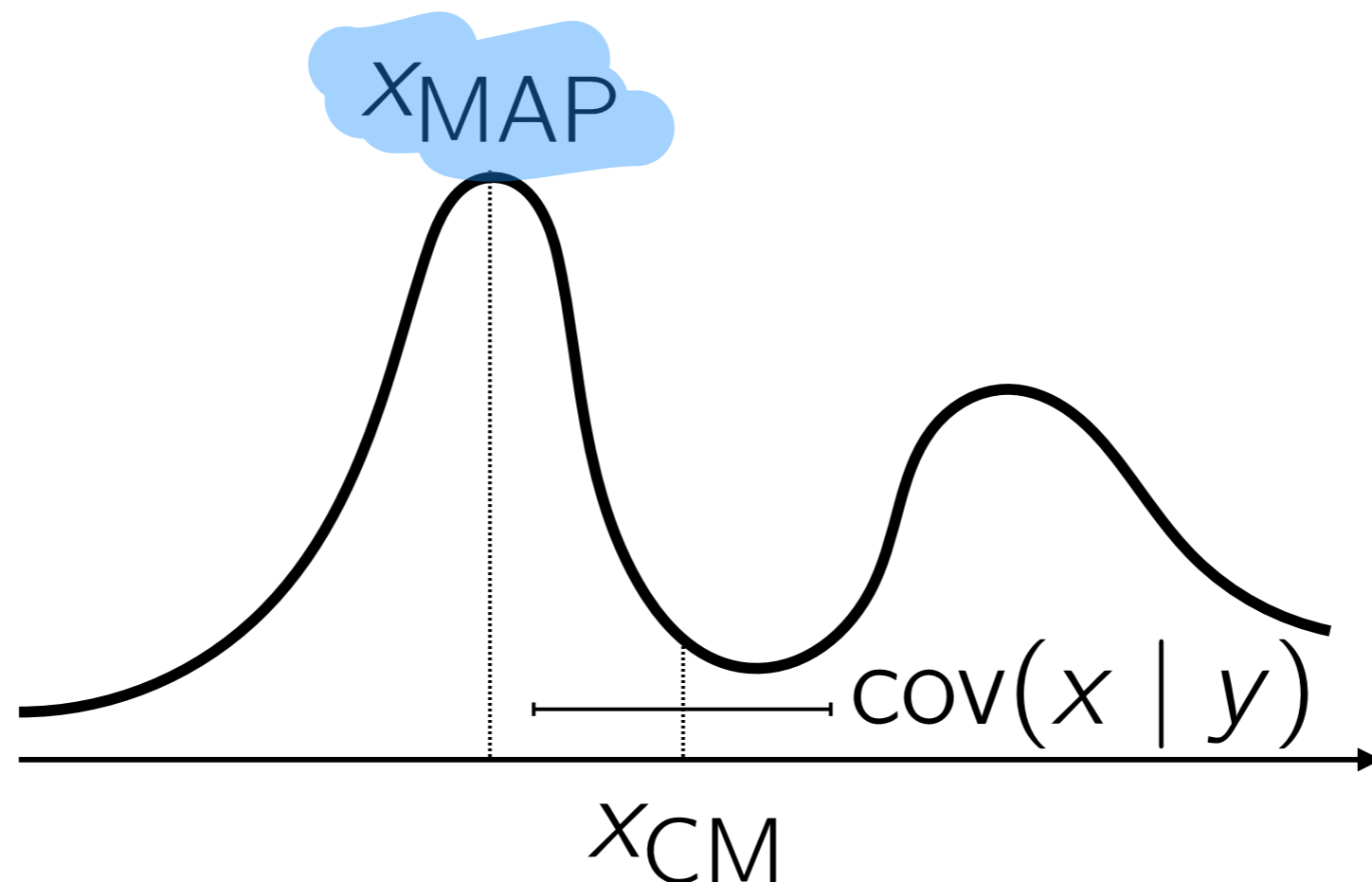
- Evaluating parameter-to-observable map is *very* expensive.
- Discretised parameter space can be *very* large.
- *Outcome:* Exploring posterior with ‘traditional sampling’ is not going to work.

# Solutions

1. Connect Bayesian approach to ideas from classical optimisation. Using derivatives of posterior in parameter-space (Girolami).
2. Exploiting low-rank structure of prior to posterior covariance updates (Flath 2012, Spantini 2015).

$$\pi_{\text{posterior}}(x | y) \propto \pi_{\text{likelihood}}(y | x)\pi_{\text{prior}}(x)$$

$$x_{\text{MAP}} = \arg \max_{x \in \mathbb{R}^n} \pi_{\text{posterior}}(x | y)$$



# Linearise

$$y = Ax$$

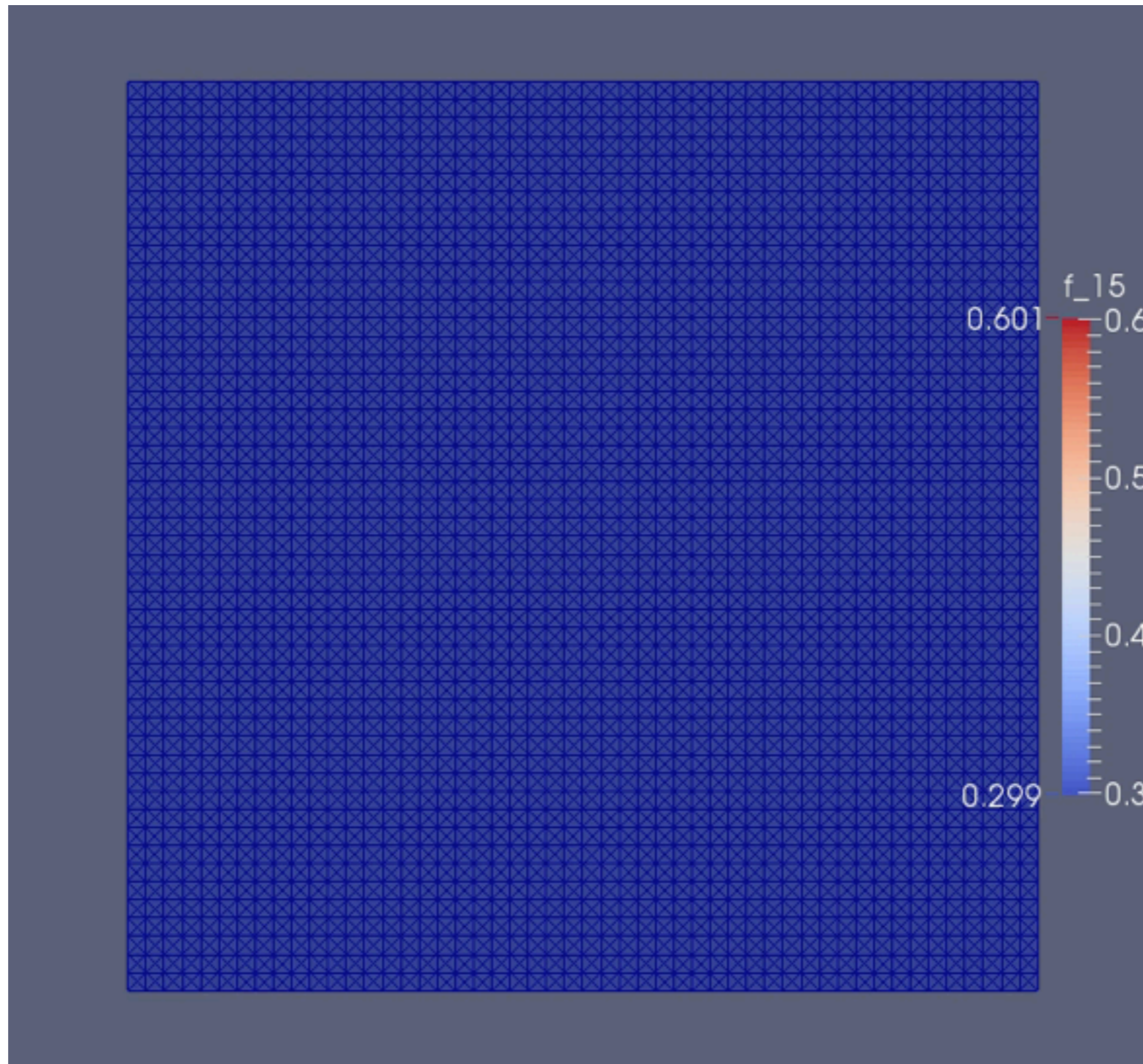
$$-\ln \pi_{\text{posterior}}(x|y) = \frac{1}{2} \|y - Ax\|_{\Gamma_{\text{noise}}^{-1}}^2 + \frac{1}{2} \|x - x_0\|_{\Gamma_{\text{prior}}^{-1}}$$



# Take the derivative

$$\begin{aligned} g(x_{\text{MAP}}) &:= \nabla_x \left( \frac{1}{2} \|y - \mathbf{A}x\|_{\mathbf{\Gamma}_{\text{noise}}^{-1}}^2 + \frac{1}{2} \|x - x_0\|_{\mathbf{\Gamma}_{\text{prior}}^{-1}}^2 \right) \Big|_{x=x_{\text{map}}} \\ &= \mathbf{A}^T \mathbf{\Gamma}_{\text{noise}}^{-1} (y - \mathbf{A}x_{\text{map}}) + \mathbf{\Gamma}_{\text{prior}}^{-1} (x_{\text{map}} - x_0) \\ &= 0 \end{aligned}$$

$$x_{\text{MAP}} = \left( \mathbf{\Gamma}_{\text{prior}}^{-1} - \mathbf{A}^T \mathbf{\Gamma}_{\text{noise}}^{-1} \mathbf{A} \right)^{-1} \left( \mathbf{A}^T \mathbf{\Gamma}_{\text{noise}}^{-1} y + \mathbf{\Gamma}_{\text{prior}}^{-1} x_0 \right)$$



*MAP estimate.* Bound-constrained Quasi-Newton BLMVM with More-Thuente line search and ‘correct’ Riesz map.

and the second derivative...

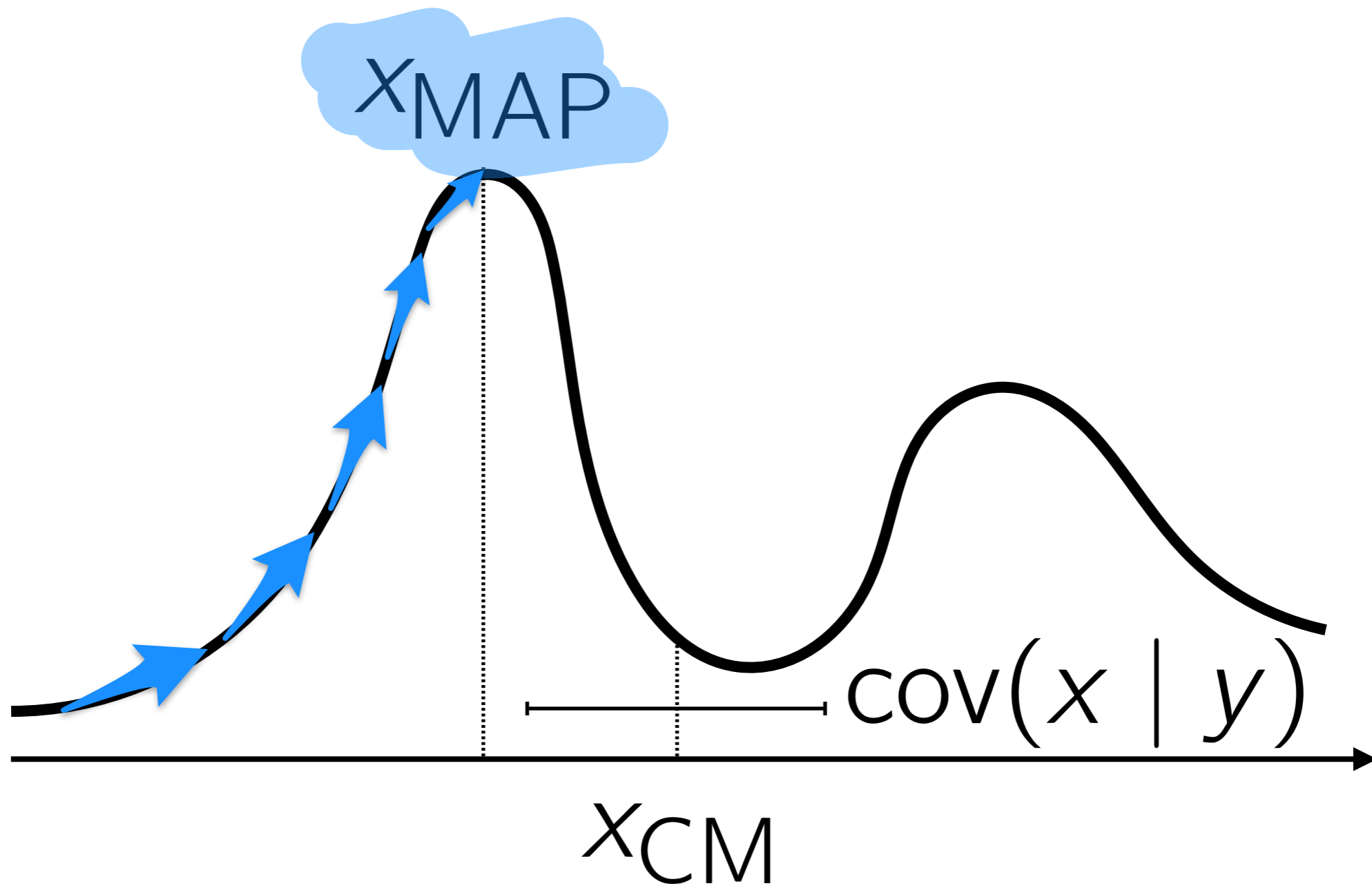
$$\mathbf{H} := \nabla_x g = \mathbf{\Gamma}_{\text{prior}}^{-1} - \mathbf{A}^T \mathbf{\Gamma}_{\text{noise}}^{-1} \mathbf{A}$$

$$x_{\text{MAP}} = \left( \mathbf{\Gamma}_{\text{prior}}^{-1} - \mathbf{A}^T \mathbf{\Gamma}_{\text{noise}}^{-1} \mathbf{A} \right)^{-1} \left( \mathbf{A}^T \mathbf{\Gamma}_{\text{noise}}^{-1} y + \mathbf{\Gamma}_{\text{prior}}^{-1} x_0 \right)$$

(After a fair bit of manipulation...)

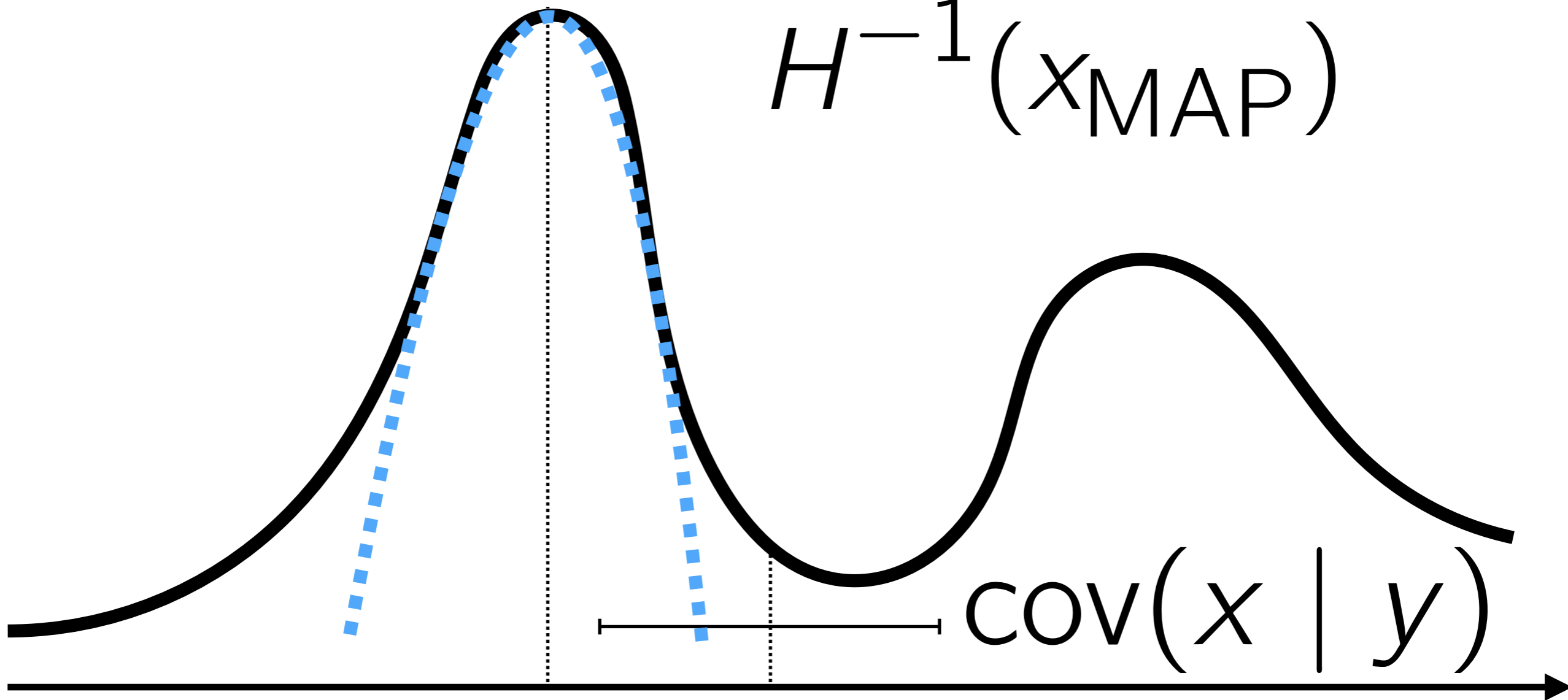
$$\pi_{\text{posterior}} \sim \mathcal{N}(x_{\text{MAP}}, \mathbf{H}^{-1})$$

# MAP estimate



$x_{\text{MAP}}$

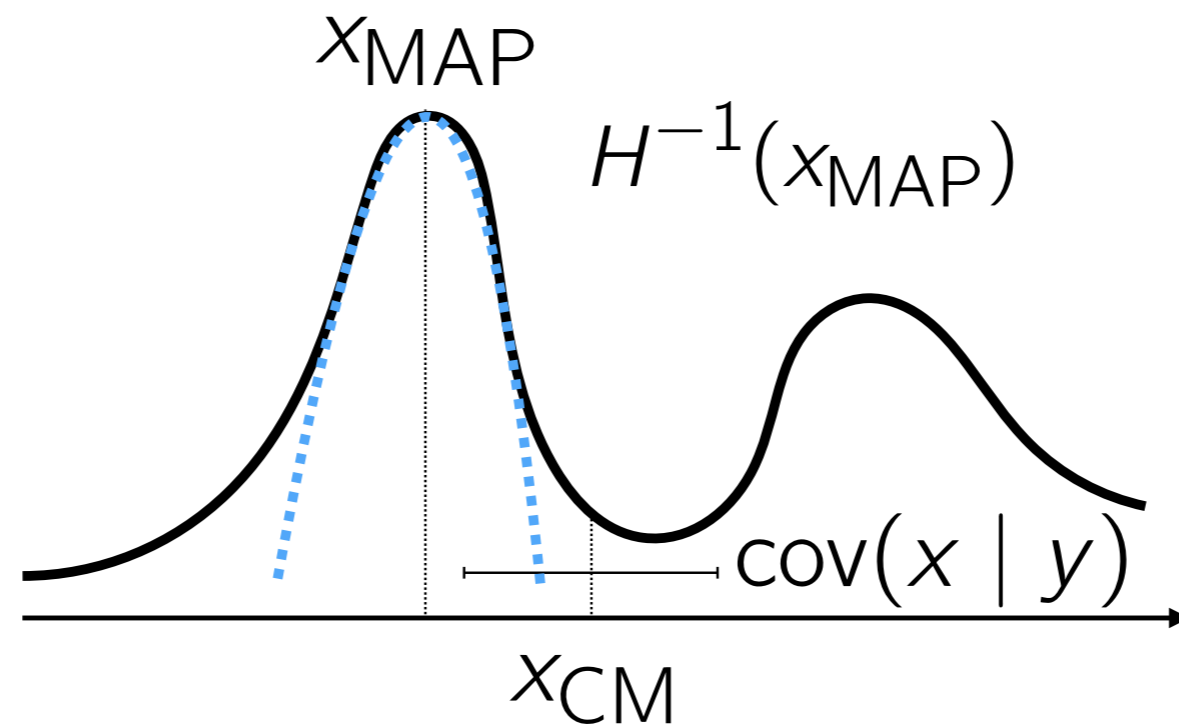
$H^{-1}(x_{\text{MAP}})$



$x_{\text{CM}}$

$$\pi_{\text{posterior}} \sim \mathcal{N}(x_{\text{MAP}}, \mathbf{H}^{-1})$$

$$\pi_{\text{posterior}}^{\text{approx}} \sim \mathcal{N}(x_{\text{MAP}}, \mathbf{H}^{-1}(x_{\text{MAP}}))$$



# Tools

- The FEniCS Project is a collection of free software for the automated, efficient solution of differential equations using the finite element method.
- dolfin-adjoint automatically derives the discrete adjoint, tangent linear and higher-order adjoint models from a high-level description of the forward model.



<http://fenicsproject.org>

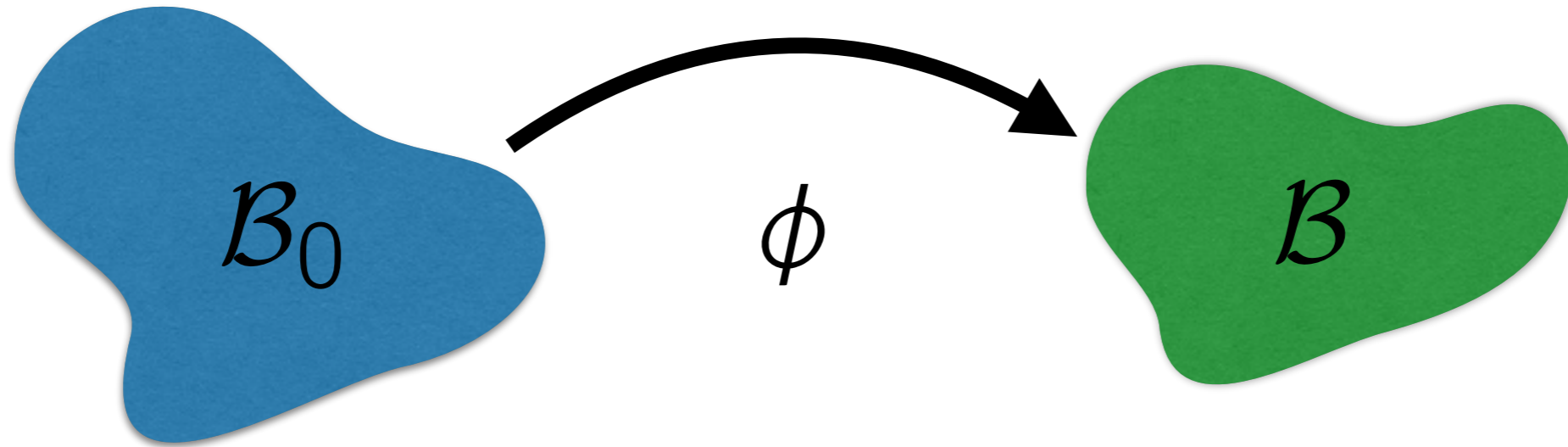
Wells, Logg, Rognes, Kirby and many, many others...



**dolfin-adjoint**

<http://www.dolfin-adjoint.org>

Farrell, Funke, Ham and Rognes.  
2015 Wilkinson Prize for Numerical Software.



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```

from dolfin import *
mesh = UnitSquareMesh(32, 32)

U = VectorFunctionSpace(mesh, "CG", 1)
V = FunctionSpace(mesh, "CG", 1)
# solution
u = Function(U)
# test functions
v = TestFunction(U)
# incremental solution
du = TrialFunction(U)
x = interpolate(Constant(1.0), V)
lambda = interpolate(Constant(100.0), V)

dims = mesh.type().dim()
I = Identity(dims)
F = I + grad(u)
C = F.T * F
J = det(F)
Ic = tr(C)

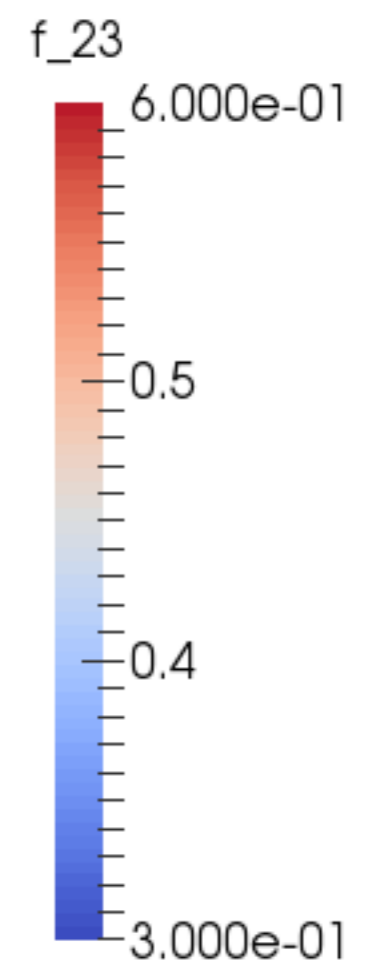
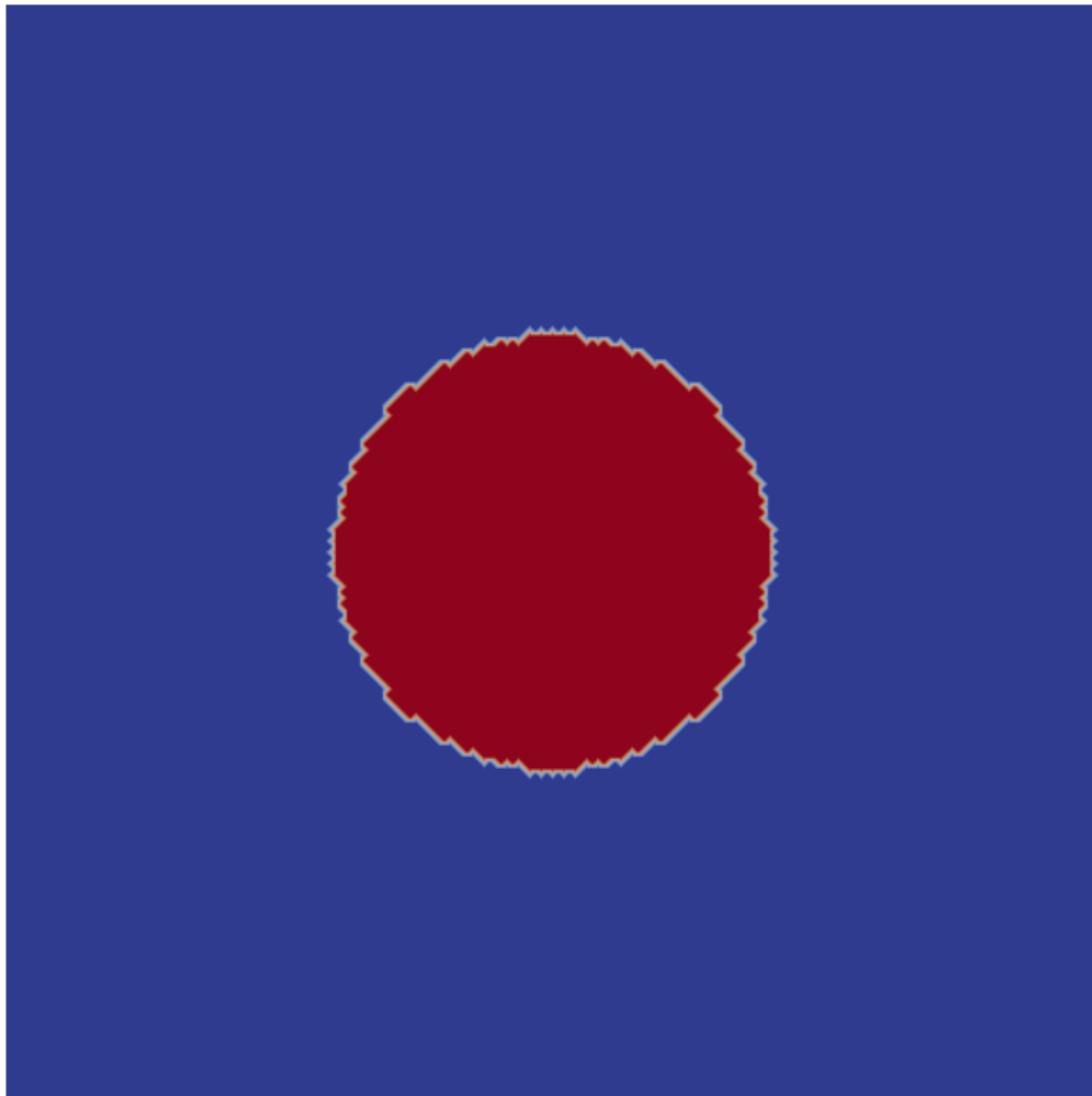
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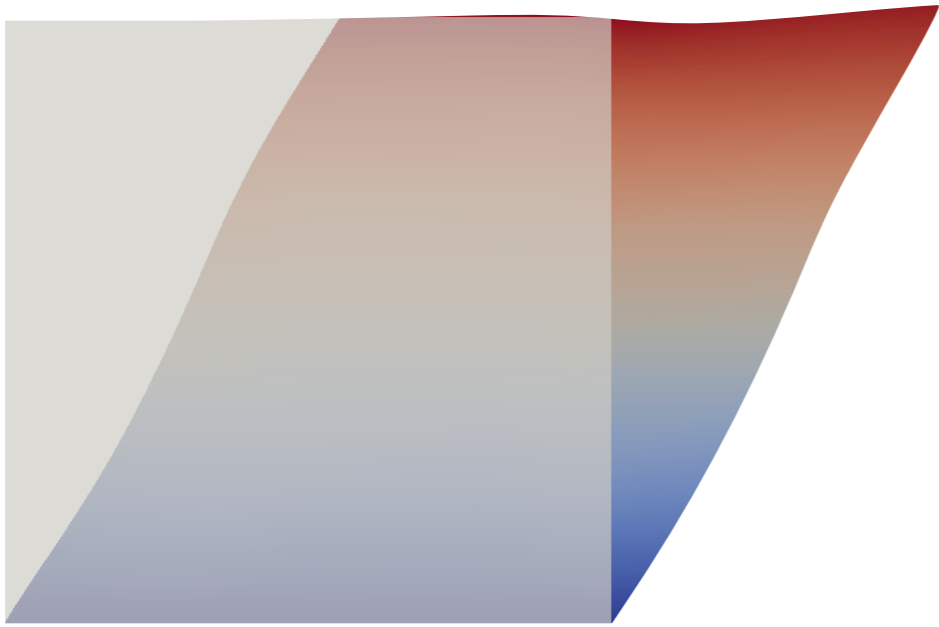
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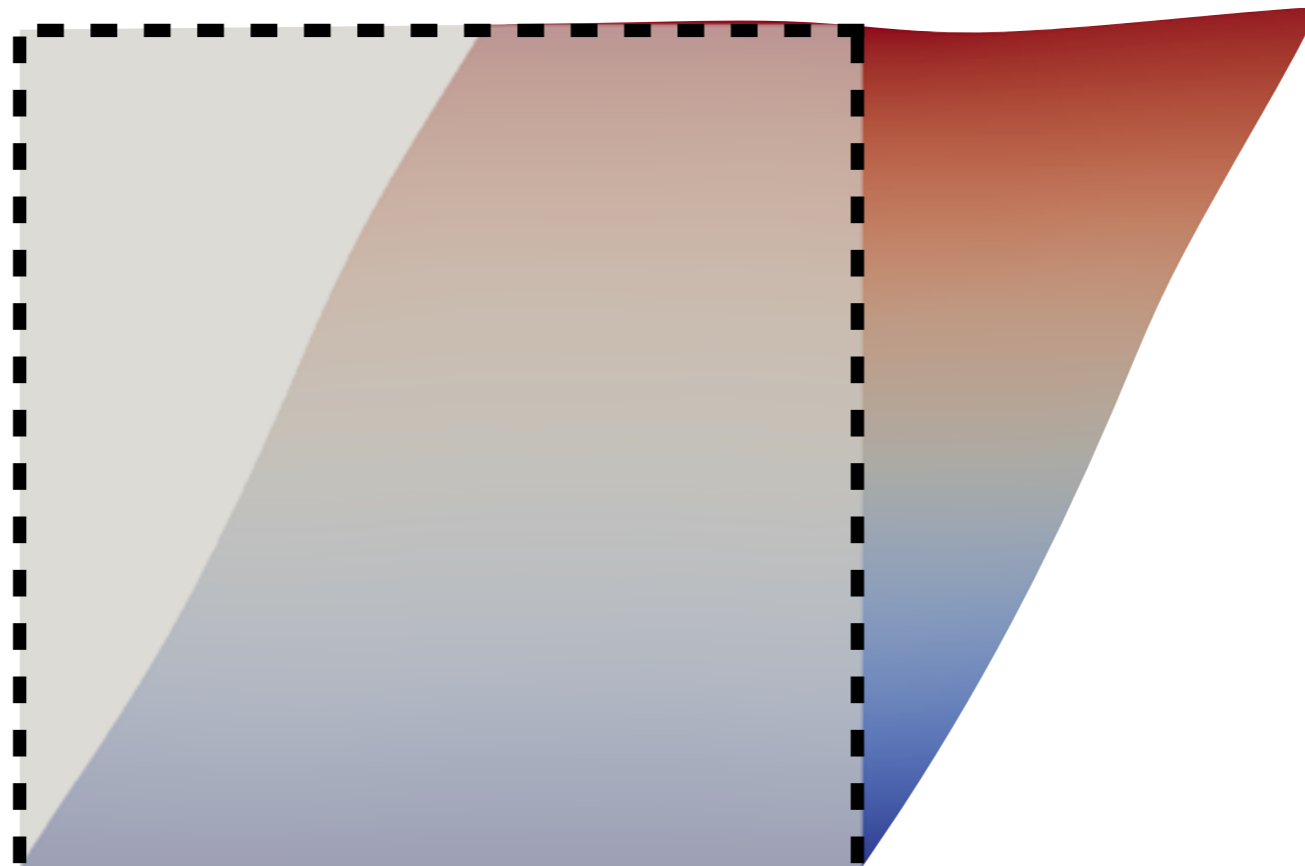
phi = (x/2.0)*(Ic - dims) - x*ln(J) + (lambda/
2.0)*(ln(J))**2
Pi = phi*dx
# gateux derivative with respect to u in direction v
F = derivative(Pi, u, v)
# and with respect to u in direction du
J = derivative(F, u, du)

u_h = Function(U)
F_h = replace(F, {u: u_h})
J_h = replace(J, {u: u_h})
solve(F_h == 0, u_h, bcs, J=J_h)

```

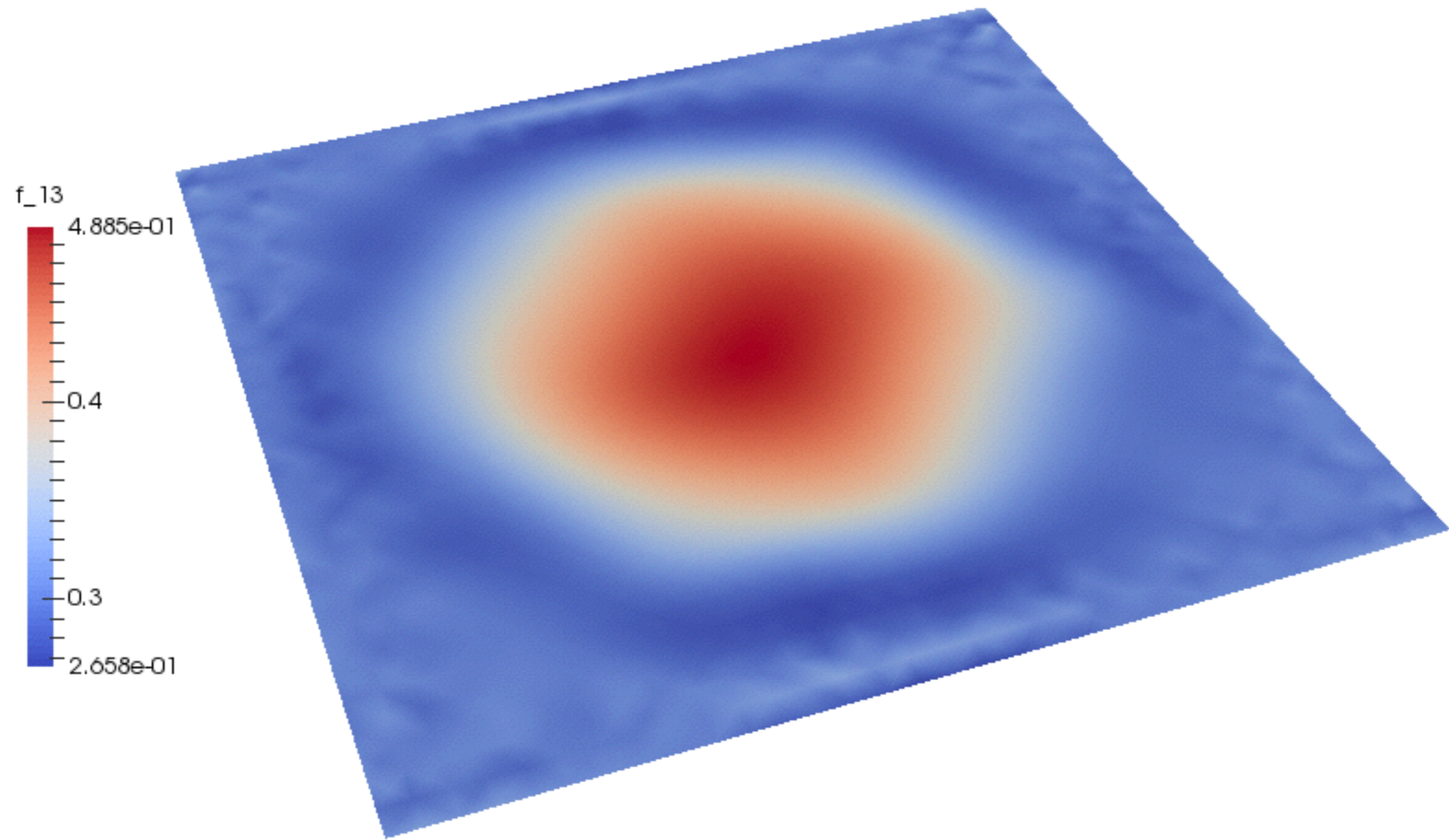






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$X_{map}$

# Optimal low-rank updates

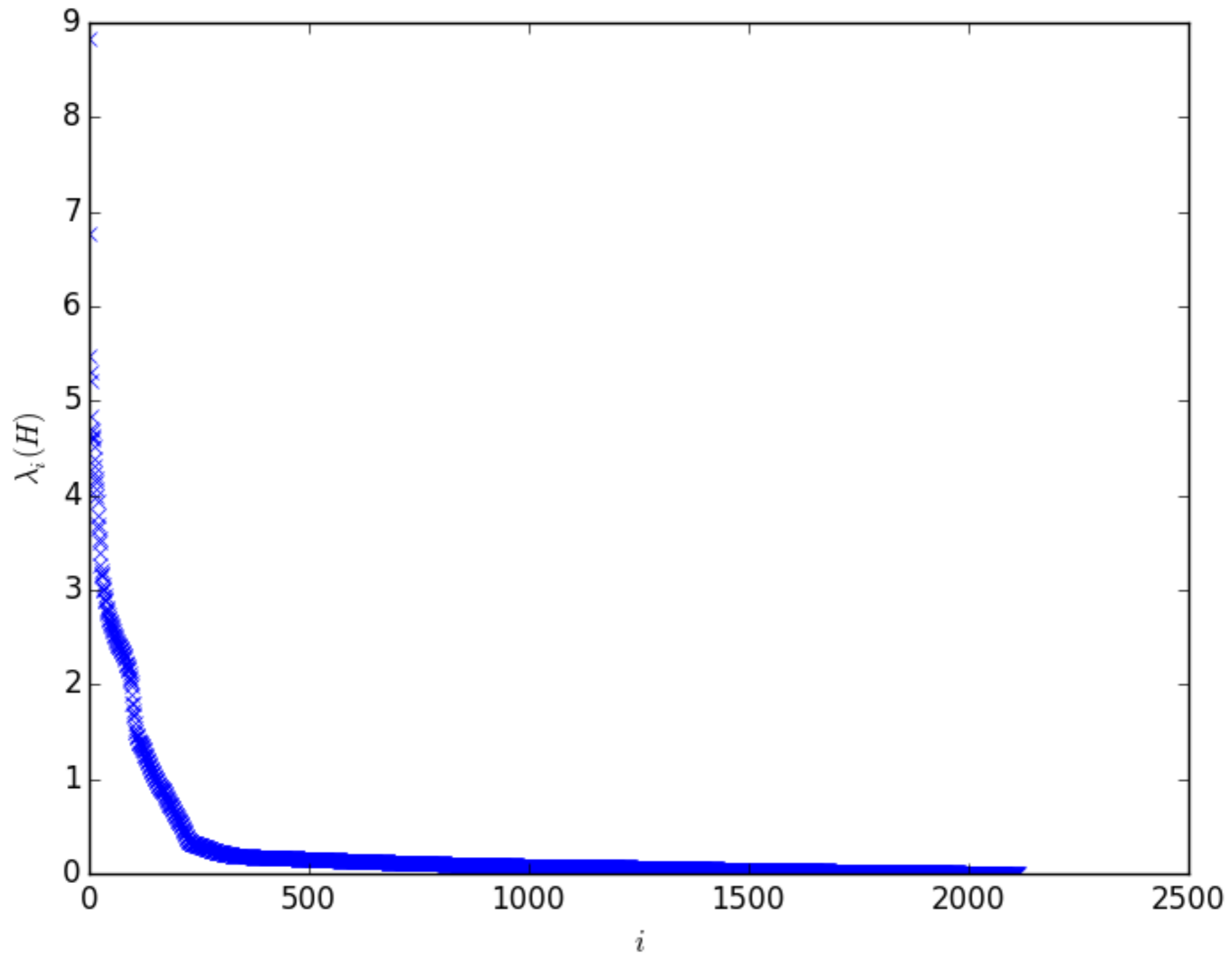


Critical idea: Observations are only informative on a low-dimensional subspace of the parameter space, *relative to the prior*. Spantini et al. (arXiv)

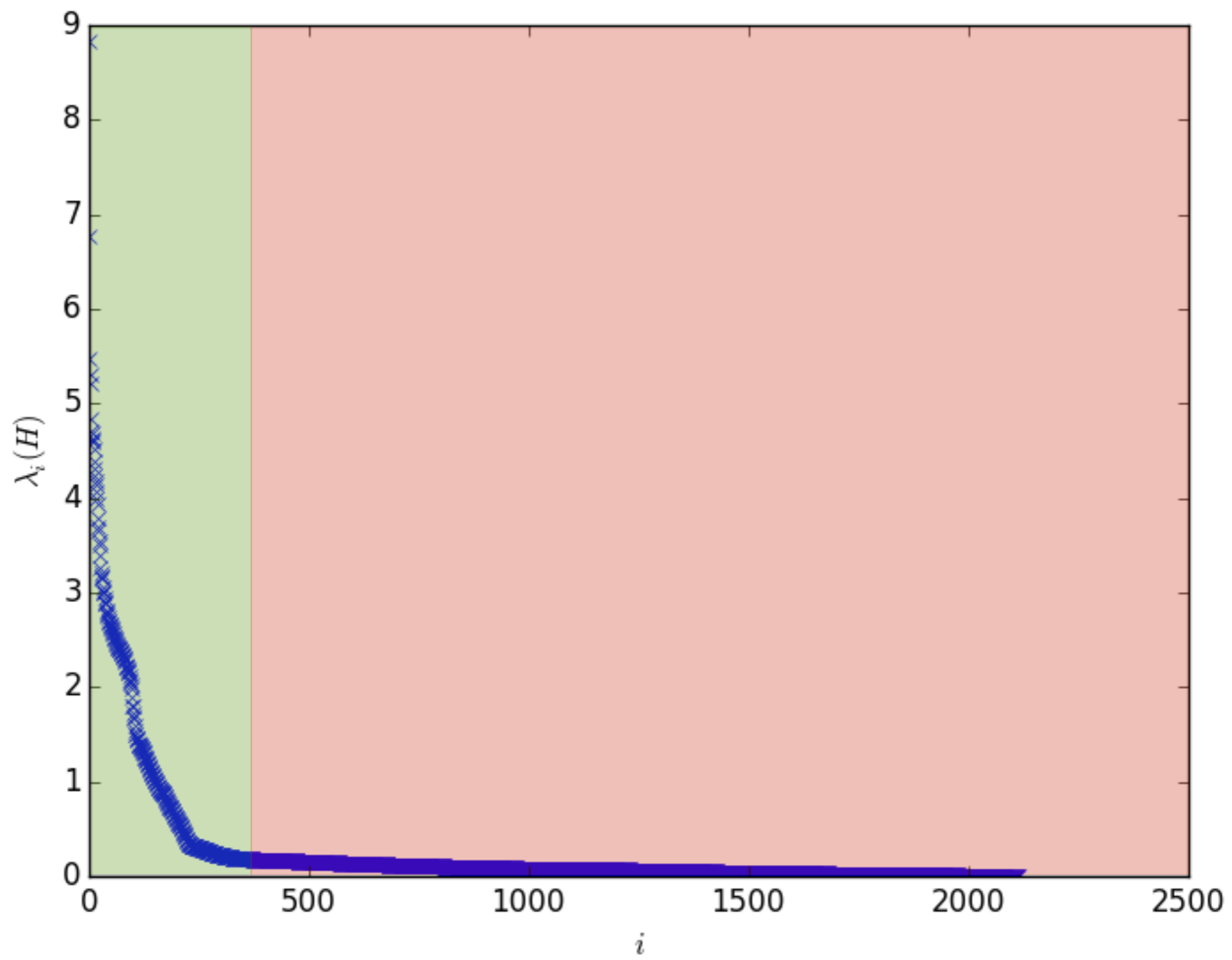
$$d_{\mathcal{F}}^2(A, B) = \sum_i \ln^2(\sigma_i)$$

$$Aw_j = B\sigma_j w_j$$

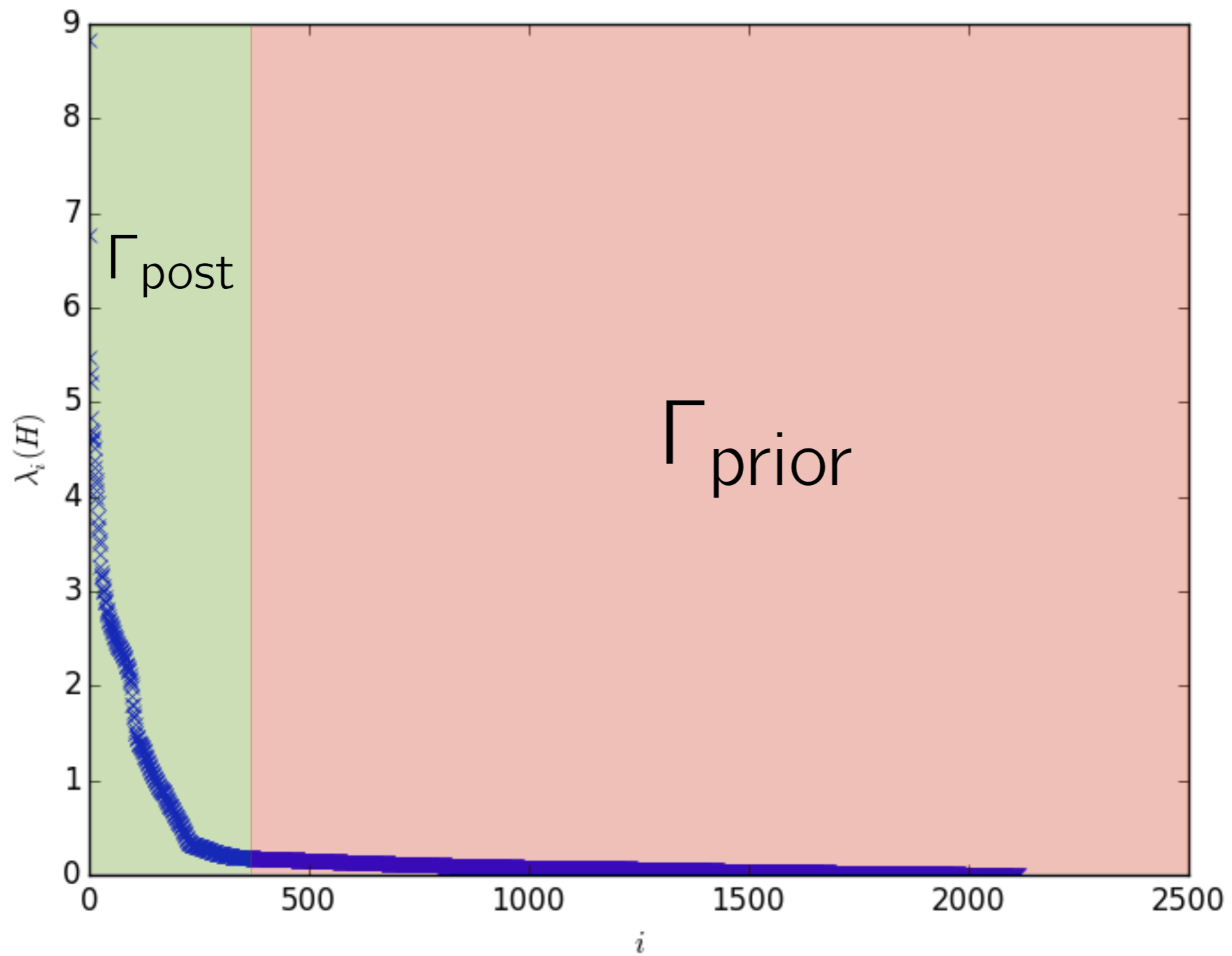
Förstner metric



Matrix-free Krylov-Schur (SLEPc).



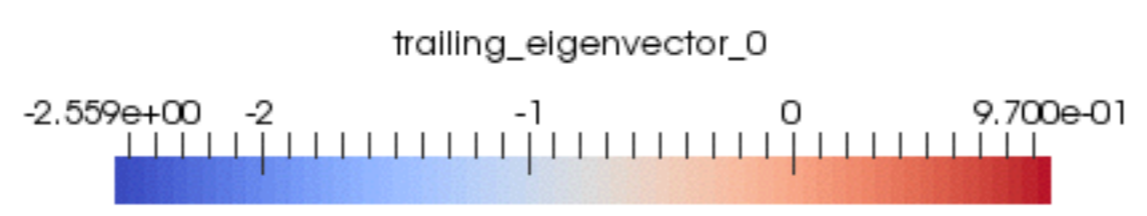
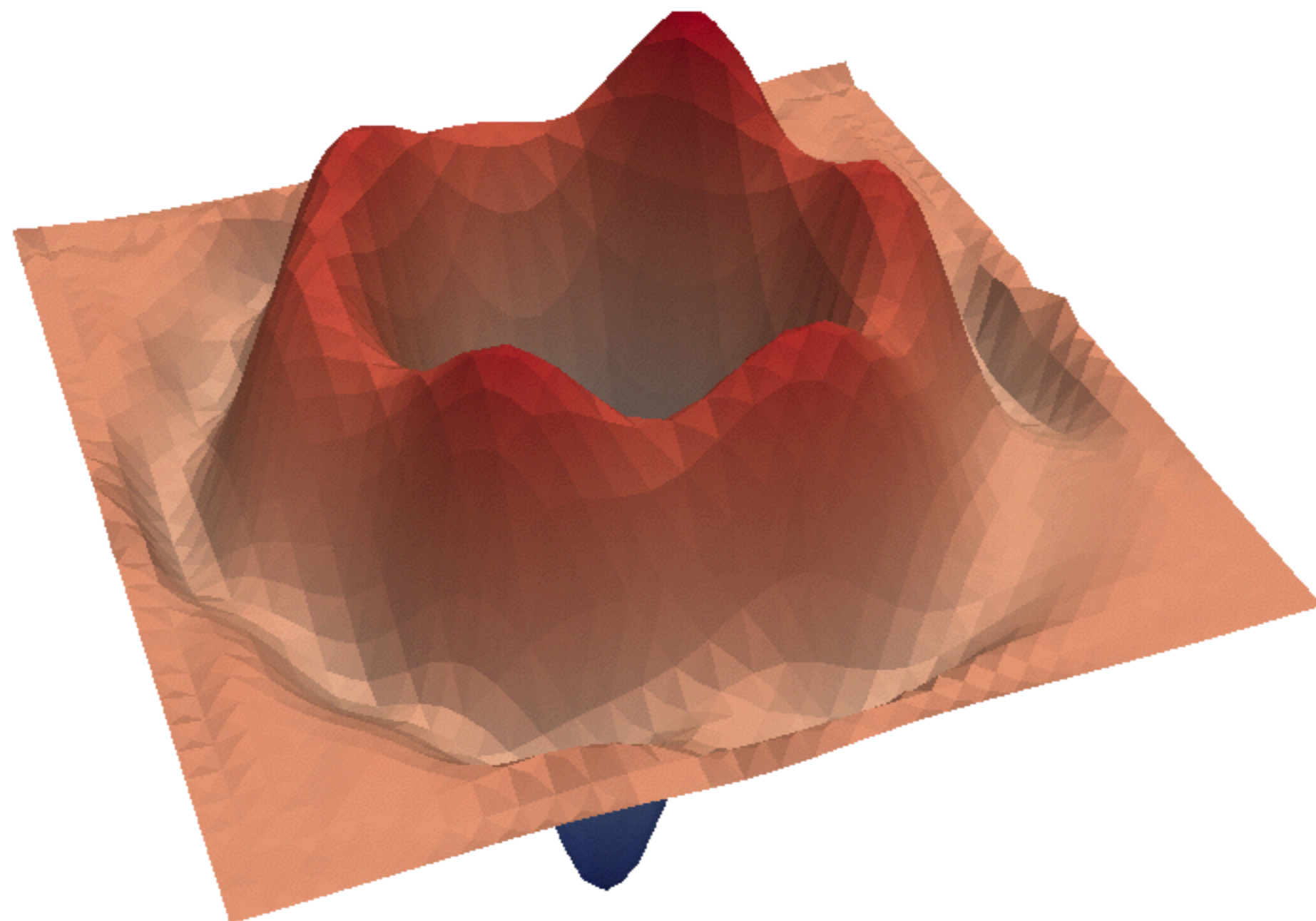


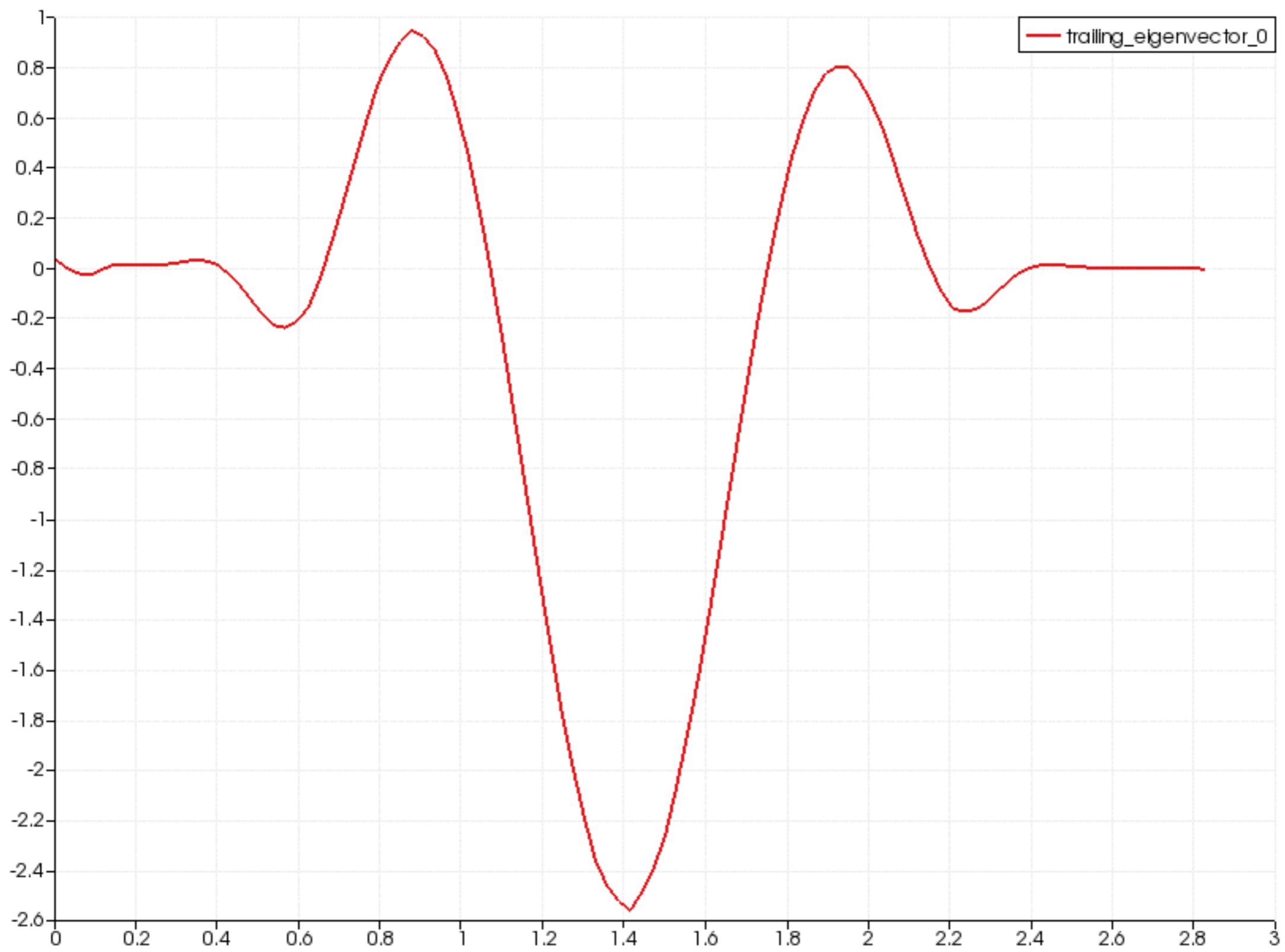


Matches trends from Flath et al. p424 for linear parameter to observable maps.

# Trailing Eigenvector

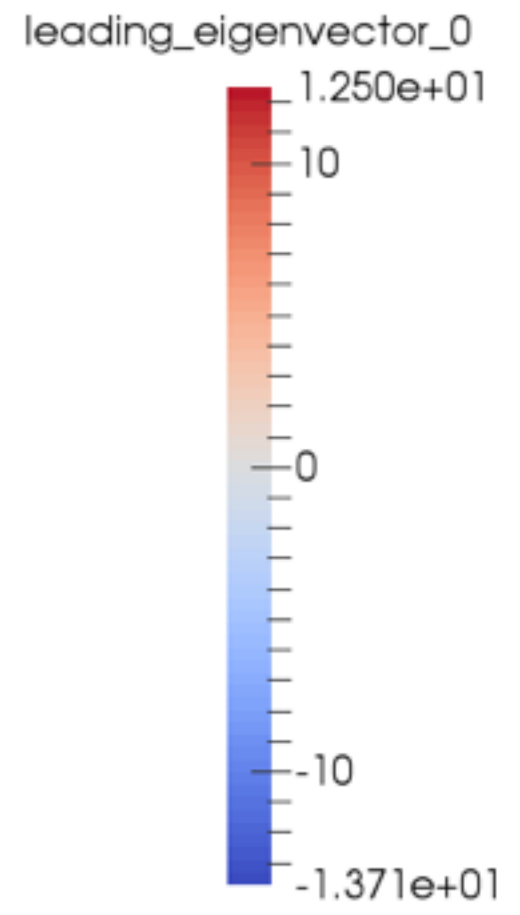
Direction in parameter space *least* constrained by the observations

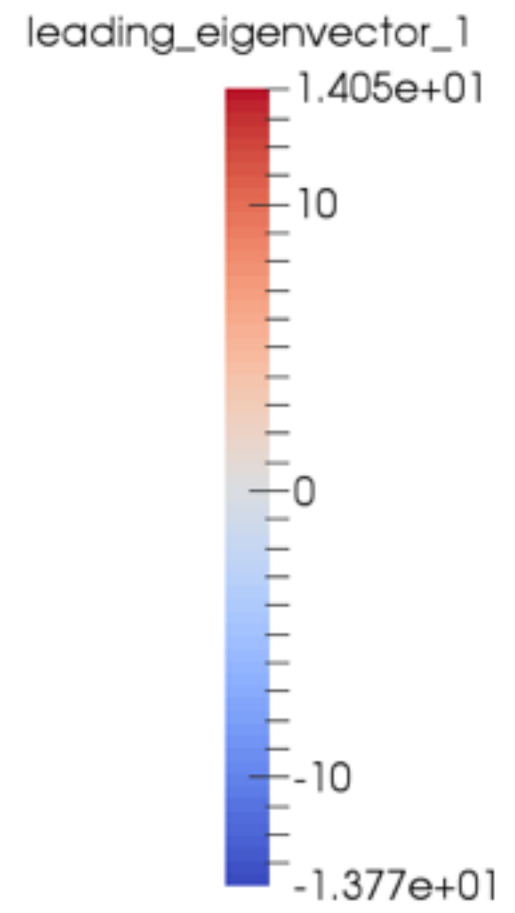


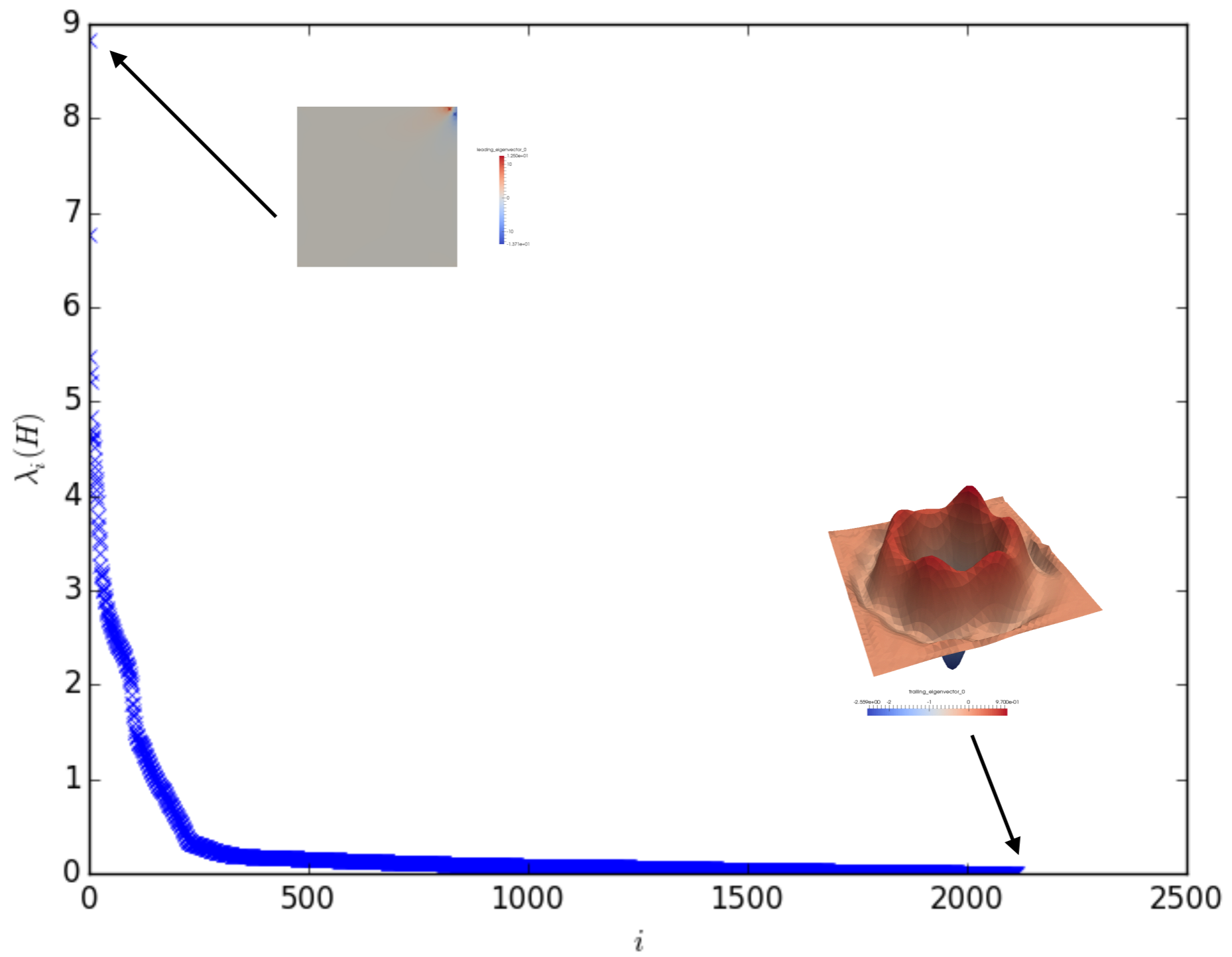


# Leading Eigenvectors

Direction in parameter space *most* constrained by the observations









*Full Hessian.*  
4000+ actions.

*Low-rank update.*  
292 actions.

**Huge** savings in computational cost.  
Scales with model dimension because *observations*  
stay the same.

# Summary

- We are developing methods to assess uncertainty in the recovered parameters in soft tissue.
- This is done within the framework of Bayesian inversion.
- FEniCS and dolfin-adjoint makes assembling the equations relatively easy, solving them is tougher!
- Next steps: exploring non-Gaussian nature of posterior using Hamiltonian MCMC. Requires derivatives.
- Paper soon on arXiv: infinite-dimensional setting, full derivations of equations, 3D problems.